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pH-Response of polycation/Ti₃C₂T_x MXene layer-by-layer assemblies for use as resistive sensors†

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The importance and widespread need for accurate pH monitoring necessitates the fabrication of new pH sensors with high sensitivity that can be used in a variety of environments. However, typical pH sensors have certain limitations (e.g., glass electrodes are fragile and require consistent upkeep, colorimetric pH strips are single use and inaccurate). Herein, we examine the pH-response of multilayers consisting of Ti₃C₂T_x nanosheets and polycations fabricated using layer-by-layer (LbL) assembly. The MXene sheets themselves are pH-responsive due to their hydroxyl surface groups, and this effect may be amplified with the choice of an appropriate polycation. Specifically, the performance of multilayers assembled with the strong electrolyte poly (diallyldimethylammonium) (PDADMA) or pH-sensitive branched polyethylenimine (BPEI) is compared. As expected, the use of a pH-sensitive constituent leads to a 464% increase in pH sensitivity (116 kΩ pH⁻¹ unit vs. 25 kΩ pH⁻¹ unit) as compared to PDADMA. This is due to the conformational changes that BPEI undergoes with (de)protonation as pH changes. Further comparisons with reduced graphene oxide (rGO), which is far less pH responsive, confirm the unique pH responsivity of MXene nanosheets themselves. The ability to enhance response to particular stimuli by changing the constituent polycation demonstrates promise for future use of MXenes in resistive sensors for a variety of stimuli.

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Design, System, Application

MXenes, a family of two-dimensional metal carbides, have drawn increasing interest for use as sensors due to their metal-like conductivity and surface functional groups. In this work, we employed layer-by-layer (LbL) assembly to fabricate uniform polycation/MXene thin films with different polycations. We then exposed the fabricated films to environments of varying pH to determine the usable range and pH response of the films. This resulted in a pH range limited by the oxidative stability of the MXenes and a linear increase in resistance with pH over the usable range. By comparing thin films assembled with either a pH-insensitive or a pH-sensitive polycation, we were able to determine both the pH sensitivity of the MXene itself and the benefits of a pH-sensitive polycation. These results were further compared to similar films containing reduced graphene oxide instead of MXenes. This work demonstrates the ability to enhance sensitivity of MXene based films by using a pH sensitive polycation and generates promise for tailoring future LbL polycation/MXene sensors to specific analytes such as VOC's and biomolecules.

1. Introduction

The ability to measure and regulate pH is necessary for a variety of applications including soil and water quality control, wound healing, and pH-sensitive reaction media.^{1–5} Due to the wide range of environments in which pH sensing is required, a variety of pH sensor-types are needed. The two most commonly used methods of measuring pH values are

glass electrodes and single-use pH strips.⁶ However, these two methods both have shortcomings. The former is fragile and unreliable for highly basic or acidic solutions.⁷ Additionally, the sensitivity is limited by the Nernstian response (59.5 mV pH⁻¹) and is temperature sensitive by the same relationship.^{8,9} The latter, while easy to use, does not provide precise pH values as it relies on a colorimetric response.¹⁰ While new types of potentiometric sensors are still popularly explored as pH sensors, they share the temperature-dependent response of glass electrodes and are typically benchmarked by a Nernstian response, although some exceptions exist.^{11–15}

An alternative approach explored herein is resistive sensors. This sensor type relies on a change in electrical properties in response to environmental stimuli. As such,

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materials used in the fabrication of resistive sensors are ideally highly conductive and have functional surface groups that can interact with the surrounding environment. One such material that satisfies both requirements is $\text{Ti}_3\text{C}_2\text{T}_x$, a 2D-nanomaterial in the MXene family. As the most commonly used MXene to date, $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets have demonstrated a conductivity of $240\,000\text{ S m}^{-1}$ and have numerous hydroxyl surface groups.^{16,17}

MXenes with the chemical formula $\text{M}_{n+1}\text{X}_n\text{T}_z$ are obtained by the selective etching of the 'A' element from a MAX phase material, in which A is a group 13 or 14 transition metal, M is a transition metal, X is either carbon or nitrogen, T is a surface terminal group (e.g., $-\text{OH}$, $-\text{O}$, and $-\text{F}$), and n is 1, 2, or 3.^{18–20} MXenes have been used for a variety of applications including energy storage, catalysis, membrane separation, and sensing.^{21–34} These applications are possible due to the intercalation of ions between the 2D nanosheets, high conductivity, abundance of hydroxyl sites, and high surface to volume ratio.^{21,35–38}

However, a major drawback of MXenes is their proclivity to oxidation when exposed to water.^{39–42} Oxidation of $\text{Ti}_3\text{C}_2\text{T}_x$ to TiO_2 leads to noticeable degradation in conductivity, flocculation of the colloidal dispersion, and -ultimately- complete conversion to TiO_2 .^{39,40} This greatly impedes the shelf life of MXenes and their longevity in devices. Our team has demonstrated that anti-oxidants (e.g., sodium L-ascorbate (NaAsc)) mitigate the effects of oxidation for $\text{Ti}_3\text{C}_2\text{T}_x$.⁴³ Adding an antioxidant enables the retention of $\text{Ti}_3\text{C}_2\text{T}_x$ conductivity in MXene films for at least three weeks.⁴³ This considerable increase in shelf life enables the use of MXenes in different applications. The new-found stability motivates us to investigate the resistive pH-response of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets when assembled with various polycations into thin films.

The colloidal pH-response of MXenes in a dispersion has been explored, but the changes in electrical properties in response to pH have not been explored in depth.^{3,44–46} For example, Natu *et al.* reported on the acid- and base-induced crumpling of $\text{Ti}_3\text{C}_2\text{T}_x$.^{44,45} Natu *et al.* also demonstrated a pH dependence of both zeta potential and hydrodynamic size for $\text{Ti}_3\text{C}_2\text{T}_x$.⁴⁴ This is attributed to the (de)protonation of the hydroxyl surface groups of the MXene and creates promise for use of $\text{Ti}_3\text{C}_2\text{T}_x$ for pH sensing. Recently, drop-cast $\text{Ti}_3\text{C}_2\text{T}_x$ films and quantum dots have successfully been used to fabricate potentiometric and photoluminescent pH sensors, supporting the pH sensitivity of $\text{Ti}_3\text{C}_2\text{T}_x$.^{3,46}

Here, we explore the layer-by-layer (LbL) assembly of $\text{Ti}_3\text{C}_2\text{T}_x$ nanosheets with two different polycations and observe the resistive response of the resulting multilayers to aqueous solutions of various pH values. LbL assembly is selected as the processing method because it forms conformal coatings that have already demonstrated utility as strain and humidity sensors.^{25,26} This potentially allows for the fabrication of thin films on a variety of substrates including glass, polyethylene terephthalate (PET), polydimethylsiloxane (PDMS), fibers, and fabrics, regardless of topography.²⁶ Cai *et al.* recently showed the benefits of LbL assembly over direct mixing when fabricating thin films, in which ordered structures obtained using LbL assembly prevented restacking of MXene nanosheets and improved recoverability of the sensors.²⁴

Two polycations are explored in this work: poly(diallyldimethylammonium) (PDADMA) and branched polyethylenimine (BPEI). As PDADMA is a “strong” electrolyte, its linear charge density does not fluctuate with pH.⁴⁷ Therefore, it is assumed that the resulting resistive response of PDADMA/ $\text{Ti}_3\text{C}_2\text{T}_x$ assemblies is attributed solely to the MXene itself. We compare this to sensors containing BPEI, which is considered a pH-sensitive “weak” polyelectrolyte,¹⁵ instead of PDADMA. As demonstrated for polyaniline-based pH sensors, we expect that BPEI will contribute to pH sensitivity due to (de)protonation of its amine groups.⁴⁸ BPEI bears three amine groups, which each have unique pK_a values (4.5 for primary amine, 6.7 for secondary amine, and 11.6 for tertiary amine). In LbL assemblies (all-polymer, no MXenes), varying pH leads to conformational changes for BPEI, resulting in changes in the thin film thickness.^{49–51} This is due to chain elongation of BPEI at low pH, resulting in minimal contribution of the polymer to film thickness. The opposite occurs at high pH. For BPEI/ $\text{Ti}_3\text{C}_2\text{T}_x$ assemblies, we hypothesized that pH would influence both the MXenes (by changing the MXene surface chemistry) and the BPEI layers (by changing the chain conformation), manifesting in compounded changes in resistance. Finally, the results are compared to LbL assemblies containing reduced graphene oxide (rGO) in place of the MXene as a control. As rGO has fewer hydroxyl functional groups as compared to $\text{Ti}_3\text{C}_2\text{T}_x$ MXene, rGO is expected to have negligible influence on pH sensitivity. Ideally, comparing PDADMA/ $\text{Ti}_3\text{C}_2\text{T}_x$ and PDADMA/rGO



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assemblies will highlight the pH sensitivity of the MXene. On the other hand, comparing PDADMA/Ti₃C₂T_x and BPEI/Ti₃C₂T_x assemblies will demonstrate the added pH sensitivity of BPEI as compared to PDADMA.

2. Experimental

2.1 Materials

Titanium (Ti, 44 μm particle size, 99.5% purity), titanium carbide powders (TiC, 2–3 μm particle size, 99.5% purity), aluminium (Al, 44 μm particle size, 99.5% purity), hydroiodic acid (HI, 55%), lithium fluoride (LiF, >98% purity), and silver conductive adhesive paste (sheet resistance <0.025 $\Omega/\square$ at 0.001 in thick) were acquired from Alfa Aesar. Slide glass (75 $\times$ 25 $\times$ 1 mm), 5 MHz Ti/Au quartz crystal substrates, acetone (>99.5%), and isopropyl alcohol (IPA, 99% purity) were obtained from VWR. Poly(diallyldimethyl ammonium chloride) (PDADMAC, MW = 200 000 to 350 000 g mol⁻¹, 20 wt% in water), branched polyethyleneimine (BPEI, MW = 25 000 g mol⁻¹, MN = 10 000 g mol⁻¹), dimethyl sulfoxide (DMSO, ReagentPlus, >99.5%), hydrochloric acid (HCl, ACS reagent, 37% w/w), sodium hydroxide (NaOH), potassium permanganate (KMnO₄), sodium nitrate (NaNO₃), and sodium L-ascorbate (NaAsc) were purchased from Sigma-Aldrich. Type E polytetrafluoroethylene (PTFE) and 18 American Wire gauge (awg) 19 Strands (silver plated copper wire) were purchased from WesBell Electronics, Inc. Sulfuric acid (H₂SO₄, 95–98%), potassium hydroxide (KOH), and hydrogen peroxide (H₂O₂, 30%) were purchased from BDH. Graphite (SP-1) was purchased from Bay Carbon. Melinex ST505 (polyethylene terephthalate substrates) was purchased from Tekra. Si wafers were purchased from University Wafer. 18.2 M Ω cm (Milli-Q) water was obtained using a Milli-Q integral water purification system for Ultrapure Water. All materials were used as received.

2.2 Nanomaterial synthesis

Ti₃AlC₂ MAX powder and Ti₃C₂T_x were synthesized following a previously reported procedure.²⁶ The procedure is described in detail in the ESI† Ti₃C₂T_x dispersion concentration was determined by vacuum filtration of a known volume of dispersion. NaAsc dissolved in water was added to the dispersion to obtain a final concentration of 0.5 mg mL⁻¹ of Ti₃C₂T_x and 1 mg mL⁻¹ of NaAsc. Atomic force microscopy (Bruker Dimension Icon AFM) of drop-cast Ti₃C₂T_x verified the lateral size and thickness of a typical nanosheet (Fig. S1a and c†). A lateral size of 0.6 to 2.3 μm was observed along with a sheet thickness of 1 nm, which is in agreement with a single layer of Ti₃C₂T_x.⁵² From dynamic light scattering (DLS, Malvern Zetasizer Nano ZS), the hydrodynamic radius of Ti₃C₂T_x was measured to be 304 nm (Fig. S2a†). Zeta potential of the Ti₃C₂T_x dispersion was -46.1 mV (Fig. S2b†).

A batch of 0.5 mg mL⁻¹ GO dispersion was synthesized following previous reports and the modified Hummers' method, see ESI†^{53,54} This method resulted in nanosheets with a lateral size of 0.3 to 0.7 μm and a sheet thickness of

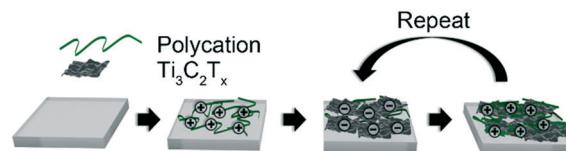


Fig. 1 Schematic of layer-by-layer assembly procedure used to make thin films. A substrate (gray) is alternately exposed to solutions and dispersion of polycation and Ti₃C₂T_x nanosheets, respectively. Each cycle constitutes a layer pair (LP), and the process was repeated until the desired number of LPs was attained.

0.9 nm (Fig. S1b and d†). While the nanosheet thicknesses of both nanomaterials were similar, there was visible aggregation of the GO nanosheets.

2.3 Sensor assembly

Polycation/Ti₃C₂T_x multilayers on slide glass, Si, PET, and quartz crystal substrates were prepared using LbL assembly following previous reports.^{25,26} Glass and PET substrates were cut to dimensions of 50 $\times$ 12.5 $\times$ 1 mm. Glass substrates were cleaned using bath sonication in IPA for 15 minutes followed by washes with acetone and water. PET, Si, and quartz crystal substrates were cleaned using water and IPA. Four lines of tape (1 mm $\times$ 20 mm) were placed on the PET substrates to create a U-shaped pathway. The cleaned substrates were then plasma treated (Harrick PDC-32G) for 3 minutes. As shown in Fig. 1, the plasma treated substrates were submerged in a 1 mg mL⁻¹ solution of the polycation, either pH 7.8 PDADMAC or pH 5 BPEI, for 15 minutes. PDADMA was used at its natural pH, and the pH of BPEI was adjusted using 0.05 M aliquots of HCl. The substrates were then submerged in Milli-Q water for 1 minute. This was repeated twice, and the substrates were then dried with compressed air. The substrates were then submerged in the 0.5 mg mL⁻¹ Ti₃C₂T_x dispersion for 15 minutes, followed by the same washing and drying steps. This constituted one layer pair (LP) and was repeated up to five times. Coated PET substrates were subsequently cut into four strips (0.31 cm $\times$ 2.5 cm). Silver-coated copper wires were placed at the opposite ends of the 'U' and attached using silver paste. The paste was then dried for 6 hours in a vacuum oven at room temperature to obtain the resistive sensors. The final path length of the sensor was 4.1 cm with a width of 0.11 cm. The coated surface area was about 0.58 cm².

Due to the hydrophilic nature and ease of processability of graphene oxide (GO), rGO-based multilayers were prepared by the chemical reduction of GO-based multilayers.⁵⁴ HI vapor was used to reduce GO-based multilayers following a previously reported procedure.⁵⁴ 1 mL of 55% HI (aq.) was added to a glass petri dish along with the GO-based multilayer. The petri dish was covered with a secondary petri dish to prevent loss of HI vapor and then heated for 8 minutes at 90 $^{\circ}\text{C}$. The reduced film was washed with ethanol and made into sensors as described previously.

Ti₃C₂T_x-only films were prepared by spray-coating onto PET substrates, combining the procedures of Zhao *et al.* and

De *et al.*^{54,55} A 0.5 mg mL⁻¹ dispersion of Ti₃C₂T_x was sprayed onto the substrate while maintaining a vertical distance of 15 cm and nozzle pressure of 80 psi. This continued for 8 minutes with constant movement (1 cm s⁻¹) over the substrate. The spray-coated substrate was then fabricated into sensors.

2.4 Characterization

X-ray powder diffraction (XRD, Bruker D8 powder X-ray diffractometer fitted with LynxEye detector), scanning electron microscopy (SEM, JEOL JSM-7500F), and X-ray photoelectron spectroscopy (XPS, Omicron XPS/UPS system with Argus detector) were used for characterization. Samples consisted of freeze-dried MXenes and LbL sensors before and after testing. Samples were dried under vacuum at room temperature for three days prior to XPS measurements to prevent outgassing and were then used as-is. AFM samples were prepared by drop casting dilute nanomaterial dispersions onto mica.

Growth profiles were obtained for all multilayers fabricated. Measurements for GO multilayers were taken prior to reduction. Film thickness and root mean square (RMS) roughness (R_q) were measured using profilometry (KLA Tencor D-100) for LbL films on glass substrates. Thickness was verified using ellipsometry (LSE Stokes Ellipsometer) for LbL films on Si substrates. Absorbance was measured using spectrophotometry (Shimadzu SolidSpec-3700 UV-vis-NIR) of LbL films on glass. A quartz crystal microbalance (QCM, MAXTEK RQCM Research) was used to measure film composition from coatings on 5 MHz Ti/Au quartz crystal substrates. Frequency was measured after every deposition, and mass deposited was calculated from the change in frequency using the Sauerbrey equation.⁵⁶

2.5 pH response testing

Once sensors were prepared, they were submerged in Milli-Q water for 24 hours to allow the multilayers to equilibrate. This time was increased to 120 hours for rGO-based

multilayers.⁵⁷ After swelling, the sensor was submerged in 150 mL of Milli-Q water. pH and resistance were recorded using a commercial pH probe (Beckman Model 350 pH/Temp/mV Meter) and a multimeter (Dawson DDM645, DC Voltage 1000 V), respectively. pH was adjusted from pH 3 to pH 7 using 0.05 M solutions of HCl and NaOH, and resistance was recorded *in situ* after a minimum of 10 minutes to allow the readings adequate time to equilibrate. The figure of merit, pH sensitivity, was calculated by two means: as the change in resistance over the change in pH (eqn (1)) or as the percent change in resistance over the change in pH (eqn (2)). Each equation normalizes the resistance against the resistance at pH 3.

All measurements were taken at room temperature.

$$\text{pH Sensitivity (k}\Omega \text{ pH}^{-1}) = \frac{(R - R_{0,\text{pH}3})}{(\text{pH} - 3)} \quad (1)$$

$$\text{pH Sensitivity (\% pH}^{-1}) = \frac{(R - R_{0,\text{pH}3})}{R_{0,\text{pH}3} \times (\text{pH} - 3)} \times 100\% \quad (2)$$

3. Results and discussion

3.1 MXene characterization

Fig. 2a shows XRD patterns of the parent MAX phase, Ti₃AlC₂, and the Ti₃C₂T_x nanosheets. Typical (002) MAX phase and (002) MXene peaks were observed at $2\theta \sim 10^\circ$ and $2\theta \sim 7^\circ$, respectively.⁴³ The decrease in the (002) peak angle was due to the larger interlayer spacing after the successful removal of Al from Ti₃AlC₂, which indicated successful etching. The SEM image in Fig. 2b displays the morphology of the nanosheets as opposed to the typical ‘accordion’ structure of Ti₃C₂T_x clay.⁵⁸ The small white dots on the sheet are TiO₂ which formed due to the minor oxidation of Ti₃C₂T_x during the synthesis and freeze-drying processes. Colloidal stability of the MXene and GO dispersions was verified by the Tyndall effect (Fig. 2c and d).

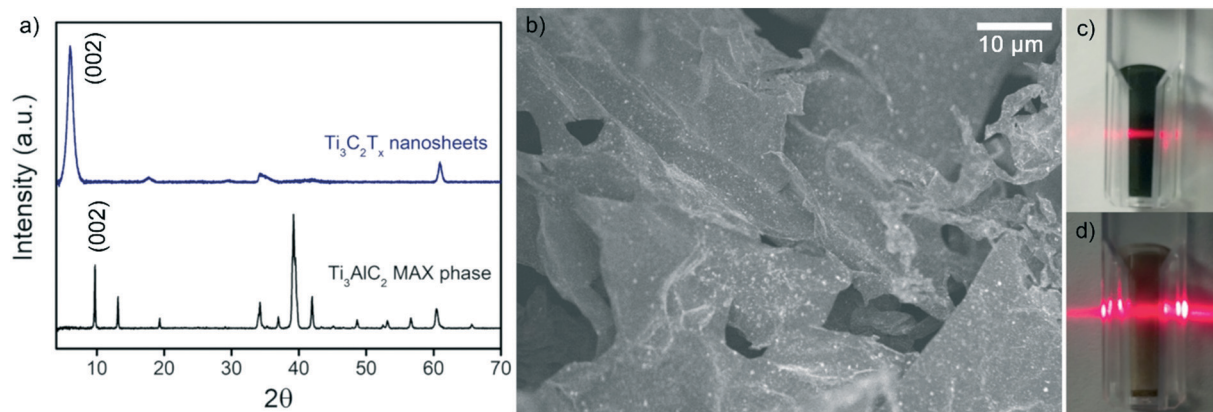


Fig. 2 (a) XRD of Ti₃C₂T_x nanosheets and Ti₃AlC₂ MAX phase. (b) SEM image of Ti₃C₂T_x nanosheets. Digital images of colloidal solutions of (c) Ti₃C₂T_x and (d) GO demonstrating the Tyndall effect.

XPS verified the composition of the $\text{Ti}_3\text{C}_2\text{T}_x$ MXenes. A survey scan (Fig. S3†) indicated the presence of the expected Ti 2p, C 1s, O 1s, and F 1s peaks associated with $\text{Ti}_3\text{C}_2\text{T}_x$. Peak fitting for each of these components is shown in Fig. S4,† and binding energy, atomic percent (at%), and full width half maximum (FWHM) are summarized in Table S1.† For Ti 2p, the Ti^{2+} (456.1 eV, 461.5 eV) and Ti^{3+} (457.9 eV, 463 eV) components correspond to the functional surface groups of the MXene ($-\text{OH}$, $-\text{O}$, and $-\text{F}$).^{43,59} The peaks at 455.2 and 460.3 eV correspond to Ti-C. Together, these peaks indicate the successful etching of the MAX phase into $\text{Ti}_3\text{C}_2\text{T}_x$. The C-OH peak (288.0 eV) of the C 1s spectra is present due to the interaction of NaAsc with the nanosheets, indicating the presence of NaAsc.⁴³ The TiO_2 peak (529.7 eV) of the O 1s spectra occurs due to the oxidation of $\text{Ti}_3\text{C}_2\text{T}_x$. The degree of oxidation is limited (11 at% of the Ti 2p spectra) and verifies the anti-oxidant properties of NaAsc, consistent with our previous findings.⁴³ The amount of oxidation of the native $\text{Ti}_3\text{C}_2\text{T}_x$ MXene will vary depending on storage time and conditions.

3.2 Layer-by-layer growth

Successful layer growth of the polycation/ $\text{Ti}_3\text{C}_2\text{T}_x$ multilayer was verified by thickness and absorbance observations. As more layer pairs (LPs) were successfully deposited, the thickness and absorbance of the multilayers underwent a linear increase. This was first verified using profilometry to measure thickness and roughness of the multilayers from one to five LPs on glass substrates (Fig. 3a). $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ films grew as 8.8 nm per LP, whereas $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ films grew as 4.2 nm per LP. (The subscript “y” indicates the number of LPs.) From the

observed MXene sheet thickness from AFM, approximately 9 and 4 sheets were deposited per LP for sensors with PDADMA and BPEI, respectively, excluding the polyelectrolyte contribution.⁵² The profilometric root-mean-square film roughness (R_q) was measured as well (Fig. 3b). The R_q values (~ 20 nm for MXene multilayers containing PDADMA and ~ 10 nm for MXene multilayers containing BPEI) indicate successful assembly of relatively smooth thin films.

The linear growth was verified using ellipsometry on silicon substrates (Fig. S5a†). Despite lower growth rates as compared to profilometry measurements (3.1 nm per LP from ellipsometry vs. 8.8 nm per LP from profilometry in the case of $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ multilayers), the linear growth profile of the films was confirmed. The difference in the magnitude of layer growth can be attributed to the indirect measurement method of ellipsometry and the interference of the MXene with the polarized light source.

Linear growth was additionally verified using spectrophotometry on coated glass substrates (Fig. 3c and S6a and b†). Digital images of the multilayers are shown in Fig. 3d and e. The absorbance of note was taken at 770 nm following previous reports.²⁵ Absorbance of the films at 770 nm grew as 0.04 a.u. per LP for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ films and 0.01 a.u. per LP for $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ films. Subsequently, the linear increase in absorbance was then correlated with the thickness to create an empirical relationship between the two. This enabled later thickness measurements for substrates on which profilometry was not possible (*e.g.*, PET substrates). QCM measurements on the Ti/Au quartz crystal were used to determine the mass composition of the polycation/ $\text{Ti}_3\text{C}_2\text{T}_x$ multilayers (Fig. S5c†). From this, a mass composition of 5.5% PDADMA and 94.5% $\text{Ti}_3\text{C}_2\text{T}_x$ was calculated for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ multilayers. $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ multilayers were determined to consist of 9.3 wt% BPEI and 90.7 wt% $\text{Ti}_3\text{C}_2\text{T}_x$. In both cases, $\text{Ti}_3\text{C}_2\text{T}_x$ dominates the growth of the film, verifying the assumption that layer growth can be primarily attributed to the MXene sheets.

3.3 pH response

Sensors utilized assemblies of 5 LPs, corresponding to a sensor thicknesses of 44 nm for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ and 19

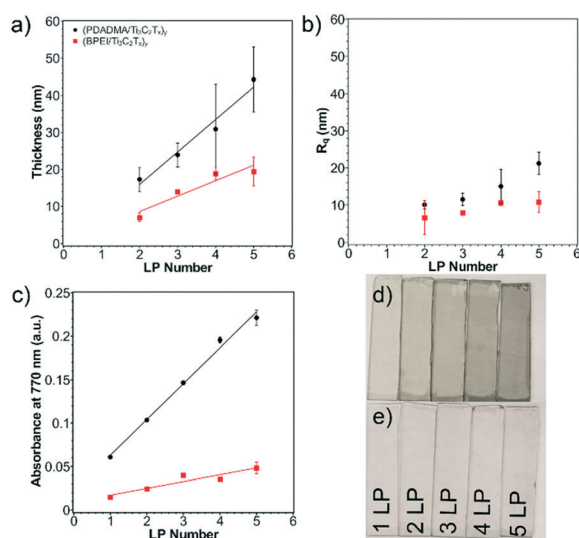


Fig. 3 (a) Profilometric thickness, (b) profilometric roughness, and (c) UV-vis absorbance at 770 nm of $\text{Ti}_3\text{C}_2\text{T}_x$ multilayers. Thickness grew as 8.8 nm per LP and 4.2 nm per LP for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ and $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$, respectively. Absorbance at 770 nm grew as 0.04 a.u. per LP and 0.01 a.u. per LP for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ and $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$, respectively. Digital images of (d) $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ and (e) $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_y$ multilayers.

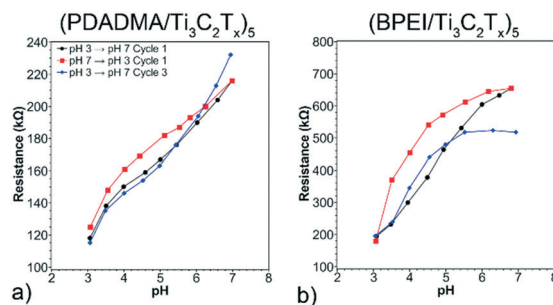


Fig. 4 pH Response of (a) $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ and (b) $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensors. The pH sensitivity was $24.8 \pm 2.6 \text{ k}\Omega \text{ pH}^{-1}$ for (a). The pH sensitivity was $115.7 \pm 20.8 \text{ k}\Omega \text{ pH}^{-1}$ for (b).

nm for $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$. 5 LP films were chosen to ensure lateral percolation of $\text{Ti}_3\text{C}_2\text{T}_x$. Kim *et al.* recently demonstrated that thinner films resulted in enhanced sensor performance.³¹ As such, films above 5 LP were not considered. Additionally, there is a trade-off between fabrication time and LP number that resulted in thicker films being impractical.

To determine the viable range for pH response testing, a wide pH range (3–10) was first examined (Fig. S7a†). There was a drastic increase in resistance as the $\text{Ti}_3\text{C}_2\text{T}_x$ multilayers were exposed to basic conditions. The increase is attributed to the rapid oxidation of $\text{Ti}_3\text{C}_2\text{T}_x$, which resulted in a noticeable color change upon exposure to basic conditions (pH ~10) for 24 hours (Fig. S7c†). While this may seem an extended period, all films were exposed to a neutral environment (Milli-Q water) for 24 hours prior to testing to allow for swelling of the multilayers and did not undergo any notable color change. Given the increased rate of oxidation in basic environments, the pH range tested was restricted to pH 3 to pH 7.

Sensor performance was quantified by the pH sensitivity. A representative $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensor was tested first to determine the contribution of $\text{Ti}_3\text{C}_2\text{T}_x$ to the pH response (Fig. 4a). The initial resistance of the film when exposed to pH 3 was 118 k Ω . As pH increased from 3 to 7, the resistance increased as 23 k Ω pH⁻¹ (19.4 % pH⁻¹). When decreasing pH back to pH 3, there was slight hysteresis – a typical observation for resistive sensors.⁷ Due to the hysteresis, the cycles were split based on whether pH was increasing or decreasing to determine repeatability (*e.g.*, pH 3 → pH 7 and pH 7 → pH 3). While the sensitivity increases to 28 k Ω pH⁻¹ by the third cycle, there is good overlap in response for pH 3 → pH 7 in Cycles 1 and 3. Using a 95% confidence interval, the sensitivity of the film was determined to be 24.8 ± 2.6 k Ω pH⁻¹. Profilometric thickness was measured before and after pH response tests to determine recoverability of thickness. Thickness changed from 40.6 ± 10.9 nm to 43.7 ± 9.6 nm, suggesting the reversibility of the response.

A representative $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensor was then examined to determine if a pH sensitive polycation would enhance sensitivity. The initial resistance of this film at pH 3 was 194 k Ω . The higher value of initial resistance as compared to $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensors is likely due to differences in thicknesses of the two films. Resistance is inversely proportional to thickness. As with the previous sensors, there was noticeable hysteresis when comparing response curves for increasing and decreasing pH. In this case, the initial pH sensitivity pH 3 → 7 was 132 k Ω pH⁻¹ (68.1% pH⁻¹), increasing to 141 k Ω pH⁻¹ by the third cycle. This pH sensitivity is five times higher as compared to that of $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensors due to the further thickness changes caused by conformational changes of BPEI with pH. Additionally, the overlap for pH 3 → pH 7 in Cycles 1 and 3 is comparable to that for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$. This indicates cyclability of the sensors up to three cycles in both cases. Using a 95% confidence interval, the sensitivity of the film

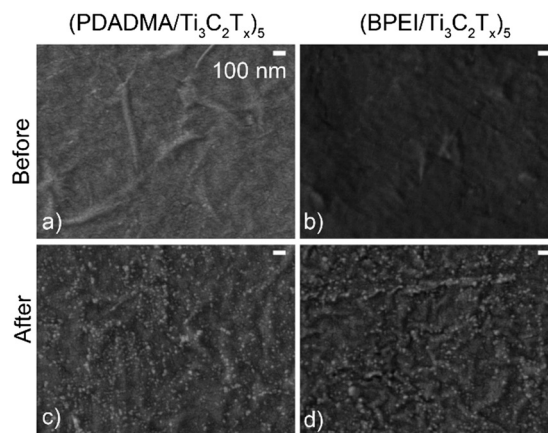


Fig. 5 SEM images of (a and c) $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ and (b and d) $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ films before (a and b) and after (c and d) pH response tests. The scale bar in (a) applies to the other panels as well.

was determined to be 115.7 ± 20.8 k Ω pH⁻¹. As with the previous sensor composition, profilometric thickness was measured before and after pH response testing. In this case, thickness changed from 22.7 ± 8.8 nm to 20.3 ± 2.9 nm, which indicates the reversibility of the response.

Given the proclivity of $\text{Ti}_3\text{C}_2\text{T}_x$ to oxidize, SEM and XPS were used to characterize the sensors before and after pH response testing to determine the extent of oxidation. Oxidation of the films was first demonstrated using SEM as there was noticeable TiO_2 on the surface of the sensors after pH response testing (Fig. 5c and d) that was not present on as-prepared sensors (Fig. 5a and b).

XPS survey scans (Fig. S8†) confirmed the presence of Ti 2p, C 1s, O 1s, and F 1s before and after pH response tests. Formation of TiO_2 was verified by peak fitting of the Ti 2p

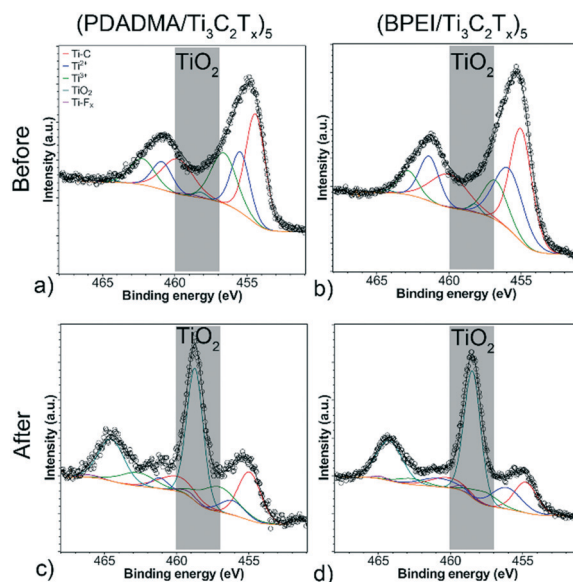


Fig. 6 Deconvoluted Ti 2p XPS spectra of (a and c) $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ and (b and d) $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ before (a and b) and after (c and d) pH response tests.

XPS spectra for both sensors before and after testing (Fig. 6). For both sensor compositions, there is a notable peak that forms at 458.7 eV, which is indicative of considerable oxidation (~1% to ~50% TiO₂ component at% of the Ti 2p spectra). Deconvolution of the other components (Fig. S9 and S10†) supports the claim that oxidation occurred. For C 1s, there is a notable decrease in the C–Ti–T_x component peaks. For F 1s, the C–Ti–F_x peak becomes noticeably smaller and much closer in area to the AlF_x peak. All XPS peak fitting results for the sensors are presented in Tables S2–S5† along with the full width half maximums (FWHM) and component at%. This oxidation likely contributed to resistance drift in the sensors from cycle to cycle.

The response for (PDADMA/Ti₃C₂T_x)₅ sensors is attributed to (de)protonation of the hydroxyl surface groups of Ti₃C₂T_x. Due to changes in the net surface charge of the Ti₃C₂T_x nanosheets and the changes in the degree of protonation of the hydroxyl surface groups, the magnitude of electrostatic attraction/repulsion and the available number of charge carrier sites will vary, causing the observed changes in resistance. This mechanism is similar to that of graphene where H₃O⁺ and OH[−] adsorb to surface sites.⁷ Recently, Natu *et al.* showed a linear decrease in zeta potential with pH over the pH range 2 to 7.⁴⁴ The linear change in zeta potential supports the moderately linear pH response we observed and is in line with the proposed mechanism.

The increase in sensitivity for (BPEI/Ti₃C₂T_x)₅ sensors is attributed to BPEI conformational changes with pH. Unlike PDADMA, BPEI is highly pH sensitive. As the exposure pH increases above the pK_a values of BPEI, the degree of protonation of the amine groups will decrease, leading to decreased electrostatic repulsion. In sum, this results in a more coil-like conformation for BPEI chains at more basic pH values.⁶⁰ We speculate that this will cause the distance between nanosheets to increase, causing the observed increase in resistance.²⁵ This compounds with the resistance changes incurred by the Ti₃C₂T_x nanosheets, leading to the enhanced sensitivity.

The performance of sensors assembled with Ti₃C₂T_x without the treatment of NaAsc was evaluated to determine the effect of the added antioxidant (Fig. S11†). The pH responsivity for the first cycle was 72 kΩ pH^{−1} for (PDADMA/Ti₃C₂T_x)₅ and 120 kΩ pH^{−1} for (BPEI/Ti₃C₂T_x)₅ when Ti₃C₂T_x was not treated with NaAsc. While the pH sensitivity of the untreated (PDADMA/Ti₃C₂T_x)₅ sensor was higher than that of the treated (PDADMA/Ti₃C₂T_x)₅ sensor, the initial resistance was significantly higher (almost double) and the cyclability from pH 3 → pH 7 for cycle 1 to cycle 3 was considerably worse. In the case of untreated (BPEI/Ti₃C₂T_x)₅, the pH sensitivity was similar to that of treated (BPEI/Ti₃C₂T_x)₅. However, the initial resistance was an order of magnitude higher, and cyclability issues were also apparent.

The higher initial resistances of sensors assembled without the NaAsc treatment are attributed to oxidation of the untreated sensors prior to testing and during equilibration. The poor cyclability issues are likely caused by

accelerated oxidation during testing, in which there was no residual NaAsc within the film. This leads to the conclusion that NaAsc can mitigate oxidation of the sensors (but not completely) and that Ti₃C₂T_x sensors treated with an antioxidant such as NaAsc are preferred.

Pure Ti₃C₂T_x sensors were assembled as a comparison as well. These were prepared by spraying a Ti₃C₂T_x dispersion onto PET to yield a film 98 nm thick. However, these sensors exhibited poor surface adhesion, similar to issues previously observed for pure Ti₃C₂T_x films.²⁶ Due to the poor adhesion, spray-assembled sensors of pure Ti₃C₂T_x nanosheets were not tested further.

3.4 Comparison to rGO-based multilayers

Due to its similar dimensions and high conductivity, rGO-based multilayers were used as a comparison against the Ti₃C₂T_x-based multilayers. rGO films were prepared using GO followed by chemical reduction. (PDADMA/GO)₅ and (BPEI/GO)₅ films had thicknesses of 620 nm and 670 nm respectively (Fig. S12†). The obtained thicknesses and roughnesses were considerably higher than that of their Ti₃C₂T_x counterparts. This is due to the aggregation of GO nanosheets leading to more nanosheets being deposited per LP in a less uniform manner (Fig. S1b†).

To compare against Ti₃C₂T_x-based sensors, rGO-based sensors were tested over the same pH range (Fig. S13†). The initial resistance of these sensors was an order of magnitude lower than that of the Ti₃C₂T_x counterparts, which we attributed to the higher thicknesses of the rGO-based sensors. As with Ti₃C₂T_x-based multilayer sensors, there was noticeable hysteresis when comparing cycles in which pH increased *vs.* decreased. For (BPEI/rGO) sensors, there were noticeable noise issues with the first cycle. As the noise issues were resolved by the second cycle, the first cycle was discarded and all other cycles were renumbered.

Table 1 pH sensitivity and range of various resistive pH sensors

Material	pH sensitivity	pH range	Reference
SWNT–PANI/PVA	20 kΩ cm ^{−2} pH ^{−1}	1–10	62
<i>p</i> -SWNT–PSS/PANI	4.56 kΩ cm ^{−2} pH ^{−1} acidic region 20.66 kΩ cm ^{−2} pH ^{−1} basic region	0.95–12	61
Graphene	2 kΩ pH ^{−1}	4–10	63
MWNT	65 Ω pH ^{−1}	5–9	64
ES–PANI/PVB	0.28 MΩ pH ^{−1}	1–8	65
Pd	5% pH ^{−1}	4–10	66
MWCNT/Ni	1% pH ^{−1}	2–10	67
(PDADMA/rGO) ₅	0.6 kΩ pH ^{−1}	3–7	This work
(BPEI/rGO) ₅	0.6 kΩ pH ^{−1}	3–7	This work
(PDADMA/Ti ₃ C ₂ T _x) ₅	23 kΩ pH ^{−1} 40 kΩ cm ^{−2} pH ^{−1} 19.4% pH ^{−1}	3–7	This work
(BPEI/Ti ₃ C ₂ T _x) ₅	132 kΩ pH ^{−1} 228 kΩ cm ^{−2} pH ^{−1} 68.1% pH ^{−1}	3–7	This work

The overall responses of both types of rGO-based sensors were nonlinear and exhibited a significantly lower resistance change ($<3\text{ k}\Omega$) over the entire tested pH range. Assuming a linear response (despite the obvious nonlinearity), the pH sensitivity of both rGO-based sensors was estimated as $0.6\text{ k}\Omega\text{ pH}^{-1}$. This was significantly lower than that of $\text{Ti}_3\text{C}_2\text{T}_x$ -based sensors, but still in line with the expectation that $\text{Ti}_3\text{C}_2\text{T}_x$ would be more pH-sensitive as compared to rGO because $\text{Ti}_3\text{C}_2\text{T}_x$ has significantly more hydroxyl functional groups.

3.5 Comparison to resistive sensors in literature

We compare our $\text{Ti}_3\text{C}_2\text{T}_x$ -based pH sensors to other resistive sensors in the literature (Table 1). To allow for comparison to all tabulated sensors, we also normalized the pH sensitivity for the $\text{Ti}_3\text{C}_2\text{T}_x$ -based sensors by surface area (eqn (3)).

$$\text{pH Sensitivity (k}\Omega\text{ pH}^{-1}\text{ cm}^{-2}) = \frac{(R - R_{0,\text{pH}3})}{A_s \times (\text{pH} - 3)} \quad (3)$$

There is variation in the literature on how pH sensitivity is reported, so we report our values here in these three ways (eqn (1)–(3)). pH sensitivities for $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ were $28\text{ k}\Omega\text{ pH}^{-1}$, $44\text{ k}\Omega\text{ pH}^{-1}\text{ cm}^{-2}$, and $19.4\%\text{ pH}^{-1}$. pH sensitivities for $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ are $132\text{ k}\Omega\text{ pH}^{-1}$, $228\text{ k}\Omega\text{ pH}^{-1}\text{ cm}^{-2}$, and $68.1\%\text{ pH}^{-1}$. As compared to the other resistive sensors,^{61–67} the pH range of our $\text{Ti}_3\text{C}_2\text{T}_x$ -based LbL sensors is generally narrower and restricted to acidic conditions. This is due to the hastened oxidation of $\text{Ti}_3\text{C}_2\text{T}_x$ in basic environments.

Despite their smaller pH range, $\text{Ti}_3\text{C}_2\text{T}_x$ -based LbL sensors exhibit considerably higher pH sensitivities as compared to other resistive sensors.^{61–64,66,67} As compared to single-walled carbon nanotube composites, the pH sensitivity is an order of magnitude higher.^{61,62} Both $(\text{PDADMA}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ and $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ outperformed graphene-based sensors by one and two orders of magnitude, respectively.⁶³ While the ES-PANI/PVB sensor had a higher reported sensitivity, the response was logarithmic and the same order of magnitude as $(\text{BPEI}/\text{Ti}_3\text{C}_2\text{T}_x)_5$ sensors.⁵⁹ Due to the logarithmic response, the actual sensitivity varies depending on what pH range the sensitivity is calculated over. As such, it is difficult to directly compare. We attribute our higher pH sensitivities to the abundance of surface functional groups on $\text{Ti}_3\text{C}_2\text{T}_x$ and to the use of a pH-sensitive polymer.^{17,68,69} The proposed mechanism of pH sensitivity of graphene and other graphenic based sensors relies on interaction of the surface of graphene with OH^- and H_3O^+ ions.⁷ As such, if there are more surface sites to interact with these ions, it is expected that the pH sensitivity will be higher. Cai *et al.* also demonstrated the benefits of the LbL structure on resistive sensor performance as compared to sensors with randomly oriented structures.²⁴ As such, it is expected that sensors fabricated using LbL assembly will exhibit higher sensitivities than those assembled using less ordered assembly methods.^{63,64,66,67}

4. Conclusions

LbL assembly was used to fabricate highly pH sensitive $\text{Ti}_3\text{C}_2\text{T}_x$ -based resistive sensors. This assembly method allowed for controlled and linear growth of sensors with low thicknesses and roughnesses, as well as improved surface adhesion at low polymer loadings ($<10\%$). Due to possible increases in spacing between nanosheets with increasing pH, an increase in intersheet resistance occurs, which may lead to the observed pH sensitivity of the MXene based films.^{25,70} The resulting resistive sensors demonstrated pH sensitivities higher than that of LbL rGO-based sensors and other resistive sensors in literature in the pH 3–pH 7 range due to the high pH sensitivity of $\text{Ti}_3\text{C}_2\text{T}_x$. The ability to enhance pH sensitivity by using a pH-sensitive polymer such as BPEI demonstrated the possibility of tuning $\text{Ti}_3\text{C}_2\text{T}_x$ -based multilayers for specific applications by changing the constituent polycation. This creates promise for the application of MXene multilayers in sensing a variety of analytes. However, there are still noticeable issues with oxidation, despite the improvements associated with inclusion of an antioxidant, that we aim to mitigate in future work. This issue limited the overall cyclability of the sensor, but might be mitigated in the future using a stronger small molecule antioxidant or a polymer that prevents oxidation.

Conflicts of interest

There are no conflicts to declare.

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