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Solution-synthesized chiral piezoelectric selenium nanowires for wearable self-powered human-integrated monitoring

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ABSTRACT

Smart sensing devices with high stretchability and self-powered characteristics are essential in future generation wearable human-integrated applications. Here we report for the first time scalable synthesis and integration of selenium (Se) nanowires into wearable piezoelectric devices, and explore the feasibility of such devices for self-powered sensing applications, e.g., physiological monitoring. The ultrathin device can be conformably worn onto the human body, effectively converting the imperceptible time-variant mechanical vibration from the human body into distinguishable electrical signals, e.g., gesture, vocal movement, and radial artery pulse, through straining the piezoelectric Se nanowires. Our results suggest the potential of solution-synthesized Se nanowire a new class of piezoelectric nanomaterial for self-powered biomedical devices and opens doors to new technologies in energy, electronics, and sensor applications.

1. Introduction

In 2006, Wang *et al.* invented ZnO-based piezoelectric nanogenerators (PENG) which could realize the conversion of mechanical energy from the ambient environment into electrical power [1]. Since then, the harvesting of mechanical energy using nanostructured piezoelectric materials has received considerable attention, including wurtzite materials like GaN [2–4], CdS [5,6], perovskite materials like BaTiO₃ [7–10], ZnSnO₃ [11–13], other inorganic lead-free piezoelectric material [14,15] and also synthetic polymers such as PVDF and its copolymers [16–18]. The low-dimensional geometries, superior mechanical properties of piezoelectric nanomaterials compared to their bulk counterparts, and the direct energy conversion in piezoelectric process facilitate the integration into deformable devices for efficiently harvesting ubiquitous mechanical energy, hinged on principles of the time-variant piezoelectric polarization induced displacement current

[19]. Ongoing efforts in the field of PENG are primarily focused on improving energy conversion by further enhancing the materials' piezoelectric properties [16,20–22] and demonstrating proof-of-concept application [23]. Progress in these fields combined with the emerging methods for deterministic production and assembly of nanomaterials [21] leads to exciting research opportunities. Nevertheless, significant roadblocks exist for realizing the technological potential of existing piezoelectric nanomaterials. For instance, the sophisticated process for synthesizing wurtzite-structured piezoelectric nanowires with orientation control limit the potential device integration and applications [24–26]. Obstacles concerning scalable, economic production of piezoelectric nanomaterials with desired piezoelectric and mechanical properties continue to prevail.

Here we demonstrate for the first time scalable synthesis and integration of selenium (Se) nanowires into wearable piezoelectric devices and explore the feasibility of such devices for self-powered sensing

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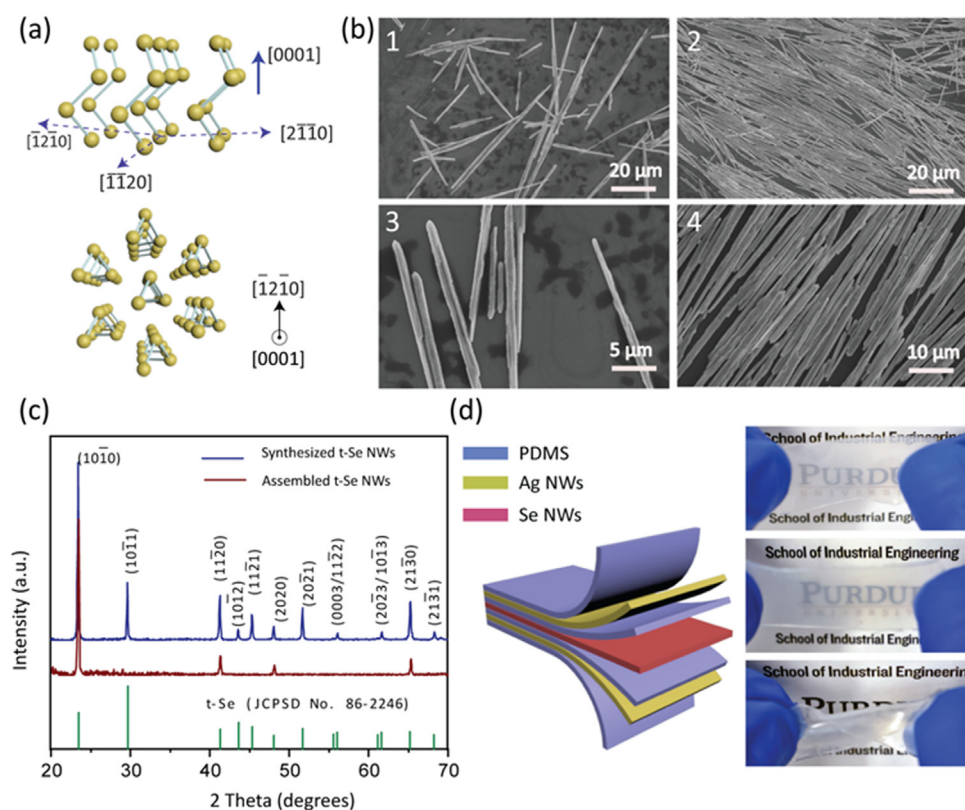


Fig. 1. (a) Schematic of the crystal structure of Se nanowires. (b) SEM images of the as-synthesized Se nanowires and the assembled Se nanowires film. (c) XRD patterns of the as-synthesized Se nanowires and assembled film. (d) 3D illustration of the Se-PENG device and the optical images of the device at the original state, being stretched and twisted, respectively.

applications, e.g., physiological monitoring. The ultrathin device can be conformably worn onto the human wrist, effectively converting the imperceptible time-variant mechanical vibration from the human body into distinguishable electrical signals through straining the piezoelectric Se nanowires.

The trigonal-structured selenium (t-Se) has an anisotropic crystal lattice where individual chiral chains of Se atoms are stacked together by weak bonding [27,28] (Fig. 1a). Each Se atom is covalently bonded with its two nearest neighbors on the same chain. t-Se has the same non-centrosymmetric structure to that of trigonal-structured tellurium (t-Te) [29,30]. Lee et al. previously demonstrated the application of t-Te nanowires for piezoelectric nanogenerator [31]. The solution-synthesized t-Te nanowires are assembled horizontally on the flexible polyimide substrates, and can generate a power density up to 9 mW/cm^3 upon straining. However, the narrow bandgap [32] of metalloid tellurium may limit the piezoelectric application of t-Te nanowires. In contrast, selenium has a sizeable bandgap of 1.7 eV [33,34], and the nanostructured t-Se is expected to exhibit strong piezoelectric property [35], leading to a potential high volume-power-density in integrated devices. Similar to the t-Te nanowire, the radial distribution of the piezoelectric polarization in the t-Se nanowire, due to the strain-induced relative displacement of the electron distribution against the Se atoms cores [36], facilitates its integration into ultrathin laminated devices through economic manufacturing approaches, e.g., roll-to-roll (R2R) printing, onto various substrates [37].

2. Results and discussion

The Se nanowires were synthesized following the procedures described in the Methods section. The morphology of the as-synthesized Se nanowires can be seen in Fig. 1b. The length of the nanowires ranges from tens of μm to $100 \mu\text{m}$, while the diameter is $\sim 500 \text{ nm}$. Fig. 1 b-1 and b-3 present the morphology of the Se nanowires before the assembly, and Fig. 1 b-2 and b-4 show the Se nanowires after the LB assembly forming a close-packed film with oriented Se nanowires. X-

Ray diffraction (XRD) was used to characterize the structure of the product. All the peaks in the XRD pattern (blue line) in Fig. 1c can be assigned to the pure trigonal phase of Se with lattice parameters of $a = 4.36 \text{ \AA}$ and $c = 4.97 \text{ \AA}$ (JCPDS 86-2246). No XRD peaks arising from impurities could be detected, indicating that only elemental Se nanowires with high crystallinity and purity were derived. Compared with the standard pattern of t-Se, it is found that the intensity of (hki0) reflection peaks of our synthesized Se nanowires is strong, which suggests that the as-obtained t-Se crystals have a preferential growth orientation of [0001]. Interestingly, when the Se nanowires are assembled and transferred onto the substrate, some high-index peaks vanish in the XRD pattern (red line in Fig. 1c) with the two most prominent peaks arising from the (10 $\bar{1}$ 0) and (11 $\bar{2}$ 0) planes. Such changes in the XRD patterns are consistent with the observed alignment of the Se nanowires in the horizontal plane after the LB assembly (Fig. 1b).

The piezoelectricity origin can be analyzed from the crystal structure and point group of the material that belongs to. Trigonal selenium belongs to point group of 32, and the space group is either $P3_121$ or $P3_221$. The single crystal material belonging to group 32 has two independent piezoelectric components, d_{11} and d_{14} . The crystal structure of the selenium is demonstrated in Fig. 1a. Two adjacent Se atoms in one spiral are nearest neighbors and stronger bound than adjacent Se atoms of two neighboring spirals (Upper part in Fig. 1a). The hexagonal cross-section of the t-Se NW and its two-dimensional hexagonal-lattice structure with equilateral triangles resulting from the projection of the helical turns of Se atoms onto (0001) planes are illustrated in the lower part of Fig. 1a. We draw a schematic here showing how the selenium atoms in one chain are distorted when they are subject to external stress (Fig. 2a). We use a right-hand coordinate system x, y, z in which x and z correspond to the crystallographic a - and c -axes, respectively. When longitudinal stress is applied along the x -axis, internal displacement of the Se atom and displacement of the electronic charge against the Se cores will occur, which would give rise to a piezoelectric polarization parallel to x -axis. This polarization is described by the piezoelectric coefficient d_{11} . As presented in Fig. 2a(ii) and 2a(iii), when the

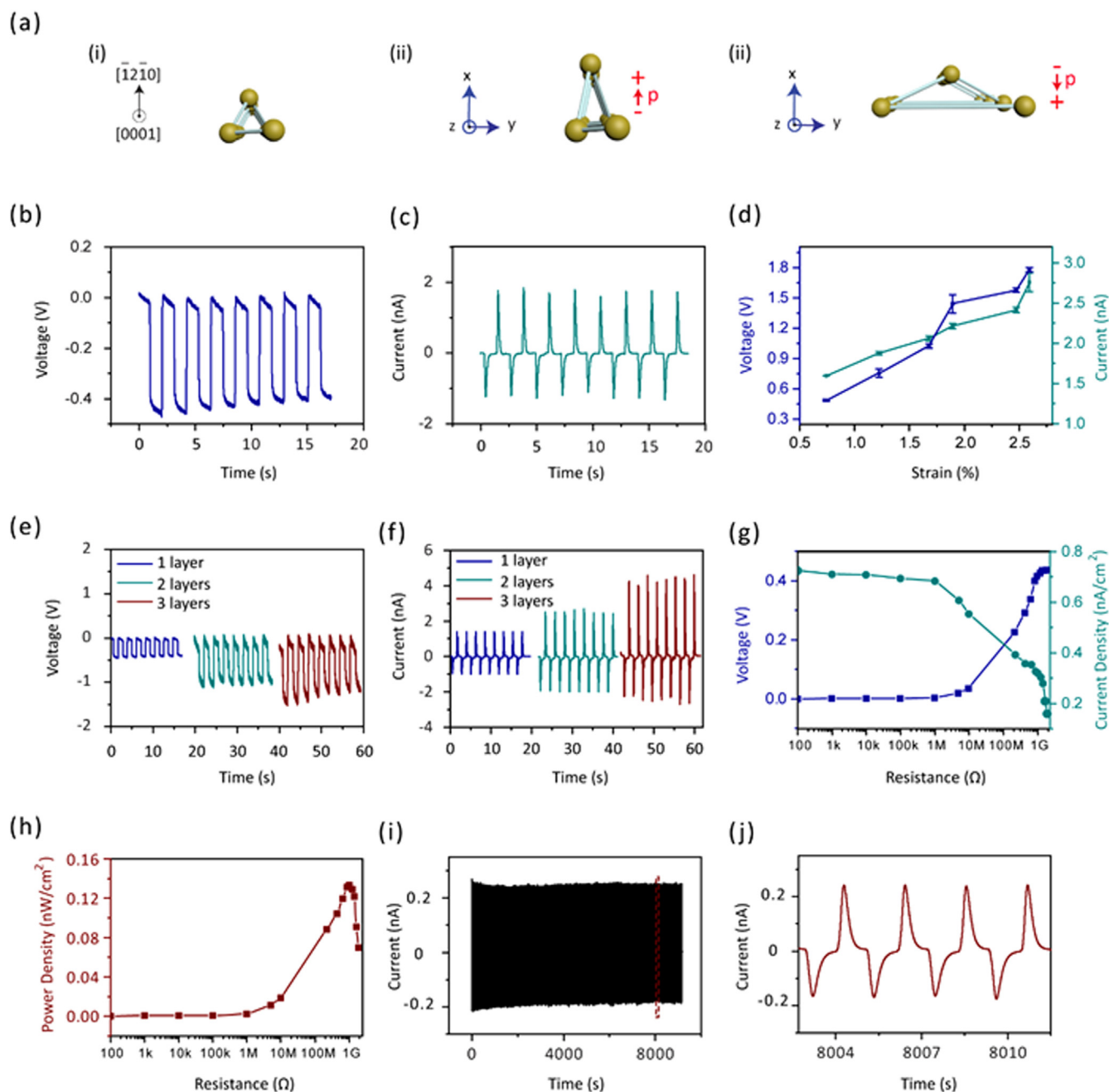


Fig. 2. (a) Schematic showing the deformed Se nanowire chain and the origin of the piezoelectric polarization. (b) open-circuit voltage (V_{oc}) and (c) short-circuit current (I_{sc}) of Se-PENGs. (d) The V_{oc} and I_{sc} as a function of strain. The output (e) voltage and (f) current are from devices with 1, 2 and 3 layers of assembled Se nanowires. (g) The output voltage/current and (h) power versus the load resistance. (i) The cyclic output of Se-PEND during a stability test. (j) The magnified view of the output signals highlighted in (i). Only one layer of Se nanowires is adopted in the device in g, h and i, and the applied mechanical strain is 0.75% for the measurement.

selenium nanowire is stretched vertically, a piezoelectric polarization pointing upward would be generated, and similarly a vertically compressed selenium nanowire would give rise to a downward-pointed piezoelectric polarization. As reported elsewhere, the piezoelectric components, d_{11} is found to be $(0.41 \pm 0.03) \times 10^{-10}$ m/V [38]. Although the piezoelectricity of selenium bulk crystal has already been reported in the prior work [35,38–40], this is our first time to report the piezoelectricity in selenium nanowire and fabricate wearable devices for energy harvesting and sensor applications.

The detailed process for fabricating the wearable PENG device based on Se nanowires (Se-PENG) is shown in the experimental section. Our Se-PENG device (Fig. 1d) consists of multiple layers stacking of

PDMS, Ag nanowires electrodes, and piezoelectric Se nanowires, which are highly flexible and stretchable. Fig. 1d shows the good deformability of our Se-PENG device which can withstand large degrees of mechanical deformation without fracture or cleavage. A cross-sectional SEM image of the layered device is demonstrated in Fig. S1, and we find that the interface of Se nanowires/PDMS and Ag nanowires/PDMS are visible. To better quantitatively characterize the mechanical properties of the fabricated device, a tensile test is applied here (Fig. S2), where the tensile strength and the maximum strain of the device that can withstand are nearly 1.78 MPa and 200%, respectively. Here the PDMS layers not only serve as the insulating layers between the Se and Ag nanowires but also encapsulate the Ag nanowires from oxidation and

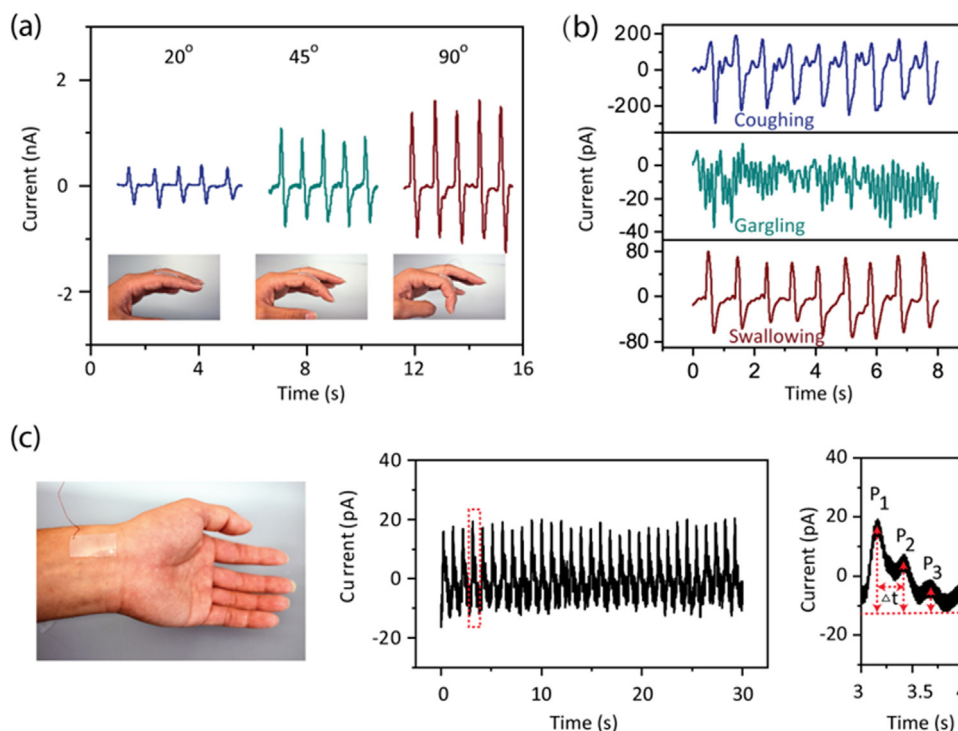


Fig. 3. (a) The output current of the Se-PENG attached on the human fingers and bent with different angles. (b) The output current of the Se-PENG attached on the human throat when the subject is coughing, gargling and swallowing. (c) The real-time artery pulse signal monitored by the Se-PENG.

performance deterioration. In our device, the sprayed Ag nanowires form an interconnected conducting network (Fig. S3, Supporting Information). The entanglement of these long Ag nanowires (lengths ~ 50 – $100\ \mu\text{m}$) is expected to lead to a good conductivity and stretchability in the electrodes structure desirable for the PENG application [41]. We also characterized the reliability of our stretchable Ag nanowires electrodes by measuring their resistance after cyclic straining (Fig. S4). A slight increase in electrode resistance was observed after the device being subjected to cyclic large-degree straining, and no observable increase in the electrode resistance can be seen after an initial “burn-in” period of 150-cycle straining. The increase in the Ag nanowire electrode resistance is negligible compared to the internal impedance of the PENG devices (from several hundred $\text{M}\Omega$ to $\text{G}\Omega$) [42–44] and is expected to not affect the output of Se-PENG devices.

Devices with a dimension of $1\ \text{cm} \times 2\ \text{cm}$ were used in our experiment for characterizing the piezoelectric output of Se-PENGs. When the devices are subjected to periodic strains with controlled magnitudes, which are applied through a linear motor (Methods), the strain-induced piezoelectric polarizations in the Se nanowires will electrostatically induce an electrical field between the top and bottom electrodes. Such a time-variant piezoelectric field due to the periodic strain leads to the displacement current in the circuit and hence the measured electrical outputs [19]. With a compressive strain of 0.74% along the alignment direction of Se nanowires, the measured open-circuit voltage (V_{oc}) and short-circuit current (I_{sc}) present to be 0.45 V and 1.67 nA, respectively (Fig. 2b and c). The switching-polarity test was further performed to verify that the measured electrical outputs are caused by the intrinsic piezoelectric properties of the assembled Se nanowires [45] (Fig. S5, Supporting information). Additional sets of characterizations were also carried out when the Se-PENGs were subjected to a tensile strain along the alignment direction of Se nanowires (Fig. S5, Supporting information), showing that the electric outputs were reversed when the strain was switched from compressive to tensile. The strain-dependent piezoelectric outputs were also characterized for the Se-PENG devices when the strain increased from 0.74% to 2.59% (Fig. 2d). Both the V_{oc} and I_{sc} increase with the strain. The monotonic dependence of the

piezoelectric outputs with the magnitudes of the applied strains suggest that the Se-PENG has a good strain resolution and can function as a self-powered mechanical sensor [46]. The small variance seen for each data point in Fig. 2d is likely due to the variations in the electrode resistance (Fig. S4). The unique crystal structure of Se nanowires and the corresponding radial distribution of the piezoelectric field in strained Se nanowires facilitates the integration of multiple Se-PENGs into ultra-thin laminated devices with enhanced outputs. Fig. 2e and f show that both the output voltage and current increase when the assembled Se layers scale up. Here the number of selenium nanowire layers can be controlled by the assembly and the following transfer times to the substrate. The output power of Se-PENG delivered to external loads is characterized by varying the load resistance connected in the circuit. Fig. 2g showed the resistance-dependent output voltage and current when the load resistor was swept from $100\ \Omega$ to $1.88\ \text{G}\Omega$. The instantaneous output power can then be calculated and plotted as a function of the load resistance (Fig. 2h), with a maximum output power determined to be $0.135\ \text{nW}/\text{cm}^2$ at a load resistance of $1\ \text{G}\Omega$. Taking advantage of the superior mechanical deformability and stability of the Se nanowire active layer, the Ag nanowires electrodes, and the PDMS layer, Se-PENG shows good long-term stability after being subjected to cyclic straining and release for more than two hours (Fig. 2i and j). No observable damage or deterioration is observed in the morphology of the Se NW encapsulated in the PDMS after repeated large deformation and recovery of the device (Fig. S6). At this moment, the piezoelectric device based on assembled t-Se nanowire layer can stably generate a voltage output equal to 0.45 V, which are already comparable to the output of a couple of previously reported 1D/2D materials (Table S1). Considering the stable voltage output and the unique radial distribution of piezoelectric polarization, we believe that the t-Se nanowire may open doors for the new piezoelectric and piezotronic devices design and integration.

Finally, we explore the feasibility of Se-PENG device for potential self-powered human-integrated applications, e.g., gesture recognition and cardiovascular monitoring. The wearable Se-PENG device can be attached to different parts of human body compliant with minimum

deformation. Fig. 3a shows the application of the Se-PENG device attached to the joint of a finger for detecting and recognizing the finger movement [47]. During the test, the finger was bent to different degrees, and the corresponding outputs were recorded. A larger bending angle gives rise to a stronger piezoelectric output (Fig. 3a). The Se-PENG device can also be attached to the throat for identifying different vocal activities, e.g., coughing, gargling, and swallowing (Fig. 3b). Furthermore, the Se-PENG device can be used to sense the radial artery pulses in real-time (Fig. 3c). The device was attached to the wrist of a healthy 24-year-old male for the non-invasive detection of pulse without using an external power source. The real-time piezoelectric current output from the device for 30 s shows the reliable detection and measurement of the human pulse signals, with distinct three-peak characteristics for the cardiac cycle (Fig. 3c). Such a pattern is consistent with the reported results [48,49] and manifests important information for the health diagnostics. Here we attempted to analyze the acquired signals. Three distinguishable determinants could be obtained from one typical pulse cycle [50–52]: namely, early systolic peak pressure ($P_1(t_1)$: percussion wave (P-wave)), late systolic augmentation shoulder ($P_2(t_2)$: tidal wave (T-wave)), and diastolic pulse waveform ($P_3(t_3)$: diastolic wave (D-wave)). These peaks can be used to quantify the augmentation index ($AI_r = P_2/P_1$) and the time delay between the first and second peaks ($\Delta t = t_2 - t_1$), which provide valuable information for evaluating the physiological conditions of the human cardiovascular system [52–54]. The calculated AI_r and Δt using Se-PENG are 0.57 and 0.26 s, respectively, which fall in a normal and healthy range [52–54]. The demonstrated self-powered sensing capability to detect the small-scale biomechanical signals from the human body, together with the facile and low-cost fabrication process, can potentially lead to broader applications of our devices for wearable self-powered biomedical devices.

3. Conclusion

In summary, Se nanowires synthesized by a hydrothermal method are explored as a new class of piezoelectric nanomaterial. The assembled Se nanowires by an LB approach are integrated into a wearable piezoelectric device for PENG application and sensing the small-scale biomechanical signals from the human body. A monolayer of assembled Se film can generate a V_{oc} and I_{sc} up to 0.45 V and 1.7 nA, respectively, when being subjected to a strain of 0.75%, with the maximum power density ~ 0.135 nW/cm². The performance and efficiency of such Se-PENG can be optimized by scaling up the number of the active Se layer through the integration of laminated devices. The Se-PENG demonstrated here shows great potential for self-powered biomedical devices, and opens doors to new technologies in energy, electronics, and sensor applications.

4. Methods

4.1. Synthesis of Se nanowires

The synthesis of Se nanowire follows procedures similar to previous report [55] with modified synthesis parameters to achieve a uniform dimension of the as-synthesized nanowires. Specifically, selenium dioxide (SeO₂), glucose (C₆H₁₂O₆), and poly(vinylpyrrolidone) (PVP, MW ≈ 55000) were dissolved in a mixture of deionized (DI) water and ethanol. After constant stirring for 20 mins, 5 mL ammonia (NH₃·H₂O, 69%) was added into the solution to adjust the pH value. The mixture solution was then transferred to a Teflon-lined autoclave and heated to 160 °C for 20 h. After the reaction, the product was collected by centrifugation and washed several times with DI water to remove the impurities. All the chemicals were purchased from Sigma-Aldrich and used as received.

4.2. Assembly of Se nanowires

After obtaining the centrifuged Se nanowires products, N, N-dimethylformamide (DMF) was added to disperse the Se nanowires and form a homogeneous solution. Chloroform (CHCl₃) was then added into the homogeneous solution, which was ready for the subsequent Langmuir-Blodgett (LB) assembly and transfer of Se nanowires onto the various substrates for further characterization.

4.3. Materials characterizations

Morphology and structural characterization of the as-synthesized Se nanowires was performed using a field emission scanning electron microscope (Hitachi S-4800) and a wide-angle X-ray diffractometer in the 20–70° range (Bruker, D8 Advance Diffractometer).

4.4. Fabrication and electric measurement of Se-PENG

Firstly, a thin layer of PDMS was spin-coated onto a PET substrate. After curing at 90 °C, the PDMS layer was treated with oxygen plasma for deriving a hydrophilic surface. Afterward, a layer of Ag nanowires network was spray-coated to function as the bottom electrode. Then, another layer of PDMS was deposited onto the Ag nanowire layer and cured. Subsequently, the Se nanowires layer was transferred onto the polymer stack through the above LB method. The second layer of PDMS was spin-coated onto the Se nanowires layer, then cured and treated with oxygen plasma before the deposition of the top Ag nanowires electrode. To complete the device fabrication, the uppermost PDMS layer was prepared with the same spin-coating method to encapsulate the whole device. The electrical outputs of the Se-PENG were measured using an electrometer (Keithley 6514) and a low-noise current pre-amplifier (Stanford Research Systems, SR570). A linear motor (LinMot) was used for applying strain to the device.

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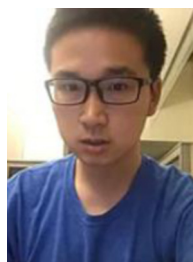
Appendix A. Supporting information

Supplementary data associated with this article can be found in the online version at doi:10.1016/j.nanoen.2018.12.003.

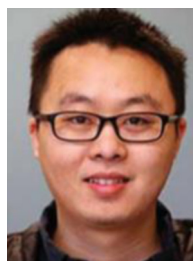
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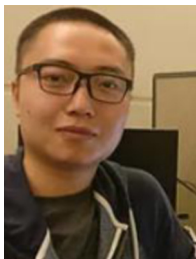
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