# Rethinking Pulmonary Nodule Detection in Multi-view 3D CT Point Cloud Representation

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Abstract. 3D CT point clouds reconstructed from the original CT images are naturally represented in real-world coordinates. Compared with CT images, 3D CT point clouds contain invariant geometric features with irregular spatial distributions from multiple viewpoints. This paper rethinks pulmonary nodule detection in CT point cloud representations. We first extract the multi-view features from a sparse convolutional (SparseConv) encoder by rotating the point clouds with different angles in the world coordinate. Then, to simultaneously learn the discriminative and robust spatial features from various viewpoints, a nodule proposal optimization schema is proposed to obtain coarse nodule regions by aggregating consistent nodule proposals prediction from multi-view features. Last, the multi-level features and semantic segmentation features extracted from a SparseConv decoder are concatenated with multi-view features for final nodule region regression. Experiments on the benchmark dataset (LUNA16) demonstrate the feasibility of applying CT point clouds in lung nodule detection task. Furthermore, we observe that by combining multi-view predictions, the performance of the proposed framework is greatly improved compared to single-view, while the interior texture features of nodules from images are more suitable for detecting nodules in small sizes.

Keywords: 3D point cloud  $\cdot$  Nodule detection  $\cdot$  Multi-view feature representation

# 1 Introduction

Lung cancer is the leading cancer killer and one of the most common cancers around the world [26]. Many efforts have been made on AI-driven computeraided diagnosis (CAD) systems for lung nodule detection and diagnosis [17, 18, 28, 30]. Most existing 3D nodule detectors [11, 30] extract spatial-temporal features from the stacked CT images as 3D volumes via 3D convolutional neural networks (3D CNNs). By extending a two-dimensional feature representation to a three-dimensional space, the significant performance improvement demonstrates the benefits of interpreting the spatial features for nodule detection. Meanwhile,

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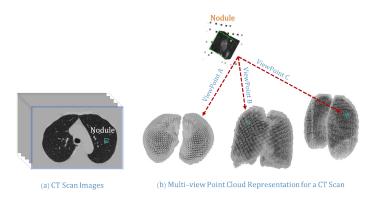


Fig. 1. Illustration of a CT scan in the image (a) and CT point cloud visualized in different views (b). Compared to CT images, as shown in (b), 3D CT point clouds naturally represent pulmonary nodules by multi-view representations in 3D coordinates. View A in (b) has the same viewpoint as the CT image. Note that the background of the lung region is excluded for both CT images and CT point clouds. Best viewed in color.)

by projecting CT images to multiple planes (i.e., axial, coronal, and sagittal), the multi-view features show the effectiveness to reduce false positives as richer features are obtained from different viewpoints [22, 23, 16, 9]. Although these existing methods can extract spatial-temporal features or multi-view features from the continuous CT images, the data representation with multi-view flexibility that can directly represent 3D spatial features is still remain exploring.

**Table 1.** Comparison between CT image representation and 3D CT point cloud representations.

Visual	Visual Geometric		Real-world	Irregular	Grid	Texture	Radiation	
Representation	Invariance	Perspective	Coordinates	Shape	Align	Feature	Intensity	
Image	No	No	No	No	Yes	Yes	Yes	
3D Point Cloud	Yes	Yes	Yes	Yes	No	No	Yes	

Recently, 3D point clouds are considered to be a natural way to capture and represent 3D objects [20, 21, 2, 4, 12]. As shown in Fig. 1, unlike CT images (Fig. 1(a)) represented by grids, 3D CT point clouds (Fig. 1(b)) are organized in an irregular manner, thereby provides more flexible feature representations of 3D geometric structure. We summarize the characters of visual representations of 3D CT point clouds and CT images in Table 1. Real-world coordinates are applied to 3D CT point clouds, representing the accurate geometric distribution of radiation intensity. Due to geometric invariance, multi-view representations can be obtained by tilting the 3D CT point cloud heading angles to obtain richer features than the single-view representation. However, the scattered 3D CT point cloud lacks the texture features as CT images that preserve the details of internal nodules. Therefore, this paper attempts to rethink the nodule detection task from multiple perspectives in CT point clouds and investigate the advantages and limitations compared to CT images.

We aim to address the challenging task of predicting nodule regions in the entire lung area. Per our knowledge, this is the first work to explore 3D point cloud data representation for the nodule detection task. The main contributions of this paper are summarized as follows: 1) We explore the possibility of applying 3D CT point cloud and the effectiveness of 3D spatial representations on nodule detection. By rotating the 3D CT point clouds, compared to a single view of stacked CT images, irregular shapes and richer spatial distributions of nodules in lung regions are extracted from multi-views. 2) A nodule proposal optimization schema is proposed to acquire a set of 3D nodule candidate proposals which simultaneously agreed by multi-view feature predictions. The rich multi-level features and point-wise segmentation are further concatenated with multi-view features for final nodule candidate refinement. 3) Experiment results show the advantages of multi-view 3D CT point clouds as spatial representations and the impact of lacking the texture feature representations on small nodule detection. Furthermore, the ablation studies demonstrate that with more multi-views involved, the performance of the proposed framework achieves encouraging improvements, proofing the effectiveness of multi-view 3D features in point clouds.

# 2 Methods

As shown in Fig. 2, N samples are acquired by combining the original 3D CT point clouds with the rotated multi-view samples, representing irregular geometric distributions from various perspectives. A 3D Sparse Convolution (SparseConv) encoder simultaneously learns the multi-view features by optimizing the nodule proposals in various viewpoints. Last, a final nodule prediction is refined by fusing the multi-level features and semantic segmentation features extracted by the 3D SpaseConv decoder, as well as the multi-view features.

**Multi-view Sample Collection:** 3D CT point clouds consist of a set of three-dimensional vertices, defined as  $\{x, y, z\}$  representing the distribution of points in a world coordinate. Besides, the unique internal texture with the radiation intensities is essential to identify nodule types. We further apply the radiant intensity I of each point to preserve internal intensity-based texture features. The nodule region is represented by (x, y, z, h, w, l), indicating the nodule location  $\{x, y, z\}$  and the nodule size in three dimensions  $\{h, w, l\}$ . During the training, the objective function consists of the BinaryCrossEntropy loss for nodule class probability and smooth - l1 loss for nodule region by comparing the predicted nodule candidates and the ground-truths.

By rotating the 3D point clouds along the world coordinate in N angles, the discriminate multi-view features of the same object can be extracted. Therefore,

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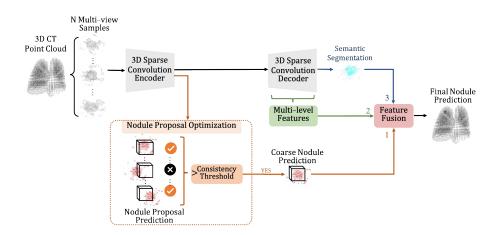
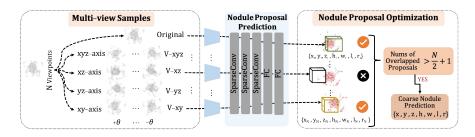


Fig. 2. The pipeline of our proposed 3D point cloud nodule detection framework. Multiview feature representations are extracted from a 3D sparse encoder-decoder network and further employed to select the coarse nodule predictions by a nodule proposal optimization (details are illustrated in Fig. 3 and explained in Section 3 - Nodule Proposal Optimization). Then, the finer candidate prediction is obtained based on the fusion of 1) multi-view features; 2) multi-level features; 3) semantic features of the region of interest (ROI).

to train a backbone network with robust spatial features from multiple perspectives, we rotate the 3D CT point clouds along the xy-axis, yz-axis, xz-axis, and xyz-axis with a set of rotation angles from  $+\theta$  to  $-\theta$ . As shown in Fig. 3, four sets of (N-1) viewpoints are added, donated as V-xy, V-yz, V-xz, and V-xyz. We implement nine viewpoint samples with the rotation angles of  $+45^{\circ}$  and  $-45^{\circ}$  for V-xy, V-yz, V-xz, and V-xyz. The multi-view features are fed into the backbone network for nodule proposal prediction.

Multi-view and Multi-level Feature Extraction: The irregular shape of the 3D point cloud brings challenges to implement feature extraction with convolutional neural networks (CNN). We follow the baseline PV-RCNN [24] and the extension work, Part-A<sup>2</sup> [25] to extract features by integrating the grids of irregular point clouds as voxels and multi-level point-wise features from the decoder network. A 3D sparse convolution (SparseConv) encoder composed of four layers as es1, es2, es3, and es4. The features are downsampled to  $1 \times, 2 \times, 4 \times, 8 \times$ as the layers go deeper. A 3D SparseConv decoder comprises four sparse deconvolutional layers as ds1, ds2, ds3, and ds4 for feature upsampling. The lateral connections are conducted through all layers, as the es1 with ds1, es2 with ds2, es3 with ds3, and es4 with ds4, extracting the multi-level point-wise features for final candidate prediction.

Nodule Proposal Optimization: Unlike typical data augmentation methods, we employ the samples from all views to predict and optimize the nodule proposals simultaneously. Reliable preliminary nodule proposals are acquired



**Fig. 3.** The detailed illustration of the proposed multi-view samples and nodule prediction optimization schema. Multi-view samples are obtained by rotating the original samples from N viewpoints. By rotating from  $+\theta$  to  $-\theta$  along the xy-axis, yz-axis, xz-axis, and xyz-axis, (N-1) additional viewpoints are obtained as V-xy, V-yz, V-xz and V-xyz. Features of N views are extracted from the 3D SparseConv encoder and the primary nodule proposals are predicted by a regression head. The coarse nodule predictions are collected if the number of consensus nodule proposals predicted by the multi-view features is greater than a consistency threshold.

from multi-views. In the meantime, compared with the ground truth, the 3D SparseConv encoder is updated by the objective function to extract multi-view features for accurate predictions. The distinguish and robust features ensure the prediction of the nodule regions. As shown in Fig. 3, a regression head (RH) is used for nodule proposal prediction, which consists of three SparseConv layers, followed by two fully connected layers to predict the confidence score and proposal region. RH takes the features of N views extracted from the last SparseConv layer of the encoder network and predicts the initial coarse nodule candidate regions. First, we choose a nodule proposal with a confidence score greater than 0.05 and then calculate the number of nodule proposals with a 3D IoU of 0.25 overlap among the multi-view predictions. If the number is higher than a consistency threshold, the nodule proposal is set as the coarse nodule prediction for a finer region regression.

Final Nodule Prediction with Multi-feature Fusion: To guarantee an accurate nodule candidate prediction, rich feature fusion is conducted by combining the multi-view features, multi-level features, and semantic segmentation features, as shown in Fig. 2. First, the point-wise attention benefits the flexible receptive field from the irregular format. We follow PV-RCNN [24], multi-scale features are extracted from ds1, ds2, ds3, and ds4 layers. Second, semantic segmentation maps are predicted by the 3D decoder network and semantic features further extracted by a SparseConv, interpreting the point level classification of nodule candidates. Finally, same as Part-A<sup>2</sup> [25], the multi-level features and the semantic features. A regression head predicts the final nodule candidate region (x, y, z, h, w, l, r) based on the rich multi-feature fusion.

## 3 Experiments

#### 3.1 Data and Training

We conduct the experiments on the LUNA16 public dataset [1], which contains 1,186 nodules with sizes ranging from 3 to 30 mm from 888 CT scans. The dataset is officially divided into ten subsets. We follow the same cross-validation protocol by applying nine subsets as training and the remaining subset as testing. One subset from the training subsets is used for validation to monitor the convergence of the training process.

**3D CT Point Cloud Reconstruction:** A CT scan consists of CT images represented by (x, y) as image coordinates and z as scan depth. To eliminate unrelated regions, we first segment the lung region from the CT images based on the lung region mask and then apply (x, y, z) as the location of each point in the world coordinates, represented by (x, y, z, radiation intensity). The air points in the lung regions are discarded based on the standard Hounsfield scale (-1000). Therefore, the CT point clouds precisely represent the nodules, tissues, organs, and lung boundaries in the lung region. Besides, to avoid sampling redundant and non-informative points in the training, we follow Drokin *et al.* [8] by applying the non-uniform sampling schema, which keeps a high sampling rate at the nodule regions and gradually reduces the sampling rate according to the increasing distance from sample points to the center of nodules.

**Table 2.** FROC performance comparison of nodule detection between the proposed 3D point cloud-based method and the state-of-the-art image-based methods on LUNA16 dataset: sensitivity and the corresponding false positives at 1/8, 1/4, 1/2, 1, 2, 4, 8 per scan with and without false positive reduction.

Methods	1/8	1/4	1/2	1	2	4	8	CPM
Without False Positive Reduction								
Zhu et al.[30]	0.692	0.769	0.824	0.865	0.893	0.917	0.933	0.842
Li <i>et al.</i> [15]	0.739	0.803	0.858	0.888	0.907	0.916	0.920	0.862
Gong $et al.[10]$	0.713	0.801	0.867	0.917	0.920	0.962	0.971	0.883
Khosravan $et al.[13]$	0.709	0.836	0.921	0.953	0.953	0.953	0.953	0.897
Liu et al.[17]	0.848	0.876	0.905	0.933	0.943	0.957	0.970	0.919
With False Positive Reduction								
Dou et al.[7]	0.677	0.737	0.815	0.848	0.879	0.907	0.922	0.827
Dou $et al.[6]$	0.659	0.745	0.819	0.865	0.906	0.933	0.946	0.839
Wang et al.[29]	0.676	0.776	0.879	0.949	0.958	0.958	0.958	0.878
Ding $et al.[5]$	0.748	0.853	0.887	0.922	0.938	0.944	0.946	0.891
Kim $et al.[14]$	0.904	0.931	0.943	0.947	0.952	0.956	0.962	0.942
Ours	0.779	0.848	0.914	0.918	0.939	0.939	0.939	0.895
Ours (w/FPR)	0.794	0.886	0.916	0.934	0.951	0.956	0.959	0.913

Model Training: The experiment is modified based on an open source project OpenPCDet [27]. The proposed framework is trained to minimize Bi-

naryCrossEntropy loss and Smooth-L1 loss. The Adam algorithm is used for optimization with an initial learning rate of  $1e^{-4}$  and decreased by 0.1 after 80 and 160 epochs. The batch size is set to 2. The multi-view proposal optimization is conducted after 20 epochs. The model is trained with a total of 200 training epochs.

#### 3.2 Experiments on LUNA16

Compare with State-of-the-art Nodule Detection Methods: We evaluate the proposed method and compare it with the state-of-the-art image-based nodule detectors in two groups: one-stage methods without false-positive reduction and two-stage frameworks with false-positive reduction. Similar to the LUNA16 challenge, the Free-Response ROC Curve (FROC) [3] is employed to evaluate the sensitivity versus the specificity of the nodule detection at 1/8, 1/4, 1/2, 1, 2, 4, 8 False Positive (FP) levels per scan with the average Competition Performance Metric (CPM) score. As shown in Table 2, the proposed 3D nodule detector reaches comparable results with the one-stage methods trained on stacked CT images, demonstrating that the spatial features are feasible to employ in the nodule detection task. We observe that performance is improved with a small margin (1.6% CPM) by implementing the false positive reduction to the proposed nodule detector and shows a comparable result with the image-based two-stage frameworks [6, 7, 29, 5]. We notice that most of the missing nodules are small, with an average size of 5 mm. With few point representations, spatial feature extraction is significantly limited for all the SparseConv encoder layers. For the image-based methods, detailed internal texture features of small nodules are better preserved by the feature pyramid extraction [29, 17].

Table 3. Ablation study of the effectiveness of proposed multi-views samples with nodule proposal optimization, multi-level features (MF) and semantic features (SF) by comparing the performance on LUNA16 dataset: sensitivity and the corresponding false positives at 1/8, 1/4, 1/2, 1, 2, 4, 8 per scan.

V-xy	V-yz	V-xz	V-xyz	MF	$\mathbf{SF}$	1/8	1/4	1/2	1	<b>2</b>	4	8	CPM
-	-	-	-	-	-	0.617	0.695	0.765	0.796	0.811	0.811	0.811	0.758
$\checkmark$	-	-	-	-	-	0.632	0.719	0.787	0.819	0.837	0.862	0.862	0.788
$\checkmark$		-	-	-	-	0.701	0.749	0.849	0.866	0.879	0.891	0.891	0.832
$\checkmark$		$\checkmark$	-	-	-	0.742	0.801	0.863	0.904	0.907	0.917	0.917	0.864
$\checkmark$		$\checkmark$	$\checkmark$	-	-	0.756	0.835	0.879	0.902	0.911	0.921	0.921	0.875
$\checkmark$		$\checkmark$	$\checkmark$	$\checkmark$	-	0.772	0.843	0.881	0.916	0.919	0.927	0.927	0.883
$\checkmark$		$\checkmark$	$\checkmark$	$\checkmark$	$\checkmark$	0.779	0.848	0.914	0.918	0.939	0.939	0.939	0.897

Ablation Study: We investigate the effectiveness of the proposed multi-view feature learning with the nodule proposal optimization schema and the feature

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fusion on the final nodule candidate predictions. For all ablation studies, the consistency threshold is set to 5 when 9 views involved as the model shows the best performance. Table 3 shows that the CPM is increased by 11.7% when all viewpoints are applied compared with the single-view baseline. As the multi-view features V-xy, V-yz, V-xz, and V-xyz gradually join for training, the sensitivities are raised by 3%, 4.4%, 3.2%, and 1.1% CPM, respectively. The performance is significantly gained by learning the multi-view feature representations through nodule proposal optimization schema. The average sensitivity is further improved 0.7% and 1.4% CPM by multi-level features (MF) and semantic feature (SF) for final nodule prediction, respectively, demonstrating the benefits of irregular point-wise feature fusion for nodule region regression. We further compare the baseline model to the existing point cloud backbone networks: PointNet [20], PointNet++ [21] and DGCNN [19]. The PV-RCNN substantially outperforms these models by 4.2%, 3.3%, and 3.6% CPM respectively.

## 4 Discussions and Conclusions

Overall, 3D CT point clouds can be feasible data representations on nodule detection tasks for medical image analysis with a very careful data preprocessing. 3D point clouds naturally present the irregular shape of lung regions in realworld coordinates, which are flexible in employing multi-view features based on the geometric invariance and acquiring the discriminative spatial features from different viewpoints. Multi-view features can be obtained by rotating the 3D point clouds and further aggregated them to acquire the coarse nodule predictions through a nodule proposal optimization schema. By simultaneously learning the multi-view features from a 3D SparseConv encoder, combined with the multi-level and semantic segmentation features extracted from a 3D SparseConv decoder, the proposed nodule detector achieves a promising performance on the pulmonary nodule detection task.

The point cloud-based backbone network tends to extract informative spatial relations for nodule prediction. As small nodules contain few points, the lack of spatial feature extraction makes it challenging to detect. In contrast, the image-based methods handle it relatively well due to detailed texture information extracted from image-based CNNs at the low-level layers. There are still opportunities for further improvements on small nodule detection. Future work will extend the 3D point-cloud representations with image-based texture features detecting nodules via a dynamic multi-view nodule proposal optimization schema. It is worth investigating to fully utilize the spatial representations from 3D CT point clouds, which have the potential to benefit the clinical diagnosis, especially in surgical operations.

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