Local Confinement Controls Diffusive Nanoparticle Dynamics in Semidilute Polyelectrolyte Solutions

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Abstract: We investigate the mobility of polystyrene particles ranging from 100 to 790 nm in diameter in dilute and semidilute sodium polystyrene sulfonate (NaPSS) solutions using fluorescence microscopy. We tune the polymer conformations by varying the ionic strength of the solution. The nanoparticle mean-squared displacements evolve linearly with time at all time scales, indicating Fickian diffusive dynamics. In solutions of high ionic strength, chains adopt a random walk conformation and particle dynamics couple to the bulk zero-shear rate viscosity according to the Stokes-Einstein picture. In solutions of low ionic strength, however, particle dynamics non-monotonically deviate from bulk predictions as polymer concentration increases and are not accurately predicted by the available models. These non-monotonic dynamics directly correlate with the non-Gaussianity in distributions of particle displacements, suggesting the emergence of a local confining length scale as polyelectrolyte concentration increases.

Introduction

Nanoparticle transport in concentrated complex fluids is important for enhanced oil recovery,[1,2] nanocomposite materials,[3,4] and targeted drug delivery.[5,6] Understanding the mechanisms controlling particle diffusion is necessary to enhance the efficacy of particle transport in these applications. The diffusion of a particle of radius R_{NP} in a homogeneous medium with viscosity η is given by the Stokes-Einstein (SE) equation, $D_{SE} = k_B T/6\pi\eta R_{NP}$. The assumptions underlying the SE model do not hold as the particle size becomes comparable to the length scales of inhomogeneities in the medium, and deviations from SE predictions appear.[7–10] In this size regime, particle dynamics depend on length scales present in solution.

In entangled solutions, the length scale controlling particle dynamics is the tube diameter a, the distance between entanglement strands. The entanglement mesh cages large particles until the time scale of reptation, after which SE behavior is recovered.[11–14] Conversely, particles that are much smaller than the entanglement mesh diffuse through the mesh and are unaffected by the polymer network. In *unentangled* polymer solutions, however, particle dynamics are controlled by the correlation length ξ, the distance between neighboring chains. Hydrodynamic models assume polymer solutions to be a homogeneous medium in which hydrodynamic interactions decay over ξ[10,15,16] and in which particle dynamics are dictated by polymer length scales, such as radius of gyration R_g and correlation length ξ.[13,17,18] These pictures have been developed for neutral polymers. In charged polymers, by contrast, electrostatic repulsion between monomers alters structure and chain flexibility.[19,20] The size of the charged group and its recurrence within the monomers results in conformations ranging from rigid rod to semiflexible chain. In turn, the local conformation determines the mesh geometry. As a result of these structural differences, the onset of entanglements in charged polymers is shifted to much higher concentrations than for neutral chains.[21,22] The pronounced differences in structure and relaxations in charged polymers likely affect the length scales controlling diffusive transport of nanoparticles. Despite recent studies of nanoparticle diffusion in charged polymer solutions and melts,[23,24] the effect of charge-induced conformation on nanoparticle transport remains incompletely understood.

Here, we probe the dynamics of nanoparticles in dilute and semidilute unentangled solutions of a model polyelectrolyte. The polymer conformation is tuned by varying the solution ionic strength. The particle dynamics are diffusive across all experimental time scales. We find that the diffusivity of large particles ($R_{NP}/R_g > 1$) follows bulk predictions at all ionic strengths. For smaller particles ($R_{NP}/R_g < 1$), however, we observe surprising dynamics with non-monotonic deviations from SE within the unentangled semidilute regime. The size-dependent dynamics do not collapse onto a master curve according to physical arguments derived for Gaussian chains. We find that the non-Gaussian parameter maps onto the same concentration dependence as scaled particle diffusivity D/D_{SE}, suggesting the rise of confinement effects despite the absence of entanglements.

Materials and Methods

Solution Preparation

Glass vials were cleaned overnight in a solution of 6.5 wt% potassium hydroxide in isopropanol, ensuring near salt-free conditions. Vials were thoroughly rinsed 10 times using Millipore water to remove any residual salt, then dried in an oven at 105°C degrees for 2 hours. Fluorescent polystyrene particles with diameters d_{NP} ranging from 100 to 790 nm (Fluoro-Max, Thermo Fisher Scientific) were dispersed in aqueous solutions of NaPSS with a weight-averaged molecular weight $M_w = 2\,200\,000$ Da (Scientific Polymer Products) at three different ionic strengths. A constant particle volume fraction $\phi = 1.5 \times 10^{-6}$ was used across all samples to minimize interparticle interactions and avoid aggregation (observed for $\phi \geq 5 \times 10^{-5}$) while maintaining good statistics for particle tracking. Deionized water was assumed to have

an ionic strength of 10^{-6} M,[25] whereas the other two sets of samples were prepared using sodium chloride to achieve ionic strengths of 10^{-3} M and 10^{-1} M. The overlap concentration c^* of NaPSS was estimated at each ionic strength from intrinsic viscosity measurements (SI), and the radius of gyration $R_{g,0}$ in each ionic strength solution was determined via $R_{g,0} = (M_w/(4/3\pi N_{av}[\eta]))^{1/3}$.[26,27] The resulting $R_{g,0}$ in dilute solutions were 190, 130, and 75 nm at ionic strengths of 10^{-6}, 10^{-3}, and 10^{-1} M, respectively.

Bulk Rheology

Steady-shear measurements of the rate-dependent viscosity were performed on Discovery Hybrid Rheometer (TA Instruments, HR-2). Polymer solutions were loaded into a single gap Couette cell with a cup diameter of 15 mm, a bob diameter of 14 mm, and a bob length of 42 mm. The inertia and torque of the instrument were calibrated prior to measurements. Samples were pre-sheared for one minute to reach equilibrium, after which the viscosity was determined as the average value over one minute.

Imaging Sample Preparation

To create a sample chamber for imaging, two cover slips (22 mm × 22 mm × 0.2 mm, Fisherbrand cover glass) were adhered on Gold Seal cover glass (48 mm × 65 mm × 0.15 mm) using UV epoxy-based adhesive to form two sides of a chamber. Another cover slip was attached on top of the two cover glass slips using UV epoxy. The particle-polymer solutions were then pipetted through one of the two open sides. Finally, the two remaining open sides were sealed with UV epoxy.
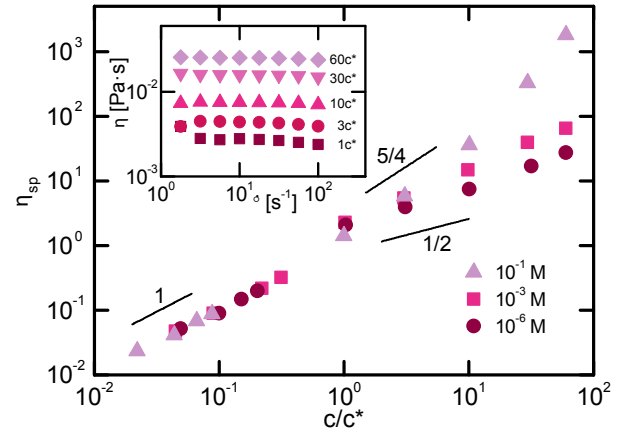
Imaging and Particle Tracking

A Leica DM4000 inverted fluorescent microscope equipped with 63x and 100x oil immersion lenses was used to acquire series of images of quiescent samples over time. For each image series, 4100 images were captured at a frame rate of 32 fps. At least five image series per sample were recorded at different locations. Particle centroids were located with a spatial resolution 25 and 35 nm for 200 and 790 nm particles, respectively, and tracked over time using particle-tracking algorithms.[28] From the particle trajectories, we calculated the one-dimensional ensemble-averaged mean-squared displacement (MSD) $\langle \Delta x^2(\Delta t) \rangle$ as a function of lag time Δt. At least 10^4 time steps were averaged for each MSD data point. To extract the diffusivity D, we fitted each MSD to $\langle \Delta x^2(\Delta t) \rangle = 2D(\Delta t)$.

Results and Discussion

We characterize the rheological properties of the polyelectrolyte solutions at three solution ionic strengths. The viscosity increases concomitant with polymer concentration c/c^* and is approximately independent of shear rate across two orders of magnitude in concentration (inset to Figure 1), indicating that the chains relax quickly in solution (10^{-3} and 10^{-1} M shear viscosity in SI).

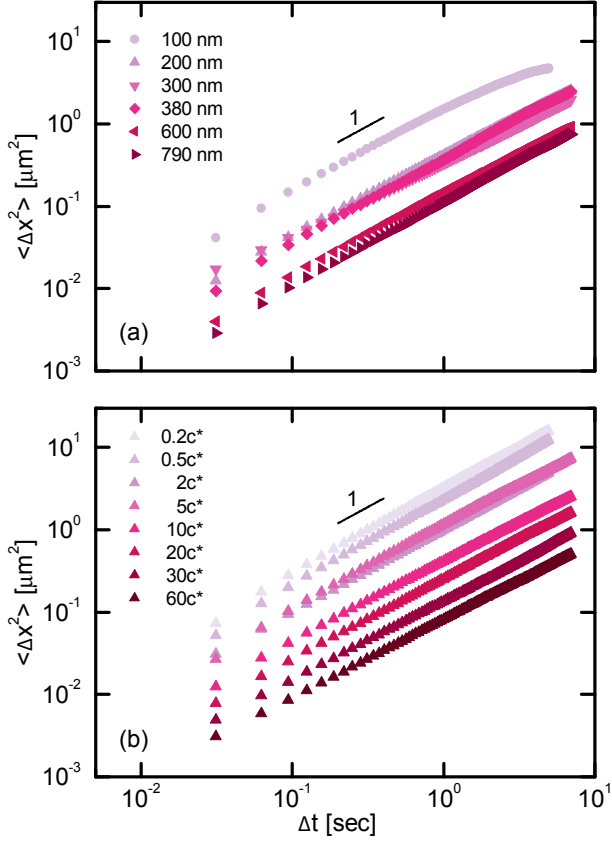The viscosity of charged polymer solutions exhibits a dependence on ionic strength that is not observed for their neutral counterparts.[22,29] We examine the changes in specific viscosity $\eta_{SP} = (\eta - \eta_0)/\eta_0$ because it offers a direct measurement of the polymer contribution to solution viscosity. The specific viscosity of the polyelectrolyte solutions increases as a function of both polymer and ionic strength. In the dilute regime, the specific viscosity scales with concentration as $\eta_{sp} \sim (c/c^*)^1$ following the theoretical prediction.[30] The specific viscosity is independent of ionic strength for concentrations $c/c^* < 1$ due to the dominance of hydrodynamic interactions.[31,32] In the semidilute regime ($c/c^* > 1$), the specific viscosity scales according to predictions[30] for polyelectrolyte solutions at low ($\eta_{sp} \sim (c/c^*)^{1/2}$) and high ($\eta_{sp} \sim (c/c^*)^{5/4}$) ionic strength.[21,22,30] When the ionic strength is intermediate between these limits, however, the specific viscosity in the semidilute regime scales with concentration as $\eta_{sp} \sim (c/c^*)^\alpha$ with $\alpha = 0.8 \pm 0.1$. The specific viscosity increases with ionic strength for constant c/c^* in the semidilute regime, consistent with an increase in chain-chain interactions as the salt screens monomeric repulsion.[22] We observe a sharp upturn in η_{sp} at high polymer concentrations only in solutions of high ionic strength, suggesting that these solutions are entangled. Such a crossover, however, is not observed at low and intermediate ionic strength, suggesting the absence of chain entanglements. These observations are consistent with the expectations for entanglements in charged polymer solutions occurring at high concentrations that are $\gg 10c^*$.[22] Thus, these polyelectrolyte solutions have rheological properties that agree well with existing theories[21,25,30] and serve as a model system to investigate how particle dynamics depend on polymer conformations.

Figure 1. Specific viscosity $\eta_{sp} = (\eta - \eta_0)/\eta_0$ as a function of normalized NaPSS concentration c/c^* for solutions of various ionic strength. *Inset:* Viscosity η for 10^{-6} M ionic strength solutions as a function of shear rate $\dot{\gamma}$. Bottom and top solid lines represent viscosity scaling predicted for polyelectrolytes in the limit of low and high ionic strength, respectively.

The mobility of nanoparticles in polyelectrolyte solutions decreases with increasing nanoparticle size (Figure 2(a)) and polymer concentration (Figure 2(b)). The mean-square displacement (MSD) scales linearly with lag time $\langle \Delta x^2 \rangle = 2D\Delta t$ across all time scales, indicating diffusive dynamics with a diffusivity D as expected for Newtonian solutions with fast relaxations. We remove explicit size dependence by normalizing D by the diffusivity of the particle in pure solvent D_0.
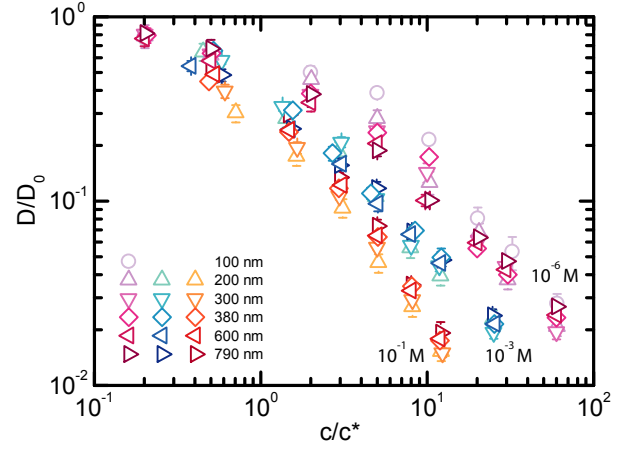
Particles diffuse according to solvent viscosity at low polymer concentrations across all ionic strengths $D/D_0 = 1$ (Fig-

Figure 2. Mean-square displacement (MSD, $\langle \Delta x^2 \rangle$) as a function of lag time Δt for (a) particles of various sizes in a solution of polymer concentration 10c* and (b) for 200 nm particles in solutions of various polymer concentrations. The ionic strength is at 10^{-6} M ionic strength (MSDs at 10^{-3} M and 10^{-1} M ionic strength can be found in SI). Solid lines represent linear scaling.
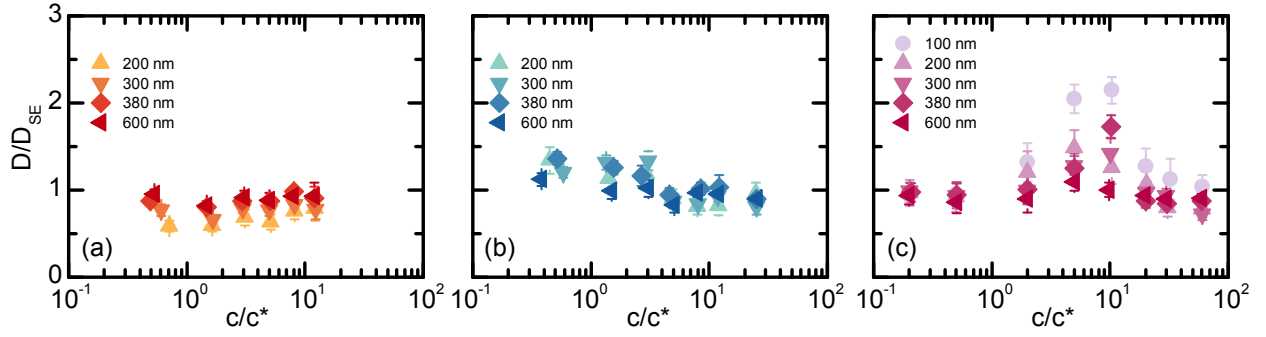

Figure 3. Normalized particle diffusivity D/D_0 as a function of polymer concentration c/c^* in solutions of different ionic strength. Error bars represent the standard deviation of five measurements per sample.

ure 3). The dynamics slow as concentration increases into the semidilute regime. At a given concentration c/c^* within the semidilute regime, the particle dynamics are faster as ionic strength decreases, consistent with the lower viscosity of the solutions (Fig. 1). The normalized diffusivities are approximately independent of particle size in solutions of ionic strength 10^{-1} M and 10^{-3} M, consistent with the idea that the particle diffusion probes the bulk solution viscosity. In solutions with the lowest ionic strength (10^{-6} M), however, the dynamics of small particles deviate from those of large particles, indicating that the dynamics of small particles decouple from the bulk solution viscosity.

To quantify the extent to which dynamics deviate from the predictions using bulk solution viscosity, we examine the particle diffusivity normalized by the Stokes-Einstein diffusivity D/D_{SE} as a function of polymer concentration. We use the dynamics of the large particles to quantify bulk solution viscosity so that $D_{\mathrm{SE}}/D_0 = D_{790}/D_{790,0}$ to overcome torque limitations of the rheometer at low solution viscosity. Particles in solutions of high (10^{-1} M) and intermediate (10^{-3} M) ionic strength exhibit diffusivities that approximately conform to the Stokes-Einstein prediction using the measured bulk viscosities (Figures 4 a and b). We attribute systematic deviations in D/D_{SE} from the predicted value of 1 to the use of the largest particles as bulk probes. In these solutions, the particles are larger than the radii of gyration of the polymers at infinite dilution, which we calculate to

be 130 and 75 nm for solutions of intermediate (10^{-3} M) and high (10^{-1} M) ionic strength. Thus the near-Stokes-Einstein diffusivities measured for these systems, for which $R_{\mathrm{NP}} > R_{\mathrm{g}}$, are consistent with earlier studies that show that the dynamics of large particles ($R_{\mathrm{NP}} > R_{\mathrm{g}}$) couple to bulk viscosity behavior according to the SE prediction.[33]

By contrast, the dynamics in solutions at low ionic strengths (10^{-6} M) depend on particle size. The diffusivities of 600 nm particles follow the predicted SE behavior at all polymer concentrations (Fig. 4(c)). The dynamics of smaller particles, however, agree with SE predictions at low polymer concentrations ($c/c^* < 1$) but exhibit a striking departure from SE predictions at higher polymer concentrations. This deviation increases with increasing polymer concentration until $c/c^* \approx 10$, at which point the particle dynamics begin to approach SE predictions again. In these low ionic strength solutions, the particles are comparable in size to the radius of gyration of the polymer ($R_{\mathrm{NP}} \sim R_{\mathrm{g}}$) and hence the solutions cannot be treated as homogeneous continua. In this limit, interactions between particles and polymer chains become more important and lead to deviations from predictions based on the bulk solution rheology.[13,34]

A number of models and scaling theories attempt to explain particle dynamics in polymer solutions. Empirical models generally fall into one of two categories: obstruction[35–40] or hydrodynamic.[10,15,16,34,41–43] Obstruction models assume that the polymer mesh is effectively immobile on time scales of particle diffusion and serve as geometric barriers to particle diffusion, but this assumption does not hold in our system because chains relax on time scales of the same order of magnitude as those characterizing the particle dynamics (SI). Hydrodynamic models assume that hydrodynamic interactions are screened over ξ so that viscous drag increases as ξ decreases. Hydrodynamic models, however, predict monotonic deviations from Stokes-Einstein behavior because ξ decreases monotonically with increasing polymer concentration. Importantly, these empirical models cannot describe the non-monotonic behavior of D/D_{SE} in our system.

A second category of models incorporate how the particle interacts with the polymer. For neutral polymer systems, the polymer may develop a depletion layer around the particle, whereas for attractive polymer systems, the surrounding

Figure 4. Diffusivity normalized to SE predictions D/D_{SE} as a function of polymer concentration c/c^* at (a) 10^{-1} M, (b) 10^{-3} M, and (c) 10^{-6} M ionic strength. Error bars represent the standard deviation of five measurements per sample.

polymer will form a bound layer covering the particle. In the depletion layer picture, the particle diffuses quickly through the depletion layer and then slowly through the polymer mesh.[34] Our data, however, does not collapse according to the scaling suggested by this picture (SI), suggesting the absence of a depletion layer surrounding the particles. In the bound-layer picture, the polymer binds to the surface of the particle and increases the viscous drag acting on the particle so that the particle diffusion is slower than expected.[44] Dynamic light scattering (DLS) on our particles in NaPSS solutions in the low and high ionic strength limits and in dilute conditions reveal that polymer chains do not significantly adsorb on the particle (SI). Moreover, we expect that particles with a bound layer would exhibit slower-than-expected diffusion, whereas in our experiments D/D_{SE} approaches 1 for solutions with high polymer concentrations and low ionic strength.

A third class of pictures, developed for particles in dielectric media, predict a non-monotonic decrease in the diffusion coefficient when a particle is surrounded by an electric double layer of comparable size[45] or when the particle dielectric constant increases.[46] The former case[45] results in slowing of particle diffusion when the particle size is on the order of the inverse of the Debye length (i.e. $d_{NP}\kappa = 1$, where κ^{-1} is the Debye length). Our experiments, however, span size ratios that are orders of magnitude larger than $2R_{NP}\kappa = 1$. Furthermore, Ref. 45 predicts that particle dynamics are slower at intermediate electrolyte concentrations $(-2 < \log(2R_{NP}\kappa) < 1)$ before recovering SE behavior at higher electrolyte concentrations $(\log(2R_{NP}\kappa) > 1)$ and hence trend in the opposite direction of our data. Finally, the predicted deviations from SE behavior are of order $\sim 10\%$[45], which are much smaller than our observed deviations (Figure 4). The latter picture[46] predicts an enhanced polymer-particle affinity as chain length or nanoparticle size increases when the dielectric constant of the particle increases beyond that of the surrounding medium. The polystyrene particles in our experiments, however, have a dielectric constant $(\epsilon = 2.5)$ that is significantly lower than the solvent, water $(\epsilon = 80)$. Additionally, we expect the negatively charged polystyrene particles and polyelectrolyte chains to further reduce the affinity of chains to adsorb on the particle surface. Thus, these models are also not able to describe the non-monotonic deviations from SE dynamics in our low-ionic-strength samples.

A final model predicts that, within certain size ranges, the particle dynamics are coupled to the relaxations of polymer segments of similar size.[13] In this theory, particle-polymer coupling results in diffusion according to an effective solu-

tion viscosity that is lower than the bulk viscosity.[13] In our earlier experiments on partially hydrolyzed polyacrylamide, the coupling theory scaling prediction $D/D_0 \sim (R_{NP}/\xi)^{-2}$ was able to collapse the diffusivities of systems with similar particle-polymer size ratios (R_{NP}/R_g).[47] This scaling, however, is not able to collapse the diffusivities measured in NaPSS solutions onto a master curve (SI). This result suggests that different physics must control particle dynamics in these solutions as compared to solution of fully flexible Gaussian chains, likely arising from effects due to the charge on the polymers in the semidilute regime.
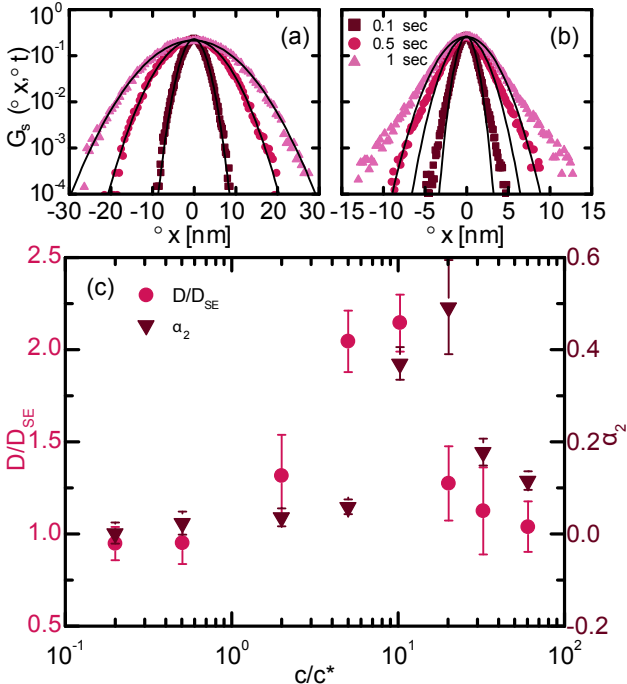
To identify the controlling physics, we examine the differences between polyelectrolytes and uncharged polymers. Both the radius of gyration $R_g \sim c^{-1/4}$ and the correlation length $\xi \sim c^{-1/2}$ (calculations provided in SI) of polyelectrolytes decrease as concentration is increased (Table 1), similar to those for neutral chains but with different scaling exponents.[22,30,32] Surprisingly, we observe non-monotonic behavior in D/D_{SE} when $R_{NP}/R_g < 1$ for all polymer concentrations (100, 200 nm diameter particles), when $R_{NP}/R_g > 1$ for all polymer concentrations (380 nm), and when R_{NP}/R_g transitions from > 1 to < 1 as concentration is increased (300 nm). Likewise, we observe non-monotonic behavior when $R_{NP}/\xi > 1$ for all concentrations (380 nm) and when R_{NP}/ξ transitions from > 1 to < 1 as concentration is increased (100, 200, 300 nm). Thus structural length scales do not directly control the non-monotonic behavior of D/D_{SE} in the semidilute regime. Second, prior studies on NaPSS revealed that chain relaxation times exhibit a local maximum at the overlap concentration,[21] first increasing with concentration in the dilute regime and subsequently decreasing with concentration in the semidilute regime.[29,48] The non-monotonic deviations from SE in our study do not occur at the crossover between dilute and semidilute regimes, but rather well-within the semidilute regime $c/c^* \sim 10$. This result suggests that the non-monotonic behavior in D/D_{SE} in the semidilute regime does not arise from non-monotonicity in the chain relaxation time.

Because length and time scales of the NaPSS do not directly control the non-monotonic particle dynamics, we assess if local polymer properties may be controlling the particle behavior. The original scaling theory of Wyart and de Gennes[17,29] predicts that small particles (whose size is comparable to the polymer blob size) that exhibit faster-than-SE diffusion at low to moderate polymer concentrations experience macroscopic viscosity above a concentration $c_{limit}/c^* = (R/R_g)^{-4/3}$ in entangled solutions. In this picture, cages in an entangled polymer mesh constrain par-

Table 1. Calculated correlation length ξ and radius of gyration R_g as a function of polymer concentration for solutions of varying ionic strength using scaling theory [21,22,30]

c/c^*		1.5	2	5	10	20	30
10^{-6} M	ξ [nm]	164	121	68	44	28	22
	R_g [nm]	174	165	140	123	108	101
10^{-3} M	ξ [nm]	98	80	43	26	16	12
	R_g [nm]	122	117	102	91	82	77
10^{-1} M	ξ [nm]	94	43	21	12	7	-
	R_g [nm]	72	70	63	59	55	-

ticles on time scales shorter than the reptation time scale, after which SE behavior is recovered. Thus, the rise in entanglements with increasing concentration controls the transition from micro- to macro-viscosity controlled diffusion. Indeed, non-monotonic deviations from SE were reported for polystyrene spheres in solutions of poly(vinyl methyl ether).[49] Although physically appealing, this picture is not directly applicable to our experiments because the polymer solutions with low ionic strength are not entangled in the range of concentrations explored in this study (as determined through rheology, SI). Additionally, although the rheological measurements of the high ionic strength polymer solutions suggest that these solutions are entangled at high concentrations (Figure 1), they follow SE predictions across all investigated concentrations (Figure 4 (a)). This comparison suggests that the chain entanglements do not significantly affect particle dynamics in this regime. Nevertheless, we are inspired by this picture to further examine the particle dynamics to look for signatures of local structural effects that may act like an entanglement-produced cage.

Figure 5. Normalized distribution of displacements G_s at various times for 100 nm particles in solutions of polymer concentration (a) $2c^*$ and (b) $20c^*$ at 10^{-6} M ionic strength. Solid lines represent Gaussian fits. (c) Scaled diffusivity D/D_SE and non-Gaussian parameter α_2 as a function of polymer concentration c/c^* for 100 nm particles at 10^{-6} M ionic strength.
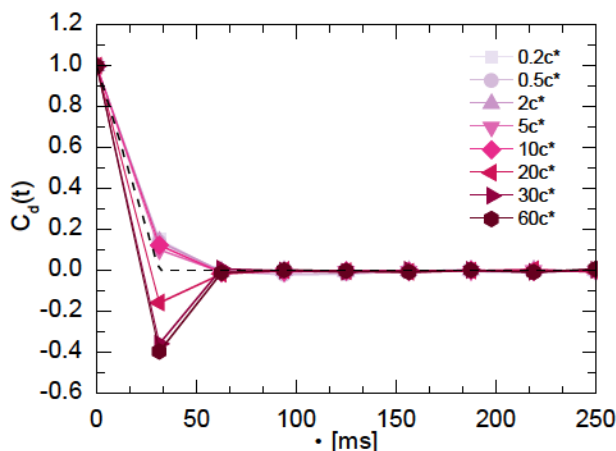
We hypothesize that the non-monotonic dynamics may be associated with particles experiencing local heterogeneity in solution. The distributions of particle displacements $G_s(\Delta x, \Delta t) = \frac{1}{N} \left\langle \sum_{i=1}^{N} \delta \left(x_i(t) - x_i(t + \Delta t) - \Delta x \right) \right\rangle$ are Gaussian on all accessible time scales for some particle sizes and polymer concentrations (e.g., 100 nm particles and $2c/c^*$ Figure 5 (a)). For 100 nm particles at $20c/c^*$, however, $G_s(\Delta x, \Delta t)$ is non-Gaussian for all accessible lag times (Figure 5 (b)). For all samples, the non-Gaussian parameter $\alpha_2 = \frac{<\Delta r^4>}{3<\Delta r^2>^2} - 1$, which characterizes the extent to which the distributions deviate from the Gaussian prediction for Fickian diffusion, is approximately independent of time. Surprisingly, we find that α_2 for the 100 nm particles is also a non-monotonic function of c/c^* and exhibits a local maximum (Fig. 5(c)). Moreover, the concentration at which it attains its local maximum, $20c/c^*$, is close to that at which D/D_SE attains its local maximum, providing additional evidence that the non-monotonic deviations from SE may be related to particles experiencing different heterogeneous environments.

Non-Gaussian distributions of particle displacements can arise from temporal[50,51] or spatial[52,53] heterogeneities in the environment or from multiple dynamic modes.[54,55] In these solutions, chain relaxations occur on time scales faster than those characterizing particle diffusion (inset to Figure 1), indicating that the solution dynamics are not temporally heterogeneous on timescales relevant for particle diffusion. Anomalously large displacements are often attributed to hopping of particles between cages in a mesh or network.[56–58] A recent theory proposes that particles whose size is comparable to or slightly larger than ξ in entangled solutions experience intermittent hopping within the mesh at long time scales.[13,18] Recent experiments attribute the non-Gaussian behavior in entangled solutions to a competition between three time scales: the short-time relaxation of an entanglement strand, the time scale for activated hopping of nanoparticles, and the long-time reptation of the polymers.[57,59] In our experiments, however, the solutions are not entangled. Instead, we propose that the return to SE diffusion arises due to increasing confinement from the polymers. These confinements behave similarly to a tube diameter in an entangled system and become more prominent as the polymer concentration is increased. Because the non-monotonic deviations from SE are not observed in the salted solutions, our results suggest that the anomalous diffusion in Fig. 4 arises from the distinctive structural properties of polyelectrolytes.

To explore the confinement picture, we calculate displacement autocorrelation functions $C_\mathrm{d}(t) = <\Delta x(t+\tau)\Delta x(t)>$ at all polymer concentrations in 10^{-6} M solutions. The displacements of 100 nm particles become anticorrelated at $t = 32$ ms, which corresponds to the first time interval in our movies, in solutions with $c > 10c^*$ (Figure 6). The degree of anticorrelation increases with increasing polymer concentration but decreases for larger particles (SI). The larger anticorrelation in 100 nm particles suggests that they experience caging-like effects, in which the particle rebounds after encountering an elastic polymer network as polymer concentration increases. Additionally, the appearance of anticorrelated displacements occurs close to the onset of non-Gaussian particle displacements and the maximum in the D/D_SE deviation. Together, these factors suggest that the observed anomalous diffusion is a result from the unique structural properties of polyelectrolytes.

Figure 6. Normalized coefficient of displacement autocorrelation $C_{\mathrm{d}}(t)$ as a function of elapsed time τ for 100 nm particles in NaPSS solutions at 10^{-6} M ionic strength. Dashed line represents the displacement autocorrelation of a Gaussian process.

Conclusions

We probe the mobility of nanoparticles of diameter $100-790$ nm in dilute and semidilute solutions of a model flexible polyelectrolyte, sodium polystyrene sulfonate, at three different ionic strengths (10^{-6}, 10^{-3}, and 10^{-1} M). We find that nanoparticles exhibit Fickian diffusion on experimental time scales with dynamics that become slower as particle size and polymer concentration are increased. Large particles ($R_{\mathrm{NP}} > R_{\mathrm{g}}$) diffuse according to Stokes-Einstein predictions at all ionic strengths. The diffusivities of small particles ($R_{\mathrm{NP}} < R_{\mathrm{g}}$) in polyelectrolyte solutions of low ionic strength, however, exhibit a non-monotonic deviation from the SE prediction that depends on polymer concentration, including a return to SE behavior at high polymer concentrations. Available models for diffusion of particles in solutions of fully flexible Gaussian chains are unable to explain the observed dynamics. In analogy with a physical picture developed for particle diffusion in entangled systems, we suggest that increasing constraints on particle motion due to confinement by the polyelectrolyte chains are responsible for the return to SE diffusion at high concentrations.

The length scale driving this confinement is still unknown. Polymer structure on short length scales may need to be considered to develop models that are capable of capturing particle dynamics in charged polymer solutions. To probe the dynamics of different size particles at the relevant size limit ($R_{\mathrm{NP}} \ll R_{\mathrm{g}}$), different dynamic techniques (such as but not limited to X-ray photon correlation spectroscopy, XPCS, or superresolution microscopy) are required to extend the dynamic range beyond the resolution limit of optical microscopy ($d_{\mathrm{NP}} \sim 100$ nm). A better understanding of the length scales controlling particle dynamics has interesting implications for a wide range of applications requiring diffusion in complex media, including rigid rods,[60] emulsions,[61] and cellular cytoplasm.[42]

Acknowledgements

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