

1 **Regulation of macrophage function by the macro- and micro-scale *in vitro***
2 **culture environment**

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13 **Abstract**

14 Macrophages hold vital roles in immune defense, wound healing, and tissue homeostasis, and have the
15 exquisite ability to sense and respond to dynamically changing cues in their microenvironment. Much
16 of our understanding of their behavior has been derived from studies performed using *in vitro* culture
17 systems, in which the cell environment can be precisely controlled. Recent advances in miniaturized
18 culture platforms also offer the ability to recapitulate some features of the *in vivo* environment and
19 analyze cellular responses at the single-cell level. Since macrophages are sensitive to their surrounding
20 environments, the specific conditions in both macro- and micro-scale cultures likely contribute to
21 observed responses. In this study, we investigate how the presence of neighboring cells and volume of
22 media influence macrophage activation following pro-inflammatory stimulation. We found that in bulk
23 cultures, higher seeding density and lower cell-to-media volume ratio negatively regulated the average
24 TNF α secretion from individual macrophages in response to inflammatory agonists. In contrast, studies
25 conducted using microwells to isolate single cells and groups of cells revealed that increasing numbers
26 of cells positively influences their inflammatory activation, suggesting that the absolute cell numbers in
27 the system may be important. Overall, this work helps to better understand how variations of
28 experimental parameters broadly influence studies in macrophage biology and provides insight into
29 how the presence of neighboring cells and the soluble environment influences macrophage activation.

30

31 Keywords: macrophages, *in vitro* culture, microwells, inflammation

32 INTRODUCTION

33 Macrophages have essential roles in tissue homeostasis, combating infection, and mediating wound
34 healing. They are also involved in the pathogenesis and progression of many chronic inflammatory and
35 autoimmune diseases, including atherosclerosis, rheumatoid arthritis, obesity, and multiple sclerosis ^{1,2}.
36 To perform their myriad of functions, macrophages are exquisitely sensitive to the surrounding
37 environment and can polarize into different phenotypes in response to diverse stimuli, including both
38 soluble and adhesive cues. At the extremes, soluble cues such as the bacterial component
39 lipopolysaccharide (LPS) and interferon-gamma (IFN γ) polarize cells to pro-inflammatory phenotypes
40 (often referred to as “M1”), while interleukin 4 and interleukin 13 (IL4 and IL13) polarize cells to pro-
41 healing phenotype (often referred to as “M2”) ³. To study the effects of these soluble cues in
42 macrophage activation, *in vitro* culture systems are often employed and have advanced our knowledge
43 about macrophage activation. These platforms provide well-controlled environments to delineate the
44 effects of different factors. In addition, recent efforts in the development of advanced *in vitro*
45 microsystems can better recapitulate the physiological environment, known as microphysiological
46 systems. These platforms can be used with a wide variety of cell systems including primary human
47 cells, enabling translationally relevant and high throughput studies. However, they also raise new
48 considerations about how the culture environment can potentially influence the function of cells.

49 Many studies of macrophage activation involve seeding cells into culture wells, followed by
50 stimulation with activating agents and evaluating the expression or secretion of phenotypic markers and
51 cytokines. However, factors including seeding density and media volume per cell can vary across the
52 many published studies. These factors have been linked to varied behaviors of immune cells. For
53 example, different seeding densities of THP-1 monocytic cells and murine bone marrow cells during
54 differentiation to macrophages causes differential expression of macrophage markers CD11b, CD14,
55 and Ly-6G ^{4,5}. Furthermore, murine macrophages differentiated at different densities responded
56 differently to the stimulation, with cells differentiated at lower densities secreting higher amounts of
57 inflammatory cytokines, including TNF α , IL6, and MIP-1 α , and expressed lower anti-inflammatory
58 markers, such as CD206 and Ym1 ⁴. In another study, murine macrophage cell line RAW 264.7
59 cultured at higher densities resulted in increased NF- κ B signaling, TNF α transcription, and TNF α
60 production ⁶. These results were attributed to the priming of the macrophages by soluble factors
61 secreted from the cells at the resting state prior to stimulation. Macrophages cultured at higher densities
62 also inhibit mycobacteria growth more effectively than those cultured at lower densities ⁷. Interestingly,
63 studies separating individual cells into microwells show that cytokine secretion from individual cells in
64 response to inflammatory activators are substantially lower than cells cultured in bulk and allowed to

share common paracrine signals^{8,9}. However, previous studies cover limited subsets of densities ranges^{10,11}, and direct comparisons between macro-scale cultures in traditional tissue culture wells with micro-scale cultures have not been established.

Recent efforts to develop more complex microphysiological systems that better recapitulate native tissue environments have revealed additional parameters for consideration in the design of *in vitro* culture studies. The miniaturized dimensions of microfluidic devices have the advantage of using fewer reagents and enabling cultures of small population or single cells, while also offering the flexibility to design structures and pattern cells or substrates to mimic native cellular environments^{12,13}. These advantages have been exploited in the construction of various organ-on-a-chip systems, for example a gut-inflammation-on-a-chip model¹⁴. However, these tools also introduce new soluble environments for cultured cells, including varied rates of accumulation for endogenous growth factors, reduced media volume conditions, and exposure to other cells. In epithelial cells, differences in the growth rates have been observed for normal mammary gland epithelial cells (NMuMG) cultured in microscopic and macroscopic systems, and accumulation of soluble factor signaling was cited as a main factor¹⁵. Macrophages are known to secrete many cytokines with paracrine effects, and these factors may exert their effects differently in between bulk and micro-scale systems. These issues further necessitate a better understanding of how density or soluble factor-dependent parameters contribute toward the macrophage responses.

Here, we systematically evaluated the roles of different cell culture parameters in the activation of macrophages. We examined the effects of cell seeding density and cell-to-media volume ratio on the inflammatory activation of bone-marrow-derived macrophages (BMDMs). We found that lower seeding density and lower cell-to-media volume ratio led to higher TNF α secretion. In addition, studies of small groups of macrophages cultured in microwells also suggest that cellular polarization may also depend on the absolute number of cells in the culture. Our results highlight several factors that needed to be considered when designing cell culture studies for macrophages, both in traditional culture systems and in miniaturized platforms.

RESULTS

Macrophage secretion of TNF α and IL10 in response to inflammatory stimuli is density-dependent

We first evaluated the effects of cell seeding density, a parameter that often varies among different studies, on macrophage activation by soluble stimuli. BMDMs were seeded at different densities and stimulated with pro-inflammatory ligands, LPS and IFN γ together or LPS alone [Fig. 1(a)]. In response

98 to LPS and IFN γ , macrophage secretion of TNF α increased as the seeding density increased from
99 2.6×10^3 to 2.6×10^5 cells/cm 2 ; however, TNF α concentration decreased when the seeding density was
100 further increased from 2.6×10^5 cells/cm 2 to 5.1×10^5 cells/cm 2 [Fig. 1(b)]. Dividing the total amount of
101 TNF α secreted by the number of cells seeded, or per cell TNF α secretion, showed a continuously
102 decreasing trend with increasing cell densities [Fig. 1(c)]. Stimulation with LPS alone also showed
103 decreasing per cell TNF α secretion with increasing seeding density and increasing overall TNF α
104 concentration with increasing cell seeding density, but no decrease at the highest seeding density [Figs.
105 S1(a) and S1(b)].

106 To understand the temporal dynamics of the density dependent TNF α secretion, macrophages
107 were seeded overnight at low (5.1×10^3 cells/cm 2), intermediate (7.7×10^4 cells/cm 2), and high (2.6×10^5
108 cells/cm 2) densities, stimulated, and the supernatant was subsequently collected at 2, 6, 12, and 24
109 hours for analysis of secreted cytokines. As expected, the LPS and IFN γ -stimulated macrophages
110 seeded at higher densities exhibited higher TNF α secretion across all time points [Fig. 1(d)]. Although
111 the general trends between cells seeded on both surfaces were similar, some differences in the fold
112 changes in cytokine secretion at different densities were observed [Figs. S2(a), S2(b), S2(e), and
113 S2(f)]. Stimulation with LPS and IFN γ or LPS alone both led to similar trends in TNF α secretion when
114 analyzed per-cell, with similar TNF α levels across all densities observed after 2 hours of stimulation
115 and decreased TNF α levels with increasing densities at all of the later time points (6, 12, 24 h) [Figs.
116 1(e), S1(c) and S1(d)]. Overall, macrophages exhibit density-dependent effects on TNF α secretion,
117 with cells seeded in higher density secreting less TNF α when evaluated per-cell. In addition, density-
118 dependent effects were less apparent at the earlier time points after stimulation but became more
119 pronounced at later stages of the activation.

120 The effects of seeding density on IL10 secretion were also examined. In macrophages
121 stimulated with LPS and IFN γ , secretion of IL10 increased with increasing densities [Fig. 1(f)], but the
122 per-cell IL10 secretion appeared to exhibit a biphasic response, with a peak at around 7.7×10^4 cells/cm 2
123 and decreasing with lower or higher seeding densities [Fig. 1(g)]. For macrophages stimulated with
124 LPS alone, a similar increasing trend in IL10 secretion with increasing seeding densities was observed
125 [Fig. S1(e)]. However, a biphasic response was not present, and the per-cell IL10 secretion exhibited
126 much less variation across all seeding densities [Fig. S1(f)]. Evaluation of IL10 at multiple time points
127 showed that higher density cultures exhibited greater concentrations of IL10 in both LPS alone and LPS
128 and IFN γ stimulation conditions across most of the time points examined [Figs. 1(h) and S1(g)]. For
129 the LPS and IFN γ stimulation condition, the per-cell IL10 secretion was similar across the different
130 seeding densities at different time points [Fig. 1(i)]. In contrast, higher seeding densities corresponded

to higher per-cell IL10 secretion across the different time points in cells stimulated with LPS alone [Fig. S1(h)]. It is worth noting again that cells were seeded onto tissue culture plastic directly for the time course study, while for the initial experiments on seeding densities, cells were seeded on glass coverslips placed in tissue culture plates. Comparing the trends from the two substrates yielded only moderate differences [Figs. S2(c), S2(d), S2(g), and S2(h)]. Overall, the secretion of IL10 by macrophages appears to be density dependent as well. However, these effects may be sensitive to different factors including the batch-to-batch variability in cell donor source, ligands used in stimulation, and culture surfaces.

Contribution of culture media volume to the density-dependent effects

The observed density-dependent effects may be a result of paracrine signaling or the physical interactions among cells, which are both enhanced as the seeding density increases. To better control the extent of paracrine signaling, we cultured macrophages within different volumes of media, but all seeded at the same density of 5.1×10^4 cells/cm², which corresponded to the cell-to-media-volume ratio of the cultures seeded at 5.1×10^4 , 7.7×10^4 , and 1.3×10^5 cells/cm² in the previous experiments [Figs. 2(a) and 2(b)]. As expected, the TNF α and IL10 concentration increased with decreasing volume of cell culture media, or as the cell-to-media-volume ratio was increased [Figs. 2(c) and 2(d)]. The per-cell IL10 secretion stayed relatively constant across different media volumes, consistent with the IL10 measurements in the corresponding cell-to-media-volume ranges in the previous density experiments [Fig. 2(f)]. However, per-cell TNF α secretion decreased in culture stimulated in less media volumes, with samples from the lowest media volume group having almost 30% lower in per-cell TNF α secretion than those in the highest media volume group [Fig. 2(e)]. Since the number of cells in the culture well was the same for both samples, these results suggested that paracrine interactions among cells partially contribute to macrophage activation in response to pro-inflammatory ligands.

Microwell culture on the coordination among small groups of macrophages and the subsequent inflammatory responses

Our work showed that macrophage activation is dependent on cell density and suggested that soluble paracrine signals play an important role. However, the effects of cell density in small populations of macrophages, which becomes critical as the cell culture platforms are miniaturized, remained unknown. To address this, we isolated individual cells or small groups of cells in arrays of microwell and assessed their response to inflammatory agonists. Here, we evaluated the expression of iNOS, an inflammatory marker, which allowed us to assess the inflammatory levels of individual cells through

164 immunofluorescence staining and compared the expression levels to cells seeded at different seeding
165 densities in bulk culture [**Fig. 3(a)**]. To ensure the media volume per cell for macrophages in
166 microwells was consistent with our earlier studies, only macrophages in wells containing 1 to 6 cells
167 were analyzed. We observed a wide range of iNOS staining intensity for cells in both microwell and
168 population studies [**Figs. 3(b) – 3(e)**]. When comparing the median intensity of iNOS staining for cells
169 in wells containing different numbers of cells, we observed an increase in iNOS expression in response
170 to an increasing number of cells in the microwells [**Fig. 3(f)**]. In contrast, a decrease in iNOS
171 expression was observed as cell density increased in tissue culture wells. Normalizing the results from
172 these studies based on equivalent cell-to-media-volume-ratio, we found that the cells cultured in bulk
173 still decrease in iNOS expression with increasing seeding densities, in contract to the results in the
174 microwells [**Fig. 3(g)**].

175 In both the bulk and microwell studies, it appeared that following the pro-inflammatory
176 stimulation, only a fraction of cells exhibits significant iNOS expression above the baseline level,
177 which we defined as two standard deviations above the mean of the iNOS signal for the unstimulated
178 population [**Figs. 5(d) and 5(e)**]. This observation agreed with other studies on macrophage activation
179 at single cell level demonstrating precociously activated cells ^{6,8}. To better characterize how
180 interactions among a small group of cells may shift the distribution of the iNOS expression for the cell
181 population, all cells included in the analysis were categorized based on their iNOS staining intensity:
182 non-expressing, 0-20, 20-40, 40-60, 60-80, and 80-100 percentile of iNOS expression [**Fig. 4A**]. This
183 analysis revealed that when the number of cells in a well increased, the overall cell population generally
184 shifted from below-baseline to higher iNOS expression. To assess whether high iNOS expressing cells
185 in a well could be associated with higher overall percentage of iNOS expression for cells in the same
186 well, the percentage of iNOS expressing cells in a well was plotted against the staining intensity of the
187 highest iNOS expressing cell in the same well [**Fig. 4B**]. We found that wells with at least one cell
188 having high iNOS expression appeared to be associated with having higher overall percentage of cells
189 expressing iNOS above baseline. This trend appeared to be maintained for wells containing 2-6 cells.
190 Together with the bulk culture data, these data suggest that communication among the macrophage
191 population depends not only on the density of the cell population, but also on absolute cell numbers. In
192 addition, higher iNOS expressing cells may promote the activation of iNOS in neighboring cells. These
193 factors likely all contribute to the coordinated response of macrophage populations.

194

195 **DISCUSSION**

196 In this study, we identified seeding density and cell-to-media volume ratio as critical *in vitro* culture
197 parameters that influence macrophage activation. Increasing seeding density caused increasing
198 inhibitory effects on macrophage polarization, as per-cell TNF α secretion exhibited a decreasing trend
199 with increasing seeding densities. Our results contrast with some earlier reports of increased TNF α
200 transcription and production with increasing seeding density ^{6,8}, possibly due to the utilization
201 macrophage cell lines compared to the primary cells in this study. We also found that seeding density
202 exerted more effects at the later phase of the inflammatory activation than the early phase, since
203 variations were minimal at the earlier time points and became more apparent at the later hours. Soluble
204 factors produced by the cells following stimulation likely contributes to the negative feedback that
205 dampens TNF α secretion, as per cell TNF α secretion was lower when cells were stimulated in lower
206 volume compared to those stimulated in higher volume. This result is consistent with the fact that
207 macrophages are known to secrete inhibitory cytokines such as IL10 to regulate their activation ^{16,17}.
208 Interestingly, culture within a microwells showed a different response, where overall activation
209 increased for small groups of cells compared to cells in isolation. In addition, having at least one cell
210 with a higher iNOS expression level was associated with higher percentage of iNOS activation in the
211 same microwell, suggesting that highly activated cells may promote the polarization of neighboring
212 cells, possibly through soluble factors. This agrees with previous studies on macrophages and dendritic
213 cells, in which a small subpopulation of precocious or high-secreting cells help coordinate the overall
214 responses of the cell population ^{8,18}. Together, these results suggest that macrophages possess feedback
215 mechanisms that help them tune their functions in response to their population size and density.

216 Increasing cell density leads to a corresponding secretion of more soluble factors, which can
217 directly feedback to regulate inflammation. For example, IL10 is a well-known negative regulator that
218 is secreted by macrophages stimulated with LPS, and leads to dampening of inflammation after the
219 initial activation period. Blocking IL10 signaling via IL10 neutralizing antibody, IL10 receptor (IL10R)
220 blocking antibody, or the use of BMDM from an IL-10R deficient mouse all resulted in increased levels
221 of TNF α secretion ^{8,19}. Other soluble factors, including IFN β , nitrogen oxide, and PGE₂, have also been
222 shown to be implicated in macrophage feedback control^{19–22}. However, in a recent study, exogenous IL-
223 10 was insufficient by itself to abrogate density-dependent effects on inflammatory activation ⁶. This
224 study utilized reporter systems to track NF κ B activity and TNF α secretion in RAW264.7 cells, and
225 revealed that cells exhibited density-dependent bimodal activation states following LPS stimulation,
226 which was independent of exogenous IL10. On the other hand, the same study suggested that soluble
227 factors secreted during the resting phase may prime macrophages to respond differently following
228 activation ⁶. At resting state, high density culture exhibited higher levels NF κ B than that of low density

229 culture. In addition, passaging cells at a higher density prior to experimentation, as well as conditioned
230 media from high density culture, increased reporter expression both with and without stimulation.
231 Together with our results, these findings suggest regulation of cellular responses by density likely
232 involve activities both before and after pro-inflammatory stimulation. How various factors may work
233 together or against each other to orchestrate a collective response will require further study.

234 Our results reveal complexities in the collective interaction within population of cells and
235 underscore the need for well-controlled *in vitro* culture systems to characterize these phenomena. When
236 comparing the results from the bulk and microwell culture system, we found that paracrine-based
237 regulation is context-dependent. Among small numbers of macrophages in a microwell, paracrine
238 interactions exerted pro-inflammatory effects. However, at higher cell numbers associated with bulk
239 culture, anti-inflammatory effects resulted. These observations were only discovered under more
240 precise control of cellular environment of a microwell system, and traditional bulk culture system itself
241 is insufficient to evaluate these parameters. In addition, macrophages are sensitive to other
242 environmental conditions, including changes in biophysical cues, which can be better controlled and
243 studied using *in vitro* platforms^{23,24}. Microphysiological systems possess many favorable characteristics
244 including flexibility in the design of the system, as well as the ability to pattern or control the
245 multicellular architecture cells to better mimic the *in vivo* environment¹². In addition, the ability to
246 integrate different physical stimuli into the system, such as mechanical stretch²⁵, also allows these
247 systems to study the possibility of macrophages communicating features of physical environments
248 through soluble signals. Further advancements in microphysiological systems may help uncover new
249 mechanisms in regulation of macrophage activation.

250 Our studies highlight several important challenges regarding the design for *in vitro* culture
251 studies, especially for micro-scale cultures. First, it is necessary to choose proper culture parameters
252 when designing experiments, since there is a possibility that the experimental results are influenced by
253 specific conditions. Both our microwell studies and other published work showed that size of the cell
254 population affects the cellular characteristics²⁶. It is also important to consider these variables when
255 comparing results from different studies. It has been previously noted that reporting of specific culture
256 parameters is necessary to ensure reproducibility²⁷, and our study reinforced this notion by
257 demonstrating that experimental design strongly influence macrophage behavior and experimental
258 outcomes. These two points suggest both opportunities and challenges for micro-scale cultures: these
259 systems enable better control and modeling of physiological cellular processes, but micro-scale and
260 macro-scale culture indeed introduce widely different environmental conditions. To facilitate better

comparisons across different studies, further study will be needed to understand how the different culture parameters between both culture formats could affect experimental outcomes.

CONCLUSION

In this study, we report that cell seeding density and cell-to-media-volume ratio, two common culture parameters, both affect macrophage activation following pro-inflammatory activation. These results signify the importance of the experimental design in *in vitro* studies of macrophage biology and offer insights about how paracrine interactions among macrophage populations influence their function. The results provided by our study may provide a starting point to help in the design of the future studies involving micro-scale culture platform, and ensure that the results could capture the *in vivo* conditions, as well as facilitating the comparison of the results with the established macro-scale culture systems.

METHODS

Cell isolation and culture

Bone marrow-derived macrophages (BMDM) were obtained by flushing bone marrow cells from the femur and tibia of C57BL/6J mice aged between 6 to 12 weeks, and then treating with ACK lysis buffer (Life Technology) to remove red blood cells. The cells were then cultured in DMEM media supplemented with 10% heat-inactivated fetal bovine serum (Cytiva), 1% penicillin/streptomycin, 2 mM L-glutamine (both from Life Technology), and 10% macrophage-colony stimulating factor (M-CSF) containing conditioned media for seven days, with a media change on the third day. For experiments, cells were lifted from the plate using cell dissociation buffer (Life Technology) and gentle scrapping for further use.

Cell density studies

BMDM were seeded in 1 ml onto 18 mm glass coverslips in 12 well plates to achieve densities ranging from 5.1×10^5 to 2.6×10^3 cells/cm². After overnight incubation, cells were stimulated with 10 ng/ml of ultrapure LPS (Invivogen) and IFN γ (R&D System) for 24 hours before supernatants were collected for analysis. To investigate the dynamics of cytokine secretion, separate experiments were set up with cells seeded in 24 well plates at the density of 5.1×10^3 , 7.7×10^4 , and 2.6×10^5 cells/cm². Following stimulation, the supernatant was collected after 2, 6, 12, and 24 hours for analysis. To assess the role of secreted factors in the observed density-dependent effect of macrophages, 2×10^5 BMDM were seeded onto 12 well plates in 1 ml to achieve a seeding density of 5.1×10^4 cells/cm², allowed to adhere

294 overnight, and stimulated with media containing 10 ng/ml of LPS and IFN γ at the volumes of 1 ml,
295 0.667 ml, and 0.4 ml. This corresponds to the cell-to-media volume ratio equivalent to cells seeded at
296 5.1×10^4 , 7.7×10^4 , and 1.3×10^5 cells/cm² in a 12 well plate. After 24 hours, the supernatant was collected
297 for analysis.

298

299 **Measurement of cytokines**

300 Supernatants were analyzed for TNF α and IL10 secretion using the ELISA kits purchased from
301 Biolegend following protocols recommended by the manufacturer.

302

303 **Fabrication of the microwell membranes**

304 Silicon wafers with arrays of microwells were fabricated using standard photolithography techniques ⁹.
305 In short, SU8 photoresist (MicroChem) was spin-coated onto a silicon wafer, baked, and then exposed
306 under UV illumination through a custom-designed mask (CAD/Art Services) with patterns of rectangles
307 of 200x300 μ m in size. The wafer was subsequently baked before it was developed in SU8 developer
308 (MicroChem) to create patterns of rectangles with a size of 200x300 μ m. To create PDMS microwell
309 membranes for single-cell experiments, PDMS and curing agent were mixed in 10:1 ratio, degassed in a
310 desiccator, and then spin-coated onto a silicon master with patterns of microwells to create membranes
311 with through-holes at a thickness of around 50 μ m. Circular PDMS rings were subsequently deposited
312 onto the master to facilitate the separation of the microwell membranes from the master. The PDMS-
313 coated master was then baked in an oven at 65°C overnight for the PMDS to cure. Afterward, the
314 PDMS microwell membranes were carefully peeled off from the master, cleaned with 70% ethanol, and
315 dried in an oven overnight before being used.

316

317 **Microwell-based cell studies**

318 18 mm coverslips were UVO-treated and then coated with fibronectin (Corning) at room temperature
319 for 1 hour. Afterward, both the coverslips and cleaned PDMS microwell membranes were UVO-treated
320 again before being bonded together and the PDMS ring support being removed. The microwell
321 membrane constructs were then coated with 2% Pluronic F-127 (Sigma Aldrich) for an hour and then
322 washed with PBS for subsequent experiments. The microwell membrane substrates were placed in a 12
323 well plate and seeded with 1.5 ml of cell suspension at a concentration of 10,000 cells/ml. After
324 overnight incubation, cells in the microwell were stimulated with 10ng/ml of LPS and IFN γ , and the
325 microwells were sealed by applying pressure to hold the substrate against a glass slide using a custom
326 holder. After 24 hours, the microwell substrates were separated from the holder and the glass slide,

327 stained with a fixable dead stain (Life Technology), and then fixed with 4% paraformaldehyde
328 (Electron Microscopy Science) for 5 minutes before being washed with PBS and blocked with 2%
329 bovine serum albumin (BSA, MP Biomedical) overnight.

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331 **Immunofluorescence staining and image analysis**

332 Fixed samples were stained with a rabbit polyclonal anti-iNOS antibody (Abcam) at a dilution of
333 1:1000 overnight. After washing with 1% BSA three times, samples were stained with Alex Fluor 488
334 (goat) anti-rabbit secondary antibody (Abcam) at the dilution of 1:1000, and Hoechst 33342 (Life
335 Technologies) at 1:1000, for 1 hour. Subsequently, samples were washed with 1% BSA three times
336 again and rinsed with phosphate-buffered saline (PBS) before being mounted onto glass slides with
337 Fluoromount-G (Southern Biotech). Samples were imaged using an Olympus IX-83 (Olympus)
338 epifluorescence microscope, at a magnification of 20X, and the resultant data were processed using
339 FIJI/ImageJ ²⁸. For microwell construct samples, substrates were scanned using Olympus IX-83 to
340 obtain images at green (iNOS), blue (Hoechst), red (dead stain), and brightfield channels. The
341 brightfield channel was used to identify the locations and boundaries of each microwell, while the blue
342 (Hoechst) channel was used to identify the locations of the cells. The latter was also used as a mask to
343 sample the intensity of the iNOS and the dead staining. The fixable dead stain was used to exclude dead
344 cells from the subsequent analysis, and the threshold was determined by taking the 1st percentile of the
345 staining intensity for cells treated with 70% ethanol. After initial image-stitching and processing using
346 the Grid/Collection Stitching plugin in FIJI/ImageJ ²⁹, cell locations were mapped onto well locations
347 using custom MATLAB (Mathworks) codes, and the resultant location and intensity data of cells were
348 analyzed using R Studio.

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350 **Statistical analysis**

351 Data were analyzed using one way ANOVA followed by Tukey's HSD Test.

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SUPPLEMENTARY MATERIALS

See the supplementary materials for Figs. S1-S3 showing the effects of cell seeding density with LPS only stimulation, comparison across different adherent surfaces, and additional data from the microwell experiments.

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AUTHOR DECLARATIONS

Conflict of interest

The authors have no conflicts to disclose

Ethics approval

All protocols involving animals were approved by the University of California Irvine’s Institutional Animal Care and Use Committee (protocol #AUP-17-85 and AUP-20-47), which is accredited by the Association for the Assessment and Accreditation of Laboratory Animal Care International (AAALACi). No human subjects were involved in this study.

DATA AVAILABLLITY

The data that supports the findings of this study are available within the article and its supplementary material. Additional data that support the findings of this study are available from the corresponding author upon reasonable request.

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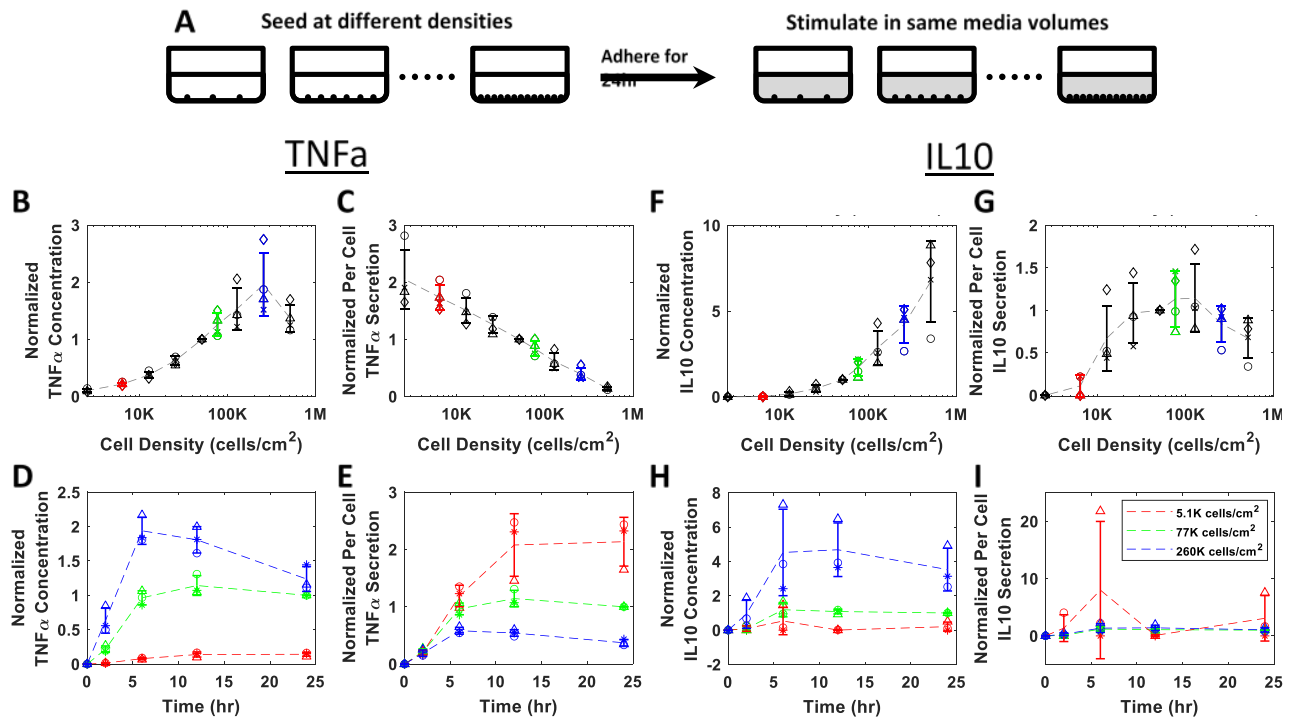


Figure 1: Macrophages exhibit density-dependent cytokines secretion under LPS and IFN γ stimulation. (A) Schematic of experiments examining cytokine secretion of macrophages seeded in different densities. (B - E) TNF α concentration (B) and per-cell TNF α secretion (C) of BMDM seeded at different densities on glass, and TNF α concentration (D) and per-cell TNF α secretion (E) at different time points after BMDM seeded at selected densities on polystyrene. (F – I) IL10 concentration (F) and per-cell IL10 secretion (G) of BMDM seeded at different densities on glass, and IL10 concentration (H) and per-cell IL10 secretion (I) at different time points for BMDM seeded in selected densities on polystyrene. n=4 for figure B, C, F, G, and n=3 for figure D, E, H, I.

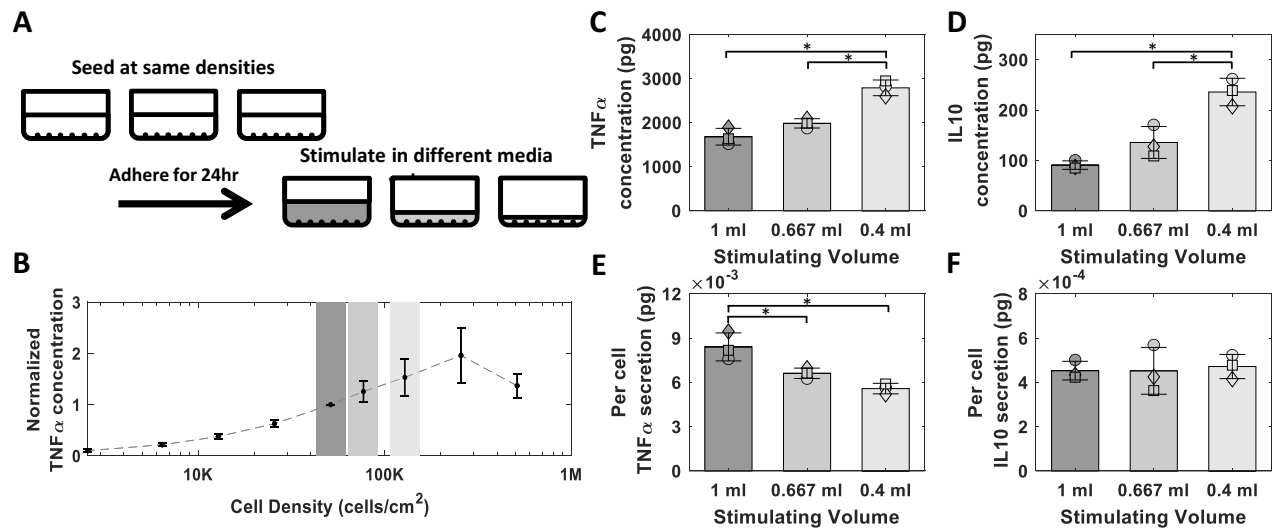


Figure 2: Soluble factors partially contribute to density-dependent effects on macrophage activation. (A) Schematic of the experiment; cells were seeded at an identical seeding density and cell-to-media-volume ratio, allowed to attach for 24 hours, and then stimulated with LPS and IFN γ at 10ng/ml in different volumes of media (1ml, 0.667ml, 0.4ml) for 24 hours. (B) Graph indicating the selected stimulation volumes (1ml, 0.667ml, 0.4ml) in relation to earlier density experiments in terms of cell-to-media volume ratio equivalence; colors corresponding to bars in C-F. (C, D) (C) TNF_α and (D) IL10 concentration of BMDM stimulated with LPS and IFN γ containing media at 1ml, 0.667ml, and 0.4ml. (e, f) per cell secretion of (E) TNF_α and (F) IL10 for BMDM stimulated with LPS and IFN γ containing media at 1ml, 0.667ml, and 0.4ml. (n=3 for all conditions, * indicates $p < 0.05$; One way ANOVA followed by Tukey HSD Test).

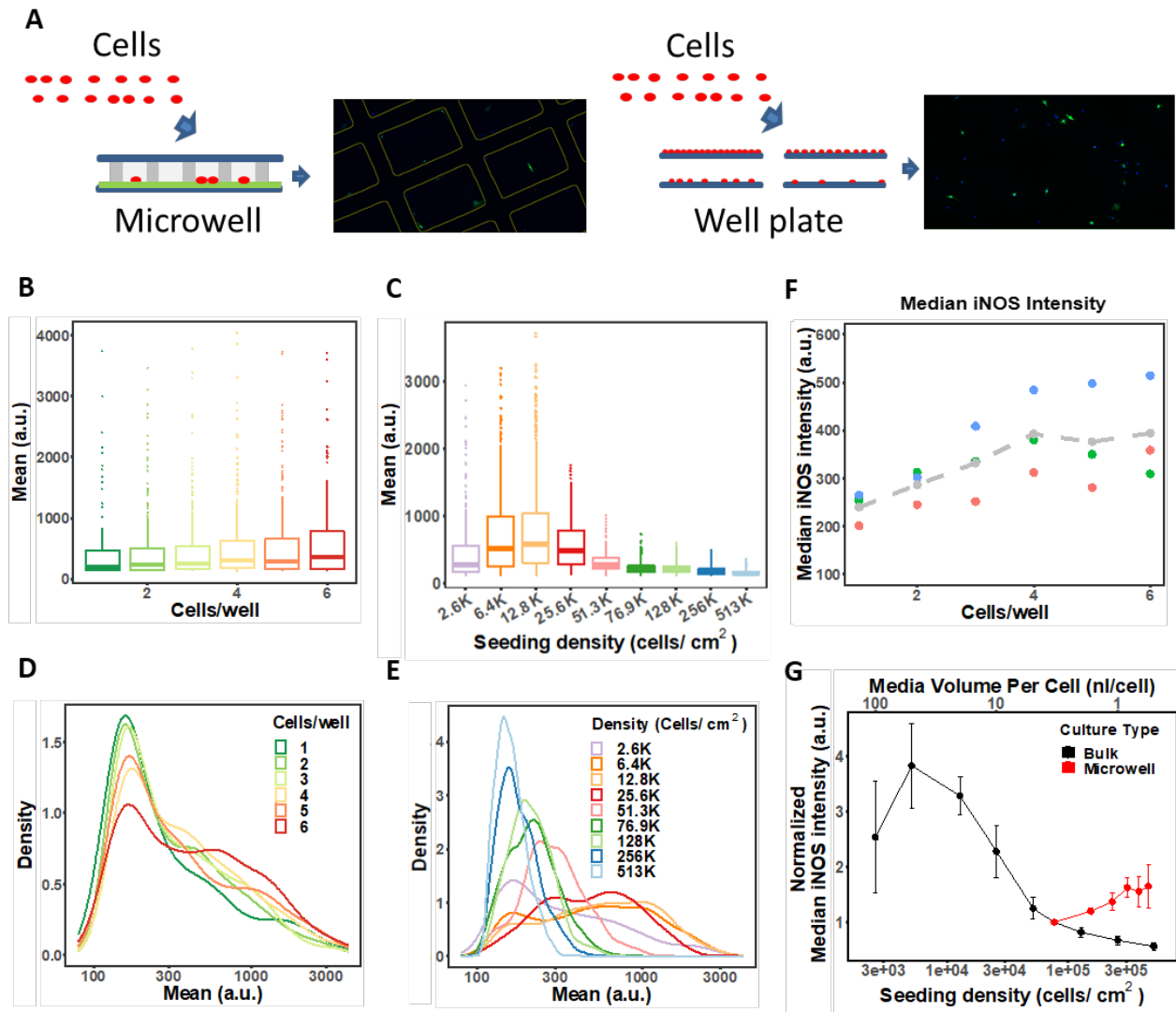


Figure 3: Comparison of density-dependent effects in micro- vs. macro-scale cultures. (A)

Schematic of the microwell experiment to delineate the effects of single cell vs groups of cells on macrophage activation, and the bulk density experiment for comparison. (B, C) Dot plots of sampled iNOS intensities for cells in (B) microwell experiments with microwells containing 1-6 cells and (C) bulk experiments for seeding densities ranging from 2.6×10^3 cells/cm² to 5.13×10^5 cells/cm². (D, E) Density plots of sampled iNOS intensities for (D) the microwell experiments and (E) the bulk experiments. (F) Median iNOS intensity for population of cells in wells containing 1-6 cells over three experiments. Different colors denote to data from different replicates, and the gray plot represents the mean value. (G) Comparison of the normalized median iNOS intensity of cells from the microwell and bulk experiments. Data were arranged so the cell-to-media volume for results from both experiments were comparable. $n=3$ for each condition in panel G.

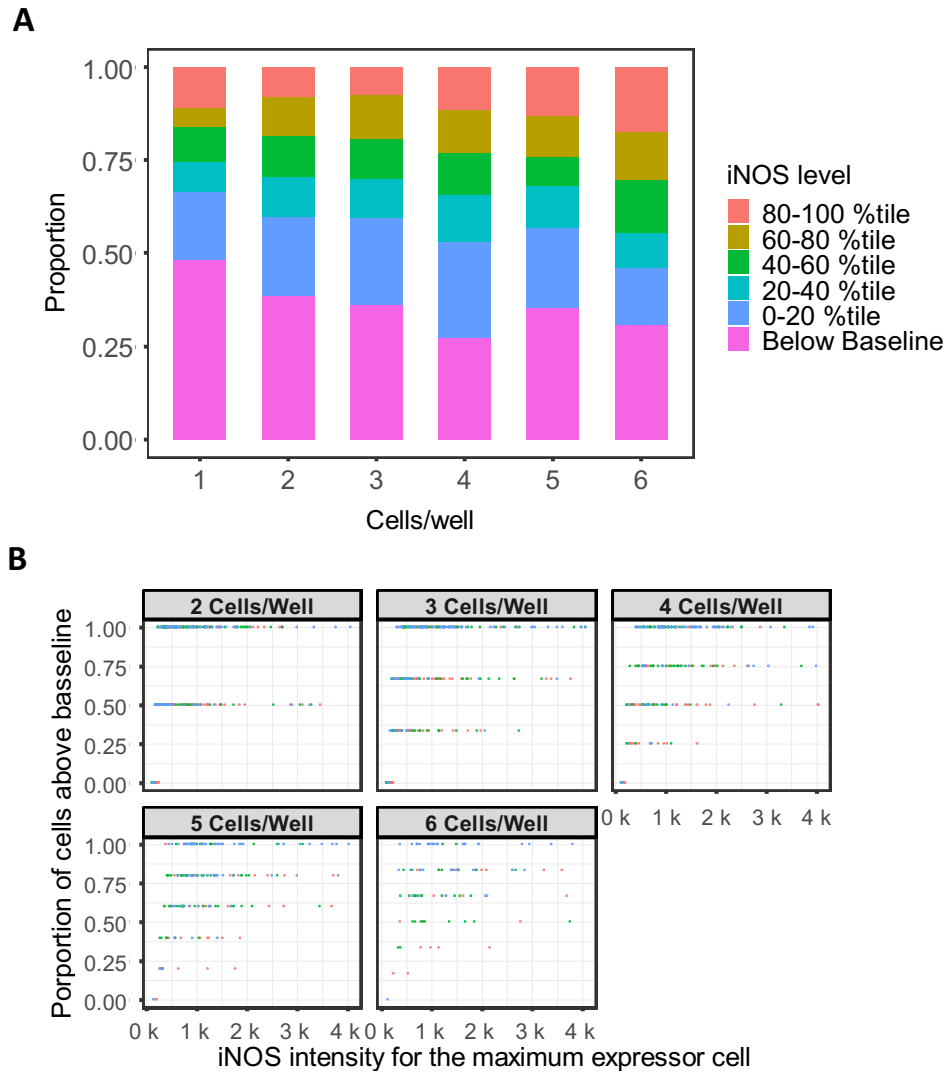
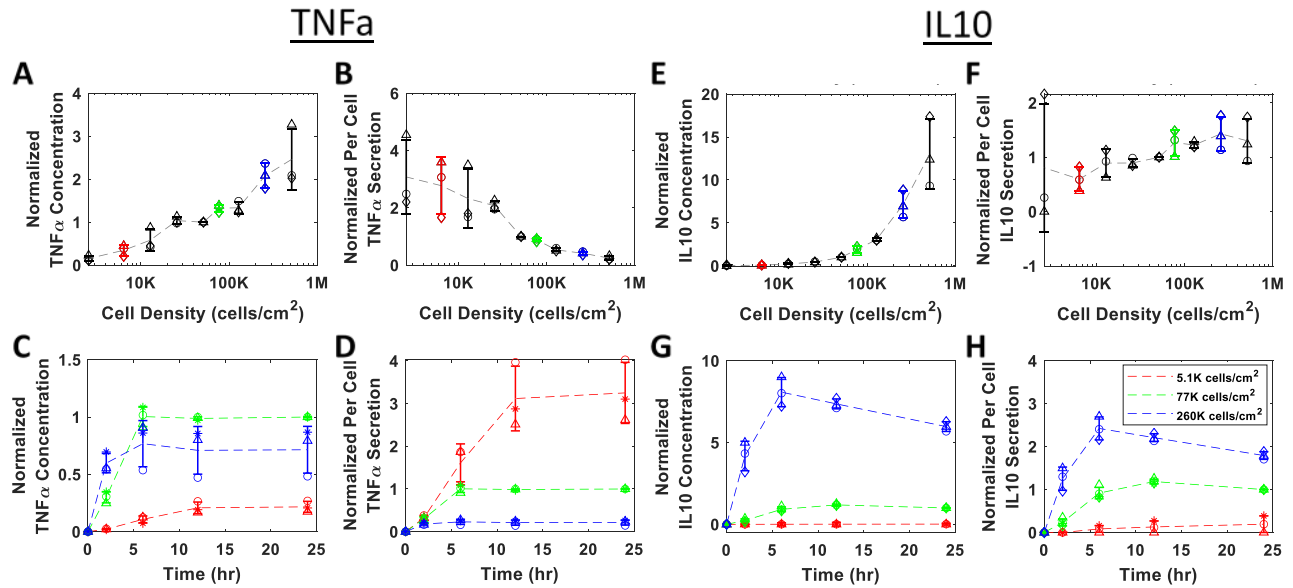
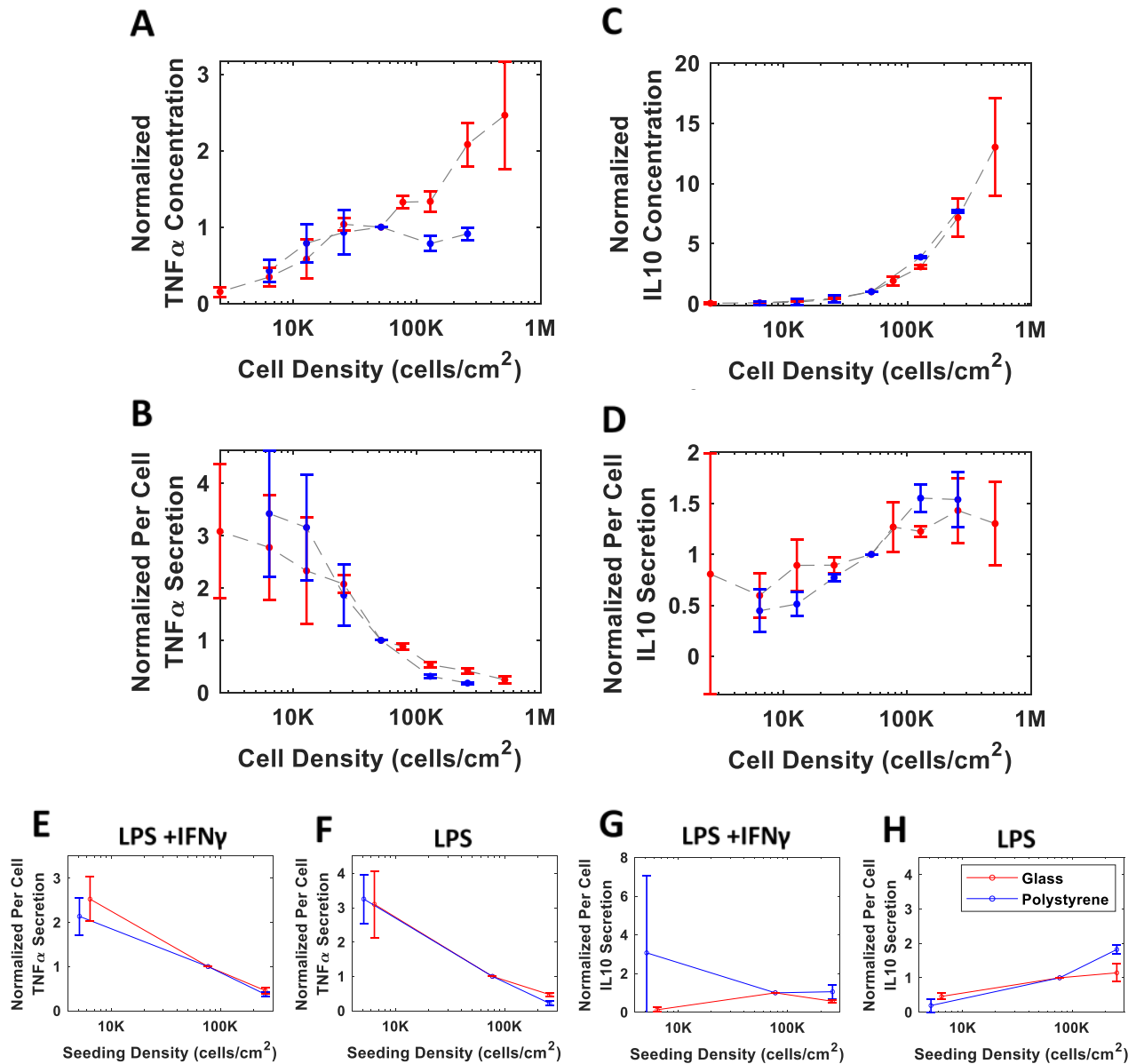


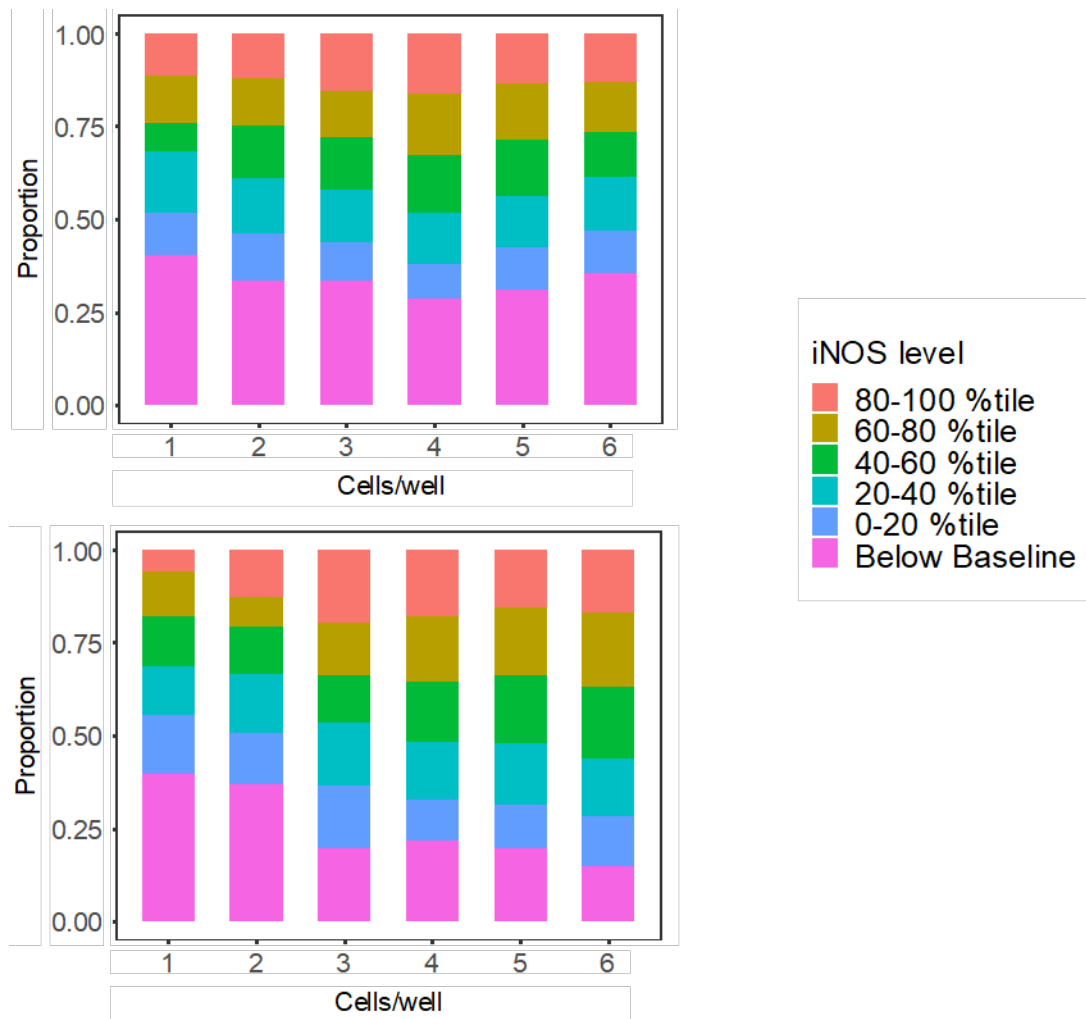
Figure 4: Microwell experiments revealed a different mode of density-dependent regulation of macrophage function. (A) A representative sample of distribution of all living cells in wells containing 1-6 cells grouped by their percentile rank. These cells were first separated based on whether their iNOS expression level is above or below the baseline. For those that were above the baseline, they were further separated into 5 groups according to their percentile ranks in iNOS expression (80-100 percentile, 60-80 percentile, 40-60 percentile, 20-40 percentile, and 0-20 percentile). (B) Graphs showing the relationship between the activation level of the highest expressing cell in a well and the percentage of positive iNOS expressing cells in the same well. The data were group based on the number of cells in a well, ranging from 2 – 6 cells, with data from three biological replicates. Each color indicates data from the same biological replicate.



Supplement figure 1: Macrophages exhibit similar density-dependent modulation of cytokines secretion when stimulated with LPS only. (A - D) Graphs showing TNF α secretion; (A) concentration and (B) per-cell TNF α secretion of BMDM seeded at different densities (on glass). (C) TNF α concentration and (D) per-cell TNF α secretion at different time points for BMDM seeded in selected densities (on polystyrene). (E - H) Graphs showing IL10 secretion; (E) IL10 concentration and (F) per-cell IL10 secretion of BMDM seeded at different densities (on glass). (G) IL10 concentration and (H) per-cell IL10 secretion at different time points for BMDM seeded in selected densities (on polystyrene). n=3 for all conditions.



Supplement figure 2: Density-dependent effects of LPS-mediated macrophage activation is maintained on different adhesive surface. (A, B) Normalized (A) TNF α concentration and (B) per-cell TNF α secretion of BMDM stimulated with LPS (10ng/ml) on either glass or tissue culture-treated polystyrene surface. (C, D) Normalized (C) IL10 concentration and (D) per-cell IL10 secretion of BMDM stimulated with LPS (10ng/ml) on either glass or tissue culture-treated polystyrene surface. (E, F) Normalized per cell TNF α secretion for cells seeded on glass (red) and TCPS (blue) in different densities stimulated with (E) LPS + IFN γ and (F) LPS only. (G, H) Normalized per cell IL10 Secretion for cells seeded on glass (red) and TCPS (blue) in different densities stimulated with (g) LPS + IFN γ and (h) LPS only. Data for cytokine secretion from cells on the glass or polystyrene surfaces were normalized to the secretion level at the density of 51K cells/cm² for each surface condition. Thus, only the trends between both groups are comparable, and the magnitude between both groups are not comparable. n=3 for all conditions.



Supplement figure 3: Compared to cells in isolation, cells in small groups generally have higher expressions of iNOS. Distribution of all cells in wells containing 1-6 cells; these cells were separated based on their iNOS expression levels. For cells above the baseline, they were further separated into 5 groups according to their percentile ranks in iNOS expression (80-100 percentile, 60-80 percentile, 40-60 percentile, 20-40 percentile, 0-20 percentile). Each graph represents a different experimental replicate.