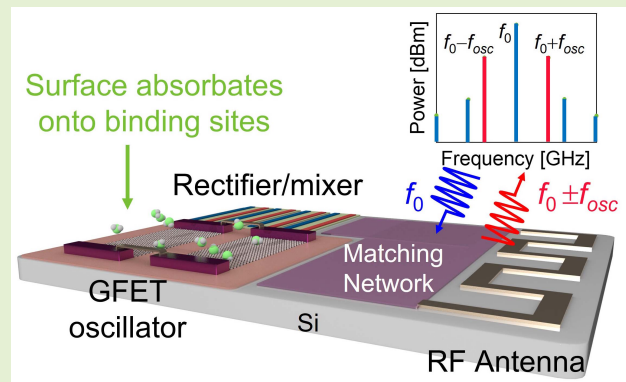


A Lightweight, Zero-Power Intermodulation Sensor Based on the Graphene Oscillator

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Abstract—Wireless sensor networks (WSNs) require a massive number of sensor nodes for data collection and storage, for which the power management and area efficiency of battery-powered sensors may be an issue. In this article, we propose and numerically study a fully passive and lightweight intermodulation sensor based on the reconfigurable graphene field-effect transistors (GFETs) oscillator and passive frequency mixer. The output frequency of the self-powered GFET-based oscillator can be sensitive to the surface doping effect caused by charged surface absorbates, reactive gases, contaminations, or aqueous solutions. In the intermodulation sensor, the low-frequency signals generated by GFET oscillator are mixed with the incident radio frequency (RF) waves, forming the retransmitted and the RF intermodulation signals. Since the intermodulation products do not mess up with the reception signal, the unwanted clutters, self-jamming, and interferences can be effectively suppressed. Our results show that the output frequency of the GFET oscillator can sensitively respond to charged molecules, and such information can be encoded in the backscatter intermodulation signal. We believe that our GFET-based intermodulation sensor may be beneficial for a variety of the Internet of Things (IoT), remote sensing, and environment monitoring applications.

Index Terms—Clutters, fully passive wireless sensor, graphene field-effect transistor (GFET), intermodulation, radio frequency (RF) sensor, self-jamming.



I. INTRODUCTION

COMPACT and energy-efficient wireless sensors capable of continuously monitoring the environmental parameters, such as temperature [1], [2], pressure [3], [4], light intensity [5], humidity [6], and air quality [7], are essential in wireless sensor networks (WSNs) [8], [9], [10] and the Internet-of-Things (IoT) [11], [12] applications. The ever-increasing demand for these countless sensors has brought several challenges, such as how to design power- and area-efficient sensors and how to operate in rich-scattering indoor and urban environments. To resolve these challenges, various types of passive wireless sensors have been proposed,

such as backscatter radio frequency identification (RFID) [13], [14], surface acoustic wave (SAW)-based RFID [15], chipless resonant tags [16], [17], [18], near-field LC sensors [19], [20], and harmonic transponder sensors [21], [22], [23], [24]. These passive wireless sensors are expected to reduce the maintenance cost and power consumption of WSNs, while increasing the lifetime, when compared with active battery-powered sensors [25], [26]. However, these devices more or less face one of the aforementioned problems. For instance, a miniature sensor is usually integrated with the passive backscatter RFID to wirelessly transmit the sensor information in the form of amplitude modulation (AM) or frequency modulation (FM). However, clutters, self-jamming, and electromagnetic interferences existing in noisy environments may affect the sensing accuracy and reliability and also shorten the readout distances of the RFID systems [27]. Although wireless sensors based on the harmonic transponders can effectively suppress interferences [28], [29], [30], they lack spectral efficiency (due to the use of harmonics) and could increase the design complexity and area of readers and sensors.

The concept of clutter suppression using intermodulation responses was first proposed for radar systems and then extended to wireless sensing, such as readout of

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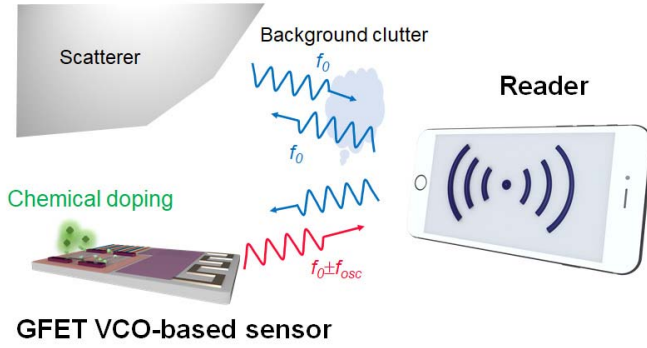


Fig. 1. Schematic of sensing setup of GFET intermodulation sensor in a cluttered environment. The GFET sensor can sensitively respond to the chemical doping (e.g., surface adsorbates or charged molecules) by a retransmitted and frequency-reconfigurable intermodulation signal, which does not mess with the incident RF signal.

micromachined wireless sensors that have a very small footprint [31], [32]. The main advantage of intermodulation-based sensors over harmonic-based sensors is that the frequency offset is much smaller, which not only facilitates circuit and antenna design to reduce area occupation but also improves the spectral efficiency to meet frequency compliance. Moreover, intermodulation sensors can still effectively suppress interferences as their harmonic counterparts. Despite of these advantages, the intermodulation sensors in [33] and [34] generally require at least two separate modules: a local oscillator implemented by nonlinear elements (e.g., MOSFETs, diodes, etc.) and a sensing module, such as a commercial capacitive sensor [33], which will increase the design complexity, device area, and cost due to packaging and integration.

To overcome this challenge, we herein propose a lightweight graphene field-effect transistor (GFET)-based intermodulation sensor for the detection of charged molecules in the air or aqueous solutions, as shown in Fig. 1. Graphene has been intensively studied owing to its excellent electronic, mechanical, and thermal properties [35], [36], [37], [38]. The linear and gapless energy dispersion at Dirac point, resulting in a relatively low density of states, make the graphene devices very sensitive to electrostatic or chemical doping environments [39], [40], [41]. To date, researchers have proposed a variety of applications of such Dirac material, ranging from ultrasensitive biosensors [23], [42], protein sensors [43], gas sensors [44], deoxyribonucleic acid (DNA) and aptamer sensors [45], [46], high-frequency field-effect transistors (FETs) [47], and tunable plasmonic devices [48], [49], [50]. Among those lines, the GFETs have gained their great success due to the remarkable ambipolar transfer ($I_{DS} \sim V_{GS}$) characteristics. A zero drain-to-source current may be achieved when the applied gate voltage equals to the Dirac voltage [51], which is also referred to as the charge neutrality point (V_{cnp}). According to the charge conservation on the graphene channel, any charged carrier absorbed on the graphene surface may lead to the shift of V_{cnp} . In addition, the mobility of carriers in the graphene layer may respond to the variation of charged carrier density, varying dynamically the drain-to-source current.

Fig. 2 shows the proposed intermodulation sensor, which comprises a radio frequency (RF) antenna, a rectifier/mixer, and a GFET-based oscillator (which simultaneously serves

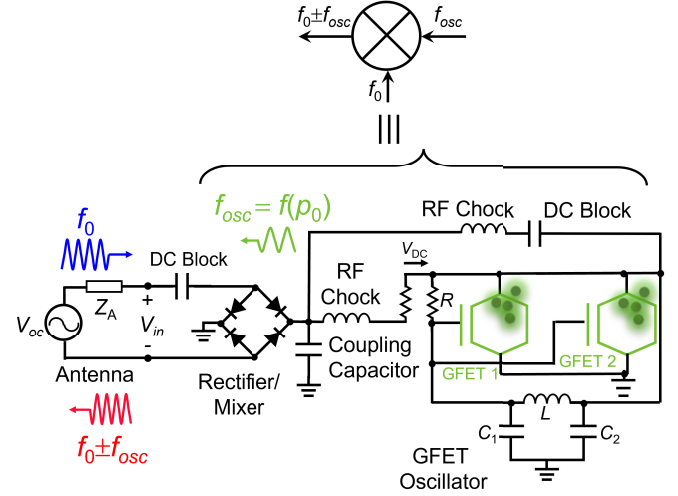


Fig. 2. Circuit diagram of GFET intermodulation sensor composed of an RF antenna, a full-bridge diode rectifier/mixer, and a nonbuffered inverter-based oscillator formed by two GFETs.

as the frequency synthesizer and the sensing element). This intermodulation sensor receives the incident radio signal at fundamental frequency f_0 (2.4 GHz) and transmits the modulated signal at the intermodulation frequency $f_0 \pm f_{osc}$, where f_{osc} (a few megahertz) is the output frequency of the GFET oscillator. Due to the orthogonality between frequencies f_0 and $f_0 \pm f_{osc}$, clutter and interference problems found in traditional backscatter RFID sensor systems can be resolved [13], [14], [15]. Since $f_{osc} \ll f_0$, a single RF antenna can be used to receive the interrogation RF signal and transmit the intermodulation signal. The diode rectifier shown in Fig. 2 can convert the RF energy into dc electricity to power up the oscillator and also serve as the nonlinear element to mix the received RF signal with the local oscillator signal to generate the intermodulation signal. When the graphene channel in the back-gate GFET is exposed to (bio)chemical agents, molecules, or reactive gases, the surface doping effect could shift the output frequency of local oscillator f_{osc} , thereby encoding the sensor information in the FM results. Compared to current harmonic and intermodulation sensors, which are generally bulky and require an additional power source (e.g., battery or solar cell), the proposed self-powered GFET-based intermodulation sensor does not require any additional energy source. More interestingly, due to the unique chemically sensitive electronic properties of graphene, a back- or side-gate GFET can simultaneously function as both a frequency synthesizer and a sensor, making the entire system compact and lightweight.

II. RESULTS AND DISCUSSION

A. Characteristics of GFET

Fig. 3(a) illustrates the back-gate GFET studied in this article, which has a surface functionalized graphene channel with receptors to selectively capture the (bio)chemical agents of interest. Here, we used a physics-based compact model to study the performance of GFET circuits. First, we measured the commercial GFETs (GFET S10 chip from Graphenea Inc.)

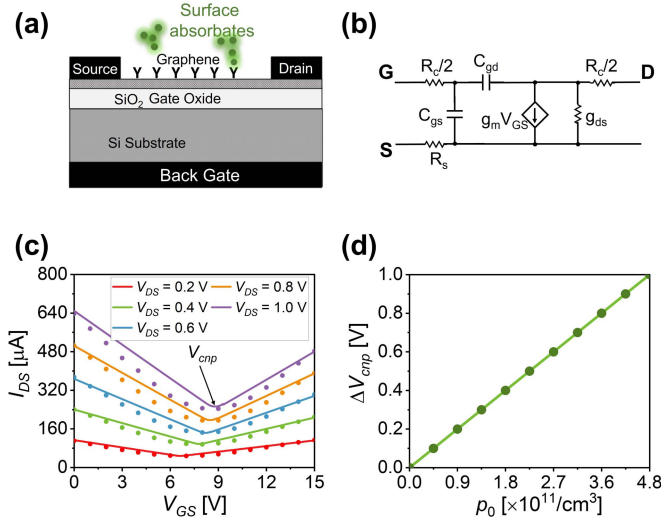


Fig. 3. (a) Schematic of a back-gate GFET and (b) its small-signal model. (c) Electrical characteristics of a back-gate GFET under different drain-to-source voltages ($V_{DS} = 0.2\text{--}1.0\text{ V}$); here, solid lines and dots represent the simulation and experimental results, respectively. (d) Simulated V_{cnp} against the surface impurity density in the GFET channel.

to verify our compact model. The monolayer graphene channel was grown using the chemical vapor deposition (CVD) and then transferred onto the silicon on insulator (SOI) substrate with a 90-nm-thick SiO_2 . Graphene channels were patterned using the oxygen plasma, and the source and drain electrodes (Ti/Au) were patterned using the electron beam evaporation. The important device parameters of the GFETs under test are listed in the following. The SiO_2 gate oxide has a thickness $t_{ox} = 90\text{ nm}$ and dielectric constant $\epsilon_{ox} = 4$. The length and the width of graphene channel are $L = 50\text{ }\mu\text{m}$ and $W = 50\text{ }\mu\text{m}$, respectively.

The I - V characteristics of the GFET can be obtained from the drift-diffusion transport model, where the drain-to-source current is given by [52]

$$I_{DS} = qW |Q_s(x)| v_{drift}(x) = \frac{W}{L_{eff}} \int_0^{V_{DS}} \mu_{eff} |Q_s| dV. \quad (1)$$

where q is the charge of a single electron, $L_{eff} = L - \int_0^{V_{DS}} 1/v_{sat} dV$ is the effective channel length resulting from the saturation drift velocity of carriers v_{drift} , which is assumed to be half of the Fermi velocity $v_F = 10^8\text{ cm/s}$, μ_{eff} denotes the effective carrier mobility, and V_{DS} represents the channel voltage drop across the graphene channel (see Appendix for explicit expressions of surface charge density Q_s and I_{DS}). The effective carrier mobility in (1) can be expressed as [53]

$$\mu_{eff} = \frac{n\mu_n + n\mu_p + n_{pud}(\mu_n + \mu_p)/2}{n + p + n_{pud}} \left(\frac{m}{m + V_{ch}^2} \right) \times \frac{1}{1 + (T/T_{ref} - 1)^\beta} \quad (2)$$

where, according to the experimental measurements, $\mu_n = 1450\text{ cm}^2/\text{V} \cdot \text{s}$, $\mu_p = 1650\text{ cm}^2/\text{V} \cdot \text{s}$, $n_{pud} = 1.65 \times 10^{12}\text{ cm}^{-2}$, $m = 1$ is an empirical fitting parameter, $T_{ref} = 300\text{ K}$, and $\beta = 3$. It is known from (2) that the surface charge density may influence the carrier mobility and hence the output

current of the GFET. Then, the transconductance and the drain conductance of the GFET can be, respectively, calculated as $g_m = dI_{DS}/dV_{GS}|_{V_{DS}=\text{const}}$ and $g_{ds} = dI_{DS}/dV_{DS}|_{V_{GS}=\text{const}}$. Fig. 3(b) shows the small-signal model of the GFET in (a), where the contact resistance is assumed to be $R_c = 0.12\text{ }\Omega$ [54], [55]. The influence of charged impurities, such as surface absorbates and chemical dopants in the graphene channel, which perturb the GFET's electrical characteristics, can be obtained from the charge conservation relation given by

$$C_{ox}(V_{GS} - V_{cnp} - V(x)) + Q_s = 0 \quad (3)$$

where C_{ox} is the gate oxide capacitance, $V(x) = (x/L)V_{DS}$, and x signifies the position along the channel. The charge neutrality points V_{cnp} with the minimal drain-to-source current depend on the charged impurities absorbed onto the graphene surface. Therefore, upon receptor binding, the density of targeted (bio)chemical agents and molecules could p- or n-shift the V_{cnp} . Here, we assume a positively charged surface absorbates absorbed on the graphene channel, which triggers the p-doping effect and makes the V_{cnp} shift toward the positive direction ($\Delta V_{cnp} > 0$). Fig. 3(c) shows the simulated I - V curves (solid lines) of the back-gate GFET under different drain-to-source voltages; here, the experimental results (dots) are also shown for making a comparison. It can be seen from Fig. 3(c) that increasing the modeling and measurement results is in a good agreement, except for the proximity of the charge neutral point (which could be ascribed to the existence of electron-hole puddles due to the fabrication flaws). Fig. 3(c) has fundamentally demonstrated that our physical compact model can predict the performance of GFET very well.

After validating the developed compact model of the back-gate GFET, we will use this compact model to design and simulate GFET-based voltage controlled oscillator (VCO). In order to achieve a higher drain-to-source current for the VCO operation, we assume $L = 7\text{ }\mu\text{m}$ and $W = 2500\text{ }\mu\text{m}$, and the rest device parameters are the same as those used in Fig. 3(c). Fig. 3(d) shows the variation of V_{cnp} with respect to the density of charged absorbates on the graphene surface. It can be seen that when the density of positively charged dopants (p_0) increases from 0 to $4.8 \times 10^{11}/\text{cm}^2$, a strong p-shift of V_{cnp} can be obtained. This linear relationship between the p-shift of V_{cnp} and the surface impurity density can be written as: $qp_0 = C_{ox}\Delta V_{cnp}$. Both μ_{eff} and V_{cnp} are affected by (bio)chemical agents, gases, and molecules appearing on the graphene surface, altering the electrical characteristics of a back- or side-gate GFET. As a result, an oscillator built based on GFET can be chemically sensitive and has a reconfigurable output frequency. This is very different from traditional CMOS oscillator and will provide a lightweight and highly integratable solution for making wireless biomolecular sensors, gas and air-quality sensors, humidity sensors, and so on.

B. Design and Evaluation of GFET Intermodulation Sensor

Fig. 2 shows the design and circuit diagram of the proposed GFET intermodulation sensor, which consists of: 1) a full-bridge diode rectifier with a matching network; 2) a chemically

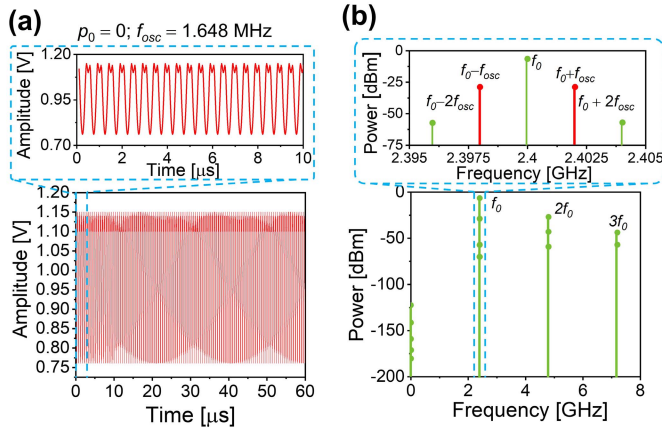


Fig. 4. (a) Time-domain waveform (transient response) of the GFET oscillator in the initial (undoped) status. The zoomed-in view window depicts the oscillation within first 10 μ s. (b) Power spectrum of the output RF harmonic and intermodulation signals. The zoomed-in view window shows the intermodulation signals centered at the interrogation frequency (2.4 GHz). Here, the input power at the antenna terminal is 0 dBm.

sensitive GFET-based oscillator; and 3) an RF antenna. Both the antenna and the rectifier are designed to operate near 2.4 GHz (f_0), which embraces the industry, science, and medical (ISM) band for many applications. The oscillator is designed based on the physics-based compact model ($L = 7 \mu\text{m}$ and $W = 2500 \mu\text{m}$) and a nonbuffered inverter topology, which can operate under a low-power bias condition, with the important design parameters: $C_1 = 68 \text{ pF}$, $C_2 = 210 \text{ pF}$, $L = 180 \mu\text{H}$, and $R = 10 \text{ M}\Omega$ (see Fig. 2). For pristine graphene without doping (i.e., $V_{\text{cnp}} = 0 \text{ V}$), the output frequency of the GFET oscillator is $f_{\text{osc}} \approx 1.648 \text{ MHz}$. The resistor R in Fig. 2 acts as the feedback loop of the oscillator to stabilize the oscillation of the system. The full-bridge diode rectifier not only converts the RF energy to dc electricity for biasing oscillator but also acts as a frequency mixer to generate the intermodulation products. Based on the small-signal model in Section II-A, we performed numerical simulations using the Advanced Design System (ADS) to analyze the proposed GFET-based intermodulation sensor. The proposed GFET-based VCO can be manufactured using the standard lithography and interconnection processes for the integration circuits (ICs). The RF antenna can be integrated into a package along with the GFET chip.

We first assume that the rectifier receives 0-dBm RF power at 2.4 GHz from the input (feed point) of the antenna and the graphene channel is undoped. It can be seen from Fig. 4(a) that the GFET oscillator can successfully oscillate under the bias voltage produced by the rectifier, with the oscillation frequency $f_{\text{osc}} \approx 1.648 \text{ MHz}$. The transient response shown in Fig. 4(a) demonstrates a high-quality and stable oscillation at the time range of interest, especially the first 10 μ s in the zoom-in window. This endows the intermodulation signal great readability and robustness. Here, we should note that since $f_{\text{osc}} \ll f_0$, the intermodulation frequency $f_0 \pm f_{\text{osc}}$ is still within the operating bandwidth of the antenna. Compared to

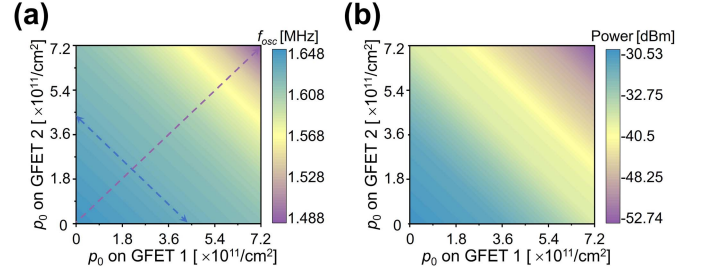


Fig. 5. Contours of (a) output oscillation frequency f_{osc} and (b) peak power at f_{osc} as a function of the surface impurity densities in GFET 1 and GFET 2 for the GFET oscillator shown in Fig. 2.

the graphene harmonic sensor that requires two antennas or diplexer for handling the fundamental frequency input (f_0) and the second harmonic output ($2f_0$) [28], [56], [57], this GFET-based intermodulation sensor requires only one antenna and operates in the same spectrum (which is compatible to the frequency-hopping spread spectrum or FHSS system in 2.4-GHz band), thereby significantly reducing the sensor size and the design complexity of the system. In addition, when compared with current intermodulation sensors, this self-powered GFET oscillator can remove the power units (e.g., battery or solar cell) to squeeze the overall area occupation of the sensor. The calculated power levels of the intermodulation signals and their harmonics are presented in Fig. 4(b), where we notice from the zoom-in window that the intermodulation signals ($f_0 \pm f_{\text{osc}}$) are close to -30 dBm with the carrier signal f_0 at -4 dBm power level, which is sufficiently high for the far-zone wireless sensing applications. The results depicted in Fig. 4 reveal that the intermodulation signal with sensing information ($f_0 \pm f_{\text{osc}}$) embedded can propagate for a relatively long distance and be distinguishable from the background noise floor ($\sim -100 \text{ dBm}$).

Next, we will evaluate the sensitivity of the GFET intermodulation sensor. We consider that the two GFETs (GFET 1 and GFET 2) in the oscillator can absorb charged impurities independently. The oscillation frequencies and their power levels as functions of p_0 introduced to GFETs 1 and 2 are shown in Fig. 5(a) and (b), respectively. From Fig. 5(a) and (b), it can be seen that both the oscillation frequency and the power level are sensitive to the total surface charge density (i.e., concentration of surface adsorbates) in the two GFETs. For instance, the sum of p_0 ($p_0 = 3.6 \times 10^{11} / \text{cm}^2$) applied onto the two GFETs is a constant along the blue dashed line, which corresponds to an unvaried oscillation frequency and the power modulation along this line. On the contrary, when the sum of p_0 disturbing the two GFETs increases along the purple dashed line from $p_0 = 0 / \text{cm}^2$ to $p_0 = 7.2 \times 10^{11} / \text{cm}^2$, the frequency oscillation is varied from 1.648 to 1.488 MHz, while the power level of the oscillation is detuned from ~ -30 to $\sim -52 \text{ dBm}$. Such a result demonstrates that the performances (i.e., oscillation frequency shift and power level modulation) of the GFET intermodulation sensor are determined by the total charged impurities in the two GFETs. Therefore, in the following analysis, we use p_0 to represent the total impurity density in the intermodulation sensor.

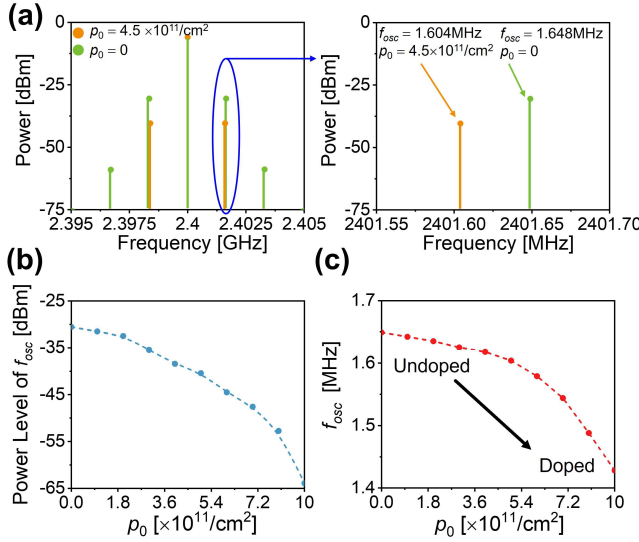


Fig. 6. (a) Output power spectra of the GFET intermodulation sensor before and after surface doping. The zoomed-in view window clearly shows that the frequency shift and the power modulation at f_{osc} are sensitive to binding of surface impurities on the graphene surface. (b) and (c) Modulation in power and output frequency of the GFET oscillator, in response to the increase in total surface charge density in the GFETs. Here, the input power at the antenna terminal is 0 dBm.

Fig. 6(a) shows the power spectra of the output intermodulation products at $p_0 = 0/\text{cm}^2$ and $p_0 = 4.5 \times 10^{11}/\text{cm}^2$. The zoom-in window clearly shows that the intermodulation signal ($f_0 + f_{\text{osc}}$) is shifted from 2401.648 to 2401.604 MHz, with the peak power being reduced from ~ -30 to ~ -40 dBm. Fig. 6(b) reports the dependency of the output power of intermodulation signal on the concentration of charged impurities p_0 , showing that the conversion loss increases with increasing p_0 and a descent interrogation distance estimated by the Friis transmission formula. Fig. 6(c) reports the dependency of the output frequency of GFET oscillator on p_0 , showing a shift from 1.648 to 1.488 MHz when the chemical dopant concentration increases. Such results suggest good sensitivity and resolvability. It is also worth mentioning that the proposed GFET-based intermodulation sensor may be integrated with a specific projection layer for maintaining uniform temperature, thereby stabilizing the sensor's performance. In this proof-of-concept demonstration, structural and material parameters of GFET were not yet optimized to achieve the maximum nonlinear frequency conversion efficiency. In a word, our work has demonstrated the feasibility of making a compact, lightweight, and fully passive GFET intermodulation sensor.

III. CONCLUSION

We have proposed a compact, lightweight, and fully passive intermodulation sensor based on a self-powered and reconfigurable GFET oscillator and a simple RF circuit. We have numerically analyzed the sensing performance of the intermodulation sensor, showing that the power and frequency of the backscattered intermodulation response are very sensitive to the amount of surface absorbates bound to the

graphene surface (e.g., receptors or binding sites of surface-functionalized graphene). Our simulated results also show that, similar to harmonic sensors, the intermodulation sensor that receives and retransmits at different frequencies can be robust to clutters, self-jamming, and electromagnetic interferences. However, an intermodulation sensor has several advantages, such as reduced design complexity and device area, as well as much improved spectral efficiency, when compared with harmonic sensors. We expect that the GFET intermodulation sensor could pave the way for a wide variety of applications, including real-time detection of reactive gases, molecules, contaminations, and (bio)chemical agents, of essential importance for IoTs, WSNs, point-of-care testing, and wake-up radio systems.

APPENDIX

A. Transfer Characteristics of GFET

The drift-diffusion transport model suggests that the drain-to-source current takes the form of (1), where the mobile charge density Q_s in graphene is obtained as: $Q_s = q \times (p - n)$. Here, the electron and hole sheet densities (n and p) in graphene can be derived by integrating the density of states $D(E)$ weighted by the Fermi-Dirac distribution $f(E)$, which can be written as

$$\begin{aligned} n(E_F) &= -\frac{2}{\pi} \left(\frac{K_B T}{\hbar v_F} \right)^2 \text{Li}_2 \left[-e^{-qE_F/(K_B T)} \right] \\ p(E_F) &= -\frac{2}{\pi} \left(\frac{K_B T}{\hbar v_F} \right)^2 \text{Li}_2 \left[-e^{qE_F/(K_B T)} \right] \end{aligned} \quad (4)$$

where the dilogarithm Li_2 is a special case of the polylogarithm $\text{Li}_n(\cdot)$ for $n = 2$, E_F is the Fermi level, $\hbar$ is the reduced Planck constant, v_F denotes the Fermi velocity ($v_F = 10^8$ cm/s), and K_B is the Boltzmann constant. By applying (4), the total mobile charge density can be expressed as

$$\begin{aligned} Q_s &= q \times (p - n) \\ &= q \times \left(\int_{-\infty}^0 D(E)[1 - f(E)]dE - \int_0^{\infty} D(E)f(E)dE \right) \\ &= q \frac{2}{\pi (\hbar v_F)^2} \int_0^{\infty} E \left[\frac{1}{e^{(E+E_F)/(K_B T)} + 1} - \frac{1}{e^{(E-E_F)/(K_B T)} + 1} \right] dE. \end{aligned} \quad (5)$$

The surface potential of the graphene channel V_{ch} is related to the Fermi level E_F , which is a function of the gate voltage V_{GS} given by [53], [58], [59], [60], [61], [62], [63], [64], [65], [66]

$$V_{\text{ch}}(x) = E_F(x)/q = \frac{C_{\text{ox}}}{C_{\text{ox}} + 0.5C_q} (V_{\text{GS}} - V_{\text{cnp}} - V(x)) \quad (6)$$

where $C_{\text{ox}} = \epsilon_{\text{ox}}/t_{\text{ox}}$, ϵ_{ox} and t_{ox} are the dielectric constant and thickness of the oxidation layer, respectively, x is the position along the graphene channel, and C_q is the quantum capacitance having the expression of

$$C_q = \frac{\partial Q_s}{\partial V_{\text{ch}}} = \frac{2q^2 K_B T}{\pi (\hbar v_F)^2} \ln \left[2 \left(1 + \cosh \frac{qV_{\text{ch}}}{K_B T} \right) \right]. \quad (7)$$

By applying (4)–(7) to (1), an explicit expression of the drain-to-source current I_{DS} can be obtained as

$$I_{DS} = \frac{\mu_{eff} K}{2} \frac{W}{L_{eff}} \left\{ \left[-\frac{V_{ch}^3(D)}{3} - \text{sgn}(V_{ch}(D)) \frac{K V_{ch}^4(D)}{4C_{ox}} \right] - \left[-\frac{V_{ch}^3(S)}{3} - \text{sgn}(V_{ch}(S)) \frac{K V_{ch}^4(S)}{4C_{ox}} \right] \right\} \quad (8)$$

where $K = 2q^3/[(\pi \hbar v_F)^2]$, and $V_{ch}(D)$ and $V_{ch}(S)$ represent the surface potential of the channel at drain and source, respectively.

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