



Label and bio-active free electrochemical detection of testosterone hormone using MIP-based sensing platform

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ABSTRACT

This proof-of-concept research reports a label and bio-active free electrochemical testosterone (hormone essential regulating body function) sensing at flow and in physiological range using molecularly imprinted polymers (MIPs)-based electrochemical sensing platform. State-of-the-art testosterone testing is often based on flow cytometry expertise, sophisticated laboratory set-up, and time-consuming testing and analysis. These consequences are limiting testosterone testing regularly suitable for an average person and a wide population. To manage these challenges, o-phenylenediamine (oPD) electropolymerized to poly(o-phenylenediamine) i.e., PoPD using cyclic voltammetry within minutes for fabricating MIP onto miniaturized screen-printed-electrode (SPE) for electrochemical testosterone sensing application. PoPD-MIPs/SPE sensor was responsive to varied concentrations of testosterone and exhibited a detection limit (LoD) of 1 ng/dL and a wide detection ranging from 1 to 25 ng/dL. The observed LoD correlates with the salivary testosterone of a healthy male. Therefore, PoPD-MIPs/SPE sensor, interfaced with a miniaturized potentiostat (MP) and smartphone, has the potential of point-of-care (POC) testosterone sensing.

1. Introduction

Hormones play an important role in regulating and upkeep our bodies. Insulin regulates the amount of glucose in our bodies, cortisol affects our mood and responds to stress, thyroid hormones regulate our metabolism, etc. Due to their importance to human biology, the body is unable to properly function without them. imbalance or deficiency to produce regular amounts of hormones causes severe and often chronic illnesses such as diabetes, cardiovascular disease, eating disorders, osteoporosis, and more. Testosterone, an anabolic steroid, is an androgen that acts as the primary sex hormone for men. The gonads, and testes in men, are responsible for the production of over 95% of endogenous testosterone, producing approximately 6–7 mg per day, leading to an average concentration between 300 and 1000 ng/dL in the blood and a concentration of around 263 to 544 pmol/L (7.58 ng/dL to 15.7 ng/dL in saliva) [1]. Testosterone can appear as either free

testosterone (unbound) or bound testosterone, which is bound to albumin or sex hormone binding globulin.

Testosterone levels, both total T and free T, are closely tied to a wide range of physiological effects on the body and can be extremely problematic if low. Male hypogonadism, or gonadal dysfunction, is present when the testes fail to produce normal or adequate amounts of testosterone, causing men to have their concentration fall below 300 ng/dL in the blood or 7.18 ng/dL in the saliva [1,2]. Low testosterone levels are linked to a lack of energy [3], bone loss [4], and decreased muscle mass [5]. Besides, low testosterone also affects a person's mental state, causing them to be more prone to negative mental states and emotions such as anger, irritability, depression, and anxiety [6]. These effects can occur in men in all ranges.

In contrast, the effects of high, but not excessively high, testosterone levels include the reduction in the odds of neurodegenerative diseases [7], depression [8], high blood pressure, and heart attacks, while also

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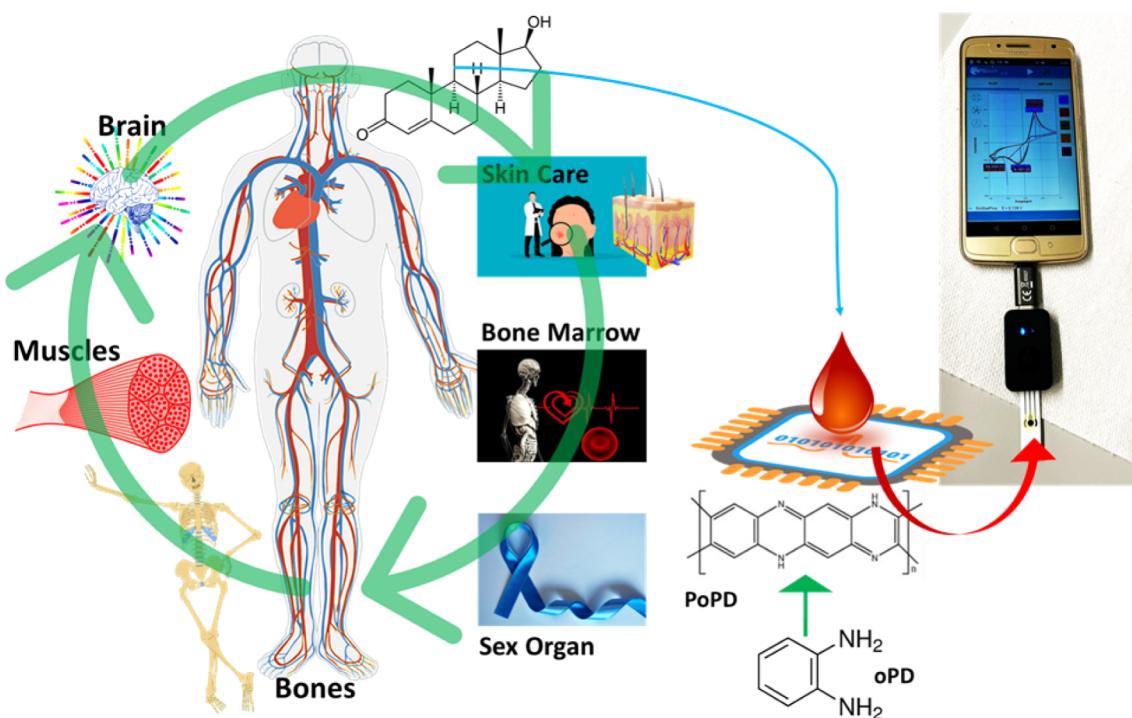


Fig. 1. Illustration of testosterone correlation with male body function and its electrochemical estimation using a sensing electrode modified with MIPs of PoPD fabricated via electro-polymerization of oPD. Such a proposed sensing approach supported miniaturized potentiostat (MIP) could be established for POC sensing of testosterone at a flow and physiological range.

increasing physical performance [9,10]. Due to its positive effect on physical performance, and to evade the negative effects of low testosterone, testosterone has been used to improve the physical ability and mental state of patients [11]. Testosterone replacement therapy (TRT) is a hormone therapy that allows for exogenous testosterone to be supplemented by a patient, typically the elderly, to counteract the effects of hypogonadism [12,13]. The stigma and controversy regarding the risks of TRT have died down in recent years and its popularity has seen a surge. This, alongside rising concern for men's health, necessitates accurate, cheap, and accessible monitoring of testosterone levels. The current means for testing testosterone, and hormones at large, involve immunoassays and liquid chromatography in tandem with mass spectrometry. These processes require state-of-the-art facilities, are inflexible, expensive, and lengthy, and have been criticized for their variability in measurements and sensitivity [14–16]. These flaws have brought about the demand for new methods to test testosterone and other hormones that are cheap, accessible, and accurate. Electrochemical sensors have been presented as a promising solution.

Recently, biosensors have been receiving attention for their ability to detect testosterone not only in a laboratory setting but with the potential for clinical and field practice as well. Various nano-enabled sensing electrodes have been investigated to develop biosensors for testosterone sensing selectively, even in vivo applications. Such biosensors are based on the successful immobilization of testosterone-specific bio-active molecules such as an enzyme, antibody, DNA/RNA, Aptamer, etc. This process demands a functionalized nanostructure or requires multi-step chemistries to generate desired functionality and cross-linking. As such, the sensing platform performs testosterone sensing according to the demand, but the involvement of multi-step fabrication processes limits the large-scale production. Further, to optimize these sensors to target organic compounds such as testosterone or cortisol, a target analyte-specific bio-recognition element (enzymes and antibody) needed to be utilized for performing selective binding to achieve selectivity. During the fabrication of a biosensor, bio-recognition agents are tricky to work with, as they require specific temperatures, pH, and

other conditions to retain their functionality. Therefore, with the importance of testosterone on the male body and the limitations in current evaluations of testosterone, there is an urgent need to develop an efficient sensing system suitable for bio-active and label-free sensing of testosterone at low and high concentrations. This need can be met with the introduction of molecule-imprinted polymers (MIPs) technology for the sensing of hormones like testosterone.

MIPs are synthetic polymers that have cavities imprinted onto their matrix, through a variety of methods, that allow for the binding of specific molecules [17]. They act as analogs to natural antibodies and have been referred to as "plastic antibodies". In the late 90's and early 00's, MIPs were touted and appreciated for their potential as biosensors since they could be used to target organic compounds with extreme sensitivity and selectivity without the complications of working with an enzyme [18]. Using electrosynthesis, one of the three primary methods of imprinting polymers, a material could develop cavities in its surface, using the proper template, that binds to a specific molecule and affect the resulting current passing through, leading to an electric signal that correlates to a certain amount or concentration of target molecule in the sample. Electrochemical MIPs-based sensors, when compared to traditional methods for testing hormones, are simpler, cost-effective, non-invasive, and mass-produced while being accurate, sensitive, and specific. MIPs have already been applied to test for a wide variety of other hormones and biomarkers such as melatonin [19], dopamine [20], oxytocin [21], tyrosine, and uric acid [22].

This proof-of-concept research demonstrates the development of a MIP-based sensing platform for direct i.e., bio-active, and label-free, electrochemical testosterone sensing at low and high concentrations. An electro-polymerization of o-phenylenediamine (oPD) using cyclic voltammetry (CV) was performed onto a miniaturized screen-printed carbon electrode (SPCE) to prepare MIP of Poly(o-phenylenediamine) i.e., PoPD. Further, MIP-PoPD/SPCE was utilized for the direct electrochemical sensing of testosterone at a low and physiological level. Poly(phenylenediamines) (PPD), derivatives of polyanilines, have been used in various fields for their use as conductive polymers. The oPD is one of

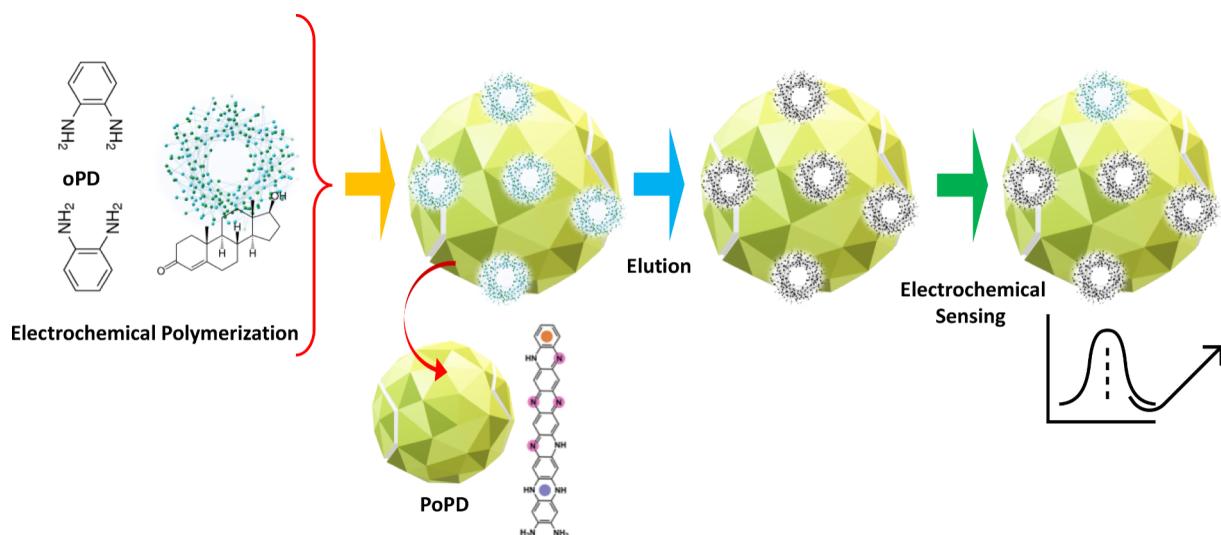


Fig. 2. Presentation of PoPD-MIP and electrochemical sensing of testosterone using PoPD-MIP/SPE electrode.

three forms of PPDs and the polymers of OPDs i.e., PoPD, are used heavily in the sensing field, as they are very thermally stable, easily manufactured, processable, and possess good solubility [23]. The manufacturing of PoPDs is simple, as they can be formed as thin layers on a conducting substrate through the process of anodic electro-polymerization, which can typically be done in a single step using cyclic voltammetry. Due to their relative simplicity and effectiveness in sensing, PoPDs have been used in a wide variety of sensing applications such as the detection of dopamine [24], ascorbic acid [25], ecstasy [26], and many more compounds. PoPD also has the potential to be doped with other chemical agents to produce higher band gap energy, electrical conductivity, and different voltammetric behaviors, allowing for the polymer to be very adaptable and enhanced if desired [27]. In this research, PoPD is selected as a sensing platform instead of other polymers due to its electrochemical stability [28] and redox activity [29].

Our developed MIP-based sensing electrodes can be easily mass-produced due to their relative simplicity and low cost, allowing for them to be easily accessible to people, allowing for quick, non-invasive, and accurate testing of salivary testosterone levels, which are good indicators of testosterone throughout the body [30]. The sensor can be promoted to achieve sensing of a targeted analyte for a POC application. Additionally, this research also paves the way for more sensors to be derived and improved upon to better the human condition and our ability to prevent and treat illnesses. As the ultimate future objective, a MIP-PoPD/SPCE testosterone sensing chip can be interfaced with an MP, operated using a smartphone, to perform sensing at the POC application, needed for personalized health wellness, as illustrated in Fig. 1. However, this testosterone sensor is yet to be tested using real samples which is the focus of future studies as it requires several interfacing approvals and logistics set-ups.

2. Material and methods

The chemicals utilized in this research include drug standard testosterone solution (1.0 mg/ml in acetonitrile), sodium acetate buffer solution, and O-phenylenediamine. All these chemicals were purchased from Sigma-Aldrich Co. (St. Louis, MO, USA). Ethanol solution was diluted with DI water forming 70% ethanol stock solution from within the laboratory. All the electrochemical experiments were performed using an electrochemical analyzer and workstation from CH Instruments (Austin, TX, USA). Potassium ferricyanide $K_3[Fe(CN)_6]$ and potassium ferrocyanide $K_4[Fe(CN)_6]$, both 5 mM, were prepared in deionized water; these chemicals were also purchased from Sigma-Aldrich Co.

All the electrochemical experiments were performed using

commercially available screen-printed carbon electrodes (SPCE) purchased from Zensor Inc. The process of using an electrochemical analyzer to assess the condition of the SPCE was commonly repeated in a triplet set to achieve identical parameters and response. This includes CV studies with varying parameters to understand the scan rate-dependent characteristics of SPCE in a buffer solution containing 5 mM of Fe (II)/Fe (III) with the potentials range 1 V to + 1 V, the scan rate of 50 mV/s, and selected A/V sensitivity as 10^{-4} for one cycle.

2.1. Fabrication of PoPD-MIP/SPCE sensor

To perform electrochemical studies, it is essential to remove contaminants from the SPCE via immersing them in a solution of 1.0 M sulfuric acid and running CV from -1.5 V to 1.5 V, at a scan rate of 0.1 V/s, sensitivity (A/V) of 10^{-4} , for a total of 10 cycles. The cleaned SPCE was washed with deionized (DI) water then dried with nitrogen (N_2) gas and kept at room temperature for drying.

The SPCE was utilized for the electro-polymerization of MIP which will be further utilized for electrochemical testosterone sensing. In this process, the SPCE then had the sodium acetate buffer solution, with the testosterone template, drop-casted onto it using a micropipette. The buffer solution contained 2.0 mM oPD, 1.0 M sodium acetate buffer, and 0.1 mM testosterone template. The buffer solution was bubbled for 5 min using N_2 gas prior to electro-polymerization. The oPD/SPCE was electropolymerized using CV from 0 V to + 1.0 V, the scan rate of 50 mV/s, and sensitivity (A/V) of 10^{-5} A, for a total of 30 cycles. Afterward, the PoPD-MIP/SPCE was washed, dried, and ran through the characterization test. The recorded CV graphs were saved, and the electrode was washed with DI water and dried with N_2 gas. The testosterone template was then removed through elution by immersing it in a 70% ethanol solution for 30 min. After elution, the sensor was washed, dried, and run through another characterization scan. Such fabricated MIP-based platform will be utilized for electrochemical testosterone sensing as illustrated in Fig. 2.

2.2. Electrochemical testosterone sensing

The sensing chip was utilized to detect various testosterone concentrations. In this process, testosterone concentrations of 1 ng/dL, 5 ng/dL, 10 ng/dL, 15 ng/dL, 20 ng/dL, and 25 ng/dL were prepared in ethanol solution. Every testosterone sample was drop-cast onto the PoPD-MIP/SPCE and incubated for 10 min. For sensing, the CV characterization tests were performed using a potential sweep from -1.0 V to 1.0 V, a scan rate of 50 mV/s, and a sensitivity (A/V) of 10^{-5} A, for

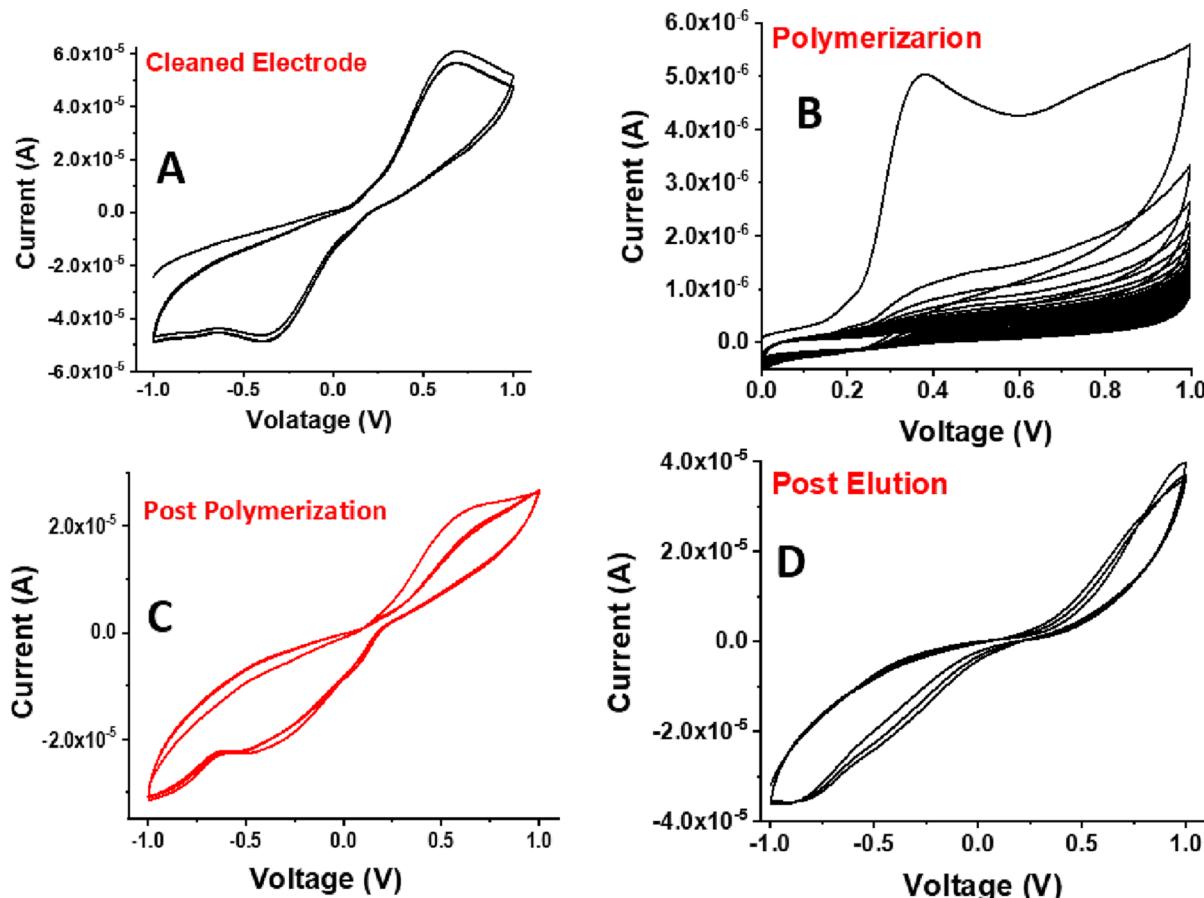


Fig. 3. (A) CV scan on the cleaned electrode. (B) CV scan while electro-polymerizing the MIP. (C) CV scan post-polymerization. (D) CV scan post-elution.

three complete cycles. This process was repeated, with the PoPD-MIP/SPCE being cleaned and dried after each step, with all dilutions, from the lowest concentration to the highest. Afterward, the CV graph of each study collected was utilized to determine the trend and properties of the increasing levels of testosterone concentration for the PoPD-MIP/SPCE sensing chip.

The resulting characterization scans reveal that as testosterone concentrations increase, the magnitudes of the scans increase as well. This is most apparent when the voltage is at 0.6 V, where the distinction between 1 ng/dL, 5 ng/dL, 10 ng/dL, and 15 ng/dL is clear and a pattern emerges. However, the 20 ng/dL and 25 ng/dL are inconsistent with this pattern and further experiments must be conducted to determine why.

3. Results and discussion

After cleaning the SPCE, the sensor was subjected to cyclic voltammetry, where a classic CV graph with well-defined oxidation and reduction peaks is observed as expected and shown in Fig. 3 (A). The CV graph indicates that the bare sensor was working as intended and could be subjected to electro-polymerization. Fig. 3 (B) shows the electro-polymerization of the MIP, whereas the CV cycles (30) continue the electrical property of the oPD on the surface of the electrode changes, resulting in PoPD. After electro-polymerization, the testosterone template solution was removed, and the PoPD/SPCE was examined using CV, where the oxidation and reduction peaks, although at a lower magnitude than bare SPCE, are present as observed in Fig. 3 (C). These outcomes conform with what the CV graph should look like when the MIP-PoPD/SPCE binds with testosterone. After verifying that the electrode surface was polymerized, elution was conducted to remove the testosterone from the resulting PoPD-MIP/SPCE. In Fig. 3 (D), the

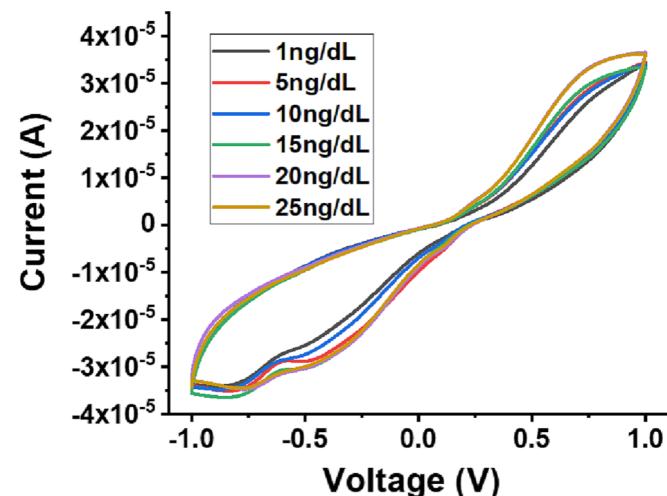


Fig. 4. Overlay of current (mA) output against voltage (V) for characterization tests of the functionalized sensor when presented with testosterone samples.

oxidation and reduction peaks that were present in post-polymerization (Fig. 3 (C)) have widened, which is due to the removal of the testosterone from the MIP's surface, as when testosterone binds to the polymer, electrons are released, causing an increase in current.

While conducting electrochemical studies of developed sensing as a function of testosterone concentration (Fig. 4), an increase in the magnitude of oxidation and reduction response current is observed on the oxidation and reduction peaks as the concentration of the

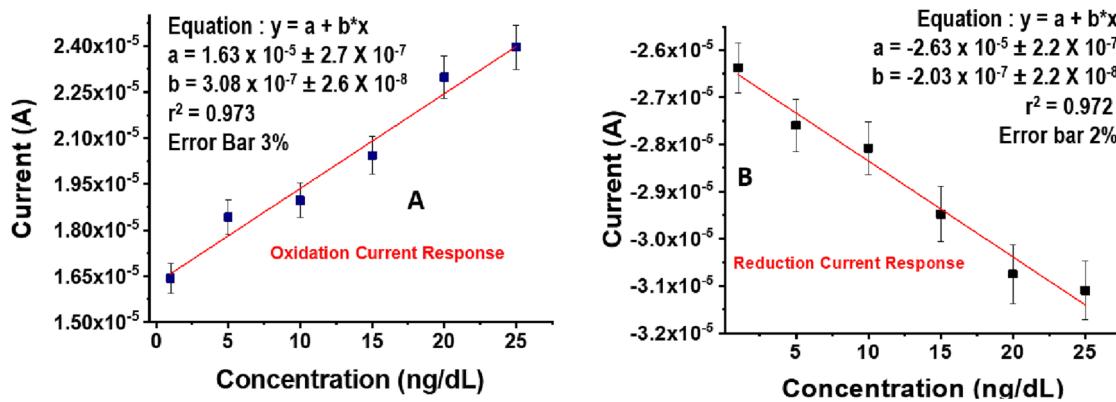


Fig. 5. (A) Electrochemical response displaying the resulting oxidation current (A) from the sensor after being presented with the predetermined testosterone concentrations (ng/dL), at 0.6 V. Electrochemical response displaying the resulting reduction current (A) from the sensor after being presented with the predetermined testosterone concentrations (ng/dL), at -0.6 V.

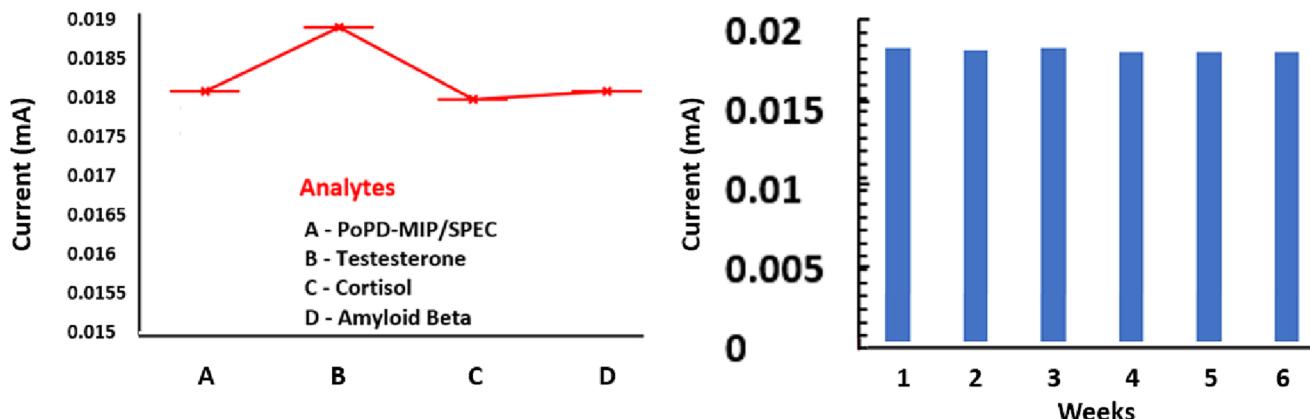


Fig. 6. The electrochemical response of the PoPD-MIP when presented with three analytes. The electrochemical response of the PoPD-MIP over the course of six weeks.

testosterone samples is increased. This indicates that the PoPD/MIP/SCE sensor is able to detect and differentiate testosterone concentrations when present in the PoPD/MIP. The developed sensor exhibited a wide detection range from 1 to 25 ng/dL with a flow limit of detection (LoD) of 1 ng/dL within 15 min. When plotting the oxidation current against the concentration of testosterone, a linear trend was observed (Fig. 5) that reflects the variation in the oxidation (Fig. 5A) and reduction (Fig. 5B) current response magnitude according to the concentration of testosterone present in the sample. The properties of the respective calibrations can be understood by the equations 1) oxidation current responses as $y = x * 3.08 \times 10^{-7} + 1.6 \times 10^{-5}$, with a regression coefficient as 0.97, and 2) reduction current responses as $y = x * -2.03 \times 10^{-7} + (-2.63 \times 10^{-5})$, with a regression coefficient as 0.97. In both cases, the current (A) and x is the concentration of testosterone (ng/dL). An observed good value of r^2 of 0.97 indicates a good correlation between the increasing testosterone concentrations and the change in the magnitude of the current response. The sensitivity was calculated as $3.08 \times 10^{-7} \text{ A/ng dL}^{-1}$ and $-2.03 \times 10^{-7} \text{ A/ng dL}^{-1}$ using calibration curves. Such observed sensing outcomes findings are indicative of the MIP-PoPD/SPCE sensor's ability to detect various concentrations of testosterone both in and outside of the physiological range. (See Fig. 6.).

To test the selectivity of our developed MIP-based sensor, testosterone, cortisol, and amyloid beta (βA_{1-40}) were incubated onto the PoPD-MIP/SPCE, and the electrical response was measured to compare outcomes. When testing, a response, an increase in current, is only observed when presented with samples that contained testosterone rather than when presented with the other two analytes. The current

Table 1

Summary of the sensing outcomes demonstrated by testosterone sensors developed recently (2015 and on) [31–39].

Sensing - Electrode	Detection Range	LoD	Refs
PU/AuE	100–1,000 nM	6.69 nM	31
Aptamer + AuNPs	25–500 nM	16 nM	32
MIP/GO	1 fM – 1 μ M	0.4 fM	33
SPR-based Systems	0.5–20 ng/mL [1.735–69.3 nM]	0.034 ng/mL (0.118 nM)	34
Aptamer + 96-well plate based on carbon	0.39–1.56 μ M	0.29 μ M	35
MIP-based on diamond-coated substrates	0.5–500 nM	0.5 nM	36
PSPCE/Pb NPs	10–100 pM 0.1–2 nM 2–20 nM	2.2 pM/L	37
DMIP/Au	10–100 fM	10 fM	38
MIP + Microfluidic Resonator	0.05–10 ng/mL [0.1735–34.67 nM]	48.7 pg/mL (0.1689 nM)	39
PoPD-MIP/SPCE – suitable for POC application	1–25 ng/dL [0.0347–0.8668 nM]	1 ng/dL [0.0347 nM]	Present Research

values for cortisol and βA_{1-40} are false responses of the bare PoPD-MIP/SPCE. These outcomes confirm that MIP-PoPD is a response to only testosterone. Further, systematic electrochemical studies were

performed to examine the stability of our developed PoPD-MIP/SPCE sensor at the interval of a week up to 6 weeks. No notable changes in the magnitude of current values confirm that the PoPD/MIP/SPE sensor exhibited stability for 6 weeks. This study was further expanded and a reduction in the electrical signal (around 20%) was observed in week 7, data not shown.

The sensing performance outcomes of the PoPD-MIP/SPCE sensor are carefully compared with some of the important testosterone sensors fabricated recently and based on various methods [31–39], as summarized in Table 1.

4. Conclusions and viewpoint

In summary, the results of the research demonstrate a consistent positive correlation between the concentration of testosterone and overall current behavior within the concentration range of 1 ng/dL to 25 ng/dL. As a proof-of-concept, this research successfully demonstrates bio-active and label-free electrochemical sensing of testosterone using PoPD-MIP/SPCE system at flow (1 ng/dL) and high levels (25 ng/dL), which is within the physiological range for male saliva, 7.18 ng/dL to 15.7 ng/dL. The developed PoPD-MIP/SPCE approach for testosterone testing is easy to execute for large-scale production and POC testing if integrated with miniaturized electronics. Additionally, easy fabrication makes this technology affordable to execute as a part of medical practice. As a future direction, we will be focused on investigating the selectivity of developed PoPD-MIP/SPCE testosterone sensors with a dedicated aim to achieve testosterone sensing in real samples such as saliva. Along with CV, we will explore PoPD-MIP/SPCE for testosterone sensing using EIS techniques as it is a non-destructive approach to signaling as well as adapting these methods to produce single-use sensing chips for miniaturized point-of-care applications.

Another benefit of using a MIP is their inherent elasticity and flexibility, which allows for them to be implemented in technologies involving wearable sensors. Future work on this testosterone sensor could attempt to detect fluctuations in testosterone using a sensor in the mouth or other biomarkers using a wearable sensor on a person's limbs. Further, utilizing an advanced MIP of PalmSens with Bluetooth capabilities can be operated using a smartphone (introduction of Internet-of-medical-things (IoMT)). By combining the existing network of health professionals and generating a quick and flexible flow of medical data, users could not only monitor testosterone levels in real time but also receive consultation and assistance. Extended studies with an emphasis on integrating the MIP-based sensing platform into stretchable electronic technologies and software development will provide an all-encompassing medical experience.

Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

Data availability

Data will be made available on request.

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