



Neutron spin echo shows pHLIP is capable of retarding membrane thickness fluctuations

Haden L. Scott^a, Violeta Burns-Casamayor^b, Andrew C. Dixon^a, Robert F. Standaert^{a,b,c}, Christopher B. Stanley^{d,e}, Laura-Roxana Stingaciu^{f,g}, Jan-Michael Y. Carrillo^{e,h}, Bobby G. Sumpter^{e,h}, John Katsaras^{d,f,i}, Wei Qiang^j, Frederick A. Heberle^k, Blake Mertz^{b,l}, Rana Ashkar^{m,n,*}, Francisco N. Barrera^{a,**}

^a Department of Biochemistry & Cellular and Molecular Biology, University of Tennessee, Knoxville, TN 37996, United States of America

^b C. Eugene Bennett Department of Chemistry, West Virginia University, Morgantown, WV 26506, United States of America

^c Biosciences Division, Oak Ridge National Laboratory, Oak Ridge, TN 37831, United States of America

^d Shull Wollan Center – a Joint Institute for Neutron Sciences, Oak Ridge, TN 37831, United States of America

^e Computational Sciences and Engineering Division, Oak Ridge National Laboratory, Oak Ridge, TN 37831, United States of America

^f Labs and Soft Matter Group, Neutron Scattering Division, Oak Ridge National Laboratory, Oak Ridge, TN 37831, United States of America

^g JCNS1, FZJ outstation at SNS, Oak Ridge National Laboratory, Oak Ridge, TN 37831, United States of America

^h Center for Nanophase Materials Sciences, Oak Ridge, TN 37831, United States of America

ⁱ Department of Physics and Astronomy, University of Tennessee, Knoxville, TN 37996, United States of America

^j Department of Chemistry, the State University of New York, Binghamton, NY 13902, United States of America

^k Department of Chemistry, University of Tennessee, Knoxville, TN 37920, United States of America

^l West Virginia University Cancer Institute, Morgantown, WV 26506, United States of America

^m Department of Physics, Virginia Tech, Blacksburg, VA 24061, United States of America

ⁿ Center for Soft Matter and Biological Physics, Virginia Tech, Blacksburg, VA 24061, United States of America

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ABSTRACT

Cell membranes are responsible for a range of biological processes that require interactions between lipids and proteins. While the effects of lipids on proteins are becoming better understood, our knowledge of how protein conformational changes influence membrane dynamics remains rudimentary. Here, we performed experiments and computer simulations to study the dynamic response of a lipid membrane to changes in the conformational state of pH-low insertion peptide (pHLIP), which transitions from a surface-associated (SA) state at neutral or basic pH to a transmembrane (TM) α -helix under acidic conditions. Our results show that TM-pHLIP significantly slows down membrane thickness fluctuations due to an increase in effective membrane viscosity. Our findings suggest a possible membrane regulatory mechanism, where the TM helix affects lipid chain conformations, and subsequently alters membrane fluctuations and viscosity.

1. Introduction

Cell membranes perform and regulate key biological functions through a delicate interplay between lipids and proteins [1–5]. Examples range from the role of membrane curvature during the photochemical cycle of rhodopsin and the gating behavior of mechanosensitive channels [6–8], to the regulatory effect of membrane thickness on the enzymatic activity of membrane proteins [3,9,10]. Overall, these studies have significantly contributed to our

understanding of how the structural features of lipid membranes, such as bilayer thickness and curvature, can influence the function of membrane-associated proteins [11–13]. Despite these advances, major gaps still exist in our understanding of how membrane proteins alter the properties of their host membranes. More importantly, while it is accepted that membranes play a key role in the spatiotemporal regulation of protein-lipid interactions, for example, in cell signaling [14–16], our knowledge of membrane dynamics is still in its nascent stages [17]. Conformational molecular changes and collective motions prompted by

* Correspondence to: R. Ashkar, Department of Physics, Virginia Tech, Blacksburg, VA 24061, United States of America.

** Corresponding author.

E-mail addresses: ashkar@vt.edu (R. Ashkar), fbarrera@utk.edu (F.N. Barrera).

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environmental cues or molecular recognition [18–20] are not only central to biological function, but can significantly inform the next generation biosensors, therapeutics, and smart biomaterials [18]. Thus, the ability to access membrane dynamics on relevant length and time scales is pivotal to understanding the dynamic cooperativity taking place in lipid-protein complexes.

Here, we explore the dynamic response of model membranes to large conformational changes in associated peptides – i.e., on the time scales of protein conformations and collective membrane fluctuations. Specifically, we use the pH-low insertion peptide (pHLIP), which assumes either a surface associated (SA) or a transmembrane (TM) state, depending on the pH of the medium. At neutral pH, pHLIP adsorbs to the membrane interface, but under acidic conditions it adopts a TM α -helix conformation [21,22]. This change is driven by pHLIP's acidic groups whose protonation triggers membrane insertion [23]. Notably, this pH-responsiveness imparts to pHLIP the ability to target aggressive solid tumors, typically marked by an acidic extracellular medium [24].

To probe changes in membrane dynamics associated with pHLIP's conformational changes, we used high-resolution neutron spin-echo (NSE) spectroscopy and molecular dynamics (MD) simulations. Findings from NSE spectroscopy experiments showed that TM-pHLIP results in a slowdown in the rate of membrane thickness fluctuations. These observations were confirmed by coarse-grained MD simulations [25]. Moreover, complementary all-atom MD simulations provided molecular-level insights into the interactions of TM-pHLIP with the membrane lipids, showing that TM-pHLIP alters lipid chain conformations and increases membrane viscosity. These findings may help us to gain insights not only into biological membrane function, but also into the design of artificial cells with tunable protein conformations.

2. Materials and methods

Reagents. 1,2-dioleoyl-*sn*-glycero-3-phosphocholine (DOPC), 1,2-dioleoyl-*sn*-glycero-3-phospho-L-serine (sodium salt) (DOPS), 1,2-dimyristoyl-*sn*-glycero-3-phosphocholine (DMPC), and cholesterol from ovine wool (Chol) were purchased from Avanti Polar Lipids (Alabaster, AL). D₂O (99.96 % D) was purchased from Cambridge Isotope Laboratories (Andover, MA). pHLIP (sequence: N₁-AAEQNPYY-WARYADWLFTPLLLDLALLVDADEGT-C₁) was synthesized using standard protocols (P3 Biosystems, Louisville, KY) and purified to >95 % purity by reverse-phase high performance liquid chromatography (HPLC). Dimethyl sulfoxide (DMSO) was purchased from Fisher Scientific (Hampton, NH). Sodium phosphate dibasic (>98.5 %) and sodium phosphate monobasic monohydrate (98 %) were purchased from Sigma-Aldrich (St. Louis, MO) and were used to prepare sodium phosphate buffer. Sodium deuterioxide (NaOD) and deuterium chloride (DCl) were purchased from Sigma-Aldrich (St. Louis, MO) and were used to adjust the final pH of the samples measured by neutron and x-ray scattering. Perdeuterated DOPC-d₆₆ and Chol-d₄₀ were synthesized as described elsewhere [26,27].

Sample preparation. DOPC:DOPS:Chol mixtures were prepared in chloroform at a molar ratio of 76:4:20, and were consequently dried under a steady flow of argon into thin films. The films were then kept under vacuum at 45 °C for 8 h to 10 h, after which they were hydrated with a 10 mM sodium phosphate (NaP_i) pH 8.0 buffer. The lipid solution was freeze-thawed 5 times with intermittent vortex-spinning and was then extruded through a polycarbonate membrane (100 nm pore size) using a Mini Extruder (Avanti Polar Lipids, Inc., Alabaster, AL) to form large unilamellar vesicles (LUVs). Samples containing pHLIP were prepared at a total lipid:peptide molar ratio of 150:1. This ratio includes any pHLIP molecules that might not be associated to the membrane. The required amount of pHLIP was introduced, in lyophilized form, into extruded vesicle suspensions at pH 8 and vortex mixed until fully incorporated. The sample pH was then changed to pH 4 to trigger the TM insertion of pHLIP. For NSE experiments, however, studies at pH 4 required a different sample preparation to avoid the flocculation of high

concentrations of membrane-unassociated pHLIP due to the high lipid concentration required in NSE measurements. In that case, pHLIP was co-dissolved with lipids in a chloroform-ethanol solution, prior to sample drying and vesicle extrusion.

Circular Dichroism. pHLIP was incubated with LUVs (prepared as described earlier) in 10 mM NaP_i pH 8.0 buffer for 1 h. Afterwards, the pH was adjusted with 100 mM NaOAc or NaP_i (62.5 μ L) to the desired final pH values. The final pH of the samples was measured after spectra were recorded. CD spectra were acquired using a Jasco (Easton, MD) J-815 spectropolarimeter interfaced with a Peltier system. Spectra were recorded at 25 °C using a 2 mm cuvette with a scan rate of 100 nm/min and 20 to 40 accumulations. Raw data were converted into mean residue ellipticity according to: $[\theta] = \frac{\theta}{10lc(N-1)}$, where θ is the measured ellipticity, l is the path length of the cell in cm, c is the protein concentration in M, and N is the number of amino acids. Appropriate blanks were subtracted in all cases.

Tryptophan Fluorescence Spectroscopy. To perform a pH insertion titration, sample pH was adjusted by mixing aliquots of 100 mM stocks of sodium acetate (NaOAc), MES [2-(*N*-morpholino) ethanesulfonic acid]], or HEPES [(4-(2-hydroxyethyl)-1-piperazine)ethanesulfonic acid]] buffers (25 μ L), to obtain the desired pH values. Final sample pH was measured using a 2.5 mm bulb pH-electrode (Microelectrodes, Inc., Bedford, NH). Tryptophan fluorescence emission spectra were recorded using a Photon Technology International (Edison, NJ) Quanta Master fluorometer at an excitation wavelength of 280 nm, an emission wavelength range of 310 nm to 400 nm, and a 3-nm excitation and emission slit setting. Lipid blanks were subtracted in all cases. Data were analyzed by monitoring changes in the fluorescence intensity (FI) at 335 nm, which is directly proportional to the population of molecular species present [28]. FI pH-titrations were then fitted to determine the pK_{FI} using: $Signal = (F_a + F_b 10^{m(pH-pK_{FI})}) / (1 + 10^{m(pH-pK_{FI})})$, where F_a is the acidic baseline, F_b is the basic baseline, m is the slope of the transition, and pK_{FI} is the FI midpoint of the curve, and signal is fluorescence changes.

Neutron Spin Echo (NSE) Spectroscopy. Suspensions of 100 nm diameter LUVs of DOPC:DOPS:Chol membranes were prepared in D₂O buffer at a concentration of 50 mg/mL. Bending and thickness fluctuation measurements were performed on protiated and perdeuterated (prepared with DOPC-d₆₆ and Chol-d₄₀) membranes, respectively. For optimal signal-to-noise, protiated and perdeuterated samples were loaded in quartz cells with path lengths of 2 mm and 4 mm, respectively. To access the different states of pHLIP, measurements were performed at two pH values, pH 8 for the surface-associated state and pH 4 for the TM state, adjusted using DCl or NaOD. Lyophilized pHLIP was weighed and added to samples at pH 8 at a lipid:peptide molar ratio of 150:1.

NSE experiments were conducted at the NIST Center for Neutron Research (NCNR) and at the Spallation Neutron Source (SNS) at Oak Ridge National Lab (ORNL). For experiments conducted on the NIST-NSE spectrometer, reduction and processing of the raw data were performed using the Data Analysis and Visualization Environment (DAVE) software [29]. The data processing yielded the normalized intermediate scattering function $S(q, t)/S(q, 0)$ as a function of Fourier time, t , for discrete q -values within the accessed q -range. For lipid membranes, the decay of the intermediate scattering function is fitted to a stretched exponential function with a stretching exponent of 2/3 such that:

$$\frac{S(q, t)}{S(q, 0)} = \exp \left[-(\Gamma(q) \cdot t)^{\frac{2}{3}} \right], \quad (1)$$

where $\Gamma(q)$ represents the decay rate at individual q -values (see Fig. S3A) and q is the wavevector transfer given by the neutron wavelength, λ , and scattering angle, θ , as: $q = 4\pi \sin(\theta)/\lambda$. Experiments carried out at the SNS-NSE spectrometer covered a q -range of 0.05 Å⁻¹ to 0.15 Å⁻¹ for both protiated and perdeuterated membranes (albeit with different λ and q configurations). The instrumental resolution and D₂O buffer were measured under the same sample configurations for proper

data reduction and normalization. Data reduction was performed using a Python script (developed at SNS) which generates the $S(q, t)/S(q, 0)$ data sets required for the characterization of membrane dynamics. Subsequent data fitting and analysis were performed following the same protocols described below.

Bending fluctuation measurements on protiated membranes were analyzed using the Zilman-Granek theory for bending relaxations [30] with refinements by Watson and Brown [31] and Nagao et al. [32]. Accordingly, membrane relaxation rates measured on protiated membranes were solely attributed to bending relaxations, expressed as:

$$\Gamma(q) = \Gamma_{\text{bend}}(q) = 0.0069 \frac{k_B T}{\eta_{D2O}} \sqrt{\frac{k_B T}{\kappa}} q^3, \quad (2)$$

where κ is the membrane bending modulus, k_B is the Boltzmann constant, T is the temperature, and η_{D2O} is the viscosity of the D₂O buffer. In this treatment, the location of the neutral surface is assumed to be at the hydrophobic-hydrophilic interface [32].

For NSE measurements performed using chain-perdeuterated membrane analogs (DOPC- d_{66} and Chol- d_{40}), those were characterized by excess dynamics in addition to the q^3 signal for bending fluctuations, as demonstrated in previous work [25,32–34]. These excess dynamics are well described by the second term in Eq. 3, such that the overall relaxation rate can be expressed as:

$$\Gamma(q) = \Gamma_{\text{bend}}(q) + \frac{q^3}{q_0^3} \frac{\Gamma_{TF}}{1 + (q - q_0)^2 \zeta^2}, \quad (3)$$

where Γ_{bend} is the decay rate of bending fluctuations obtained from protiated membrane analogues as defined in Eq. 2, Γ_{TF} is the relaxation rate of membrane thickness fluctuations, q_0 is the peak position of the Lorentzian at which thickness fluctuation dynamics are most pronounced, and $1/\zeta$ is the half width at half maximum (HWHM) determined by the thickness fluctuation amplitude, Δd_m , such that $\zeta \approx 2D_C/(q_0 \Delta d_m)$ where $2D_C$ is the bilayer hydrocarbon thickness.

Here we note that the fits of the thickness fluctuations signals yield two physical parameters, Δd_m and Γ_{TF} , corresponding to the average fluctuation amplitude and average fluctuation rate, respectively. Given the interplay of these physical parameters with membrane biophysical parameters, including the area compressibility modulus and the in-plane viscosity, a modified theoretical expression can be used to fit the thickness fluctuations signal, such that [32]:

$$\frac{\Gamma}{q^3} = \frac{\Gamma_{\text{bend}}}{q^3} + \frac{K_A k_B T}{\mu q_0^3 k_B T + 4\mu q_0 K_A A_L (q - q_0)^2}, \quad (4)$$

where K_A is the area compressibility modulus determined from bending rigidity measurements of protiated membranes, $k_B T$ is the thermal energy, A_L is the area per lipid obtained from small-angle neutron/X-ray scattering (SANS/SAXS) measurements, and μ is the membrane viscosity – which is the only fit parameter for the thickness fluctuations signal.

Coarse-Grained Molecular Dynamics (CG-MD) Simulations. The coarse-grained model used in this work is based on the solvent-free approach developed by Cooke et al [35], where each lipid molecule is represented by three beads connected by two FENE bonds, a “head” bead representing the lipid headgroup and two “tail” beads representing the lipid hydrocarbon region. The interactions between the beads are modeled by an attractive term for tail-tail interactions and a purely repulsive term of the Weeks-Chandler-Andersen (WCA) form for head-head and head-tail interactions as described in earlier work [25]. The width of the tail-tail potential well was set to $w_c = 1.6 \sigma$ (where σ is the diameter of a tail bead) to achieve a membrane bending rigidity of $23.4 k_B T$. The simulations were performed using an initial vesicle configuration consisting of $N = 18,996$ lipid molecules preassembled with an approximate radius of 30σ and an area per lipid of $\sim 1 \sigma^2$ for both the inner and outer leaflets. For lipid vesicles containing transmembrane peptides, 300 rods composed of 8 connected beads were included within

the membrane. The stiffness of the rods was maintained through an angle potential with a bending rigidity of $64 k_B T$, which results in an approximate rod persistence length of 62σ . The transmembrane configuration of the rods within the membrane was obtained by assigning repulsive interactions between the first and last beads of the rod and the tail beads of lipid molecules. The remaining rod-beads experienced attractive interactions with those of the lipid tails, similar to those of tail-tail lipid interactions. To avoid rod aggregation, a repulsive potential was assigned to all bead-bead interactions within the rod. Notably, the coarse-grained lipid model was demonstrated in previous studies to accurately capture NSE signals for membrane bending and thickness fluctuations [25]. In this work, we adapt the same model to illustrate the effect of pHLIP insertion on membrane thickness fluctuations.

Simulated NSE data were produced as follows: The static scattering function, $S(q)$, of simulated vesicles was calculated from the density – density correlation function by taking the discrete Fourier transform of the density distribution of all lipid beads, such that $S(q) = 1/N \langle \rho_{\vec{q}} \rho_{-\vec{q}} \rangle$. Membrane fluctuation signals were calculated from simulations as $S(q, t)/S(q, 0) = 1/N \langle \rho_{\vec{q}}(\Delta t) \rho_{-\vec{q}} \rangle$, which represents the time autocorrelation of the scattering function, $S(q)$, after an elapsed time Δt . This is analogous to the intermediate dynamic scattering function measured by NSE. Analysis of the temporal decays in $S(q, t)/S(q, 0)$, following the procedure developed in a previous work [25], yielded the relaxation rates of membrane thickness fluctuations.

Atomistic MD Simulations. All systems were prepared using the CHARMM-GUI web server [36]. Coordinates for pHLIP (GGEQNPIY-WARYADWLFTPLLLDLALLVDADEGT) were obtained from the X-ray crystal structure of bacteriorhodopsin (PDB 1FBB) using residues 72 to 107. The Q105E mutation was carried out to be consistent with the composition of pHLIP, and all acidic residues (E3, D14, D25, D31, D33, E34) were protonated. pHLIP was inserted as a transmembrane α -helix into a lipid membrane with the same compositions described above, i.e., DOPC:DOPS:Chol at 76:4:20 mol fraction. The simulations were set up with 50 waters per lipid and 100 mM NaCl, via the replacement method. All systems were equilibrated for 50 ns with a 2 fs timestep in NAMD 2.13 [37] in the NPT ensemble ($T = 310$ K and $P = 1$ atm), using the Langevin thermostat [38] and Nosé-Hoover barostat [39]. For equilibration, the charmm36 force field for lipids [40] and proteins [41] and the TIP3P model for water [42] were used, with standard cutoffs applied (10 Å switching and 12 Å cutoff) for non-bonded forces. For production runs, the coordinates of the last frame of the equilibration trajectory were converted to be consistent with AMBER force field topology (ff14SB [43], lipid17 [44], and OPC for water [45]). A small minimization and equilibration of 1 ns was performed, with a 2 fs timestep in the NPT ensemble ($T = 310$ K and $P = 1$ atm) using the Monte-carlo barostat with semi-anisotropic pressure coupling to preserve the aspect ratio of lateral plane of the bilayer and the Langevin thermostat. Minimization and equilibration were performed employing the sander MD engine in AMBER18 [46], with a cutoff for non-bonded forces of 8 Å. Production runs were carried out with the GPU-accelerated version of the Particle Mesh Ewald Molecular Dynamics (PMEMD) in AMBER18 using the same configurations as minimization and equilibration. Ten simulations per system were conducted with an aggregate time of 10 μ s each. Analysis was performed using a combination of VMD [47], CPPTRAJ in AmberTools [46], LOOS [48] and in-house scripts. Snapshots of trajectories were rendered in VMD, and plots were generated with gnuplot [49], respectively.

Small-Angle X-ray and Neutron Scattering (SAXS/SANS): D₂O suspensions of 100-nm diameter LUVs composed of DOPC, DOPS, and Chol (as well as their perdeuterated variants DOPC- d_{66} and Chol- d_{40}) were prepared at ~ 20 mg/mL. To access the two states of pHLIP, measurements were performed at two pH values, pH 8 for surface-associated pHLIP and pH 4 for TM pHLIP, obtained using either NaOD

or DCL, respectively.

Scattering data were analyzed following data analysis protocols outlined by Doktorova et al. [50]. Differently contrasted scattering data (i.e., SANS data for different deuterated lipid variants, and SAXS data) were jointly refined with a model that accounts for coherent scattering contributions from transverse scattering length density (SLD) variations within the bilayer. Transverse SLD profiles probed by SANS and SAXS determined the nuclear and electronic composition, respectively, of the lipid headgroup and hydrocarbon regions in the lipid bilayers. For protein-membrane complexes, the SLD profile is, in principle, influenced by the presence of surface-bound or inserted protein. However, due to the low mass fraction of protein used in these experiments ($< 1\%$), we neglected the protein contribution to the SLD profile. Thus, any detectable changes in the scattering curves are due to the effect of the protein on the lipid bilayer structure. The transverse SLD profiles were derived from the underlying lipid volume probability distributions within the bilayer, modeled as the sum of separate distributions for the lipid headgroups and hydrocarbon chains. The total unit cell volume was calculated as a mole-fraction weighted sum of lipid volumes obtained from literature (Table S1) and constrained in the fit, leaving as adjustable parameters the area per lipid A_L and headgroup thickness, D_H . Additional structural parameters, including the total bilayer thickness D_B and the hydrocarbon thickness, $2D_C$, were derived from relationships between the adjustable parameters and the lipid headgroup and hydrocarbon volumes. From the unit cell volume probability profile, neutron SLD and electron density (ED) profiles were then obtained as a sum of the separate headgroup and hydrocarbon volume probability distributions multiplied by their respective total scattering lengths (Table S1).

For each nominal sample composition (e.g., molar ratio of DOPC: DOPS:Chol is 76:4:20) SANS samples were prepared with two different contrasts using protiated and perdeuterated variants of DOPC (i.e., DOPC or DOPC- d_{66}) and Chol (i.e., Chol or Chol- d_{40} , Fig. S9). Joint analysis of all available SANS and SAXS data for a given sample composition and pH was implemented in Mathematica 11.0 (Wolfram Research, Champaign, IL). Uncertainties in structural parameters were obtained from a bootstrap method [51]. Briefly, a synthetic scattering data set consistent with experimental noise was generated as follows:

$$\begin{aligned} I_{\text{syn}}(q) &= I_{\text{fit}}(q) + X(q), \\ X(q) &\sim N[0, \sigma_{\text{exp}}(q)]. \end{aligned} \quad (5)$$

In the previous equations, I_{fit} is the best-fit intensity value and X , which represents noise, is a random variable drawn from a Gaussian distribution whose standard deviation corresponds to the experimentally determined uncertainty, σ_{exp} . Synthetic data sets for X-ray and neutron data were jointly analyzed as previously described. This process was repeated 100 times to generate populations of synthetic structural parameters; the uncertainties reported in Table S1 are the standard deviations of these populations.

Complementary SANS data analysis was performed using the core-multi-shell model in the SasView software, specifically a three-shell vesicle model (head-tail-head) [52]. The model assumes a Gaussian distribution of the vesicle radius (fitted over the low- q range of the data) but does not consider gradients in the interfaces between the headgroup and hydrocarbon layers (due to the Gaussian distribution of different lipid subgroups). The results of this analysis are presented in Table S1 and are compared to the more refined approach described above.

3. Results

Previous biophysical studies on pHLIP have largely focused on understanding how the membrane influences pHLIP cancer treatment efficacy [53–55]. As previously demonstrated, pHLIP adsorbs to the membrane surface at neutral pH but inserts into the membrane under acidic conditions [21]. Here, we studied the effect of pHLIP on membrane dynamics and structure. Measurements were performed at room

temperature (25 °C) on lipid vesicles composed of a 76:4:20 mixture of 1,2-dioleoyl-*sn*-3 glycerol-3-phosphocholine (DOPC), 1,2-dioleoyl-*sn*-glycerol-3-phosphoserine (DOPS), and cholesterol (Chol) [56] at a lipid: peptide (L:P) molar ratio of 150:1. The anionic lipid DOPS was used to ensure vesicle unilamellarity [57,58], as shown in Fig. S1. This choice of membrane composition was motivated by earlier studies reporting optimal pHLIP insertion in DOPC membranes with 20 mol% Chol [59], indicating minimal hydrophobic thickness mismatch between TM pHLIP and the membrane.

Using circular dichroism measurements, we showed that at pH 8 pHLIP adsorbs to the vesicle surface in a largely unstructured conformation (Fig. S2) [60], but it inserts into the membrane when the pH is dropped to pH 4 where pHLIP transforms in to a TM helix [23,61]. The membrane insertion of pHLIP is characterized by its pK , which depends on lipid composition [61–63]. For instance, the presence of the negatively charged lipid phosphatidylserine (PS) decreases the membrane insertion pK [62,61] as does the presence of cholesterol [59]. Here, we observed that the inclusion of both PS and Chol in PC membranes decreases pHLIP's pK to its lowest value yet observed for the peptide, i.e., $pK = 4.90 \pm 0.08$ (Fig. S2), suggesting that the membrane's chemical properties have an additive effect on the pK of insertion.

Here, we specifically inspect how changes in pHLIP conformations affect membrane bending and thickness fluctuations. Bending fluctuations are controlled by the mechanical properties of the membrane, typically described by the bending rigidity modulus, and have been studied extensively both experimentally and theoretically [64,65]. On the other hand, fluctuations around the average membrane thickness have been less explored despite being linked to several vital membrane phenomena, including ion channel gating and hydrophobic mismatch [66,67]. Unlike other spectroscopy methods, NSE can simultaneously access the length (a few nm) and timescales (~ 100 ns) over which membrane thickness fluctuations occur [66,68,69]. Fig. S3A shows typical NSE intermediate scattering functions, $S(q, t)/S(q, 0)$, as described above. Fits of the intermediate scattering functions using the elastic-sheet fluctuation model $S(q, t)/S(q, 0) = \exp[-(\Gamma(q)t)^{2/3}]$, yielded the relaxation rates, $\Gamma(q)$, of bending and/or thickness fluctuations at different q -values (or inverse length scales) [30]. Plots of $\Gamma(q)$ for protiated vesicles in deuterated buffer showed the typical q^3 -dependence (Fig. S3B, blue data points) of membrane bending fluctuations [30]. Fitting the data to the model described in Eq. 2 yielded the membrane bending modulus, κ . We observed that pHLIP did not cause substantial changes to κ , neither in its SA (pH 8) nor TM (pH 4) states, as all κ values were within experimental error (Table 1 and Fig. S4).

In contrast to results from protiated membranes, NSE measurements of chain-perdeuterated membrane analogs (i.e., DOPC- d_{66} and Chol- d_{40}) showed a clear deviation from the q^3 dependence in the relaxation rates at $q \sim 0.08 \text{ \AA}^{-1}$, a value which corresponds to the membrane thickness (Fig. S3B). The observed excess dynamics are associated with membrane thickness fluctuations [32–34] and were analyzed using Eq. 3 (Fig. S3, red data points). Analysis of these signals (Fig. 1) yielded key physical descriptors of membrane thickness fluctuations, namely the fluctuation rate, Γ_{TF} , and the fluctuation amplitude, Δd_m (Fig. 1A and Table 1). The results revealed that TM-pHLIP induced a four-fold decrease in Γ_{TF} , but SA-pHLIP had little impact on Γ_{TF} . Control experiments of lipid-only samples showed that variations in pH had no effect on either κ [70] or membrane thickness fluctuations (Fig. S5 and Table 1). Interestingly, no changes to Δd_m were observed in either conformation of pHLIP (Fig. S6 and Table 1). The data, therefore, imply that the suppression of thickness fluctuations due to TM-pHLIP is the result of a slowdown in the thickness fluctuation rate, and not the result of a decrease in the thickness fluctuation amplitude.

Conclusions from our NSE studies were supported by coarse-grained molecular dynamics (CG-MD) simulations of membrane fluctuations. CG-MD were performed on large unilamellar lipid vesicles with and without transmembrane peptide-like inclusions resembling TM-pHLIP

Table 1Dynamic membrane parameters obtained from the analysis of NSE and all-atom MD simulations. Error bars represent ± 1 standard deviation.

pH	pHLIP	Bending Fluctuations		Thickness Fluctuations			Diff. const.
		κ ^[a] (k _B T)	K_A ^[b] (N/m)	Γ_{TF} ^[c] (10^{-3} ns ⁻¹)	Δd_m ^[d] (Å)	μ ^[e] (nPa.s.m)	
8	–	30.3 $\pm$ 2.5	0.26 $\pm$ 0.02	7.3 $\pm$ 0.9	3.5 $\pm$ 0.6	31.9 $\pm$ 3.5	1.28 $\pm$ 0.72
4	–	29.2 $\pm$ 1.3	0.26 $\pm$ 0.02	7.3 $\pm$ 1.7	3.4 $\pm$ 0.8	32.0 $\pm$ 4.1	
8	+	26.9 $\pm$ 1.8	0.23 $\pm$ 0.02	6.5 $\pm$ 2.3	3.4 $\pm$ 1.0	30.5 $\pm$ 3.5	
4	+	32.9 $\pm$ 2.7	0.28 $\pm$ 0.03	1.7 $\pm$ 0.6	3.8 $\pm$ 1.5	105.9 $\pm$ 54.8	0.59 $\pm$ 0.06

NSE parameters: ^[a] bending rigidity modulus obtained from measurements on protiated membranes with the bending rigidity modulus as the only fit parameter (see Eq. 2); ^[b] area compressibility modulus calculated by the polymer-brush model, $K_A = 24\kappa/(2D_C)^2$ using the experimentally measured κ values; ^[c] relaxation rate of membrane thickness fluctuations obtained on chain-perdeuterated membranes following Eq. 3; ^[d] amplitude of membrane thickness fluctuations, calculated as $\Delta d_m \approx 2D_C/\zeta q_0$, using the mechanical thickness, $2D_C$, as well as q_0 and ζ corresponding to the peak-position and width of the Lorentzian distribution describing the excess dynamics due to thickness fluctuations (see the NSE section for more details); and ^[e] membrane viscosity obtained from analysis of the membrane thickness fluctuations using Eq. 4. ^[f] Diffusion constant calculated from mean-square displacements in all-atom MD simulations.

(Fig. S7). As seen in Fig. 1B, the simulated vesicle with TM peptides of the same hydrophobic thickness as the membrane showed a noticeable suppression in the membrane thickness fluctuation signal, relative to the lipid-only vesicle. Analysis of the simulation results (Fig. 1B and Table S2) corroborated the conclusions from NSE experiments, indicating that the presence of a transmembrane helix decreases the rate of membrane thickness fluctuations but not the fluctuation amplitude.

To relate membrane thickness fluctuations to other biophysical membrane properties, we used the polymer-brush model that we modified according to previous studies [56,71]. This analysis describes the area compressibility modulus as $K_A = \zeta\kappa/(2D_C)^2$ [72], where ζ is a constant that defines the degree of coupling between the two bilayer leaflets [73] (herein set to $\zeta = 24$) and $2D_C$ is the mechanical thickness of the membrane. In the q -range where thickness fluctuations dominate, the relaxation rates are dictated by the membrane viscosity, μ , such that $\Gamma_{TF} \approx K_A/\mu$ [74–76]. Put together, this yields a modified expression (Eq. 3) that enables direct determination of μ (see Eq. 4). Based on this, the minimal changes in the measured bending rigidities (Fig. S4) indicate that neither SA- nor TM-pHLIP alter K_A (Table 1 and Fig. S8). Further, the constant thickness fluctuation rate, Γ_{TF} , obtained with SA-pHLIP indicates that the surface association of the peptide does not affect μ , in striking contrast to TM-pHLIP which caused a large increase in μ (Fig. 1C and Table 1).

To understand the molecular mechanism by which TM-pHLIP modulates membrane thickness fluctuations and viscosity, we used all-atom MD simulations. We first determined the effect of pHLIP on lipid dynamics, as measured by the mean square displacement (MSD) of the DOPC headgroups and then used the MSD data to calculate the lipid diffusion constant. Doing this, we observed that TM-pHLIP strongly decreased lipid mobility (Fig. 2 and Table 1), as it is expected for a more viscous membrane. MSD analysis included both in-plane lipid diffusion and lipid movement along the membrane normal. The average MSD in the direction normal to the membrane plane had similar values in the absence ($20.3 \times 10^3 \text{ Å}^2/\text{ps}$) and presence ($20.8 \times 10^3 \text{ Å}^2/\text{ps}$) of TM-pHLIP. This observation indicates that the effect of pHLIP insertion on lipid mobility is limited to in-plane motions and supports the NSE and CG-MD results, implying that pHLIP does not alter the amplitude of membrane thickness fluctuations (Table S2).

These observations were further validated by SAXS/SANS measurements on membranes with SA- and TM-pHLIP. With SANS, we used deuterium labeling to maximize the neutron contrast between the protiated lipid headgroups and deuterated acyl chains of the membrane [77]. Joint analysis of the SANS and SAXS data [78–80] resulted in membrane structure, including membrane thickness, D_B , and area per lipid, A_L . Our results indicate that the addition of pHLIP does not alter D_B , A_L , or the average membrane hydrophobic thickness (Table S1, Fig. S9–12), in agreement with measurements made by all-atom MD

simulations (Fig. S13). These observations are also in agreement with a previous pHLIP study using 1-palmitoyl-2-oleoyl-*sn*-glycero-3-phosphocholine (POPC) membranes [81] in which neither pHLIP adsorption nor insertion were found to alter membrane structure, even at elevated peptide concentrations. Based on recently measured scaling relationships [82], the negligible effect of pHLIP on A_L supports the NSE conclusion that K_A is not affected by the different states of pHLIP (Table 1), further adding to the evidence that the decrease in the rate of thickness fluctuations ($\Gamma_{TF} \approx K_A/\mu$) induced by TM-pHLIP is due to increased membrane viscosity.

In fluid membranes, acyl chain dynamics allow for the interaction between the lipid's acyl chain terminal methyl group (CH_3) and the polar headgroups – a phenomenon that has been referred to as lipid snorkeling [83,84]. We hypothesize that if TM-pHLIP indeed promoted lipid tails to experience dynamic excursions into the headgroup region, this would lead to increased molecular friction within the bilayer, causing an increase in membrane viscosity and an observable slowdown of thickness fluctuations. To investigate acyl chain dynamics, we measured the distance between the C_α of the lipid headgroup and the terminal CH_3 group from atomistic MD simulations in the presence of TM-pHLIP (Fig. 3). In the absence of pHLIP, we observed that, as expected, most CH_3 groups were located at the bilayer midplane, approximately 21 Å from the headgroup (Fig. 3A, black line) [83]. However, in the presence of TM-pHLIP, the distance distribution changed, and new features appeared at shorter distances, indicating that acyl chains close to pHLIP explored the headgroup region more frequently. For the lipid molecules found within a 15 Å radius of pHLIP, we observed two discrete acyl chains populations with CH_3 - C_α distances of ~ 11 Å and ~ 15 Å, and a reduction of extended acyl chains (~ 21 Å) (Fig. 3A top, inset). These results suggest that in pHLIP's vicinity, lipid acyl chains snorkel with increased frequency (Fig. 3C). However, for lipids 15–25 Å away from pHLIP, their CH_3 - C_α distance is similar to the peptide-free membranes. This result indicates pHLIP's influence on lipid dynamic excursions is limited to lipids in its vicinity (2–3 lipid shells around TM-pHLIP).

4. Discussion

Experiment and simulation indicated that TM-pHLIP suppressed the rate of membrane thickness fluctuations, Γ_{TF} (Fig. 1 A-B), in membranes with no hydrophobic mismatch and resulted in an “effective” increase in membrane viscosity, μ . On the other hand, SA-pHLIP did not affect either Γ_{TF} or μ (Fig. 1 and Table 1), indicating that changes to these two parameters are specific to the interaction of TM-pHLIP with the lipid acyl chains. It is important to point out that although the increase in μ is fully supported by our analysis of the NSE data, its magnitude requires further assessment. Specifically, our analysis of thickness fluctuations

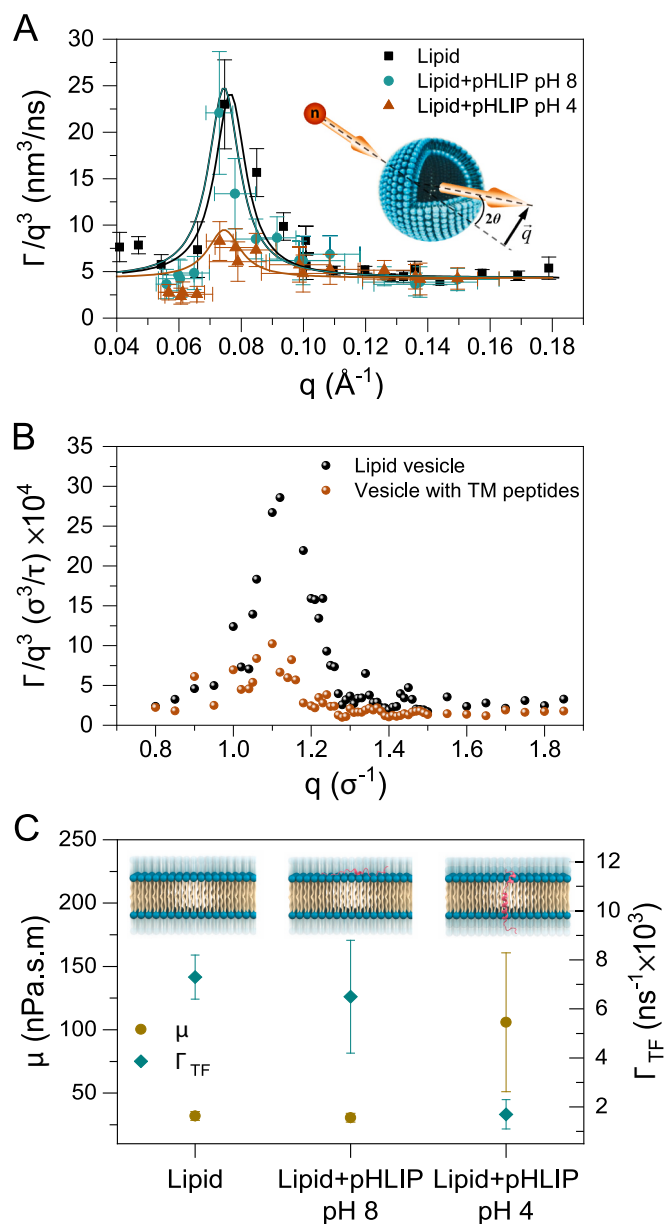


Fig. 1. (A) NSE data showing the normalized relaxation rate, Γ/q^3 , as a function of q for tail perdeuterated membranes. Data are shown in the absence (black) and presence of pHILP in its SA (cyan, pH 8) and TM (brown, pH 4) states. Lines are fits to the data using Eq. 3. Inset shows a schematic where lipid vesicles scatter neutrons with a scattering angle 2θ and wavevector transfer $\vec{q}$. (B) CG-MD simulation of membrane fluctuation signals as detected by NSE, for vesicles without (black) and with (brown) TM peptide incorporated. (C) The rates of thickness fluctuations show remarkable suppression in the presence of TM pHILP and no changes with SA pHILP. Membrane viscosity changes exhibit a similar trend, as only TM pHILP increases viscosity. Error bars represent ± 1 S.D. Experiments were performed at a 150:1 lipid to peptide molar ratio.

assumed that the two bilayer leaflets are coupled according to the polymer-brush model and that the transition of pHILP to its TM state does not change the interleaflet coupling. In the polymer brush model, the two bilayer leaflets are loosely coupled with a coupling constant $\zeta = 24$ that is proportional to the coupling strength between the leaflets. However, variations in the coupling constant have been previously observed [85,86]. If we consider this possibility and assume an extreme coupling scenario in which TM-pHILP causes the two leaflets to be fully coupled (i.e., $\zeta = 12$), this would still result in a two-fold increase in

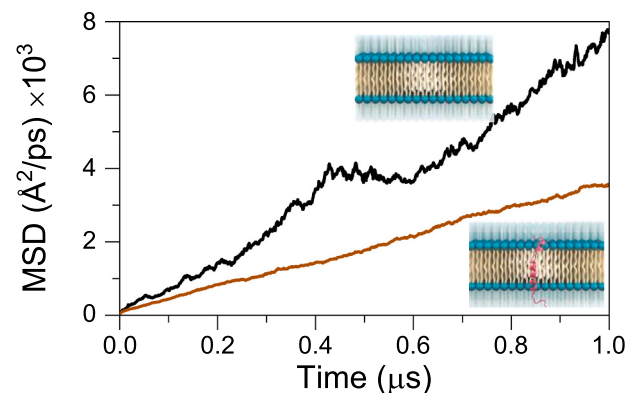


Fig. 2. Atomistic MD simulations show a decrease in the mean-squared displacement (MSD) of the lipid headgroups in the presence of TM-pHILP (brown) compared to lipid-only membranes (black).

membrane viscosity relative to pHILP-free membranes. Assuming that the membrane viscosity and diffusion constant are inversely proportional, this would suggest that TM-pHILP causes an approximate 2-fold decrease in the diffusion constant, in close agreement with the MSD results from all-atom MD simulations. Although one would expect an intermediate value for the bilayer leaflet coupling constant, a more accurate estimate of this parameter would require additional experimental studies that are beyond the scope of this work.

A feature of fluid bilayers that is often overlooked is the fact that their acyl chain terminal methyl groups snorkel to the membrane surface and interact with the lipid headgroups. For example, 2D NMR studies of different composition lipid bilayers have shown that the terminal methyl groups of lipid fatty acid chains interact with the choline headgroups [83]. This effect was also observed in our atomistic MD simulations, which show a smooth distribution of CH₃-C_α distances with a long tail at low values (black line, Fig. 3A). In comparison, simulations with TM-pHILP showed a shift in the distribution to smaller distances indicating longer residence times of the CH₃ groups near the lipid headgroups (see supplementary Video). More importantly, our probability distribution contained peaks at ~ 11 Å and ~ 15 Å, indicating a statistical increase in the number of acyl chains that explore the lipid headgroup region (brown line, Fig. 3A top). The acyl chain snorkeling of lipids may facilitate the intermolecular proximity between the tail methyl groups and choline headgroups. This result indicates that for lipids in the vicinity of pHILP, their terminal methyl groups snorkel to the lipid-water interface at an increased frequency. As a result, this would increase the free space available to nearby lipids, allowing their chains to explore a larger conformational space. Based on these findings, we propose that the increased frequency in acyl chain snorkeling results in higher in-plane friction due to increased acyl chain entanglement, in a way that is analogous to irregularly-shaped epithelial cells exhibiting reduced 2D mobility [87]. Additionally, lipid tails from the opposite monolayer can fill the space left by a snorkeled tail, increasing inter-leaflet coupling [88,89]. Any combination of these two effects would cause an apparent increase in membrane viscosity, which can result in a dampening of the thickness fluctuation rate.

Supporting Information is provided for supplementary results, details of data analysis, and additional figures. Supplementary data to this article can be found online at doi:<https://doi.org/10.1016/j.bbamem.2024.184349>.

CRediT authorship contribution statement

Haden L. Scott: Writing – review & editing, Writing – original draft, Investigation, Formal analysis. **Violeta Burns-Casamayor:** Investigation, Formal analysis. **Andrew C. Dixon:** Investigation. **Robert F. Standaert:** Investigation. **Christopher B. Stanley:** Investigation.

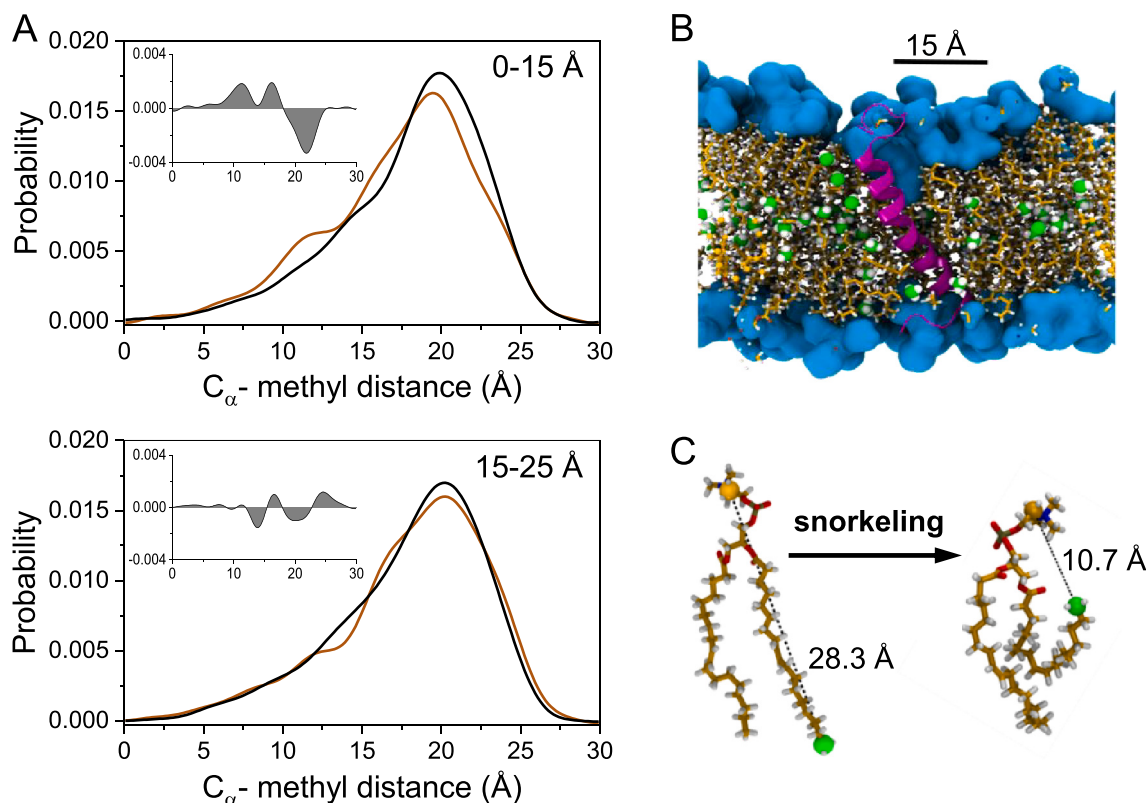


Fig. 3. (A) Probability distribution of the distance between the CH₃ groups of DOPC oleoyl chains and the plane formed by the C_α of the choline headgroups. Black lines show data from neat bilayers, and brown lines consider only lipids within 15 Å of pHLIP (top), or between 15 and 25 Å from the helix (bottom). Insets show the subtraction between the probability distributions with and without pHLIP. (B) Representative snapshots of a DOPC:DOPS:Chol bilayer containing TM pHLIP. Phospholipid headgroups are shown in blue, and tails in yellow. CH₃ groups are shown as green spheres. Cholesterol molecules are shown in a ball and stick representation. (C) A representative DOPC molecule with fully extended acyl chains can snorkel reducing the distance to the choline headgroup in the presence of TM-pHLIP. C_α (yellow) and CH₃ (green) are shown as spheres and are used for distance measurements.

Laura-Roxana Stingaciu: Methodology, Investigation, Formal analysis, Data curation. **Jan-Michael Y. Carrillo:** Writing – original draft, Validation, Investigation, Formal analysis. **Bobby G. Sumpter:** Investigation. **John Katsaras:** Writing – review & editing, Writing – original draft, Investigation, Conceptualization. **Wei Qiang:** Investigation. **Frederick A. Heberle:** Writing – review & editing, Writing – original draft, Supervision, Investigation, Formal analysis, Conceptualization. **Blake Mertz:** Writing – review & editing, Writing – original draft, Supervision, Methodology, Investigation, Formal analysis. **Rana Ashkar:** Writing – review & editing, Writing – original draft, Visualization, Validation, Supervision, Resources, Project administration, Funding acquisition, Formal analysis, Conceptualization. **Francisco N. Barrera:** Writing – review & editing, Writing – original draft, Supervision, Project administration, Methodology, Investigation, Funding acquisition, Conceptualization.

Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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