



Application of Laser Microirradiation in the Investigations of Cellular Responses to DNA Damage

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OPEN ACCESS

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equally to this work

Specialty section:

This article was submitted to
Optics and Photonics,
a section of the journal
Frontiers in Physics

Received: 22 August 2020

Accepted: 30 November 2020

Published: 25 January 2021

Citation:

Kong X, Wakida NM and Yokomori K
(2021) Application of Laser
Microirradiation in the Investigations of
Cellular Responses to DNA Damage.
Front. Phys. 8:597866.
doi: 10.3389/fphy.2020.597866

Since the laser has been invented it has been highly instrumental in ablating different parts of the cell to test their functionality. Through induction of damage in a defined sub-micron region in the cell nucleus, laser microirradiation technique is now established as a powerful real-time and high-resolution methodology to investigate mechanisms of DNA damage response and repair, the fundamental cellular processes for the maintenance of genomic integrity, in mammalian cells. However, irradiation conditions dictate the amounts, types and complexity of DNA damage, leading to different damage signaling responses. Thus, in order to properly interpret the results, it is important to understand the features of laser-induced DNA damage. In this review, we describe different types of DNA damage induced by the use of different laser systems and parameters, and discuss the mechanisms of DNA damage induction. We further summarize recent advances in the application of laser microirradiation to study spatiotemporal dynamics of cellular responses to DNA damage, including factor recruitment, chromatin modulation at damage sites as well as more global damage signaling. Finally, possible future application of laser microirradiation to gain further understanding of DNA damage response will be discussed.

Keywords: laser microirradiation, DNA damage response, PARP1, complex DNA damage, chromatin, metabolism

HISTORY OF APPLICATION OF LASER MICROIRRADIATION IN BIOLOGY

The application of the microbeam to cell microscopy provided a means for scientists to noninvasively remove subcellular material from living cells. Bessis was the first to modify a part of the cell with this technique by targeting the mitochondria [1]. This provided the foundation for a valuable tool used to mechanically damage subcellular structures without the worry of contamination or membrane rupture inherent with conventional micromanipulation techniques.

The first improvement of micromanipulation of cells with light was a shift in light sources, from the use of ultraviolet (UV) microbeams to classic laser sources. In 1969, Berns and colleagues utilized an argon laser microbeam to successfully irradiate preselected sites on chromosomes [2] and nucleoli [3] sensitized with acridine orange. The intense, coherent nature of the laser resulted in a powerful, focused tool that successfully ablated submicron regions of condensed chromosomes.

Advancement of laser technology provided access to lasers that could provide focal spots with higher energy density. With the development of the Q switched Nd:YAG laser, sensitization of cells was not necessary to successfully irradiate chromosomes [4]. Strahs and Berns then demonstrated via transmission electron microscopy analysis that damage with the Nd:YAG laser at three different wavelengths was identical to damage produced by UV irradiation at 280 nm. Comparison of

ultrastructure damage showed that laser ablation of biomolecules was not restricted to specific molecules [5]. Elimination of the need for sensitizing agents was important as their binding to DNA would alter chromatin configuration and skew DNA damage response (DDR).

Short pulsed Nd:YAG lasers with nanosecond pulse durations became a popular and versatile laser source for inducing DNA damage [6–8]. Recently, laser technology has progressed with decreases in pulse duration. Currently the most common laser utilized in the field is the Ti:Sapphire near-infrared (NIR) laser with femtosecond pulse duration [9–14]. König et al described NIR femtosecond laser damage to chromosomes at lower thresholds (not causing membrane rupture) controlled to sub-femtoliter volume and caused by optical breakdown and plasma formation [9]. The most common wavelength used in recent studies vary between 780–800 nm, due to the efficiency of femtosecond pulse width Ti:Sapphire laser and the confinement of the DNA lesion. A comprehensive review by Gassman and Wilson discussed studies using different laser sources (UV, visible, and NIR) both with and without sensitizers [15].

The development of confocal imaging systems brought new potential, where ingenuity of scientists changed the function of imaging lasers to selectively damage nuclear regions by increasing the output power of the lasers. Recently, Gaudreau-Lapierre et al. [16] describes the methodology behind the use of a laser scanning confocal microscope to irradiate regions within the nucleus using the fluorescence-recovery after photobleaching module common with commercially available software for confocal microscopes. Studies utilizing confocal systems to induce DNA damage allowed tracking of the DDR response in 4 dimensions, conventional 3 dimensions (as optical laser can be focused to a specific spot, see below) and the temporal response [16, 17]. Ultraviolet A (UVA) laser wavelength (355–365 nm) is also commonly used for DNA damage induction, including confocal microscope sources [18–21]. The mechanism of DNA damage by UVA laser sources is considered to result from single-photon absorption [22].

Use of lasers to activate compounds is a technique that has grown in recent popularity. Photodynamic therapy in the past has utilized photosensitizers, activated by lasers as clinical treatment for cancer and other diseases. A recent example in this field by Lan et al utilizes the Killer red compound to generate ROS-induced DNA damage at specific sites combining with artificially changing the chromatin states (open and closed) [23]. Yanuk et al. continues the search for photosensitizers with three chlorophyll derivatives for photo inducible DNA damage including one that cleanly induces single strand breaks [24]. Efforts to develop tools that can induce specific types of DNA damage with spatiotemporal control continue in the field.

LASER DAMAGE MECHANISMS

Laser ablation utilizes energy from photons of light interacting with biomolecules within the targeted cellular structure. A large population of photons of high energy focused to a small beam

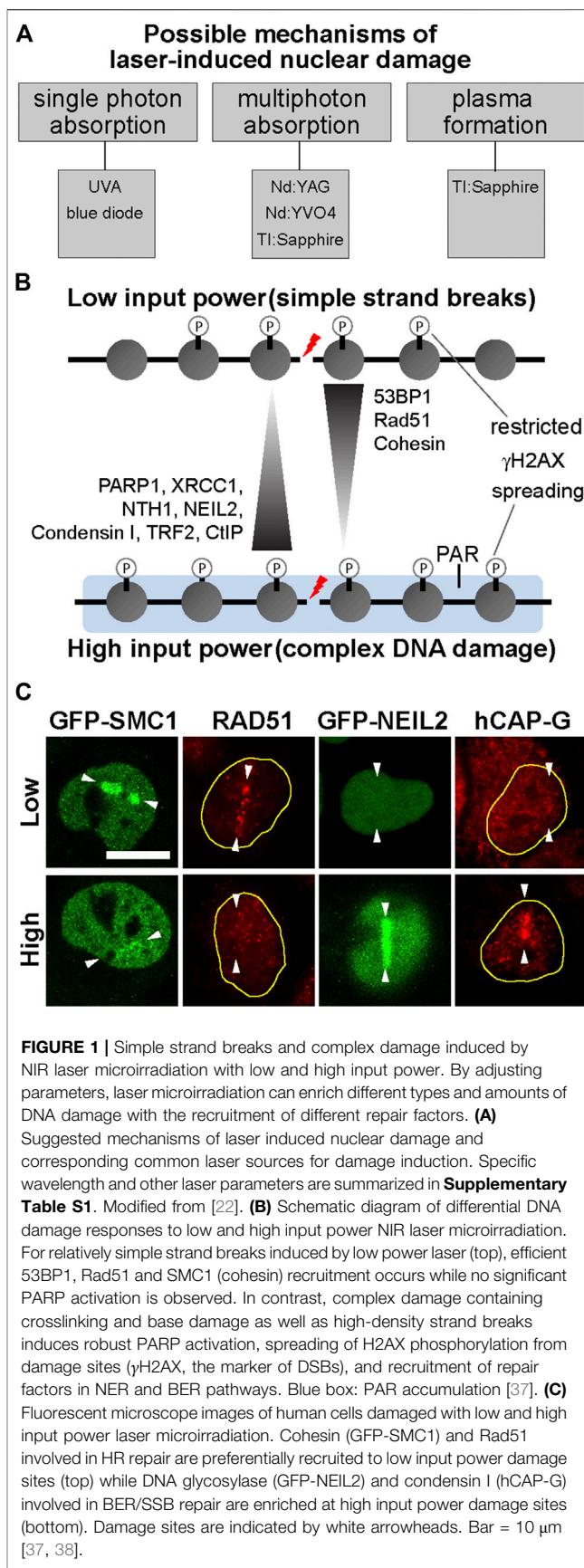


FIGURE 1 | Simple strand breaks and complex damage induced by NIR laser microirradiation with low and high input power. By adjusting parameters, laser microirradiation can enrich different types and amounts of DNA damage with the recruitment of different repair factors. **(A)** Suggested mechanisms of laser induced nuclear damage and corresponding common laser sources for damage induction. Specific wavelength and other laser parameters are summarized in **Supplementary Table S1**. Modified from [22]. **(B)** Schematic diagram of differential DNA damage responses to low and high input power NIR laser microirradiation. For relatively simple strand breaks induced by low power laser (top), efficient 53BP1, Rad51 and SMC1 (cohesin) recruitment occurs while no significant PARP activation is observed. In contrast, complex damage containing crosslinking and base damage as well as high-density strand breaks induces robust PARP activation, spreading of H2AX phosphorylation from damage sites (γ H2AX, the marker of DSBs), and recruitment of repair factors in NER and BER pathways. Blue box: PAR accumulation [37]. **(C)** Fluorescent microscope images of human cells damaged with low and high input power laser microirradiation. Cohesin (GFP-SMC1) and Rad51 involved in HR repair are preferentially recruited to low input power damage sites (top) while DNA glycosylase (GFP-NEIL2) and condensin I (hCAP-G) involved in BER/SSB repair are enriched at high input power damage sites (bottom). Damage sites are indicated by white arrowheads. Bar = 10 μ m [37, 38].

diameter result in consistent, and targeted regions of damage. Laser induced damage is affected by laser parameters including energy level, pulse duration, number of pulses delivered, and wavelength. Additionally, variation in the physical mechanism of light interaction with biological molecules is also dependent on the laser manufacturer, as well as optimal focusing of the beam through the optical path. The diameter of the induced damage can be controlled to a diffraction-limited spot size defined by $1.22 \lambda/NA$. Damage area can be further extended by repositioning the beam to multiple locations, which in some software is referred to as “zoom factor”.

The combination of laser parameters used dictates the types of DNA damage induced by the laser. We previously utilized multiple laser sources and parameters, such as wavelength, peak irradiance, input power, pulse frequency and duration of exposure, to induce DNA damage, and systematically analyzed the resulting DNA damage by immunofluorescent detection of crosslinking and base damage, recruitment and modification of DDR and pathway-specific repair factors [22]. We proposed four potential mechanisms of laser-induced DNA damage: (i) temperature rise produced by linear or two photon absorption; (ii) generation of large thermo-elastic stresses; (iii) various photochemical processes by linear or two photon absorption including DNA cross-linking damage and production of free radicals and reactive oxygen species; and (iv) optical breakdown (plasma formation) produced by a combination of multiphoton and cascade ionization processes, leading to thermal, mechanical and chemical damage (Figure 1A) [22].

Many studies support the mechanism of multiphoton processes when inducing nuclear damage with short-pulsed lasers. Göppert-Mayer first defined the nonlinear absorption mechanism, which allows DNA and other molecules to absorb multiple photons of lower energy resulting in effects similar to the absorption of a single photon of higher energy [25]. Early studies by Calmettes and Berns demonstrated the phase “paling” of chromosomes and nucleoli suggests this observation was a result of multiphoton processes by 532 nm laser photons and two-photon processes for 266 nm UV light [26]. Phase paling as observed with these multiphoton mechanisms are similar to those resulting from Ti:Sapphire NIR lasers with femtosecond pulse widths [13]. Damage mechanisms of NIR are based on low density plasma formation, and well defined by Vogel and Venugopalan [27, 28]. Damage mechanisms of continuous wave (CW) lasers like the blue diode lasers commonly utilized with confocal imaging systems are based on linear absorption, similar to longer pulse width UV lasers [28].

INDUCTION AND DETECTION OF DIFFERENT TYPES OF DNA DAMAGE AND FACTOR RECRUITMENT

Living cells experience various types of DNA damage that may lead to gene mutations if not corrected. Correspondingly, multiple DNA damage signaling and repair pathways are activated by the damage to maintain genome stability. Photoproducts such as pyrimidine-pyrimidone (6-4)

photoproducts (6-4PPs) and cyclobutane pyrimidine dimers (CPDs) caused by UV light are repaired by the nucleotide excision repair (NER) pathway. Base damage, such as oxidation damage 8-oxoguanine (8-oxoG), is repaired via the base excision repair (BER) pathway. DNA double-strand breaks (DSBs) can be repaired by two major pathways, homologous recombination (HR), non-homologous end joining (NHEJ), or alternative/back-up pathways, such as single-strand annealing (SSA) pathway [29]. DNA single-strand breaks (SSB) repair is also the downstream step of BER [30], since base damage is processed by DNA glycosylases and AP endonuclease into a SSB intermediate [22, 31].

As described above, laser microirradiation became a powerful tool to analyze DNA repair *in vivo* at a single cell resolution. The use of laser ablation with cells expressing fluorescently-tagged DNA repair-related proteins make it possible to study the association and dissociation of repair factors at DNA damage sites with high spatial resolution and tight temporal control. A laser source integrated into a confocal microscope equipped with an incubator for temperature and CO₂ control allows time-course analyses of DDR in real time. With advanced fluorescence imaging techniques, it is also possible to investigate cellular responses beyond the repair protein accumulation at damage sites, such as chromatin structural changes and metabolic changes in response to DNA damage [21, 32–35].

The NIR laser-induced damage results in a wide variety of DNA damage types including SSBs, DSBs, and pyrimidine dimers [36]. It was suggested that the use of visible and NIR laser wavelengths may be challenging due to the complexity of induced damage [15]. Complex DNA damage, however, is what is commonly induced by ionizing radiation and genotoxic agents, and thus, it is important to understand the cellular responses to this type of damage. We found that it is possible to control the complexity of DNA lesions by titration of NIR laser input power [37, 38]. Unlike UVC lasers [36], we found that the NIR laser can generate simple low density SSBs and DSBs at low input power and complex DNA damage (SSBs, DSBs, 6-4PP, CPD, and 8-oxoG) with high input power (Figures 1B,C) [37, 38]. Importantly, complex DNA damage induced by high input-power NIR laser triggers robust poly (ADP-ribose) polymerase 1 (PARP1) recruitment and activation [37]. We found that PARP1 activation at complex damage sites is required for telomeric repeat binding factor 2 (TRF2) recruitment, but inhibits 53BP1 recruitment, having differential effects on DSB repair pathway choice [37, 39] (Figure 1B). PARP1 is a rapid and sensitive DNA nick sensor that catalyzes the synthesis of poly (ADP-ribose) (PAR) chains on itself and target proteins [40]. Local PAR accumulation at damaged lesions was proposed to cause phase separation and recruitment of various factors [41, 42]. 53BP1, which restricts DNA end resection for HR and promotes NHEJ [43, 44], is the first example of repair factor whose recruitment is inhibited by PAR, providing one possible explanation for hyperactivation of NHEJ by PARP inhibitors [37]. Furthermore, we observed accumulation of BER factors, such as DNA glycosylase NEIL1, and condensin I [38, 45] at high power damage sites (Figure 1B). Interestingly, even high-linear energy transfer (LET) α -particles

irradiation, which can induce up to 90% complex damage [46] failed to induce robust PARP activation and thus no TRF2 recruitment was observed [47, 48]. This may be due to differences in damage density and induction mechanism. High input power NIR also causes pan-nuclear phosphorylation of H2AX (γ H2AX), which disperses MDC1 from damage sites [37]. This is similar to what was reported with high-LET irradiation [49]. Because 53BP1 and Rad51 accumulation at the DNA damage sites requires MDC1 [50, 51] MDC1 dispersion by pan-nuclear γ H2AX also suppresses their clustering at damage sites. Thus, despite the induction of complex DNA damage, the DDR patterns can be different between high-LET IR and high input power NIR. Nevertheless, these studies indicate that with careful titration of laser parameters and characterization of resulting DNA damage by immunofluorescent detection of key damage markers, NIR laser should be a valuable tool to investigate dynamics of DDRs in response to simple strand breaks and complex DNA damage, and is particularly suitable for studying PARP signaling [34, 37–39].

SYSTEMATIC STUDIES OF FACTOR RECRUITMENT TO LASER-INDUCED DAMAGE SITES

While laser microirradiation can be used to examine the dynamics of DDR at the single-cell level with high spatiotemporal resolution, it is time-consuming to define laser-irradiated subcellular regions manually and analyze large sets of images. In early DNA damage studies that utilized a laser beam, the number of repair factors tested were limited [36, 52]. The kinetics of individual DNA repair factors at damage sites have been reported [53, 54], but it is difficult to compare these studies because the laser parameters were different, which might have induced different types and amounts of DNA damage [22]. Furthermore, artificial overexpression of the recombinant tagged proteins used for the analyses may cause these proteins to behave differently from the endogenous untagged proteins expressed from their own promoters [37, 55]. To circumvent these potential problems and compare different factor recruitment side by side, bacterial artificial chromosome (BAC)-transduced cell lines expressing EGFP-tagged DNA repair proteins from their endogenous promoters were used for recruitment kinetics study [20]. They systematically measured and mathematically modeled the kinetics of 70 DNA repair proteins to laser-induced DNA damage sites comparing to co-expressed mCherry-tagged PCNA as a control.

In addition to the studies of known repair factor recruitment, laser microirradiation has been employed to identify factors that were not previously known to be involved in DDR and repair. Those include various histone and chromatin remodeling factors that appear to promote efficient DNA repair [17, 56, 58]. However, these previous studies were also limited to investigation of each individual protein factor. Using the lentivirus expression system, Izhar et al. screened hundreds of gene products with potential roles in DNA repair and other nuclear processes, and identified more than 120 proteins that

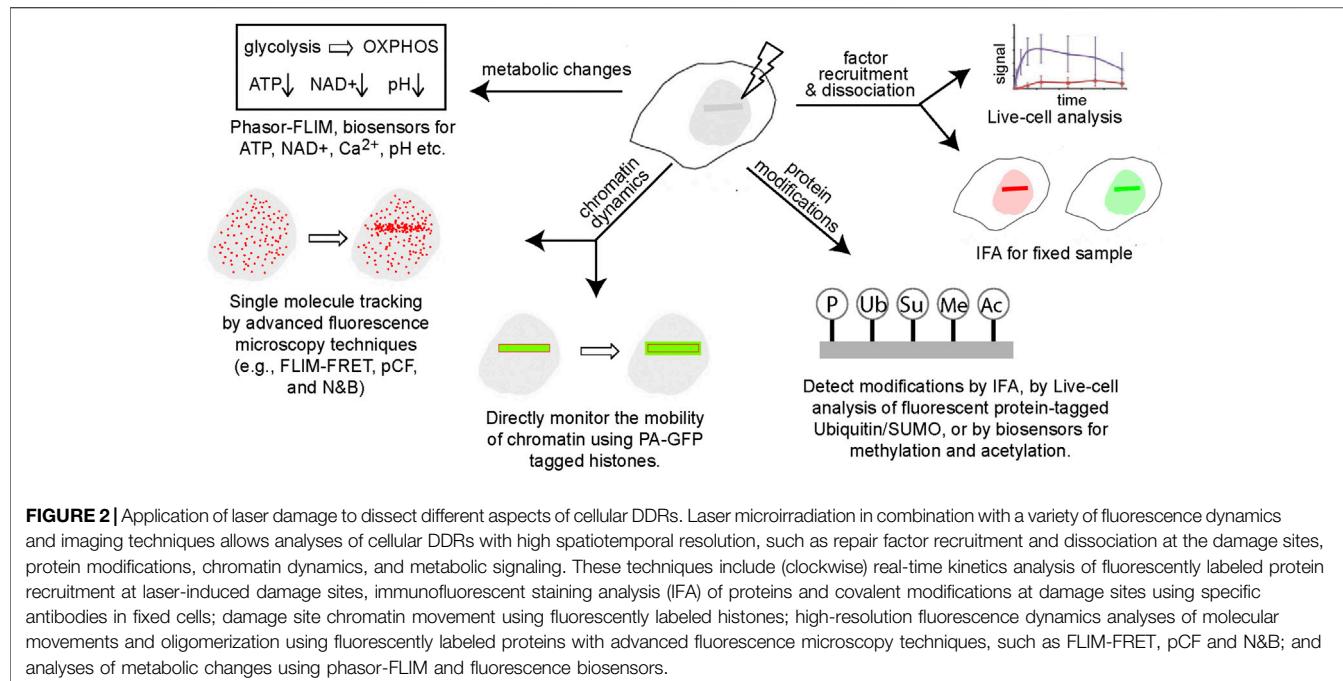
localized to sites of UVA laser-induced DNA damage [59]. Many positive hits were transcription factors that were recruited to DNA damage sites in a PARP-dependent manner. Most of these had not previously been reported to localize to sites of DNA damage.

It is challenging to perform quantitative analyses of factor recruitment kinetics with sufficient statistical power, due to a limited number of cells that can be analyzed at one time. To increase through-put, several approaches have been developed to analyze fluorescence intensity or area under the curve of micro-irradiated regions [54, 60]. Mistrik et al. [61] exposed a bulk of cells simultaneously to a UVA laser beam in a defined pattern of collinear rays. The induced striation pattern was automatically evaluated by custom-coded software, which provides a quantitative assessment of laser-induced phenotypes. Oeck et al. developed an ImageJ-based, high-throughput evaluation tool to standardize and accelerate the quantitative analysis of local protein accumulation at sites of DNA damage [62]. The continuous development of analysis tools will improve high-throughput data analysis of repair factors dynamics at laser induced-DNA damage sites.

ANALYSES OF SECONDARY DAMAGE SIGNALING

Chromatin Dynamics

Chromatin dynamics modulates DNA damage site accessibility of repair factors. Damage induction at the define subnuclear region by laser microirradiation allowed tracking of damaged chromatin movement and change of chromatin compaction [17]. Kruhlak et al. [17] tracked mobility and structure of chromatin containing DSBs in living cells by using photoactivatable GFP (PA-GFP)-tagged histone H2B. Initial studies using photo-activatable GFP fused to histone H2B revealed that DNA damage triggers the localized relaxation of chromatin followed by the localized compaction of chromatin, in an ATP and PARP-dependent manner [63, 64]. Several advanced fluorescence microscopy techniques were employed to visualize dynamic chromatin changes at laser induced damaged and undamaged sites [32, 33, 35]. For example, pair correlation function (pCF) analysis of EGFP molecular flow in and out of chromatin before and after damage induction revealed that DNA damage induces a transient decrease in chromatin compaction at the damage site and an increase in compaction to adjacent regions [35]. Dispersion and compaction surrounding the damage site was suggested to facilitate DNA repair factor recruitment to the lesion [35]. Lou et al. were able to directly measure nanometer changes in chromatin compaction at DNA damage sites using a biophysical method based on phasor image-correlation spectroscopy of histone fluorescence lifetime imaging microscopy (FLIM)-Förster resonance energy transfer (FRET) microscopy on live cells coexpressing H2B-eGFP and H2B-mCherry [32]. They found that the fraction of compact chromatin within the NIR laser-induced damage lesion sharply increased in the first 30 min after DSB induction and persisted for up to 3 h, while there was no significant change in the percentage



of compact chromatin nucleus-wide [32]. Another group, however, demonstrated that 405 nm laser-induced DNA damage in Hoechst-sensitized cells led to a global compaction of undamaged chromatin through analysis with fluorescence anisotropy imaging of histone H2B-EGFP [33]. The controversial results from different groups may be caused by the different damage conditions (as discussed above). Nevertheless, the combination of laser microirradiation and fluorescence dynamics techniques makes it possible to distinguish changes of chromosome dynamics at damage sites and in the rest of the nucleus (with undamaged chromatin) in response to DNA damage.

Cell-wide Metabolic Response

In addition to studies on DNA damage responses in the nucleus, use of laser microirradiation in conjunction with fluorescence imaging allows investigation of cell-wide DDR because it is possible to distinguish damaged and undamaged cells in the same field under microscope and to track damage-induced changes in realtime. Using fluorescence-based ATP and NAD⁺ biosensors, pH indicator, and phasor-FLIM capturing autofluorescence of NADH, we systematically measured metabolic dynamics in living cells in response to NIR laser-induced DNA damage with different input power [34]. We observed a rapid cell-wide increase of the bound NADH fraction in response to complex DNA damage, which is triggered by PARP1-dependent transient depletion of NAD⁺. We found that this change is linked to the increased cellular metabolic reliance to oxidative phosphorylation(oxphos) over glycolysis, which is critical for damaged cell survival [34]. Recent evidence suggests that other cellular processes are also involved in DDR, such as autophagy and immune response [65, 66]. Damage-induced changes in subcellular localization or oligomerization revealed

previously unrecognized roles of proteins in DDR and repair processes [67, 68]. Thus, combinatorial use of spatiotemporally defined laser microirradiation and fluorescent imaging will have many future applications in realtime dissection of cellular responses to DNA damage.

DISCUSSION AND FUTURE PERSPECTIVE

With careful parameter setting and characterization of induced damage, laser microirradiation offers valuable opportunities to study *in vivo* cellular responses to DNA Damage with high spatiotemporal resolution. It was highly instrumental in identifying new factors and modifications involved in DDR, determining the order of factor recruitment and kinetics, chromatin and cellular metabolic changes associated with DNA damage, furthering our knowledge of DNA damage response in human cells (Figure 2). Precise input power titration and parameter setting led to better understanding and control of the types of damage induced, which now allow us to characterize specific DDR signaling associated with simple strand breaks and complex damage. With further technology development and refinement, laser microirradiation will continue to be a powerful tool to study DDR. For example, with CRISPR technology, it is now feasible to generate cell lines that express multiple fluorescently tagged factors from their endogenous loci (to avoid artifactual overexpression) and examine their realtime interplay at laser-induced damage sites using multi-color confocal microscopy. Knowing exactly which cell is damaged, it is also possible to analyze the DDR signaling in cell-cell communication. Advanced fluorescence microscopy techniques, such as number and brightness (N&B) analysis, fluorescence recovery after photobleaching (FRAP),

fluorescence localization after photobleaching (FLAP), and FLIM-FRET, may be utilized effectively to further dissect DDR at a single-molecule resolution [69]. Development/improvement of integrated microscopy systems that allow automated laser damage and fluorescent image data acquisition and tracking would allow high-throughput DDR analyses and screening of small molecules, RNAi, or CRISPR libraries to identify critical factors and harness DDR and repair processes, which may be applicable to disease therapy development.

DATA AVAILABILITY STATEMENT

The original contributions presented in the study are included in the article/**Supplementary Material**, further inquiries can be directed to the corresponding author.

AUTHOR CONTRIBUTIONS

XK, NW, and KY planned the outline, XK and NW wrote the review under KY's supervision.

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FUNDING

The work in the Yokomori laboratory was supported in part by NSF MCB-2013798. NW is supported by AFOSR Grant FA9550-20-1-0052.

ACKNOWLEDGMENTS

We would like to thank Michelle Digman and Enrico Gratton at Laboratory of Fluorescence Dynamics for phasor-FLIM and pCF studies and the support of the Chao Family Comprehensive Cancer Center Optical Biology Core (LAMMP/OBC) Shared Resource for our studies mentioned in this review. We apologize to the researchers whose work we could not cite in this review due to space limitations.

SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fphy.2020.597866/full#supplementary-material>.

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Conflict of Interest: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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