ICASSP 2023 - 2023 IEEE International Conference on Acoustics, Speech and Signal Processing (ICASSP) | 978-1-7281-6327-7/23/$31.00 ©2023 IEEE | DOI: 10.1109/ICASSP49357.2023.10097185

An Edge Alignment-based Orientation Selection Method for Neutron Tomography

Diyu Yang[§1], Shimin Tang[§2], Singanallur V. Venkatakrishnan[2], Mohammad S. N. Chowdhury[1], Yuxuan Zhang[2], Hassina Z. Bilheux[2], Gregery T. Buzzard[1] and Charles A. Bouman[1]

[1]Purdue University, West Lafayette, IN 47906
[2]Oak Ridge National Laboratory, One Bethel Valley Road, Oak Ridge, TN 37831

Abstract—Neutron computed tomography (nCT) is a 3D characterization technique used to image the internal morphology or chemical composition of samples in biology and materials sciences. A typical workflow involves placing the sample in the path of a neutron beam, acquiring projection data at a predefined set of orientations, and processing the resulting data using an analytic reconstruction algorithm. Typical nCT scans require hours to days to complete and are then processed using conventional filtered back-projection (FBP), which performs poorly with sparse views or noisy data. Hence, the main methods in order to reduce overall acquisition time are the use of an improved sampling strategy combined with the use of advanced reconstruction methods such as model-based iterative reconstruction (MBIR). In this paper, we propose an adaptive orientation selection method in which an MBIR reconstruction on previously-acquired measurements is used to define an objective function on orientations that balances a data-fitting term promoting edge alignment and a regularization term promoting orientation diversity. Using simulated and experimental data, we demonstrate that our method produces high-quality reconstructions using significantly fewer total measurements than the conventional approach.

I. Introduction

Neutron computed tomography (nCT) is a 3D imaging technique used for the non-destructive characterization of samples in biology [1], [2] and materials science [3], [4]. nCT proceeds by placing a sample in the path of a neutron beam, usually at a nuclear reactor or pulsed neutron source facility, and making measurements of the transmitted projection images (also known as views) at various sample orientations. Typical nCT systems use a fixed angular step size to rotate the sample about a single axis; the resulting measurements are processed using the filtered back-projection (FBP) algorithm [5].

The conventional approach for nCT can be extremely time-consuming due to the time required for each view and the number of views required. Using conventional scanning and reconstruction methods (such as FBP), each view can require from a few minutes (at a reactor) to several hours (at a pulsed source) to obtain sufficient SNR, especially as is the case for hyperspectral systems [6], [7]. These factors, plus high operating costs and limited beam time at neutron facilities, create a need for more efficient acquisition and reconstruction methods to shorten nCT scan times.

To reduce the measurement time for nCT, model-based iterative reconstruction (MBIR) methods have been developed and applied to sparse-view interlaced scanning [8] or golden ratio [9], [10] acquisition protocols. This approach can produce high-quality reconstructions throughout the course of the scan, even before all measurements have been obtained, and can dramatically reduce overall scan time [11]. However, this method is still inefficient because the sampling pattern is fixed and does not take into account the geometry and morphology of the samples that are being measured.

In the context of some computational imaging systems, sample adaptive strategies in which the next measurement is chosen based on previously measured data have been recently proposed. Such methods can use either supervised learning based on training data [12] or unsupervised methods based on a model for the underlying objects to be measured [13]–[15]. All of these approaches have been developed for scanning microscopy or MRI systems, in which the time to measure is significantly longer than the time to reorient and process the measurements, but none of them are tuned for CT applications. In contrast, existing dynamic sampling approaches for CT [16], [17] select new samples using information from the existing projection data rather than from the image domain, which limits the information available for sample selection.

In this paper, we propose an adaptive orientation selection method for nCT, in which an MBIR reconstruction performed on previous measurements is used to define an objective function on orientations. We formally define the orientation selection criterion as a joint optimization problem between (a) a data-fitting term promoting alignment between measurement direction and dominant edges in the reconstruction and (b) a regularization term promoting orientation diversity. Using simulated and experimental data, we demonstrate that our adaptive orientation selection method performs better than MBIR with golden ratio sampling [10], [11] in terms of the convergence speed of the normalized root mean square error (NRMSE), thereby enabling a significant reduction in measurement time for a given reconstruction quality.

[§]These authors contributed equally.

This manuscript has been authored by UT-Battelle, LLC, under contract DE-AC05-00OR22725 with the US Department of Energy (DOE). The US government retains and the publisher, by accepting the article for publication, acknowledges that the US government retains a nonexclusive, paid-up, irrevocable, worldwide license to publish or reproduce the published form of this manuscript, or allow others to do so, for US government purposes. DOE will provide public access to these results of federally sponsored research in accordance with the DOE Public Access Plan (http://energy.gov/downloads/doe-public-access-plan).

II. Methodology

In tomographic imaging, radiograph measurements are sequentially collected from different view angles/orientations during the scanning process. In order to design a method for dynamic selection of new orientation, we make two key observations:

1) Orientations aligned with the edges of the object of interest contain more information.
2) An orientation contains less information if a similar orientation has been scanned previously.

The proposed orientation selection method is designed to select new view angles to balance these competing considerations.

A. Optimization problem formulation

Let θ_n be the n^{th} view angle to be selected, $\Theta^{\vec{}}_{n-1} = \theta^{\vec{}}_0, \ldots, \theta^{\vec{}}_{n-1}$ be the set of previously selected view angles, and x_n be the preliminary reconstruction from CT projections collected at angles $\Theta^{\vec{}}_{n-1}$. The angle selection problem is formulated as a joint optimization problem:

$$\theta^{\vec{}}_n = \arg\max_{\theta_n \in [0,\pi)} f(\theta_n; x_n) + \gamma h(\theta_n; \Theta^{\vec{}}_{n-1}), \quad (1)$$

where $f(\theta; x)$ is a data fitting term promoting edge alignment, $h(\theta, \Theta^{\vec{}})$ is a regularization term promoting angle diversity, and $\gamma > 0$ is a scalar weight controlling the importance of regularization relative to data fitting.

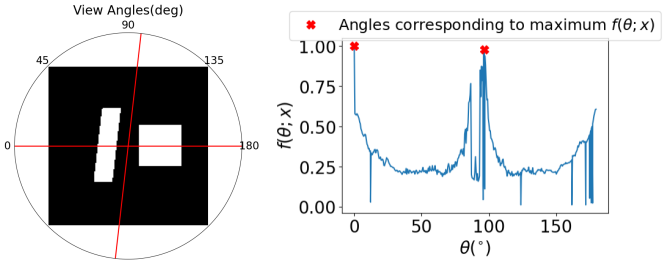
B. Edge alignment function

Algorithm 1 Edge Alignment Function Calculation

Input: View angle: $\theta \in [0, \pi)$
Input: Preliminary reconstruction: $x \in \mathbb{R}^{N_z \times N_x \times N_y}$
Output: Edge alignment function: $f(\theta; x) \in [0, 1]$
(Note that $x[k] \in \mathbb{R}^{N_x \times N_y}$ is the kth slice of x.)

```
f(θ; x) ← 0
for k ← 0 to N_z − 1 do
    x̄[k] ← Canny(x[k])                    ▷ Canny edge detection
    {l_0, ..., l_{M_k − 1}} ← PPHT(x̄[k])   ▷ Hough feature
    for m ← 0 to M_k − 1 do
        Calculate b_m(θ)                  ▷ Alignment mask from Eq. 2
        f(θ; x) ← f(θ; x) + b_m(θ) · x̄[k]
f(θ; x) ← f(θ; x) / max_{φ∈[0,π)} {f(φ; x)}   ▷ Normalization
return f(θ; x)
```

The edge alignment function $f(\theta; x)$ (Algorithm 1) determines how well the view angle θ is aligned with the edges of the attenuation image x. First, we apply the Canny edge detection algorithm [18] to each slice $x[k] \in x$ to give a binary edge image slice $\bar{x}[k]$, where 1 indicates an edge pixel in the corresponding slice. Next, we apply the Progressive Probabilistic Hough Transform (PPHT) [19] to $\bar{x}[k]$ to yield a collection of line segments $L_k = \{l_0, \ldots, l_{M_k - 1}\}$, each representing a component of a the edge. For each line segment $l_m \in L_k$, we evaluate how well it aligns with the view angle θ by defining a binary mask, $b_m(\theta)$, which is 1 in a conical neighborhood of l_m and 0 elsewhere. More precisely, let $C_\epsilon(l_m)$ be a double-sided cone with vertex at the center of l_m, direction-aligned with l_m, and with angle of opening ϵ.



(a) Single image slice (b) Plot of edge alignment function

Fig. 1: (a) Illustration of an binary image of size 150×150 pixels to demonstrate the edge alignment terms in the cost function. Red lines indicate the angles at which the edge alignment function is maximized. (b) Edge alignment function vs. view angle, showing angles for which the function is maximized (i.e. best aligned with existing edges). Notice that the function is maximum at the orientations that are aligned with the dominant edges of the image.

Then

$$b_m(\theta)[i, j] = \begin{cases} 1, & \text{if pixel } (i, j) \text{ is in } C_\epsilon(l_m) \\ 0, & \text{otherwise.} \end{cases} \quad (2)$$

The edge alignment function for x[k] is then the inner product between $\bar{x}[k]$ and the binary masks $b_m(\theta)$, summed over $m = 0, \ldots, M_k - 1$. This is then summed over all slices and normalized to give

$$f(\theta; x) = \frac{1}{K_f(x)} \sum_{k=0}^{N_z - 1} \sum_{m=0}^{M_k - 1} b_m(\theta) \cdot \bar{x}[k], \quad (3)$$

where $K_f(x)$ is chosen so that $\max_{\theta \in [0,\pi)} f(\theta; x) = 1$.

Fig. 1a shows an example of a binary image, and Fig. 1b shows the corresponding plot of the edge alignment function. In this example $f(\theta; x)$ takes on maximum values at $\theta = 0^\circ$ and 95°, with a slightly smaller peak at 90°, corresponding to the orientations of the dominant edges in the attenuation slice.

C. Angle spacing cost function

Given a view angle θ and all previously selected view angles $\Theta^{\vec{}} = \theta^{\vec{}}_0, \ldots, \theta^{\vec{}}_{n-1}$, the angle spacing function is defined as

$$h(\theta; \Theta^{\vec{}}) = \frac{1}{K_h(\Theta^{\vec{}})} \exp^{\vec{}} -\alpha \sum_{j=0}^{n-1} \frac{1}{d(\theta, \theta^{\vec{}}_j)}, \quad (4)$$

where $K_h(\Theta^{\vec{}})$ is chosen so that $\max_\theta h(\theta; \Theta^{\vec{}}) = 1$, $d(\theta, \theta^{\vec{}}_j) = \min \left| \theta - \theta^{\vec{}}_j \right|, 180^\circ - \left| \theta - \theta^{\vec{}}_j \right|$ is angular distance, and α is a scaling parameter to control the importance of proximity to previously measured angles.

Fig. 2 shows an example plot of $h(\theta; \Theta^{\vec{}})$ with four existing view angles. As θ approaches an existing view angle, h decreases quickly, while h is relatively constant for θ values reasonably spaced from all existing angles.

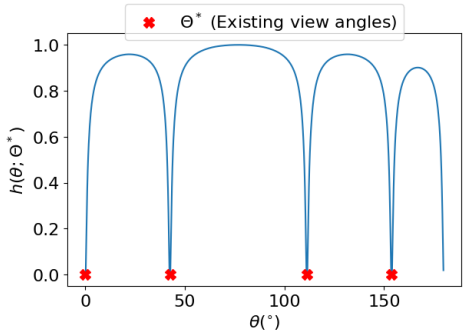


Fig. 2: Normalized angle spacing cost function vs. view angles showing existing view angles (red marks). We note that the cost function strongly discourages the selection of angles that are close to previously selected angles.

D. Parameter selection

One interpretation of the joint optimization problem in Eq. 1 is as an exploration-exploitation trade-off. Edge alignment, promoted by $f(\theta; x)$, encourages exploitation of existing edge information, while angle spacing, promoted by $h(\theta; \Theta^{\vec{}})$, encourages exploration of new orientations, and the relative importance of each is governed by γ. While the choice of γ could be influenced by prior knowledge of the prevalence of edges in a sample or by preliminary reconstructions, we use $\gamma = 1$ for simplicity and to establish a baseline for future work. Likewise, we choose $\alpha = 1$ in Eq. 4 for simplicity and to establish a baseline for future work.

III. Numerical Implementation

We solve Eq. 1 numerically using a discretized solution space $\Theta = \{0, \Delta\theta, \ldots, \pi - \Delta\theta\}$. Algorithm 2 shows the pseudocode of the proposed orientation selection algorithm, which first calculates a reconstruction x_n using previous angles, then evaluates the functions f and h over the discrete set Θ, then does the optimization. We obtain the reconstruction x_n from $\Theta^{\vec{}}_{n-1}$ by using the previous reconstruction x_{n-1} as initialization for the svMBIR reconstruction package [20], which rapidly yields high-quality reconstructions with an automated choice of regularization parameters. As a result, the angle selection of Algorithm 2 completes quickly relative to the long measurement time of each projection measurement in nCT. Algorithm 3 describes the complete angle selection and reconstruction workflow, in which an initial reconstruction is performed, a view angle is selected, the corresponding projection is measured, and the reconstruction is performed with all measured projections.

Algorithm 2 Single-Step Orientation Selection Algorithm

Input: Previously measured angles: $\Theta^{\vec{}}_{n-1}$
Input: Previous reconstruction: x_{n-1}
Input: Discretized candidate angles: Θ_n
Output: Next view angle: $\theta^{\vec{}}_n$

1: Calculate $f(\theta; x_{n-1})$, $\forall \theta \in \Theta_n$ using Algorithm 1
2: Calculate $h(\theta; \Theta^{\vec{}}_{n-1})$, $\forall \theta \in \Theta_n$ using Eq. 4
3: $\theta^{\vec{}}_n \leftarrow \arg\max_{\theta \in \Theta_n} f(\theta; x_{n-1}) + \gamma h(\theta; \Theta^{\vec{}}_{n-1})$
4: return $\theta^{\vec{}}_n$

Algorithm 3 Proposed Neutron Imaging Workflow

Input: Initial view angles: $\Theta^{\vec{}}_0$
Input: Discretized view angle space: Θ
Input: Initial measurement data: Y_0
Input: Number of additional views to acquire: N
Output: Final Reconstruction: x_N

1: $x_0 \leftarrow \text{Recon}(Y_0, \Theta^{\vec{}}_0)$ ▷ Initial reconstruction
2: for $n \leftarrow 1$ to N do
3: $\quad \Theta_n \leftarrow \Theta \setminus \Theta^{\vec{}}_{n-1}$ ▷ Update candidate view angles
4: $\quad \theta^{\vec{}}_n \leftarrow \text{SelectAngle}(x_{n-1}, \Theta^{\vec{}}_{n-1}, \Theta_n)$ ▷ Algo. 2
5: $\quad y_n \leftarrow$ measurement of projection at angle $\theta^{\vec{}}_n$
6: $\quad Y_n \leftarrow \{Y_{n-1}, y_n\}$ ▷ Update measurement data
7: $\quad \Theta^{\vec{}}_n \leftarrow \{\Theta^{\vec{}}_{n-1}, \theta^{\vec{}}_n\}$ ▷ Update existing view angles
8: $\quad x_n \leftarrow \text{Recon}(Y_n, \Theta^{\vec{}}_n)$ ▷ Update reconstruction
9: return x_N

IV. Results

In this section, we present experimental results from both synthetic and real nCT scans of various 3D objects. In each case, we compare reconstructions using the proposed orientation selection algorithm to reconstructions using MBIR in conjunction with the golden ratio acquisition method.

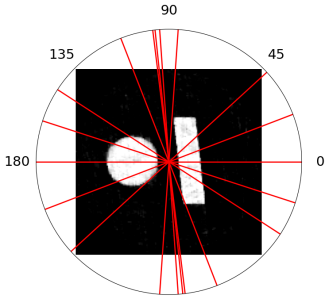
For synthetic 3D data, we generated two binary ground truth volumes composed of multiple geometric shapes such as sphere, prism, cube, etc. Each ground truth volume has 50 axial slices, with 150×150 pixels per slice. We then scaled the ground truth volume by a factor of 0.01 in order to make the attenuation values physically realistic. For each ground truth volume, we generated a synthetic data by first forward projecting the volume at selected view angles using svMBIR's [20] parallel beam projector and then modeling the measurement using Poisson counting with values similar to typically observed real experiments.

The experimental data is from a sample of a volcanic rock held on a metal ring, with densely sampled measurements obtained at the imaging instrument High Flux Isotope Reactor (HFIR) at Oak Ridge National Lab (ORNL). For the NRMSE calculation, we used an MBIR reconstruction from 1200 projections to generate a reference volume with 5 axial slices and 400×400 pixels per slice.

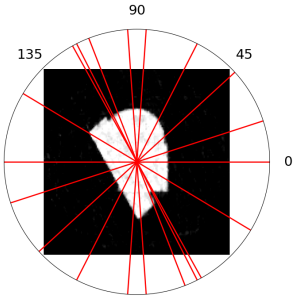
We compare the proposed algorithm to the golden ratio method in Fig. 3 (simulated data) and Fig. 4 (real data). In both cases, the proposed algorithm outperforms the golden ratio method in terms of the convergence speed of NRMSE between the reconstruction and the reference volume. This improvement is especially pronounced in the early stages of angle selection in Fig. 3(e) and Fig. 4, in which there are prominent edges that are better resolved by appropriate angle selection, which in turn yields a significantly better reconstruction. In the case of Fig. 3(f), the object has fewer clearly defined edges, and the initial reconstruction from 3 view angles is better than that in Fig. 3(e), so the improvement over the golden ratio

(a) Ground truth

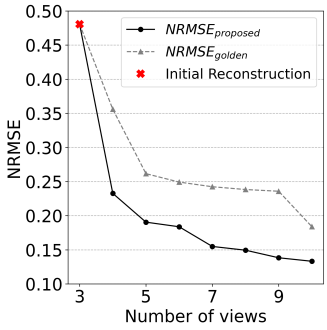
(b) Ground truth



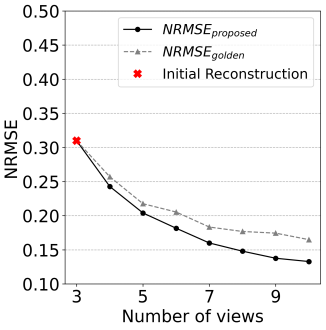
(c) Selected angles and reconstruction



(d) Selected angles and reconstruction

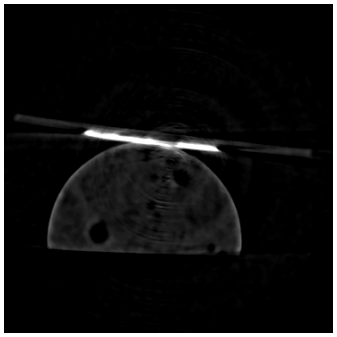


(e) NRMSE vs #views

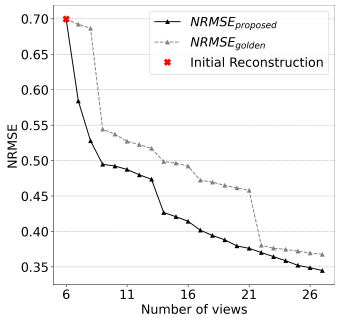


(f) NRMSE vs #views

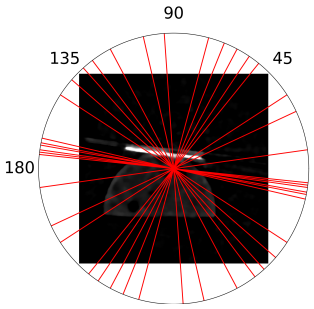
Fig. 3: Results using simulated data. (a) and (b) show representative slices from ground truth volumes; (c) and (d) show the angles selected by the proposed algorithm and the corresponding reconstructions using MBIR; (e) and (f) show the corresponding NRMSE as a function of the number of view angles for each of the golden ratio method and the proposed method. For both sample geometries, the NRMSE converges faster when using the proposed method.



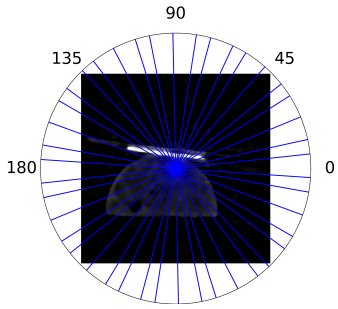
(a) Reference image



(b) NRMSE vs #views



(c) Proposed method: Selected angles and reconstruction with 20 projections



(d) Golden ratio: Selected angles and reconstruction with 20 projections

Fig. 4: Results using experimental data. (a) shows the reference image (MBIR from 1200 projections). (b) shows the NRMSE as a function of number of view angles for the proposed method and the golden ratio method. (c) and (d) respectively show the first 20 angles selected by the proposed method and the golden ratio method (after 6 evenly spaced initial angles) and the corresponding reconstructions using MBIR. We note that the proposed orientation selection method leads to a faster convergence to the reference compared to the traditional golden ratio method.

method is still apparent, but less pronounced.

V. Conclusion

In this paper, we introduced a sample adaptive measurement strategy that can significantly reduce the measurement time of neutron CT scans. Our method uses existing measurements to perform an MBIR reconstruction, which is then used to construct an edge image to locate prominent edges in the object. The reconstruction and edge image are used to define the orientation selection criterion as a joint optimization problem between a data-fitting term promoting edge alignment and a regularization term promoting angle spacing to ensure a diversity of views. Using simulated and experimental data, we demonstrated that our orientation selection method performs better than MBIR applied with the conventional golden ratio sparse acquisition scheme in terms of the convergence speed of NRMSE, thereby yielding a significant reduction in measurement time for a given quality of reconstruction.

Acknowledgment

A portion of this research used resources at the High Flux Isotope Reactor and Spallation Neutron Source, DOE Office of Science User Facilities operated by the Oak Ridge National Laboratory. Oak Ridge National Laboratory is managed by UT-Battelle, LLC, for the U.S. DOE under contract DE-AC05-00OR22725. We give special thanks to Professor Mattia Pistone from University of Georgia, who provided permission for use of the volcanic rock dataset.

REFERENCES

[1] H. Z. Bilheux, M. Cekanova, J. M. Warren, M. J. Meagher, R. D. Ross, J. C. Bilheux, S. Venkatakrishnan, J. Y. Lin, Y. Zhang, M. R. Pearson et al., "Neutron radiography and computed tomography of biological systems at the oak ridge national laboratory's high flux isotope reactor," JoVE (Journal of Visualized Experiments), no. 171, p. e61688, 2021.

[2] N. Rudolph-Mohr, S. Bereswill, C. Tötzke, N. Kardjilov, and S. E. Oswald, "Neutron computed laminography yields 3D root system architecture and complements investigations of spatiotemporal rhizosphere patterns," Plant and Soil, vol. 469, no. 1, pp. 489–501, 2021.

[3] A. Griesche, E. Dabah, T. Kannengiesser, N. Kardjilov, A. Hilger, and I. Manke, "Three-dimensional imaging of hydrogen blister in iron with neutron tomography," Acta Materialia, vol. 78, pp. 14–22, 2014.

[4] W. J. Richards, G. McClellan, and D. Tow, "Neutron tomography of nuclear fuel bundles," Mater. Eval.;(United States), vol. 40, no. 12, 1982.

[5] A. C. Kak and M. Slaney, Principles of Computerized Tomographic Imaging. Philadephia, PA: Society for Industrial and Applied Mathematics, 2001.

[6] R. Woracek, D. Penumadu, N. Kardjilov, A. Hilger, M. Boin, J. Banhart, and I. Manke, "3D mapping of crystallographic phase distribution using energy-selective neutron tomography," Advanced Materials, vol. 26, no. 24, pp. 4069–4073, 2014.

[7] A. Gregg, J. Hendriks, C. Wensrich, A. Wills, A. Tremsin, V. Luzin, T. Shinohara, O. Kirstein, M. Meylan, and E. Kisi, "Tomographic reconstruction of two-dimensional residual strain fields from bragg-edge neutron imaging," Physical Review Applied, vol. 10, no. 6, p. 064034, 2018.

[8] K. Aditya Mohan, S. V. Venkatakrishnan, J. W. Gibbs, E. B. Gulsoy, X. Xiao, M. De Graef, P. W. Voorhees, and C. A. Bouman, "TIMBIR: A method for time-space reconstruction from interlaced views," IEEE Transactions on Computational Imaging, vol. 1, no. 2, pp. 96–111, 2015.

[9] T. Kohler, "A projection access scheme for iterative reconstruction based on the golden section," in IEEE Symposium Conference Record Nuclear Science 2004., vol. 6. IEEE, 2004, pp. 3961–3965.

[10] A. P. Kaestner, B. Munch, and P. Trtik, "Spatiotemporal computed tomography of dynamic processes," Optical Engineering, vol. 50, no. 12, p. 123201, 2011.

[11] S. Venkatakrishnan, Y. Zhang, L. Dessieux, C. Hoffmann, P. Bingham, and H. Bilheux, "Improved acquisition and reconstruction for wavelength-resolved neutron tomography," Journal of Imaging, vol. 7, no. 1, p. 10, 2021.

[12] G. M. D. P. Godaliyadda, D. H. Ye, M. D. Uchic, M. A. Groeber, G. T. Buzzard, and C. A. Bouman, "A framework for dynamic image sampling based on supervised learning," IEEE Transactions on Computational Imaging, vol. 4, no. 1, pp. 1–16, 2018.

[13] M. Ziatdinov, Y. Liu, K. Kelley, R. Vasudevan, and S. V. Kalinin, "Bayesian active learning for scanning probe microscopy: from gaussian processes to hypothesis learning," ACS nano, 2022.

[14] M. Seeger, H. Nickisch, R. Pohmann, and B. Schölkopf, "Optimization of k-space trajectories for compressed sensing by bayesian experimental design," Magnetic Resonance in Medicine: An Official Journal of the International Society for Magnetic Resonance in Medicine, vol. 63, no. 1, pp. 116–126, 2010.

[15] J. P. Haldar and D. Kim, "Oedipus: An experiment design framework for sparsity-constrained mri," IEEE transactions on medical imaging, vol. 38, no. 7, pp. 1545–1558, 2019.

[16] K. J. Batenburg, W. J. Palenstijn, P. Balázs, and J. Sijbers, "Dynamic angle selection in binary tomography," Computer Vision and Image Understanding, vol. 117, no. 4, pp. 306–318, 2013.

[17] A. Dabravolski, K. J. Batenburg, and J. Sijbers, "Dynamic angle selection in x-ray computed tomography," Nuclear Instruments and Methods in Physics Research Section B: Beam Interactions with Materials and Atoms, vol. 324, pp. 17–24, 2014.

[18] J. Canny, "A computational approach to edge detection," IEEE Transactions on pattern analysis and machine intelligence, no. 6, pp. 679–698, 1986.

[19] C. Galamhos, J. Matas, and J. Kittler, "Progressive probabilistic hough transform for line detection," in Proceedings. 1999 IEEE computer society conference on computer vision and pattern recognition (Cat. No PR00149), vol. 1. IEEE, 1999, pp. 554–560.

[20] SVMBIR Development Team, "Super-Voxel Model Based Iterative Reconstruction (SVMBIR)," Software library available from https://github.com/cabouman/svmbir, 2020.