

# **Osteocyte intrinsic TGF $\beta$ signaling regulates bone quality through perilacunar/canalicular remodeling**

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## Summary

Poor bone quality contributes to bone fragility in diabetes, aging, and osteogenesis imperfecta. However, the mechanisms controlling bone quality are not well understood, perpetuating the current lack of strategies to diagnose or treat bone quality deficits. TGF $\beta$  signaling is a crucial mechanism known to regulate the material quality of bone, but its cellular target in this regulation is unknown. Studies showing that osteocytes directly remodel their perilacunar/canalicular matrix motivated our hypothesis that TGF $\beta$  controls bone quality through perilacunar/canalicular remodeling (PLR). Using inhibitors and mice with an osteocyte-intrinsic defect in TGF $\beta$  signaling (T $\beta$ RII<sup>ocy-/-</sup>), we show that TGF $\beta$  regulates PLR in a cell-intrinsic manner to control bone quality. Altogether this study emphasizes that osteocytes are key in executing the biological control of bone quality through PLR, and thereby highlighting the fundamental role of osteocyte mediated perilacunar/canalicular remodeling in bone homeostasis and fragility.

## Keywords

Osteocyte, TGF $\beta$ , bone quality, perilacunar/canalicular remodeling, bone fragility

## Highlights

- TGF $\beta$  is an osteocyte-intrinsic regulator of perilacunar/canalicular remodeling (PLR)
- Osteocytes actively maintain bone quality through regulated control of PLR
- Osteocytic PLR is the cellular mechanism by which TGF $\beta$  controls bone quality. Defects in PLR cause severe bone fragility, even when bone mass is normal

## eTOC Summary

Resistance to fracture requires healthy bone mass and quality. However, the cellular mechanisms regulating bone quality are unclear. Dole et al. show that osteocyte-intrinsic TGF $\beta$  signaling maintains bone quality through perilacunar/canalicular remodeling. Thus, osteocytes mediate perilacunar/canalicular remodeling and osteoclast-directed remodeling to cooperatively maintain bone quality and mass and prevent fragility.

## Introduction

Bone fragility is determined by bone mass and quality. Bone quality encompasses parameters including bone geometry, porosity, trabecular microarchitecture, and bone extracellular matrix (ECM) material properties (Hernandez and Keaveny, 2006; Seeman, 2008). Historically the prognosis of fragility fractures has focused on bone mass but it is now known that compromised ECM properties plays a causal role in bone fragility in diabetes, aging, and osteogenesis imperfecta (OI) (Delmas and Seeman, 2004; Fleischli et al., 2006; Grafe et al., 2014; Lane et al., 2006; Nalla et al., 2004; Ott, 1993; Van Staa et al., 2003). Despite the clinical importance of this and other aspects of bone quality, the management of fragility currently focuses on improving bone mass. Overcoming this clinical gap in diagnosing and treating bone quality requires elucidation of mechanisms that orchestrate the biological control of bone quality in skeletal health and disease.

Currently, the transforming growth factor beta (TGF $\beta$ ) pathway is one of the few signaling pathways known to regulate bone mass and quality (Alliston, 2014; Balooch et al., 2005; Mohammad et al., 2009; Chang et al., 2010; Edwards et al., 2010). In bone, TGF $\beta$  produced by bone forming osteoblasts is sequestered in the ECM in an inactive latent form (Sinha et al., 1998). When released upon osteoclastic resorption of the ECM, TGF $\beta$  exerts pleiotropic effects on osteoblasts, osteoclasts, and their progenitors to coordinate bone remodeling (Dallas, 2008; Tang and Alliston, 2013). Aberration in TGF $\beta$  signaling leads to altered bone mass and poor bone quality in multiple skeletal diseases including Camurati Engelman Disease (CED) and OI (Grafe et al., 2014; Kinoshita et al., 2000). While the pathogenesis of the poor bone quality associated with these diseases have been attributed to imbalanced osteoclast and osteoblast activity, not much is known about the causal role of osteocytes and osteocyte intrinsic TGF $\beta$  signaling in bone fragility.

In addition to regulating the activity of osteoclasts and osteoblasts, osteocytes also engage in perilacunar/canalicular remodeling (PLR), during which they directly resorb and deposit bone matrix surrounding their intricate lacuno-canalicular network (Qing and Bonewald, 2009). This process was originally called 'osteocyte osteolysis' when it was observed in pathologic conditions, or 'perilacunar/canalicular remodeling' in metabolically demanding situations such as lactation or hibernation (Haller and Zimny, 1977; Qing et al., 2012; Qing and Bonewald, 2009; Teti and Zallone, 2009; Wysolmerski, 2013). It is now clear that PLR is a homeostatic mechanism that helps to maintain mineral homeostasis and the lacuno-canalicular network. Several studies demonstrate the essential role in PLR of matrix metalloproteinases (Mmps, namely Mmp2, Mmp13 and Mmp14), cathepsin K (Ctsk), carbonic anhydrase 2, and tartrate resistant acid phosphatase (Acp5/ TRAP) (Kogawa et al., 2013; Qing et al., 2012; Qing and Bonewald, 2009; Wysolmerski, 2013). Through loss-of-function studies in mice, these genes were found to be essential for an intact lacuno-canalicular network, organization of collagen, and bone matrix mineralization (Holmbeck et al., 2005; Inoue et al., 2006; Kogawa et al., 2013; Kulkarni et al., 2012; Qing and Bonewald, 2009; Tang et al., 2012; Tang and Alliston, 2013; Wysolmerski, 2013), all of which contribute to bone quality. Macro-mechanical testing of MMP13-deficient bone revealed a correlation between the loss of PLR and bone fragility (Tang et al., 2012). Nonetheless, many questions remain about the relationship between osteocyte-mediated PLR and bone quality.

In an effort to elucidate the cellular and molecular mechanisms that control bone quality, we tested the hypothesis that TGF $\beta$  acts directly on osteocytes to control PLR, and that

this mechanism accounts for the TGF $\beta$ -dependent control of bone quality. Several lines of evidence support this model, including the ability of TGF $\beta$  to directly regulate the expression of several Mmps implicated in PLR (Krstic and Santibanez, 2014; Selvamurugan et al., 2004). To investigate this possible mechanism, we employed novel *in vivo* and *in vitro* models and pharmacologic TGF $\beta$  antagonists similar to those in human clinical trials for the treatment of bone fragility in OI. Using this approach, we uncovered the essential role of osteocyte-intrinsic TGF $\beta$  signaling in the control of PLR and fracture resistance and demonstrate the importance of PLR in bone fragility.

## Results

### Pharmacologic inhibition of TGF $\beta$ signaling dysregulates perilacunar/canalicular remodeling

We previously showed that pharmacologic inhibition of the TGF $\beta$  receptor type I (T $\beta$ RI-inhibitor, SD-208) increases trabecular bone mass through stimulating osteoblastic bone formation and repressing osteoclastic resorption (Mohammad et al., 2009). However, the effect of SD-208 or other T $\beta$ RI-inhibitory agents on osteocytes (OCY) is unknown. To investigate the role of TGF $\beta$  signaling in osteocytes, the most abundant bone cells in cortical bone (Franz-Odenaal et al., 2006), we examined histologic and molecular outcomes of osteocyte-mediated perilacunar/canalicular remodeling (PLR) in mice treated with SD-208. As expected, 6 weeks of T $\beta$ RI-inhibitor treatment significantly increased trabecular bone mass (Fig. S1). Histologic analysis shows a dense and organized network of osteocyte canaliculi in cortical bone of vehicle-treated mice. However, T $\beta$ RI-I treatment caused severe deterioration of the osteocyte canalicular network with a 50% reduction in canalicular length (Fig. 1A-B).

The dysregulated canalicular network in T $\beta$ RI-I-treated bone resembles that seen in bones deficient in enzymes essential for PLR (Holmbeck et al., 2005; Inoue et al., 2006; Kulkarni et al., 2012; Tang et al., 2012). Therefore, we evaluated the effect of T $\beta$ RI-inhibition on the expression of genes encoding PLR enzymes, including matrix metalloproteinases *Mmp2*, *Mmp13* and *Mmp14*, Cathepsin K (*Ctsk*), and tartrate resistant acid phosphatase (*Acp5*) in cortical bone. T $\beta$ RI-I treatment coordinately reduced the level of mRNA encoding all five enzymes, relative to vehicle-treated controls (Fig. 1C). Expression of the ATPase *Atp6v0d*, is increased in T $\beta$ RI-treated bone (Fig. S2). Moreover, T $\beta$ RI-I treatment also causes a decline in osteocytic protein expression of MMP13, MMP14 and CTSK without impacting their viability (Fig. 1D-F). This strong, concerted repression of several genes required for osteocyte-mediated PLR upon TGF $\beta$  inhibition indicates the critical role of TGF $\beta$  in controlling osteocyte function.

### TGF $\beta$ regulates perilacunar/canalicular remodeling in a cell intrinsic manner

While systemic inhibitors of TGF $\beta$  clearly impact lacuno-canalicular networks and the expression of genes associated with PLR, it was unclear if TGF $\beta$  exerts its effects on osteocytes directly or indirectly. Therefore, we examined the cell-intrinsic effects of TGF $\beta$  on MLO-Y4 osteocyte-like cells and OCY454 osteocytes, which more faithfully mimic osteocytic gene expression. Within 6 hours of treatment, TGF $\beta$  induced expression of *Mmp13*, *Mmp14* and *Ctsk* mRNA, as well as *Serpine1*, a well-known TGF $\beta$ -inducible gene in MLO-Y4 cells (Fig. 2A-B) (Graycar et al., 1989). TGF $\beta$  also induced expression of *Mmp13* and *Ctsk*, but not *Mmp14*, in OCY454 cells (Fig. 2 C-D). Further supporting the osteocyte intrinsic role of TGF $\beta$ , TGF $\beta$  induced the expression of

the osteocyte marker genes Sclerostin (*Sost*) and dentin matrix protein-1 (*Dmp1*), without affecting Phosphate Regulating Endopeptidase Homolog, X-Linked (*Phex*) (Fig.S3).

In addition to expressing PLR enzymes, osteocytes engaged in PLR acidify their microenvironment. Using the pH-sensitive dye 5-(and-6)-carboxy SNARF-1, AM, we examined the effect of TGF $\beta$  on MLO-Y4 cell acidification. As shown by others (Kogawa et al., 2013), recombinant sclerostin (rhSCL) induces PLR and lowers the intracellular pH (pHi) of MLO-Y4 cells. TGF $\beta$  treatment resulted in a larger acidification than sclerostin treatment. In contrast, blocking TGF $\beta$  signaling with an *in vitro* inhibitor of T $\beta$ RI (SB-431542) relieved this acidification, such that pHi was equivalent to untreated cells (Fig. 2E-F). Altogether, our findings support the possibility that TGF $\beta$  induces PLR in an osteocyte-intrinsic manner.

### **Osteocyte-specific inhibition of TGF $\beta$ signaling impairs perilacunar/canalicular remodeling**

To evaluate the osteocyte-intrinsic role of TGF $\beta$  signaling *in vivo*, TGF $\beta$  receptor II (T $\beta$ RII) was deleted in osteocytes using DMP1-Cre mice, resulting in T $\beta$ RII<sup>ocy-/-</sup> mice. We validated the specific reduction of T $\beta$ RII expression in osteocytes (but not in other cell types) of T $\beta$ RII<sup>ocy-/-</sup> bone relative to DMP1<sup>Cre-/-</sup>; T $\beta$ RII<sup>fl/fl</sup> (WT) littermate controls (Fig.3 A-B). Abrogation of TGF $\beta$  signaling in T $\beta$ RII<sup>ocy-/-</sup> bone was validated by reduced *T $\beta$ RII* and *Serpine1* gene expression (Fig. 3C). Furthermore, using primary bone marrow cultures from WT and T $\beta$ RII<sup>ocy-/-</sup> mice, we verified the osteocyte-specific defect in TGF $\beta$  signaling by confirming that osteogenic gene expression is normal until after these cells differentiate into osteocytes (Fig S5A-D).

Since systemic inhibition of TGF $\beta$  signaling causes severe deterioration of the osteocyte canalicular network, and since TGF $\beta$  regulates osteocytic expression of PLR enzymes, we evaluated the lacuno-canalicular network in T $\beta$ RII<sup>ocy-/-</sup> cortical bone. Upon osteocytic deletion of T $\beta$ RII, the canalicular network was abrogated and visibly blunted. Relative to WT, the canalicular projections in T $\beta$ RII<sup>ocy-/-</sup> bone were reduced by 50% and the total lacuno-canalicular area was reduced by 32% (Fig. 3D-E, Fig. S4A).

Among the panel of PLR genes, expression of *Mmp2*, *Mmp13*, *Mmp14*, *Ctsk*, and *Acp5* was downregulated in T $\beta$ RII<sup>ocy-/-</sup> mice (Fig. 3F, Fig. S4B). In fact, the effect of osteocyte-intrinsic T $\beta$ RII ablation on PLR gene expression was even more profound than that produced by T $\beta$ RI-inhibitor treatment. Expression of osteocalcin (*Oc*) and bone sialoprotein (*Ibsp*), *Dmp1* and *Phex* genes the control systemic mineral homeostasis was unaffected by the absence of osteocytic TGF $\beta$  signaling. Expression of *Sost*, which is known to be induced by TGF $\beta$  (Loots et al., 2012; Nguyen et al., 2013), was downregulated in T $\beta$ RII<sup>ocy-/-</sup> bones (Fig.3G). Protein expression of MMP13, MMP14 and CTSK in osteocytes of T $\beta$ RII<sup>ocy-/-</sup> mice was also significantly reduced 27-40% compared to WT mice, without apparent changes in osteocyte number and viability as determined by H&E and TUNEL staining (Fig. 3H-I, Fig S4B-C). These findings corroborated the observations in the T $\beta$ RI-I mouse model and revealed the direct role of osteocytic TGF $\beta$  signaling in the regulation of PLR.

To rigorously evaluate the effect of T $\beta$ RII deletion on lacunar size, orientation and shape, we utilized synchrotron radiation micro-tomography (SR $\mu$ T), which visualizes and quantifies the osteocyte lacunae in a 3-D space. In spite of the dramatic differences in

the canalicular network seen histologically, osteocyte lacunar volume, shape, and orientation relative to the long axis of the bone did not differ significantly between  $T\beta RII^{ocy-/-}$  and WT cortical bone (Fig. 3J-M, Fig. S4E-H). Also using SR $\mu$ T, we detected a 3% reduction ( $P=0.06$ ) in peak bone mineral concentration in diaphyseal cortical bone of  $T\beta RII^{ocy-/-}$  mice compared to WT (Fig. 3M, Fig. S6H). Therefore, osteocyte-intrinsic TGF $\beta$  signaling regulates the expression of enzymes required for PLR, and is essential for the integrity of the canalicular network and bone matrix mineralization. Not only does this reveal a novel role for TGF $\beta$  in osteocytes, but it also adds TGF $\beta$  to the short list of factors shown to regulate PLR.

### **Osteocyte-specific deletion of $T\beta RII$ increases trabecular bone mass by inhibiting bone resorption**

Because alterations in TGF $\beta$  signaling often impact bone mass (Balooch et al., 2005; Mohammad et al., 2009), we analyzed the impact of ablated osteocyte-specific TGF $\beta$  signaling on trabecular and cortical bone mass and geometry. Bones of  $T\beta RII^{ocy-/-}$  mice showed no gross abnormalities relative to WT mice. Micro-computed tomography ( $\mu$ CT) analysis revealed a 35% increase in trabecular bone mass in 8-week old  $T\beta RII^{ocy-/-}$  mice relative to WT littermates. This gain in mass was attributed to the corresponding increase in trabecular number (26%) and complementary decrease in trabecular spacing (25%) (Fig. 4A-D, Table 1). However, osteocytic deletion of  $T\beta RII$  did not affect cortical bone thickness or geometry (Fig. 4K-M). Cortical bone mineralization (Fig. 4N) of  $T\beta RII^{ocy-/-}$  mice was reduced by 4.8%, consistent with the 3% decrease in peak bone mineral concentration detected by SR $\mu$ T (Fig. 3M). Therefore, osteocyte-intrinsic TGF $\beta$  regulates the mass and geometry of trabecular, but not cortical bone.

To understand the cellular mechanism underlying the elevated trabecular bone phenotype of  $T\beta RII^{ocy-/-}$  mice, histomorphometry was performed. Neither static nor dynamic histomorphometric analyses revealed significant differences in osteoblast or bone formation parameters in  $T\beta RII^{ocy-/-}$  bone (Fig. 4E-G, Table 1). On the other hand, measures of bone resorption implicate osteocyte-intrinsic TGF $\beta$  in the control of osteoclast function. Specifically, TRAP-positive osteoclasts were reduced by 40%, along with a 34% reduction in osteoclast surface in  $T\beta RII^{ocy-/-}$  mice (Fig. 4H-I, Table 1). Furthermore,  $T\beta RII^{ocy-/-}$  mice showed a substantial reduction in the ratio of RANKL/OPG mRNA expression due to low levels of the osteoclastogenic factor RANKL (*Rankl*), but unaffected levels of OPG (*Opg*), a RANKL antagonist (Fig. 4J, Fig. S5D-G). Together these results attribute the high trabecular bone mass phenotype of  $T\beta RII^{ocy-/-}$  mice to decreased osteoclast function, which essentially results from decreased production of RANKL by  $T\beta RII$ -deficient osteocytes.

### **Osteocyte deletion of $T\beta RII$ reduces fracture resistance of bone**

Given that  $T\beta RII^{ocy-/-}$  cortical bone mass and thickness are normal, evidence of bone fragility in these mice would be consistent with defects in bone quality. Despite our prior implication of TGF $\beta$  in bone quality regulation (Balooch et al., 2005; Chang et al., 2010; Mohammad et al., 2009), the cellular target responsible for the control of bone quality has since been elusive. The disruption of PLR and cortical bone mineralization in  $T\beta RII^{ocy-/-}$  bone led us to hypothesize that TGF $\beta$  controls bone quality through regulation of osteocytic PLR. To test this hypothesis, we performed a series of tests to evaluate the macromechanical and material behavior of  $T\beta RII^{ocy-/-}$  bone.

Macromechanical testing showed reduced fracture resistance of  $T\beta RII^{ocy-/-}$  cortical bone. Using flexural testing, we found that  $T\beta RII^{ocy-/-}$  femora exhibited a 26% decline in the bending modulus relative to WT bone, indicating a reduced capacity to resist elastic deformation (Fig. 5A). Similarly, the yield stress was reduced by 27% in  $T\beta RII^{ocy-/-}$  bones (Fig. 5B). Using nanoindentation to examine the material properties of the  $T\beta RII^{ocy-/-}$  bone revealed that the Young's modulus of  $T\beta RII^{ocy-/-}$  bone matrix was significantly lower than for WT bone (Fig. 5C), a finding that is consistent with the reduced  $T\beta RII^{ocy-/-}$  cortical bone mineralization (Fig. 4N). The most dramatic effects were observed in fracture toughness testing, in which notched  $T\beta RII^{ocy-/-}$  cortical bone exhibited a 65% decrease in total work of fracture compared to WT bone (Fig. 5D). These findings are particularly remarkable, given that the severe fragility of  $T\beta RII^{ocy-/-}$  bone could not be attributed to differences in cortical bone mass or geometry.

Accordingly, we sought to learn more about the material mechanisms responsible for  $T\beta RII^{ocy-/-}$  bone fragility. For example, resistance to crack *initiation* is primarily imparted through intrinsic toughening mechanisms, representing a material's inherent resistance to microstructural damage. On the other hand, crack *growth* toughness stems from extrinsic toughening mechanisms, which act to shield the crack from the applied driving force to limit crack propagation (Launey and Ritchie, 2009).

To distinguish between the effects of osteocyte  $T\beta RII$  deficiency on crack initiation and crack growth, we conducted fracture toughness testing in a variable pressure scanning electron microscope to simultaneously visualize and quantify crack behavior. While crack initiation toughness could not be conclusively differentiated between genotypes, the shallow slope of the R-curve for  $T\beta RII^{ocy-/-}$  bones is indicative of reduced crack growth toughness and a loss of extrinsic toughening mechanisms (Fig. 5E). *In situ* images of crack growth show evidence of extrinsic toughening by crack deflection and uncracked ligament bridging in WT bone (Fig. 5E i-iii). Conversely, the path of cracks in  $T\beta RII^{ocy-/-}$  bone tended to be more linear and shorter relative to their profile extension (Fig. 5F-G). Therefore we conclude that TGF $\beta$  regulates bone quality in an osteocyte-intrinsic manner, specifically through extrinsic toughening mechanisms that limit crack growth. Identification of osteocytes as crucial cellular targets in the biological control of bone quality raises new questions about the role of osteocytes and PLR in human bone fragility.

## Discussion

This study advances our understanding of bone homeostasis and fragility by revealing an osteocyte-intrinsic role for TGF $\beta$  signaling. Here we implicate TGF $\beta$  as a novel regulator of perilacunar/canalicular remodeling and pinpoint osteocytes as the cell type principally responsible for the biological control of bone quality. Either using pharmacologic TGF $\beta$  receptor type I kinase inhibitors or a genetic model of osteocyte-specific TGF $\beta$  receptor ablation, we demonstrate that suppression of TGF $\beta$  signaling causes a severe deterioration of osteocyte canalicular network, and dysregulates the expression of a host of PLR genes. Loss of osteocyte-intrinsic TGF $\beta$  signaling also reduces bone matrix mineralization (Fig. 6). Since  $T\beta RII^{ocy-/-}$  cortical bone mass and geometry are normal, the profound fragility of these bones reveals that TGF $\beta$  controls bone quality through an osteocyte-intrinsic mechanism that relies on PLR. These findings strongly support the idea that PLR plays a fundamental role in bone homeostasis, specifically as the cellular mechanism responsible for the maintenance of the lacuno-canalicular network and bone quality.

Our findings revealed TGF $\beta$  signaling to be a cell-intrinsic regulator of perilacunar/canalicular remodeling. Osteocyte-specific inhibition of TGF $\beta$  signaling decreases the expression of several genes that have been functionally implicated in PLR, including *Mmp2*, *Mmp13*, *Mmp14*, *Ctsk* and *Acp5*. The coordinated regulation of these PLR genes by TGF $\beta$  is consistent with the effects of other PLR-regulatory pathways. Most of these genes are induced by PLR agonists, such as sclerostin and PTH, but repressed by PLR-antagonists such as glucocorticoids (Fowler et al., 2017; Kogawa et al., 2013; Qing et al., 2012). In each case, including in this study, these changes in gene expression correspond to alterations in the organization of the canalicular network. Interestingly, expression of vacuolar ATPases, that function in osteocyte acidification, is upregulated in T $\beta$ RII<sup>ocy-/-</sup> bone, raising the possibility that a feedback loop compensates for the low level of proteases mediating PLR.

The effects of TGF $\beta$  and other PLR-regulatory pathways on the lacuno-canalicular network and on bone matrix differ in important ways. In addition to alterations in the canalicular network, lactation and glucocorticoid treatment cause changes in lacunar size (Fowler et al., 2017; Qing et al., 2012). Furthermore, collagen organization is disrupted in MMP13-deficient mice and in mice treated with glucocorticoids. In T $\beta$ RII<sup>ocy-/-</sup> mice neither collagen organization nor lacunar volume, shape, and orientation was impacted. In this study, PLR mediated changes were observed at osteocyte canaliculi alone. Interestingly, emerging data from our lab and others (Fowler et al., 2017; Kaya et al., 2017; Tang et al., 2012) suggests that remodeling by osteocytes may be spatially defined, such that some circumstances favor remodeling at lacunae, whereas others will promote remodeling around canaliculi. Additional studies will be needed to determine the extent to which this is true.

The *in vitro* analysis of osteocyte acidification is a useful surrogate of PLR, but additional research is needed to better understand the cell biology of PLR. Nonetheless, TGF $\beta$  clearly acts directly on osteocytes to calibrate the extent of PLR and is required for the maintenance of the lacuno-canalicular network. Importantly, it is possible that the degenerated canalicular networks in our mouse models of impaired TGF $\beta$  signaling result from defective osteocyte integration into the bone matrix. A shorter time course or an inducible model would be needed to conclusively address this question. However, our previous studies have shown similar canalicular degeneration within 21 days of glucocorticoid treatment (Fowler et al., 2017) or a week of lactation (unpublished data)(Kaya et al., 2017; Qing et al., 2012; Qing and Bonewald, 2009; Wysolmerski, 2013), thereby indicating that changes in the canalicular network can occur rapidly in a manner that is independent of a maturation defect.

The critical role of TGF $\beta$  in osteocytes complements its actions in osteoblasts, osteoclasts, and their progenitors, where it couples bone formation to resorption (Dallas, 2008). Thus, it is not surprising that osteocyte-intrinsic ablation of T $\beta$ RII would inhibit osteoclast function due to reduced levels of RANKL expression by osteocytes. Whether by systemic T $\beta$ RI inhibition, expression of a dominant negative TGF $\beta$  type II receptor in osteoblasts, or in T $\beta$ RII<sup>ocy-/-</sup> mice, trabecular bone mass is increased due to reduced RANKL expression and reduced osteoclastogenesis (Edwards et al., 2010; Filvaroff et al., 1999; Mohammad et al., 2009). Though we cannot completely exclude a causal role of T $\beta$ RII<sup>ocy-/-</sup> osteocyte canalicular degeneration in the trabecular bone phenotype, our current and previous data suggest that TGF $\beta$ 's regulation of RANKL expression is cell intrinsic. On the other hand, the complexity of TGF $\beta$  crosstalk in bone underlies the unique, and at times apparently contradictory, bone phenotypes that result from

manipulating TGF $\beta$  signaling in one cell type or another (Dallas, 2008; Tang and Alliston, 2013). Furthermore, in bone and in many other tissues, the effect of TGF $\beta$  is nonlinear; such that either increased and decreased TGF $\beta$  signaling can produce an osteoporotic phenotype (Balooch et al., 2005; Borton et al., 2001; Erlebacher and Derynck, 1996). Despite this known complexity, we were surprised by the low mineral concentration of T $\beta$ RII<sup>ocy-/-</sup> bone, given that mineralization is increased by systemic post-natal T $\beta$ RI-I treatment (Edwards et al., 2010; Mohammad et al., 2009). Given that osteocyte canaliculi are sites of secondary mineralization, it is possible that the reduced canalicular length in the T $\beta$ RII<sup>ocy-/-</sup> bones reduces surface area available for mineralization. Moreover, the increased expression of vacuolar ATPase may create an acidic microenvironment that is unfavorable for mineralization. Additional studies will be needed to discern the mechanisms by which pharmacologic disruption of TGF $\beta$  signaling affects bone mineralization differently from genetic ablation of T $\beta$ RII specifically in osteocytes.

Bone strength relies on bone mass and bone quality, both of which depend on the ability of TGF $\beta$  to coordinate the function of osteoblasts, osteoclasts and osteocytes. In spite of the fact that bone quality contributes to at least half of fractures in people with clinically normal bone mass (Schuit et al., 2004; Sornay-Rendu et al., 2007), the cellular mechanisms controlling bone quality have remained unclear. Understanding these mechanisms is a critical step in improving the diagnostics and therapeutics for fragility fractures (Hernandez and Keaveny, 2006; Seeman, 2008). This study represents the most definitive evidence so far implicating osteocyte-mediated PLR in the control of bone quality. Previous studies by our group and others show that bone quality is impaired following glucocorticoid treatment or systemic ablation of MMP13, and that PLR is impaired in each case (Fowler et al., 2017; Lane et al., 2006; Tang et al., 2012). Here we find that osteocyte-specific deletion of TGF $\beta$  signaling caused defects in PLR and in cortical bone mineralization, flexural strength, ECM material properties, and fracture toughness without impacting cortical bone mass. In diseases like Camurati Engelman syndrome and osteogenesis imperfecta, both of which are characterized by excessive TGF $\beta$  signaling (Grafe et al., 2014; Kinoshita et al., 2000; Tang et al., 2009), deregulation of osteocyte-mediated remodeling may contribute to the bone fragility in these diseases. Similarly the extent to which dysregulated PLR contributes to the fragility in other skeletal diseases, including renal osteodystrophy, secondary hyperparathyroidism, and glucocorticoid-induced osteoporosis, is an important area of further investigation. If so, PLR could be an attractive therapeutic target for improving fracture resistance in many conditions.

In conclusion, this study emphasizes the need to identify the cellular and molecular mechanisms regulating bone quality to develop new therapies to address the significant unmet clinical need for the treatment of bone fragility. Current therapeutics can improve 70% of trabecular fractures but only 20-40% of cortical bone fractures, which is precisely where PLR dysregulation is most profound (Ahmed et al., 2015; Chen and Sambrook, 2011; Rivadeneira and Mäkitie, 2016). A combination of systems analysis of GWAS data from clinical cohorts, along with functional in vivo and in vitro studies, can shed light on new molecular targets to control bone fragility and expand the pool of genetic markers needed for fracture risk assessment and prevention.

## **Experimental Procedures**

### **Mice**

To block TGF $\beta$  signaling systemically, 5-week old equally weighing C57BL/6 male mice were administered either vehicle (1% methylcellulose) or a specific inhibitor of the TGF $\beta$  type I receptor (T $\beta$ RI-I), (SD-208, 60 mg/kg twice daily by oral gavage) for 6 weeks (Mohammad et al., 2009). We also generated mice with osteocyte-specific ablation of TGF $\beta$  type II receptor (T $\beta$ RII), which effectively blocks osteocyte sensitivity to TGF $\beta$  ligand. Homozygous T $\beta$ RII-floxed mice that possess *loxP* sites flanking exon 4 of the targeted gene were backcrossed for 3 generations into a C57BL/6 background and subsequently bred with hemizygous -10kb-DMP1-Cre<sup>+/-</sup> mice, which express Cre recombinase primarily in osteocytes (Leveen et al., 2002; Lu et al., 2007). Half of the mice from the resulting cross were DMP1-Cre<sup>+/-</sup>;T $\beta$ RII<sup>fl/fl</sup> (named T $\beta$ RII<sup>ocy-/-</sup> mice) and half were DMP1-Cre<sup>-/-</sup>;T $\beta$ RII<sup>fl/fl</sup> littermate controls (named Wild-type (WT) mice), as confirmed by PCR genotyping. All animal procedures were approved by the Institutional Animal Care and Use Committee of the University of California San Francisco and the Indiana University School of Medicine.

### **Morphological analysis.**

For skeletal phenotyping, femurs harvested from 8-week old male mice (n=8 mice per group) were cleaned of soft tissue and fixed in 10% neutral buffered formalin for micro-computed tomography (microCT,  $\mu$ CT). For  $\mu$ CT, fixed femurs were stored in 70% ethanol. For histomorphometry, 7-week old male mice were administered with two intraperitoneal injections of calcein (20 mg/kg body weight, Sigma) 10 and 3 days prior to euthanasia and the harvested femurs were fixed in 10% neutral buffered formalin for 48 hours, processed and embedded in a MMA plastic resin. Additional details of  $\mu$ CT and histomorphometry procedures are described in the Supplemental Data.

### **Quantitative RT-PCR analysis**

We purified RNA from cells in culture and from bones dissected from soft tissues using the miRNeasy mini kit (Qiagen, Valencia, CA), following the manufacturer's protocol. In vitro results are representative of n=3 replicates/ group and 3 independent experiments. For bones (humeri from n $\geq$ 8 mice/ group), proximal and distal regions were cut off and marrow was removed by centrifugation before RNA extraction. The majority of RNA obtained from bone using this method is osteocyte derived, with very little contribution from osteoblasts (Halleux et al., 2012). Additional details of quantitative RT-PCR analysis are described in the Supplemental Data).

### **Immunohistochemistry**

For immunohistochemistry, paraffin embedded (7 $\mu$ m thick) sections were incubated with primary antibodies for anti-MMP13 (1:100; Abcam, ab39012); anti-MMP14 (1:100; Abcam, ab38971); anti-CTSK (1:75; Abcam, ab19027), or anti-T $\beta$ RII (1:500; Abcam, ab186838). This was followed by incubation with corresponding biotinylated secondary antibody, avidin-conjugated peroxidase, and diaminobenzidine substrate chromogen system (Innovex Universal Animal IHC kit). Corresponding nonimmune IgGs were used as negative controls. Hematoxylin and eosin (H&E) and TUNEL-DAPI staining were performed to visualize osteocyte number and apoptosis. Ploton silver staining (Jauregui et al., 2016; Ploton et al., 1986) was performed for visualization of the osteocyte lacuno-canalicular network. Images were acquired using a Nikon Eclipse E800 bright-field microscope and analyzed with ImageJ. Sections were evaluated for one femur from each of n $\geq$ 4 mice/ group. Additional details of immunohistochemistry and image analysis are described in the Supplemental Data.

### **Cell culture**

The MLO-Y4 osteocyte-like cell line (generously provided by L. Bonewald) was maintained in  $\alpha$ -MEM supplemented with 2.5% fetal bovine serum, 2.5% bovine calf serum, and 1% penicillin-streptomycin. The OCY454 osteocyte cell line (generously provided by P. Divieti-Pajevic) was cultured in  $\alpha$ -MEM supplemented with 10% fetal bovine serum and 1% antibiotic/ antimycotic (Gibco). For treatment, cells were cultured in  $\alpha$ -MEM containing 0.5-1% fetal bovine serum, supplemented with 5 ng/ml TGF $\beta$ 1 (Humanzyme, HZ-1011), 10  $\mu$ M SB431542 (Sigma, S4317) or 10 ng/ml recombinant human sclerostin (rhSCL, R&D Systems) for the indicated times.

### **Intracellular pH assay**

Intracellular pH (pHi) was measured in transfected or untransfected MLO-Y4 cells treated with TGF $\beta$ 1, SB431542 or rhSCL using the pH-sensitive fluorescent dye, 5-(and-6)-carboxy SNARF-1, AM (Molecular Probes, Inc.) as described (Kogawa et al., 2013). Briefly, after 3 days of culture in the indicated conditions, cells were washed with PBS and loaded with 5-(and-6)-carboxy-SNARF-1, AM at 37°C for 30 minutes, at a final concentration of 10  $\mu$ M and visualized under a Leica TCS SPE confocal microscope. n=4 replicates/ group and 3 independent experiments. Additional details of the procedure are provided in the Supplemental Data.

### **Synchrotron radiation Micro-Tomography (SR $\mu$ T)**

SR $\mu$ T studies were used to assess the degree of mineralization of bone as well as the volume and degree of anisotropy of osteocyte lacunae. The mid-diaphysis of 8-week old male mouse femurs were scanned with 20 keV x-ray energy, with a 300 ms exposure time, using a 5X magnifying lens for a spatial resolution of 1.3  $\mu$ m (N=3-4 mice/ group). Additional details of the SR $\mu$ T procedure are described in the Supplemental Data.

### **Mechanical tests**

To measure bone quality, we assessed the macromechanical properties and the bone matrix material properties using flexural strength tests, *in situ* fracture toughness tests, and nanoindentation. Briefly, from 8-week old T $\beta$ RII<sup>ocy-/-</sup> and WT mice (n=3-5 mice/ group) intact femurs were isolated, cleaned of soft tissue and stored in Hanks' Balanced Salt Solution (HBSS). Details of the flexural strength tests, *in situ* fracture toughness tests, and nanoindentation procedures are described in the Supplemental Data.

### **Statistical Analysis**

We expressed all values as mean  $\pm$  S.E.M or mean  $\pm$  S.D as appropriate for each assay. Group sizes were determined by power calculations providing 80% probability of detecting a significant difference ( $p \leq 0.05$ ). Group size "n" is denoted in figure legends. For *in vivo* data, n refers to the number of mice analyzed per group. For *in vitro* data, n refers to the number of independent experiments performed. Unpaired two-tailed Student's *t*-test was used to compare the means of two groups using GraphPad Prism (GraphPad Software). Data points falling more than 2 standard deviations from the mean were excluded. Variances ranged from 12.5% to 20% and were similar between groups. No blinding was used during analysis. In all figures,  $p \leq 0.05$  was considered statistically significant.

### **Author Contributions**

Conceptualization, N.S.D., T.W.F., K.S.M., T.A.; Investigation, N.S.D., C.M.M., C.A., J.P.L., D.A.M., B.G., J.N.R., F.W., D.E., T.F.L., B.Z.; Data Curation, S.M.; Analysis, all authors; Writing – Original Draft, N.S.D.; Writing – Review & Editing, all authors; Visualization, N.S.D., C.M.M., T.A.; Supervision, R.O.R., K.S.M., T.A.; Project Leadership, N.S.D., T.A.; Funding Acquisition, T.A.

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## Figure and Table Legends

### Figure 1. Pharmacologic TβRI inhibition impairs perilacunar remodeling (PLR)

(A, B) Silver nitrate stained images of femoral cortical bone from vehicle and TGF $\beta$  receptor I kinase inhibitor (T $\beta$ RI-I, SD-208) treated mice show osteocyte lacuno-canalicular network (A) and canalicular length (B). Scale bar, 20  $\mu$ m (n=6 mice/group). (C) qPCR analysis of PLR genes *Mmp2*, *Mmp13*, *Mmp14*, *Ctsk*, and *Acp5* in bones from vehicle and T $\beta$ RI-I treated animals (n=8 mice/group). (D-F) Immunohistochemistry (IHC) of MMP13, MMP14 CTSK and H&E staining of femoral cortical bone of vehicle and T $\beta$ RI-I treated animals. Arrows in the image indicate positively stained osteocytes that were quantified and normalized to total bone area. Scale bar, 50  $\mu$ m (n=4 mice/group). Error bars indicate mean  $\pm$  SEM, \*p<0.05 compared to vehicle from Student's t test.

### Figure 2. TGF $\beta$ promotes cell intrinsic osteocytic perilacunar remodeling

(A-D) qPCR analysis of PLR genes *Mmp13*, *Mmp14* and *Ctsk* and *Serpine1* upon TGF $\beta$  (5ng/mL) treatment in MLO-Y4 (A,B) and OCY454 (C,D) cells. (n=3 replicates/group). (E, F) Intracellular pH (pHi) of MLO-Y4 cells after 3 days of TGF $\beta$  (5ng/ml), T $\beta$ RI inhibitor SB-431542 (10  $\mu$ M), or recombinant sclerostin (rhSCL, 10 ng/ml). The representative image (E) shows the shift in the emission peak from 580 nm to 640 nm after TGF $\beta$  treatment of MLO-Y4 cells. Scale bar, 100 nm). TGF $\beta$ -induced acidification is blocked by SB-431542 (F) (n=4 replicates/group). Error bars indicate mean  $\pm$  SD of 3 independent experiments, \*p<0.05 different from control mRNA, a-p<0.05 different from control pHi, b-p<0.05 different from TGF $\beta$  pHi, and c-p<0.05 different from rhSCL pHi. Statistics calculated from Student's t test.

### Figure 3. Osteocytic deletion of T $\beta$ RII dysregulates perilacunar remodeling.

(A, B) T $\beta$ RII-stained osteocytes (A) (arrow, scale bar, 50  $\mu$ m) in the femoral cortical bone from WT and T $\beta$ RII<sup>ocy-/-</sup> mice (8-week old males) were quantified as percentage of positively stained osteocytes normalized to total bone area (B) (n=5 mice/group) (C) qPCR analysis of T $\beta$ RII and *Serpine1* in WT and T $\beta$ RII<sup>ocy-/-</sup> femoral bones. (n=8-10 mice/group). (D, E) Silver nitrate stained images of WT and T $\beta$ RII<sup>ocy-/-</sup> femoral cortical bone shows the osteocyte lacuno-canalicular network (D) and canalicular length (E) (scale bar, 20  $\mu$ m, n=5 mice/group). (F, G) qPCR analysis of PLR genes, *Mmp2*, *Mmp13*, *Mmp14*, *Ctsk*, and *Acp5* (F) and OCY-specific genes, *Sost*, *Dmp1* and *Phex* (G) in the WT and T $\beta$ RII<sup>ocy-/-</sup> bones (n=8-10 mice/group) (H, I) IHC of MMP13, MMP14, CTSK and H&E staining of WT and T $\beta$ RII<sup>ocy-/-</sup> femoral cortical bone. Arrows in the image indicate positively stained osteocytes (H) that were quantified and normalized to total bone area (I), (n=4 mice/group). (J-M) SR $\mu$ T shows volume (J), degree of anisotropy (K), orientation (L) and mineralization (N) of osteocyte lacunae of WT and T $\beta$ RII<sup>ocy-/-</sup> bone (n=3-4 mice/group). Error bars indicate mean  $\pm$  SEM with \*p<0.05 compared to WT from Student's t test.

### Figure 4. Osteocytic deletion of T $\beta$ RII increases trabecular bone mass but does not affect cortical bone mass.

(A-D)  $\mu$ CT analysis of femur from WT and T $\beta$ RII<sup>ocy-/-</sup> mice (8-week old males), Representative  $\mu$ CT reconstructions of trabecular bone (A) from mice and trabecular bone parameters: trabecular bone volume fraction (BV/TV) (B), trabecular number (Tb.N.) (C), and separation (Tb.Sp.) (D). Scale bar, 100  $\mu$ m (n=10-11 mice/group) (E-I) Histomorphometric analysis of femur from WT and T $\beta$ RII<sup>ocy-/-</sup> mice (8-week old males) measures osteoblast number normalized to bone surface (N.Ob/BS), bone formation rate (BFR) and percent mineralizing bone surface per bone surface (MS/BS), osteoclast number normalized to bone surface (N.Oc/BS), osteoclast surface normalized to bone

surface (Oc.S/BS) (n=6-7 mice/group). (J) qPCR analysis of mRNA harvested from WT and  $T\beta RII^{ocy-/-}$  bones shows the *Rankl/Opg* ratio (n=8-10 mice/group). (K-N) Representative  $\mu$ CT reconstructions of femoral cortical bone femur from WT and  $T\beta RII^{ocy-/-}$  mice (8-week old males) (K) and cortical bone parameters: cortical area fraction (Ct. BA/TA) (L), cortical thickness (Ct. Th) (M), and cortical mineralization (Ct. Min) (N). Scale bar, 100  $\mu$ m (n=10-11 mice/group). Data are presented as mean  $\pm$  SEM and \* $p < 0.05$  compared to WT from Student's t test.

**Figure 5. Osteocytic deletion of  $T\beta RII$  reduces bone material properties at multiple length scales.**

Mechanical testing on femurs from WT and  $T\beta RII^{ocy-/-}$  mice (8-week-old males). (A-B) Flexural tests of intact femurs shows bending modulus (A) and yield stress (B) (n=5 mice/group). (C) Nanoindentation of mid-diaphyseal femoral bone shows that tissue elastic modulus (n=3 mice/group). (D-E) *In situ* fracture toughness testing of notched femurs subjected to 3-point bending in a variable pressure SEM shows total work of fracture (WoF) (D) (n=5 mice/group), WoF R-curves, produced by calculating WoF at each instance of crack propagation (E) (n=3 mice/group). Three stages of crack growth are shown for a WT sample (i-iii), with pre-existing notch or crack in black and new crack extension in red, and the corresponding points are indicated in the R-curve. (F-G) The decrease in  $T\beta RII^{ocy-/-}$  bone of the extrinsic toughening mechanism, crack deflection, is readily seen in two representative samples (F) (scale bar = 100  $\mu$ m) and in quantification of the ratio of total crack length to crack extension (G) (N=5 mice/group). Data are presented as mean  $\pm$  SD. 95% confidence intervals in (E) are calculated based on a power fit. \* $p < 0.05$  different from WT group.

**Figure 6.  $TGF\beta$  regulates bone fragility**

A schematic summarizes the role of osteocytic  $TGF\beta$  signaling in PLR and bone quality.

**Table 1. Skeletal phenotyping of 8-week old WT and  $T\beta RII^{ocy-/-}$  mice**

$\mu$ CT and histomorphometry analysis revealed significant differences in trabecular bone phenotype, cortical mineralization, and osteoclast behavior between wildtype and  $T\beta RII^{ocy-/-}$  mice, but no differences were observed in cortical bone volume or osteoblast behavior. Bone parameters measured by microCT include trabecular bone volume fraction (TBV); connectivity density (Conn D); trabecular number (Tb. N); trabecular thickness (Tb. Th); trabecular separation (Tb. Sp); structural model index (SMI); trabecular mineralization (Tb. Min); cortical bone volume fraction (Ct. BV/TV); cortical thickness (Ct. Th); cortical SMI, and cortical mineralization (Ct. Min), with N=10-11 mice per group. Histomorphometry parameters measured include osteoid volume (OV/BV); osteoid surface (OS); osteoid width (O. Wi); osteoblast number (N. Ob); osteoblast surface (N. Ob/BS); osteoclast surface (Oc.S); eroded bone surface (Oc.S/BS); osteoclast number (N. Oc); osteoclast number (N.Oc/BS); mineralization surface (MS/BS); bone formation rate (BFR); and mineral apposition rate (MAR), with N=6-7 mice per group. Data are presented as mean  $\pm$  SEM with \* $p < 0.05$ , #  $p = 0.06$ , and †  $p = 0.07$  different from WT group.

| MicroCT                                        | WT              | TβRII <sup>ocy-/-</sup> |
|------------------------------------------------|-----------------|-------------------------|
| <b>Distal Femur</b>                            |                 |                         |
| TBV (BV/TV) (%)                                | 0.192 ± 0.016   | 0.259 ± 0.028 *         |
| Conn D (1/mm <sup>3</sup> )                    | 377.74 ± 29.29  | 493.37 ± 71.58          |
| Tb. N (1/mm)                                   | 6.275 ± 0.215   | 7.557 ± 0.542 *         |
| Tb. Th (μm)                                    | 0.043 ± 0.002   | 0.043 ± 0.001           |
| Tb. Sp (mm)                                    | 0.155 ± 0.006   | 0.126 ± 0.009 *         |
| SMI                                            | 1.720 ± 0.184   | 1.063 ± 0.287 #         |
| Tb. Min (mg HA/cm <sup>3</sup> )               | 1020.98 ± 9.31  | 1014.23 ± 13.36         |
| <b>Midshaft Femur</b>                          |                 |                         |
| Ct. BV/TV (%)                                  | 0.437 ± 0.006   | 0.445 ± 0.008           |
| Ct. Th (μm)                                    | 0.188 ± 0.004   | 0.189 ± 0.003           |
| Ct. SMI                                        | -0.442 ± 0.239  | -1.066 ± 0.339          |
| Ct. Min (mg HA/cm <sup>3</sup> )               | 1279.69 ± 15.30 | 1217.59 ± 16.136 *      |
| <b>Static parameters</b>                       |                 |                         |
| OV/BV                                          | 0.007 ± 0.001   | 0.004 ± 0.001           |
| OS                                             | 0.14 ± 0.02     | 0.12 ± 0.04             |
| OS/BS (%)                                      | 0.04 ± 0.01     | 0.03 ± 0.01             |
| O. Wi (μm)                                     | 3.28 ± 0.21     | 2.79 ± 0.36             |
| N.Ob                                           | 61.00 ± 5.61    | 60.94 ± 8.81            |
| N.Ob/BS (/mm)                                  | 19.01 ± 2.57    | 18.24 ± 2.38            |
| Oc.S                                           | 0.83 ± 0.07     | 0.68 ± 0.01 †           |
| Oc.S/BS (%)                                    | 0.12 ± 0.01     | 0.08 ± 0.01 *           |
| N.Oc                                           | 39.57 ± 3.10    | 30.17 ± 1.66 *          |
| N.Oc/BS (/mm)                                  | 5.63 ± 0.44     | 3.40 ± 0.28 *           |
| <b>Dynamic parameters</b>                      |                 |                         |
| MS/BS (%)                                      | 0.15 ± 0.01     | 0.16 ± 0.01             |
| MAR (μm/d)                                     | 1.84 ± 0.13     | 1.89 ± 0.17             |
| BFR/BS (μm <sup>2</sup> . μm <sup>3</sup> . d) | 0.28 ± 0.03     | 0.30 ± 0.03             |