

Minimal Cylinder Analysis Reveals the Mechanical Properties of Oncogenic Nucleosomes

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Abstract

Histone variants regulate replication, transcription, DNA damage repair, and chromosome segregation. Though widely accepted as a paradigm, it has not been rigorously demonstrated that histone variants encode unique mechanical properties. Here, we present a new theoretical approach called Minimal Cylinder Analysis (MCA) that uses strain fluctuations to determine the Young's modulus of nucleosomes from all-atom Molecular Dynamics (MD) simulations. Recently, we validated this computational tool against *in vitro* single-molecule nanoindentation of histone variant nucleosomes. In this report, we further extend MCA to study the biophysical properties of hybrid nucleosomes that are known to exist in human cancer cells and contain H3 histone variants CENP-A and H3.3. Here, we report that the heterotypic nucleosome has an intermediate elasticity (8.5 ± 0.5 MPa) compared to CENP-A (6.2 ± 0.4 MPa) and H3 (9.8 ± 0.7 MPa), and that the dynamics of both canonical and CENP-A nucleosomes are preserved and partitioned across the nucleosome pseudo-dyad. Further, we investigate the mechanism by which the elasticity of these heterotypic nucleosomes augments cryptic binding surfaces. From these analyses, we predict that the heterotypic nucleosome is permissive to the binding of one copy of the kinetochore protein CENP-C, while still retaining a closed DNA end configuration required for linker histone H1 to bind. We discuss that the ectopic deposition of CENP-A in cancer by H3.3 chaperones, HIRA and DAXX, may fortuitously result in hybrid nucleosome formation. Using these results, we propose biological outcomes that might arise when such heterotypic nucleosomes occupy large regions of the genome.

Statement of Significance

Nucleosomes are the base unit of eukaryotic genome organization. Histone variants create unique local chromatin structures that are thought to fine-tune transcription, replication, DNA damage repair, and faithful chromosome segregation. It is becoming evident that the mechanical response of chromatin, through material properties such as elasticity, regulates genetic function.

We developed a theoretical method, validated by previous *in vitro* nanoindentation studies, called Minimal Cylinder Analysis (MCA), to determine the Young's modulus of nucleosomes from Molecular Dynamics (MD) simulations. Here, apply MCA to oncogenic hybrid nucleosomes containing histone H3 variants, from which we postulate biological predictions. MCA allows for inexpensive analysis of MD simulations to discern how diverse, cylindrically shaped macromolecular systems respond to mechanical forces.

1. Introduction

The elastic properties of chromatin regulates genetic function in a manner distinct from classically understood properties such as key binding partners (1). Early evidence of the elastic behavior of chromatin comes from the classic micromanipulation experiments of grasshopper chromosomes (2). Several subsequent studies have shown that chromatin acts as an elastic medium and that its constituent linker DNA behaves as an entropically driven elastomer (3, 4). Such studies on the physics of chromatin have led to new biological insight. For example, the pericentromere, a region flanking the site of microtubule attachment, can act as a mechanical spring, governing chromosome separation and spindle length during mitosis (5). Chromatin physics can help to address questions about chromatin ordering (6–8), how DNA is both stable

and distortable (9, 10), how glassy DNA dynamics give rise to cell-to-cell variability (11), and even how the mechanical micro-environment tunes genetic expression (12, 13). Chromatin states are altered by posttranslational modifications (PTMs) (14) and by histone variant deposition at the macromolecular scale (9). Consequently, the additive effects of nanoscale modifications are an essential component of chromatin chemical signaling pathways and may alter chromatin's mechanical behavior.

Previously, we carried out structural analysis of CENP-A dynamics *in silico* (15). In a subsequent recent study, we also investigated the material properties of CENP-A nucleosomes and binding partners, located primarily at centromeres, and H3 nucleosomes found throughout the chromosome arms (16). More specifically, to gain new insights into the initial effects of kinetochore formation, we performed the first comprehensive *in vitro* nano-indentation study of nucleosomes, experimentally determining their Young's moduli and compared these measurements to our *in silico* predictions, carried out in parallel (16). This report presents our new algorithm to perform elasticity measurements *in silico*, denoted Minimal Cylinder Analysis (MCA), and for the first time outlines the theory and derivation for how to obtain Young's modulus from stain fluctuations of nucleoprotein complexes.

Furthermore, in this work we have applied MCA to investigate the material properties of hybrid nucleosomes containing simultaneously CENP-A and H3.3 histones. Such nucleosomes are found in human cancer cells and appear to be detrimental to chromosome integrity (17, 18). In many aggressive forms of cancer, CENP-A, a centromeric histone H3 variant, is overexpressed (18–20). Studies have demonstrated that either in cancer cells derived from patient tumors, or when artificially over-expressed, excess CENP-A is deposited outside the

centromere, and stably retained there in the form of unexpectedly stable (17) hybrid nucleosomes containing CENP-A and H3.3 (18, 20, 21). This complex has been technically challenging to study experimentally due to its low abundance *in vivo*, therefore, motivating us to rely on MCA to explore the material properties and biological impacts of hybrid CENP-A:H3.3 nucleosomes in cancer cells.

Elasticity, as defined by Hooke's Law, is the ability of a material to return to its initial state after deformation by an applied force. The reversibility of this process implies that mechanical energy is stored as elastic strain energy during deformation and is conserved during recoil (22). Additionally, the proportion of stress to strain in the linear regime is described by Young's modulus. Although Young's modulus is a salient mechanical property of a material, it is applicable for small deformations, and, hence, may not be sufficient to predict all biologically germane deformation processes. The function of elastic materials also depends on extensibility and the amount of work required to fracture the material, referred to as toughness (22). For example, exceptionally tough biological materials exist, such as viscid spider silk, which is far more elastic (0.002 GPa) than Kevlar (130 GPa) and yet is remarkably tougher than Kevlar (150 vs. 50) MJ m⁻³ respectively (22).

There exist several computational approaches to model the elastic properties of macromolecules. One such method is finite element analysis (FEA), where a mesh network describes the structure, and energy is minimized in response to deformation (23, 24). However, the accuracy of this method requires system-specific parameterization to account for atomic interactions such as Coulombic forces. FEA at the nanoscale has produced results consistent with Molecular Dynamics (MD) when informed by atomistic simulation (25), but FEA lacks the

built-in portability and resolution of MD. To achieve all-atom resolution, force-probe MD simulations have been implemented (26, 27). However, large systems such as macromolecular complexes are computationally costly, and unphysical force loading rates are typically required due to short simulation time. Lastly, coarse-grained MD force-fields have also been developed that are, excitedly, able to study the non-elastic deformation and fracture of macromolecules to simulate nanoindentation (28). The longer timescales achieved by coarse-grained methods are promising, but they lack the resolution of all-atom and may not resolve differences due to PTMs or variants. In the methodology we present here, we analyze all-atom resolution simulations of nucleosomes at extended time scales, and then use surface fluctuations to derive the modulus of elasticity in the absence of applied forces. The strength of our methodology is that it does not require expensive computational resources beyond equilibrated simulations.

The elastic modulus is derived by connecting equilibrium strain fluctuations with stress response (29). We employ this logic to obtain the elasticity of nucleosomes without applying an external force. Furthermore, we have introduced a simple temporal hierarchy when implementing our algorithm: first, the equilibrium trajectory is averaged over short timescale windows, and the resulting structures snugly fit into encompassing cylindrical bounding domains. Afterward, the sequence of fluctuating cylinders is analyzed using solid mechanics, while also estimating the energy of the corresponding low-frequency vibrational mode from the equipartition theorem. Overall, our algorithm produces the absolute values of nucleosomes' Young's moduli, without freely adjustable parameters that are tuned to fit any specific experiment.

2. Methods

The goal of our analysis method is to calculate the Young's modulus of nucleosomes in the absence of applied forces. Essentially, this technique connects structural fluctuations observed in unbiased MD simulations, with the nucleosome's mechanical response. To analyze all-atom simulation data in such a way, we first treat the nucleosomes as mechanically homogenous elastic cylinders vibrating in a thermal bath. Next, we calculate the dimensions and fluctuations of what we term "minimal" cylinders over the ensemble of each trajectory. We define the cylinder dimensions as the minimum volume that contains the rigid exterior surfaces of the nucleosome.

To develop a simplified model for elasticity calculations, we make assumptions based on the known physical properties of nucleosomes. First, we apply an averaging technique to all-atom simulation data using continuum mechanics. Elastic continuum theory has been shown to predict material properties on the nanoscale when compared to experiments and analytical predictions (30, 31). We further reduce degrees of freedom and variability by utilizing the pseudo-symmetry and geometry of nucleosomes to treat them as homogenous circular cylinders. Next, we make simplifications on the mode of deformation studied. To compare to single-molecule nanoindentation, we assume that nucleosomes are compressed perpendicular to the axis of the cylinder. Therefore, we model nucleosome fluctuations as compression and expansion in the absence of shearing motions and attribute to this mode an equipartition of energy.

The workflow we used to determine the Young's modulus of nucleosomes from atomistic trajectories is as follows:

- 2.1.1. Define the all-atom nucleosome coordinate system
- 2.1.2. Probe for rigid external cylinder bases and lateral surfaces
- 2.1.3. Retrieve average cylinder dimensions and variances

The output of these steps is then used to calculate the Young's modulus. Next, we will describe in detail each of these steps.

2.1.1. Define the all-atom nucleosome coordinate system

Analogous to the requirement of consistent orientation of nucleosomes in nanoindentation studies, we must first choose a standard nucleosome orientation. The question asked is this: if nucleosomes were to lie 'flat' on a surface, what would this orientation be? The chosen alignment influences the cylinder dimensions that will be measured. Since we constrain our analysis to right circular cylinders, if the nucleosomes are tilted, the measured dimensions will be altered. Prior to analysis, we removed the nucleosome's rotational and translational motions from our trajectories and moved the center of mass (COM) of residues analyzed in MCA to the origin. To define our coordinate system, we computed the principal axes of rotation and oriented the cylinder base to the plane of the first two principal axes (Fig. 1A) (Supporting Material). The nucleosome core particles (NCP), which we analyzed with MCA, were built as described in section 2.2 without flexible histone tails. After simulation, during MCA we did not include in the dataset the first and last ten DNA base pairs from simulation so that the NCP fits more snugly into a cylinder. The coordinates of the protein C- α and nucleic phosphorus atoms were used to calculate the nucleosome dimensions, elaborated next.

2.1.2. Probe for rigid external cylinder bases and lateral surfaces

Since we are measuring elasticity without an applied force, we consider the following thought experiment: if one were to hypothetically push down on the nucleosome surface, at what point would compression become more significantly hindered? Such determination would, in turn, suggest the coordinates of the rigid surface of the nucleosome. For example, an intrinsically disordered region or loop is configurationally highly distortable compared with regions comprised of α -helices or β -strands. The elastic moduli of the former structures, which are largely entropic in origin, are expected to be orders of magnitude smaller compared with the latter, hence, are neglected in our subsequent analysis. Thus, we need a specific metric for local stiffness. The rigidity of residues can be quantified by the root mean square fluctuations, RMSF, of each residue throughout the simulation. High RMSF values correspond to increased fluctuation or decreased stiffness. Since RMSF is a time-averaged parameter, multiple time steps are required to calculate fluctuations of residues. Therefore, we divide the 1 μ s simulation (from 0.6-1 μ s) into a number of temporal segments and output each atom's RMSF per segment.

There are two input parameters in MCA: the 'Averaging Window Length' (AWL), which defines the length of the temporal segments; and the 'Flexible Exterior Residue Number' (FERN), which defines how many residues over an RMSF value, the 'Residue Flexibility Cutoff' (RFC), are excluded from the cylinder volume. We probed for how sensitive MCA is to AWL (Fig. S2A) and FERN (Fig. S3A, B), and explain our parameter choices to analyze nucleosome core particles (Supporting Material). MCA calculates the RFC value, which demarcates rigid and flexible residues and is dependent on AWL (Fig. S2B). Additionally, we plot how the RFC value compares to the atom RMSFs (Fig. S2C).

2.1.3. *Retrieve average cylinder dimensions and variances*

We first sort the C- α and phosphorus atoms by their z-axis coordinates and select the z coordinate of the residue such that the number of residues specified by FERN are minimally excluded outside the cylinder bounds from the top and subsequently the bottom surface. For our analysis of NCPs, we rationally selected a FERN value of 10 residues (Fig. S3). Maximal separation among the remaining coordinates determines the cylinder height, z . We repeat this process for the radial coordinate to calculate the radius, r , of the cylinder per temporal segment. The collection of (r,z) tuples, which are treated as stochastic variables, are histogrammed as illustrated in Fig. 1B for an example trajectory. From this stochastic realization for a given simulation we compute the average of the distributions, z_{avg} and r_{avg} ; and the standard deviations, Δr and Δz . These data are then used in our derivation for the Young's modulus as described below. We have made our MCA code for calculating the Young's modulus available as an open-source tool (32).

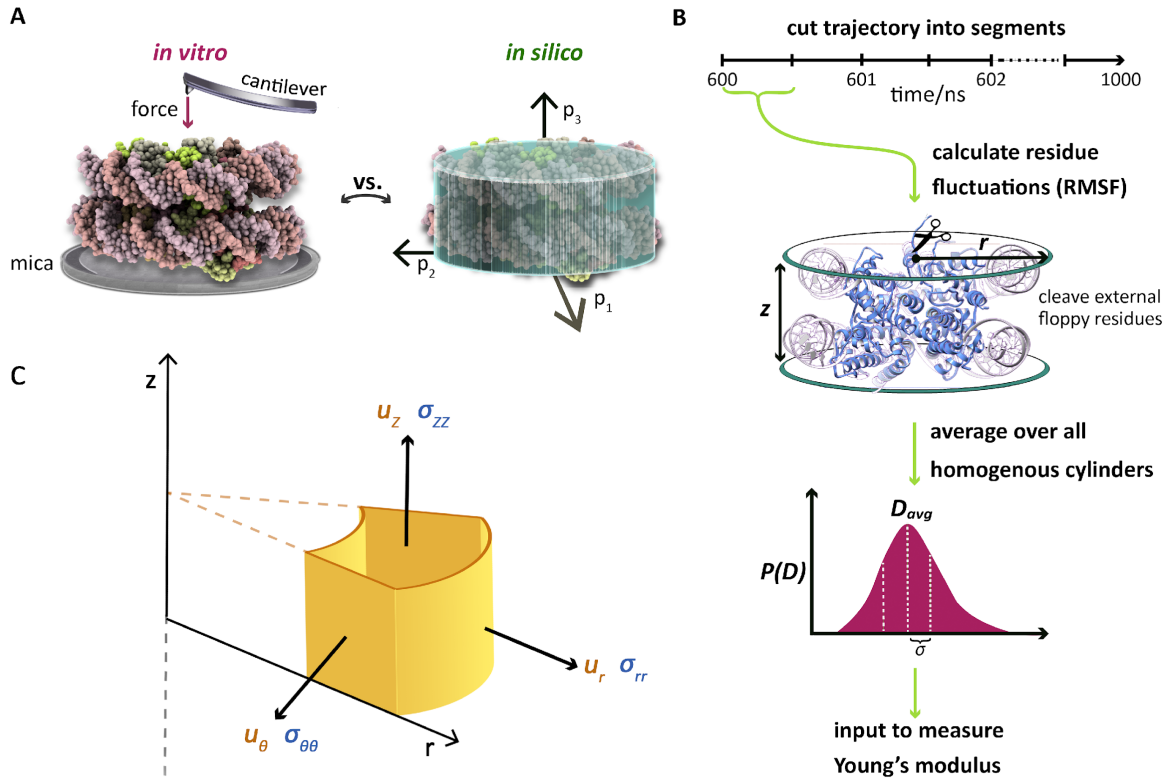


Figure 1: (A) Schematic that compares *in vitro* AFM single-molecule nanoindentation force spectroscopy, left, to our *in silico* modeling and analysis, right. In AFM, the applied force from the cantilever is normal to the mica surface. For our computational analysis, nucleosomes were oriented by the principal axes of the moment of inertia and then modeled as homogenous elastic cylinders. (B) The workflow for calculating Young's modulus *in silico*. Residue RMSF is calculated for each segment of the simulation to obtain an ensemble of cylinders. The average dimensions, D_{avg} , of the radius and height (r , z) and the standard deviation, σ , are then input to calculate Young's modulus. (C) A diagram to show the orientation of cylinders in relation to variables introduced in Eq. 2 and Eq. 4. Displacements (u_r , u_θ , u_z) are shown in yellow. Stresses in the i -th direction from forces applied in the j -th direction, σ_{ij} , are shown in blue.

2.2. All-atom computational modeling

The software suite GROMACS 5.0.4 (33) was used to perform all-atom MD simulations. The force fields used were amber99SB*-ILDN (34, 35) for proteins, amber99SB parmbsc0 (36) for DNA, ions08 (37) for ions, and the TIP3P water model. Two nucleosome systems were built for simulation and compared to our prior simulations of H3 as a control (15). First, the heterotypic CENP-A:H3.3 nucleosome was built from the crystallographic structure PDB ID: 3WTP (17). Subsequently, the CENP-A nucleosome was built with PDB ID: 3AN2 (38). The unresolved residues, CENP-A' 79-83, from the crystal structure (3AN2) were inserted using MODELLER (39). Histone tails were not added to the experimentally solved structures. For energy minimization of the inserted residues, the N- and C-terminus were unconstrained. The 146 base pair α -satellite DNA, PDB ID: 3WTP (17), was aligned to all systems, as a control, using the CE algorithm (40) of PyMOL (41).

We used Gromacs tool `pdb2gmh` to assign residue charges at biological pH around 7 (42): a charge of +1 on Lys (side chain pKa = 10.67) and Arg (side chain pKa = 12.10), 0 for Gln, -1 for Asp (side chain pKa = 3.71) and Glu (side chain pKa = 4.15), and His with hydrogen on the epsilon nitrogen (side chain pKa 6.04) (43). The boundaries of the simulation were set to a cuboid box with a minimum distance of 1.5 nm from the nucleosome with periodic boundary conditions. Counter ions of Na⁺ and Cl⁻ were introduced to neutralize the system and to model an ionic physiological concentration of 150 mM NaCl. The Particle Mesh Ewald method was used for electrostatics with the Verlet cutoff scheme. Coulombic and Van der Waals potentials

were used for non-bonded interactions with a cutoff distance at 1.0 nm. The LINCS algorithm was used to constrain hydrogen bonds.

Energy minimization was performed using steepest descent to a maximum energy of 100 kJ/mol. Following this, equilibration of the structure was carried out. The systems were heated to 300 K for 2000 ps with a DNA position restraint of $K = 1000 \text{ kJ mol}^{-1} \text{ nm}^{-2}$ in the Canonical ensemble. Following this, thermal equilibration was performed for both DNA and protein at 300K for 2000 ps with weak position restraints defined as $K_{\text{het}} = 2.1 \text{e-}5 \text{ kJ mol}^{-1} \text{ nm}^{-2}$ assigned to the heterotypic nucleosome and $K_{\text{cpa}} = 2.5 \text{e-}5 \text{ kJ mol}^{-1} \text{ nm}^{-2}$ for the CENP-A nucleosome. These weak position constraints vary based on atom number in each simulation and restrain nucleosome rotations. Finally, the pressure was equilibrated for 1500 ps in the Isothermal-isobaric ensemble at 300 K, 1.0 bar pressure, and weak position constraint (Fig. S1A).

Each production simulation was run for 1 microsecond at 300 Kelvin. Simulation temperature was V-rescaled using the modified Berendsen thermostat (44) with time constant 1.0 ps. The Parrinello-Rahman barostat (45) was used for pressure regulation at 1.0 bar, time constant of 2.0 ps. To investigate the possibility of barostat pressure regulation resonating with the thermal fluctuations of the nucleosomal dimensions, we calculated the natural frequency of our system (46, 47), treating the nucleosome as a homogeneous elastic cylinder, and found two orders of magnitude difference between the faster barostat coordinate rescaling frequency and the slower axisymmetric, acoustic deformation mode frequency considered in MCA.

A simulation time step of 2 femtoseconds was used and coordinates, velocities, and energies saved every 2 ps. The non-bonded neighbor lists were updated at intervals of 20 femtoseconds.

In order to analyze equilibrated sections of the production runs, the first 600 nanoseconds were not included in analysis. We checked for convergence of the production runs of the heterotypic nucleosome by tracking the change in RMSD from the initial production run configuration (Fig S1B). Published equilibrium analyses of trajectories CENP-A and CENP-A bound to CENP-C are available in Fig. S9 of (16). Equilibration analysis of the control system, H3, is available in Fig. S2 of (15). Detailed methods on all-atom structural analysis are provided in the Supporting Material.

3. Results

3.1. Outline of the derivation of Young's modulus from MCA

We will present here main highlights from the derivation for Young's modulus from MCA. For those interested, a full, extended derivation is also included (Supporting Material). The work done in the deformation of an elastic material is stored in the form of strain energy, U . The strain energy density, u , the energy stored in small volume elements, can be useful to describe variable strains along a body that sum to the total strain energy:

$$U = \iiint_R u(r, \theta, z) r dr d\theta dz . \quad (1)$$

Because the extent of cylinder fluctuations is relatively small, around the range of 0.5 to 1.5 percent of the average radial or lateral dimension, we rely on linear elasticity and small-deformations' theory. Under these conditions, the strain energy density in cylindrical coordinates can be calculated for low magnitude stresses from arbitrary directions (48) as

$$u = \frac{1}{2} \left(\sigma_{rr} \varepsilon_{rr} + \sigma_{\theta\theta} \varepsilon_{\theta\theta} + \sigma_{zz} \varepsilon_{zz} \right) + \left(\sigma_{r\theta} \varepsilon_{r\theta} + \sigma_{\theta z} \varepsilon_{\theta z} + \sigma_{zr} \varepsilon_{zr} \right) = \frac{1}{2} Tr(\sigma \varepsilon) , \quad (2)$$

where σ_{ij} is the stress in the i-th direction from force applied in the j-th direction and ε_{ij} is the strain in the i-j plane (Fig. 1C). Further explanation for the form of Eq. 2 in cylindrical coordinates is provided in section S4 where, briefly, we apply the cyclic property of trace on the second order symmetric tensors, stress and strain, to arrive at Eq. 2 (Supporting Material). In the absence of shear stresses and using Hooke's law, the strain energy density in Eq. 2 can also be written in the form

$$u = \frac{\nu\mu}{1-2\nu}(\varepsilon_{rr} + \varepsilon_{\theta\theta} + \varepsilon_{zz})^2 + \mu(\varepsilon_{rr}^2 + \varepsilon_{\theta\theta}^2 + \varepsilon_{zz}^2), \quad (3)$$

where μ is the shear modulus and is related to Young's modulus, E , by $\mu = E / 2(1 + \nu)$ and ν is the Poisson ratio (48). We used a value 0.4 used in prior nanoindentation simulations of macromolecules (49). For displacements (u_r, u_θ, u_z) in cylindrical coordinates (r, θ, z) as shown in Fig. 1C (50):

$$\varepsilon_{rr} = \frac{\partial u_r}{\partial r}, \quad \varepsilon_{\theta\theta} = \frac{u_r}{r} + \frac{1}{r} \frac{\partial u_\theta}{\partial \theta}, \quad \varepsilon_{zz} = \frac{\partial u_z}{\partial z}. \quad (4)$$

In the special case of a homogeneous axisymmetric cylinder where the center-of-mass is at the

origin (Fig. 1C), $\frac{\partial u_\theta}{\partial \theta} = 0$ and at the walls of the cylinder $\frac{\partial u_r}{\partial r} = \frac{u_r}{r_{avg}}$, (6) which is $\frac{\Delta r}{r_{avg}}$ from

MCA. Therefore, in this specific case, $\varepsilon_{rr} = \varepsilon_{\theta\theta}$ in Eq. 4. More detail on how we arrive at these conclusions is provided (Supporting Material).

To calculate the strain energy density in Eq. 3, we input the dependence of the shear modulus on E and relations found from Eq. 4 to obtain

$$u = \frac{E}{2(1+\nu)} \left[\frac{\nu(\varepsilon_{zz} + 2\varepsilon_{rr})^2}{(1-2\nu)} + \varepsilon_{zz}^2 + 2\varepsilon_{rr}^2 \right]. \quad (5)$$

Strain values in Eq. 5 are calculated from the measured quantities r_{avg} , z_{avg} , Δr , and Δz from MCA (Methods 2.1.3). We next focus on the acoustic cylindrical mode of motion that describes compression in the z-axis along with radial extension (and *vice versa*). Since we are studying only small deformations, or harmonic modes, we estimate the average potential energy from equipartition theorem, $U = \frac{1}{2}k_b T$, where k_b is the Boltzmann constant and T is the simulation temperature, 300 K. We then integrate Eq. 5 over the body volume, Eq. 1, and with the above-mentioned energy from equipartition theorem, we solve for Young's modulus:

$$E = \frac{k_b T(1-\nu-2\nu^2)}{V(\epsilon_{zz}^2 - \nu\epsilon_{zz}^2 + 2\epsilon_{rr}^2 + 4\nu\epsilon_{zz}\epsilon_{rr})} \cdot (6)$$

This final form for the derivation of Young's modulus, shown in Eq. 6 is one of the main findings of this work.

3.2. Experimental validation of MCA model

For our analyses from our previous work (16), we used the Hertz model with spherical indenter geometry for Young's Modulus measurements (51). The Hertz model assumes that the substrate is an isotropic, elastic solid and is valid for small indentations and low forces, in the linear regime. To check for elastic dependence on the point probed, we experimentally measured the Young's modulus across mononucleosomes and found that the effective elasticity is surprisingly homogenous across the surface (16). This finding is consistent with the model of MCA, which treats nucleosomes as homogenous elastic solids.

3.3. Experimental validation for *in silico* Young's modulus calculations

In our study of the mechanical properties of nucleosome variants on the chromatin fiber, we applied our *in silico* methodology to measure the Young's Modulus of nucleosomes (16). We measured the elasticity three systems: (1) the canonical nucleosome, H3, (2) the centromeric variant of H3, CENP-A, (3) and CENP-A nucleosomes bound to CENP-C. We also measured the elasticity of these substrates *in vitro* using single-molecule nanoindentation force spectroscopy. Our *in silico* algorithm to determine Young's modulus quantitatively agrees with *in vitro* nano-indentation measurements (Fig. 2A). Thus, experimental nanoindentation studies provide a validation for our model and suggest that the various assumptions made in MCA are acceptable simplifications.

3.4. *Young's modulus of the hybrid CENP-A:H3.3 vs. the CENP-A nucleosome*

After validating MCA against *in vitro* single-molecule force studies previously (16), we apply this method to study the elastic properties of a heterotypic cancer-specific nucleosome. This unique variant nucleosome has one copy of CENP-A and one copy of H3.3, and is enriched at CENP-A ectopic sites in chromatin (20), some of which are well documented fragile sites in the chromatin fiber (18). The heterotypic nucleosome was found to be surprisingly stable, regardless of the unique docking interface formed between two divergent H3 variants (17). What, then, causes the measured stability?

To explore this question, we computationally assessed the elastic properties of the heterotypic nucleosome. We discovered an intermediate Young's modulus of hybrid CENP-A:H3.3 nucleosomes (8.5 ± 0.5 MPa) compared to CENP-A nucleosomes (6.2 ± 0.4 MPa), and canonical H3 nucleosomes (9.8 ± 0.7 MPa, Fig. 2A). Values for nucleosome dimensions and

standard deviations are provided for a trial from this dataset (Table S1). This result contradicts the idea that unfavorable contacts may form between the CENP-A:H3.3 heterodimer and disrupt the stability of the hybrid nucleosome. Since our methodology uses an averaging technique over the structure of the nucleosome, we next asked how the dynamics of the heterotypic nucleosome gives rise to its intermediate elasticity. Two hypotheses were considered: first, the heterotypic nucleosome presents an averaged global shift in nucleosome dynamics; or secondly, there may be sequestered regions within the heterotypic nucleosome that display canonical or centromeric nucleosome dynamics.

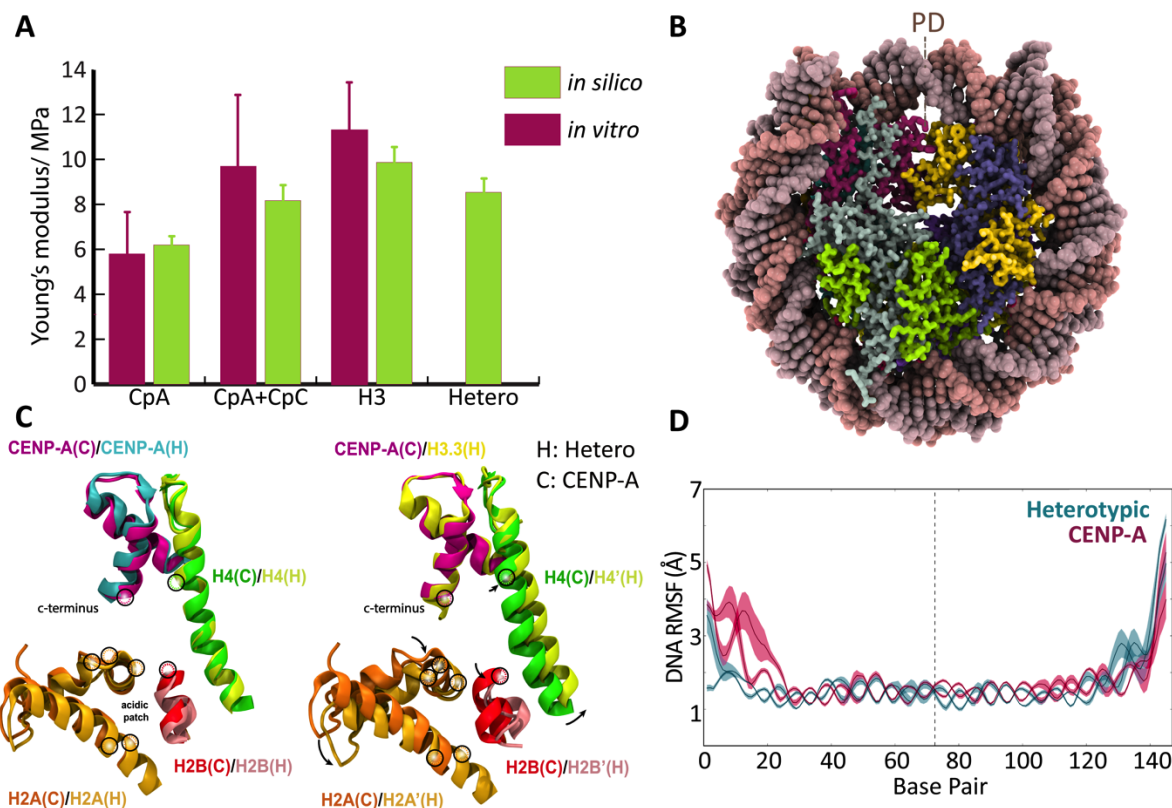


Figure 2: (A) Young's modulus of CENP-A nucleosomes, CpA; CENP-A bound to CENP-C, CpA+CpC; the canonical nucleosome, H3; and the CENP-A:H3.3 containing heterotypic

nucleosome, hetero. AFM measurements *in vitro* are shown in magenta and *in silico* measurements are shown in green. Experimental values are referenced from our companion work (16). (B) The structure of the heterotypic nucleosome. Histones CENP-A are shown in magenta, H3.3 in yellow, H4 in dark slate-blue, H2A in light grey, and H2B in green. (C) The overlay of the CENP-C binding sites by minimum RMSD obtained from the representative structure of the first principal component (Movie S1). Histones labeled with a 'C' are from the CENP-A nucleosome and histones labeled with 'H' are from the heterotypic nucleosome. Black circles indicate CENP-C binding residues. (D) Root-mean squared fluctuations (RMSF) of DNA residues of the CENP-A nucleosome, in magenta, and the heterotypic nucleosome, in blue.

3.5 The rigidified heterotypic nucleosome is permissive to CENP-C binding

The essential docking protein to initiate kinetochore formation is CENP-C, which binds to the surface of CENP-A (52). The structure of the CENP-C binding domain on the surface of the CENP-A nucleosome can be found at Fig. S4A. It is still unknown if the heterotypic CENP-A:H3.3 nucleosome is implicated in the formation of neocentromeres. Consistent with reduced flexibility compared to CENP-A (Fig. 2A), we found a more tightly bound four-helix bundle interface between H3.3 and CENP-A in the heterotypic nucleosome (Fig. S5A, Supporting Material). CENP-C docks by interaction with the c-terminal tail of CENP-A in this region and binds across the nucleosome surface with the basic residues of H2A (residues 60, 63, 89-91 in *Drosophila melanogaster*) and H2B (53).

Therefore, we analyzed the CENP-C binding platform to see if the heterotypic nucleosome is permissive to CENP-C. To do so, we performed Principal Component Analysis (PCA) and

animated the first major mode of motion, the first Principal Component (PC1). Visualization of PC1 revealed that the CENP-A containing tetramer of the heterotypic nucleosome rocks apart less than the H3.3 tetramer and is more compact, similar to the CENP-A nucleosome (Movie S1). Indeed, the heterotypic nucleosome contains asymmetric and partitioned dynamics, where features of CENP-A nucleosome behavior are maintained. In PC1, we see that the CENP-C binding site from the CENP-A nucleosome is preserved in the heterotypic nucleosome (Fig. 2C, left). The acidic patch and c-terminal CENP-A domain provide the scaffold for CENP-C binding (17). On the H3.3 face of the heterotypic nucleosome, the acidic patch, shown as H2A'(H) in light orange, is extended away from the c-terminus of H3.3 (Fig 2C, Fig. S5B). This analysis shows that the correct coordination of binding residues for CENP-C is maintained in the CENP-A facing side of the heterotypic nucleosome, making it permissive to the double arginine anchor mechanism of both the CENP-C central domain, R522, R525 (53), previously observed *in vitro* (17), and to the CENP-C motif, R717, R719 (40), which we modeled *in silico* in our prior work (14). We further discuss the dynamics of the heterotypic nucleosome and the high exposure of the CENP-N binding site, the CENP-A RG loop (Supporting Material).

3.6 DNA dynamics of histone variants is partitioned by the heterotypic nucleosome pseudo-dyad

Intriguingly, linker histones (LHs) are excluded from centromere-specific CENP-A nucleosomes, principally because of a clash with entry/exit dynamics of DNA (54, 55). Thus, a fundamental question is whether CENP-A:H3.3 hybrid nucleosomes are able to bind LHs to form a chromatosome unit similar to the canonical nucleosome (56, 57). The LH globular domain docks to the entry-exit sight of canonical nucleosomes (58), illustrated at Fig. S4B. The

LH disordered tails bind to linker DNA, holding DNA ends together (55). A distinctive difference between H3 nucleosomes and CENP-A nucleosomes is the markedly lower affinity of the latter for LHs (54).

It was experimentally demonstrated that the α N helix in canonical histones binds DNA and restricts DNA end motions, creating a more closed DNA end configuration. In contrast, in CENP-A the α N helix is shorter and experimentally resulted in more open DNA ends and a lack of H1 binding (54). Further, experimentally it was found that unstable entry and exit DNA strands inhibit LH binding (54). A picture of the solved chromatosome structure of the canonical nucleosome bound to the LH globular domain, with the α N helix indicated, is provided for structural reference (Fig. S4B) (59). We asked how the intermediate rigidity of the heterotypic nucleosome (Fig. 2A) affects DNA dynamics.

First, we calculated the root-mean-square fluctuation (RMSF) of DNA over three segments of our analyzed trajectories. We found that the presence of both CENP-A and H3.3 results in a symmetry breaking in DNA dynamics across the pseudo-dyad (Fig. 2D). We observed increased DNA motion in the heterotypic nucleosome proximal to the CENP-A histone in contrast to the H3.3 histone. This region is of interest because the globular domain of H1 binds to the DNA minor groove on-dyad (60).

Furthermore, the asymmetry in DNA dynamics propagates to the DNA entry-exit ends. In the heterotypic nucleosome, we found increased DNA end fluctuations on the end proximal to CENP-A and decreased fluctuations proximal to H3.3 (Fig. 2D). The disordered tails of H1 rely on the presence of DNA crossing at the entry and exit ends for nucleosome affinity and to compact the fiber (60, 61). Therefore, we next measured the DNA end-to-end distance in

comparison to CENP-A nucleosomes. We found that the DNA ends of the heterotypic are closer together with a probability similar to that of canonical nucleosomes (Fig. S5D). More open configurations were least likely to occur by the heterotypic nucleosome Fig. S5D). The increased likelihood of close DNA end configurations suggests that heterotypic nucleosomes may bind LHs.

The principal, somewhat unexpected finding from these simulation analyses is that neither the H3.3 or CENP-A histone dominates the hybrid particle's properties. Indeed, the heterotypic nucleosome displays the dynamics of *both* canonical and centromeric nucleosomes, resulting in an overall intermediate elasticity. Our findings show that the presence of one H3.3 histone variant induces increased rigidity whereas the CENP-A histone intrinsically induces a more elastic phenotype. These results provide further structural analysis for experimental findings that reported on the surprising thermal stability of the CENP-A:H3.3 containing nucleosome (17).

Discussion

When CENP-A is overexpressed in human cancer cells (18, 62, 63), CENP-A appears to take advantage of H3.3 chaperones, such as HIRA and DAXX (19, 20). The role of H3.3 chaperones in CENP-A deposition away from the centromere provides a logical pathway for the formation of hybrid CENP-A:H3.3 nucleosomes as dimer H3.3/H4 and CENP-A/H4 pairs may fortuitously co-assemble into tetramers on the DNA at regions of high turnover (64–66). Indeed, H3.3 chaperones are implicated in the ectopic formation of heterotypic nucleosomes in cells with increased survivability in the presence of DNA damage (20) and with increased DNase I sensitivity (18, 19).

The formation and retention of heterotypic nucleosomes on the chromatin fiber could be further augmented by our findings here that CENP-A:H3.3 hybrid is more rigid (8.5 ± 0.5 MPa) than CENP-A alone (6.2 ± 0.4 MPa) (Fig. 2A). It is important to note that elasticity in the linear regime cannot be extrapolated to either fracture or thermodynamic stability. However, it has been shown that CENP-A nucleosomes are less thermodynamically stable and disassemble more easily than H3 *in vitro* by NAP-1 or heparin destabilization (61), and by magnetic tweezers (67). Intriguingly, the cause for H3 stability was shown to be a more closed DNA end configuration (61). We found that the heterotypic nucleosome had the highest likelihood of being in a closed DNA end configuration (Fig. S5D). Indeed, the heterotypic nucleosome was measured to have higher thermal stability than CENP-A nucleosomes (17). The heterotypic nucleosome may then be a safe harbor for ectopically located CENP-A histones to be less easily evicted. In other words, the structural features of these hybrid particles might be part of the reason why they persist ectopically, whereas non-hybrid CENP-A nucleosomes may be more readily removed by transcription or remodeling, were they to stochastically accumulate ectopically in normal conditions (68).

Even more fascinating to consider is the dynamics of the heterotypic nucleosome, which is predicted to alter the accessibility of cryptic bindings sites, resulting in downstream biological effects. For example, our findings suggest that heterotypic nucleosomes are competent to bind CENP-C, the structural scaffold for inner kinetochore assembly (69) while still retaining the ability to bind LH H1. The CENP-A:H3.3 containing nucleosome binds the CENP-C central region *in vitro* (17) and ectopic mislocalization of CENP-A results in neocentromeres (18, 19, 21, 63, 70). However, the biological impact of these phenomena depends on the subsequent

recruitment of proteins for microtubule attachment, and whether H1 could interfere with the binding affinities or steric space normally available to kinetochore proteins. Minimally, bound LHs or inner kinetochore proteins may further rigidify the heterotypic nucleosome and facilitate CENP-A retention ectopically.

Conclusion

The elasticity of nucleosomes has biological relevance due to the mechanical sensing of large macromolecules and histone variant-specific assemblies such as, in the case of CENP-A, CENP-C and the entire inner kinetochore complex. In the absence of irreversible distortions to the structure, where binding partners or nanomachines exert forces in the elastic range, our newly developed method, MCA, can be applied to measure Young's moduli of various nucleosome complexes that are of low abundance in cells of specific lineages.

Our quantitative elasticity measurements of nucleosomes are likely to also be tunable in varied contexts of biological systems. One process that could alter the elasticity of the nucleosome variants measured here is the presence of binding partners such as proteins, DNA, or RNA. The charge environment, considering the plethora of posttranslational modifications of nucleosomes (71), is also likely to affect the *in vivo* elasticity of nucleosomes and may differ noticeably from the Young's moduli calculated here. Interestingly, nucleosomes are highly responsive to charge perturbations, and slight changes in histone core charge from physiological values thermodynamically destabilize the nucleosome and can cause DNA unwrapping (72). In contrast to these thermodynamic studies, it is still unknown to what extent individual or combinations of site-specific charge modifications alter the elasticity of nucleosomes. Our

specific quantitative elasticity measurements are therefore dependent on the environment and state of the nucleosome variant.

The specific structural features of nucleosomes or macromolecules are highly controlled *in silico*. When performing elastic studies *in vitro*, additional sources of potential error arise from structural inhomogeneity and orientation and must be rigorously controlled for (16). In order to make testable predictions *in vivo*, it is then important to consider the specific state of the macromolecule of interest due to increased complexity, inhomogeneity, and cell cycle dependent ensembles of structural states.

A significant benefit of MCA is that it can be applied to equilibrium trajectories, enabling a computationally efficient way to analyze new or existing time-continuous simulations. This has the advantage of providing a means to obtain elastic measurements without doing a series of stretching studies on large systems where single all-atom trajectories are already costly. However, we would like to note that sufficiently long simulations, such the microsecond simulations presented here, are required to produce a sufficient number of decorrelated segments needed to achieve convergence. In future research, MCA could be extended to different geometries, varied modes of deformation, or augmented to calculate other mechanical properties.

Author Contributions

Conceptualization of MCA: MP, GAP; Conceptualization of Oncogenic Project: YD, GAP.

Derivation: MP; Methodology and code: MP; Investigation: MP; Writing: MP, GAP, and YD.;

Funding Acquisition: GAP, and YD; Visualization: MP; Supervision: GAP and YD.

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Supporting Citations

References (73–75) appear in the Supporting Material.

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