# Classification of Emerging Neural Activity from Planning to Grasp Execution using a Novel EEG-Based BCI Platform

## 1st Anna Cetera

Dept. of Electrical, Computer and Biomedical Engineering
University of Rhode Island
Kingston, RI, USA
annacetera@uri.edu

# 3<sup>nd</sup> Sima Ghafoori

Dept. of Electrical, Computer and Biomedical Engineering
University of Rhode Island
Kingston, RI, USA
sima.ghafoori@uri.edu

### 5<sup>th</sup> Reza Abiri

Dept. of Electrical, Computer and Biomedical Engineering
University of Rhode Island
Kingston, RI, USA
reza\_abiri@uri.edu
member, IEEE

Abstract—There have been different reports of developing Brain-Computer Interface (BCI) platforms to investigate the noninvasive electroencephalography (EEG) signals associated with plan-to-grasp tasks in humans. However, these reports were unable to clearly show evidence of emerging neural activity from the planning (observation) phase - dominated by the vision cortices - to grasp execution - dominated by the motor cortices. In this study, we developed a novel visionbased-grasping BCI platform that distinguishes different grip types (power and precision) through the phases of plan-to-grasp tasks using EEG signals. Using our platform and extracting features from Filter Bank Common Spatial Patterns (FBCSP), we show that frequency-band specific EEG contains discriminative spatial patterns present in both the observation and movement phases. Support Vector Machine (SVM) classification (power vs precision) yielded high accuracy percentages of 74% and 68% for the observation and movement phases in the alpha band, respectively.

Index Terms—brain-computer interface (BCI), reach-to-grasp tasks, vision control, object isolation, filter bank common spatial pattern, grip type classification, alpha Frequency band, support vector machine.

This project was supported by the Rhode Island INBRE program from the National Institute of General Medical Sciences of the National Institutes of Health under grant number P20GM103430 and National Science Foundation under award ID 2245558. This research was also supported by URI foundation grant on Medical Research. Author 5 is the corresponding author.

## 2<sup>rd</sup> Ali Rabiee

Dept. of Electrical, Computer and Biomedical Engineering
University of Rhode Island
Kingston, RI, USA
ali.rabiee@uri.edu

# 4th Yalda Shahriari

Dept. of Electrical, Computer and Biomedical Engineering
University of Rhode Island
Kingston, RI, USA
yalda\_shahriari@uri.edu
member, IEEE

#### I. Introduction

The ability to independently navigate and interact with the surrounding environment through reaching and grasping is fundamental to an individual's autonomy and quality of life. Neural correlates associated with natural reach-and-grasp actions can be decoded and identified through invasive brain recording methods [1], offering insights into the emergence of neural activity before and during movement onset.

While current invasive-based BCI systems have been explored for assisting individuals with grasp disabilities, existing control methods often lack a natural and intuitive feeling of control [2], [3]. Common laboratory experimental set-ups attempt to employ a naturalistic reach-to-grasp set-up by presenting multiple objects to the participant simultaneously [4], [5]. In these setups, the lack of object isolation may introduce bias to the data, creating difficulties in understanding the relationship between the visual and motor cortices associated with individual objects and their specific grip types.

To eliminate the possibility of data bias, we employed a novel EEG vision-based-grasping platform that distinguishes the neural activity between the observation (planning) phase and movement (grasp execution) phase through vision control and object isolation. Gaining control over the timing at which the participants observe the object presented before them enables us to analyze the emergence of neural activity across

different phases of plan-to-grasp tasks. Meanwhile, isolating the object presented before them allows for the exploration of distinct neural patterns associated with the object and its specific grip type (power vs precision).

In this study, we aim to achieve two primary goals. Firstly, to obtain results that are consistent with the frequency-band-specific neural spatial patterns reported in invasive studies to validate our platform, particularly within the alpha band due to its strong association with motor planning [6]–[8]. Secondly, to introduce the possibility of additional frequency-band-specific features that may be involved with motor planning during the observation phase without explicit motor imagery instructions [9], [10]. By implementing FBCSP, we examine the frequency-specific-spatial patterns during plan-to-grasp tasks and perform feature extraction to classify between grasp types using SVM during the observation and movement phases within specific frequency ranges.

Investigating the emerging neural activity from the planning (observation) phase - dominated by the vision cortices - to grasp execution - dominated by the motor cortices within specific frequency bands may offer new insight for a naturalistic control strategy for noninvasive BCI systems and improve the quality of life for those with impaired hand dexterity.

#### II. MATERIALS AND METHODS

#### A. Data Collection Platform

In this study, two distinct objects were selected to execute two specific reach-to-grasp actions most used in daily life: the precision and power grasp types. The objects were (i) a pen for precision grasp execution and (ii) a water bottle for power grasp execution (Figure 2b). The object was presented to the participant on a sectioned, motorized turntable while wearing a pair of developed "smart glasses" capable of alternating states of transparency (Figure 1a). To eliminate the possibility of data bias, no object was presented between object A and object B, the selection of the objects was randomized, and the smart glasses transitioned from a transparent to an opaque state during the rotation of the turntable.

## Hardware

The presentation of object A, object B, and no object required a novel, PC-controlled, motorized turntable divided into 3 sections. Each object was individually placed in one of the three sections (Figure 1b). Two Arduino Uno microcontrollers were programmed to control the motor driver (TB6600 4A 9-42V Stepper motor driver), the motor (Bipolar 1.7A Nema 17 Stepper Motor), the audio cue, and the smart glasses. The smart glasses enabled/disabled object visibility due to the transparent/opaque states of PDLC electronic smart film.

#### *Software*

The developed software ensured synchrony between EEG data acquisition and the hardware components for accurate event logging. PySerial was utilized to send numerical commands from Python to Arduino IDE to control audio cue

timings and state changes of the motorized turntable/smart glasses. A simple, real-time graphical user interface (tkinter) was developed to run in synchrony with the platform at the time of data collection for the researcher (Figure 1c).

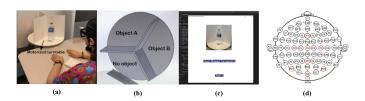


Fig. 1. Experimental setup and EEG electrode placement. (a) Participant wearing an EEG headset and "smart glasses" seated facing the motorized turntable with an object to perform a reach-to-grasp task. (b) 3D-designed motorized turntable with object A, object B, and no object sections. (c) Synchronized graphical user interface during data collection. (d) Standard EEG 10-20 system electrode placement with highlighted electrodes (red) used for analysis.

#### B. Data Collection

#### **Participants**

Data was collected from five human subjects (3 female, 2 male) aged between 20 and 35. Each participant was right-hand dominant with no known motor deficits or neurological impairments. Each participant attended a single data collection session (approximately 75 minutes).

#### Data Acquisition

EEG signals were acquired using the 8-channel Unicorn Hybrid Black headset with wet electrode setup (manufactured by g.tec) at a sampling rate of 250 Hz. Electrodes were placed in the following positions according to the international 10/20 system: Fz, C3, Cz, C4, Pz, PO7, Oz, PO8 (Figure 1d). Reference and ground electrodes were placed on the left and right mastoid respectively. Quality testing of EEG signals was performed before each data recording session within the Unicorn Suite Hybrid Black software environment (g.tec).

#### Protocol Design

In our study, the participant was instructed to perform a reach-to-grasp task with enabled vision capabilities and motor movement execution. The participant was positioned 30 cm from the center of the object with their palms facing downwards. The structure of the data collection protocol is centered on an audio-cue-based paradigm, where each data recording session included 5 blocks, each containing 10 trials, resulting in a total of 50 trials for each object presented (Figure 2).

Before the audio cue, the participant was instructed to observe the object for two seconds. Following the audio cue, the participant performed a naturalistic reach-to-grasp task toward the object presented by the motorized turntable for four seconds. If no object was presented, the participant was instructed to execute no movement.

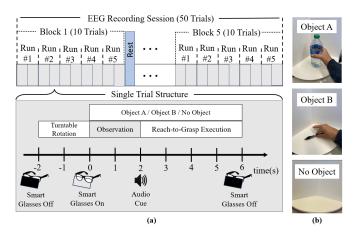


Fig. 2. Structure of data collection session and singular EEG trials. (a) One collection session for each subject involves multiple blocks, rest periods, and the sequence of events within a single trial including the periods of turntable rotation, object observation, reach-to-grasp execution, and auditory cues. (b) Presented objects on the motorized turntable during the experiment: object A (a water bottle), object B (a pen), and the 'no object' condition.

#### C. Data Processing and Feature Extraction

The acquired EEG data was initially filtered with a 60 Hz notch filter to suppress power line noise. To eliminate low-frequency drift, a zero-phase, 4th-order Butterworth bandpass filter with cutoff frequencies of 0.5 and 40 Hz was applied. To implement the Filter Bank Common Spatial Pattern algorithm, subject-specific and object-specific single trial EEG were decomposed into the following filter banks: (delta: 0-4Hz, theta: 4-8Hz, alpha: 8-13Hz, beta: 13-30Hz, gamma: 30-40Hz), using zero-phase 4th-order Butterworth bandpass filters.

Two windows of interest were extracted for binary classification: two seconds before the audio cue (observation phase) and two seconds after the audio cue (movement phase). The CSP projection matrices were calculated for each object across different filter banks using the epochs of the filtered data, which were then applied to spatially filter the raw, single-trial EEG data. The feature set included the normalized log variances of the most and least discriminative spatial components that capture the maximum and minimum variances across trials for each class. In each filtered trial, four CSP features were derived and utilized for binary classification.

## D. Classification

The FBCSP features were utilized for binary classification to distinguish between the power grasp and precision grasp during the observation and movement phase within different frequency bands. The Support Vector Machine (SVM) algorithm was used to perform binary classification. Table I displays subject-based binary classification results (percent accuracy) within each frequency band during both the observation and movement phases of the experiment.

#### III. RESULTS

#### A. Common Spatial Pattern

The extracted alpha band CSPs during both the observation and movement phases are shown in Figure 3. During the observation phase, CSP #1 displays an increase of brain activation within the temporal and occipital regions of the brain (indicated by red) while being surrounded by lower alpha activity (indicated by blue) in the frontal regions of the brain. CSP #2 features lateralized activity as lower and higher alpha band activity is localized over the left and right hemisphere regions respectively. Both CSP #3 and CSP #4 display reduced alpha activity in the occipital region, while CSP #1 and CSP #2 display increased alpha activity in the same location.

The first common spatial pattern during the movement phase (CSP #1) exhibits localized alpha activity in the central region of the brain. CSP #3 and CSP #4 display an increase of alpha activity in the occipital region, however, opposite alpha activities occur across the motor cortex region between the two patterns.

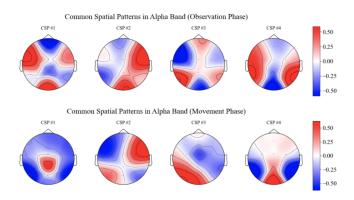


Fig. 3. Topographical plots of extracted common spatial patterns (CSPs) in the alpha band during different task phases for subject 3. The upper panel illustrates CSPs #1 to #4 during the observation phase. The lower panel displays the corresponding CSPs during the movement phase. Each map is scaled from -0.50 to +0.50, reflecting changes in amplitude within the alpha

#### B. Classification

The classification results in Table I display that analysis of the mean percent accuracy scores for binary classification between power grasp and precision grasp during both the observation and movement phases yields insightful trends, particularly in the alpha, delta, and gamma frequency bands. Across all subjects, the features within the alpha band contributed to the highest mean accuracy 74% in the observation phase and 67% in the movement phase. Furthermore, mean percent accuracy scores in the delta and gamma bands increase during the observation phase compared to the movement phase, with delta band accuracy rising from 55% to 68% and gamma from 63% to 65%.

The box-and-whisker plots in Figure 4 depict the distribution of SVM classification accuracy across different EEG filter bank frequency bands during the observation and movement

TABLE I
SUBJECT-BASED GRIP TYPE CLASSIFICATION DURING OBSERVATION AND MOVEMENT PHASE

	Observation Phase (%)					Movement Phase (%)				
Subjects	Delta	Theta	Alpha	Beta	Gamma	Delta	Theta	Alpha	Beta	Gamma
s1	45	55	80	50	60	45	50	65	45	70
s2	75	60	70	60	50	65	40	60	50	45
s3	80	65	70	75	65	60	65	80	80	75
s4	80	60	85	60	70	65	75	75	65	60
s5	60	65	65	75	55	40	65	55	55	65
Mean	68	61	74	64	65	55	59	67	59	63

phases. Upon observation, there is an increase in overall percent accuracy across all subjects during the observation phase (excluding the gamma band), contributing to the distinction in brain activity between the two phases. The alpha band exhibits the highest median accuracy during both phases compared to all other frequency bands, suggesting that features derived from the alpha band are the most discriminative for classifying grip types. The median accuracy in the alpha band surpass those in the delta, theta, beta, and gamma bands, which indicates it as a consistent feature with less variability in the classification performance in distinguishing between the power and precision grasps across different trials or subjects.

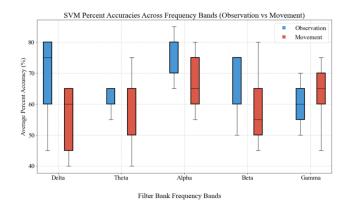


Fig. 4. Box-and-whisker plots illustrating the distribution of SVM classification accuracies across five frequency bands during the observation and movement phases. Blue boxes represent accuracies during the observation phase, while red boxes correspond to the movement phase.

#### IV. DISCUSSION

Our novel platform enables the separation of phases during plan-to-grasp tasks and object isolation, allowing us to observe distinct trends in neural activity during the observation and movement phases of reach-to-grasp tasks respective to the specific object presented. The derived CSP topographies, specifically in the alpha band during the observation phase, could have significant implications for understanding motor planning. Alpha activity is known to be associated with

motor planning [7], and the trends observed in our study are consistent with this connection since the the decreased activation patterns during the observation phase are evident in our results. The decrease in activation patterns in the occipital regions (responsible for processing visual stimuli) of the brain is specifically observed in the alpha activity levels within the third and fourth CSPs topographical plots. This desynchronization pattern in neural activation may indicate that prior to movement onset, the occipital region is engaged in interpreting and responding to the object presented in front of them, which is crucial for precise motor planning and execution in reach-to-grasp tasks.

The SVM classification accuracies derived from the FBCSP features, specifically within the alpha band, demonstrated the highest percent accuracy across all subjects during the observation phase. These results are consistent with previous literature findings in that this particular frequency band plays a pivotal role in discriminating between the two grasps types. These results validate our novel platform, while also introducing the possibility of exploring delta and gamma frequency bands that may be involved in motor planning without explicit motor imagery instructions due to their high percent accuracy scores. Although these percent accuracy scores are less significant than those observed in the alpha band, they could be indicative of the delta band's association with integrative sensory processing and the gamma band's link to higher-level cognitive functions. The increased accuracy in these bands during the movement phase may reflect the increased demand for sensorimotor integration and the heightened cognitive engagement required for executing the motor task.

#### V. Conclusion

The ability to control vision and separate the observation phase from the movement phase during reach-to-grasp tasks with our novel platform enabled us to uncover neural mechanisms and activity associated with object-specific visually guided tasks using noninvasive EEG. Isolating the object presented introduced the possibility of novel findings regarding how delta and gamma frequency activity might play a role in motor planning for grasp classification. Without explicit

motor imagery instructions, we were able to detect significant neural activation patterns during the observation phase within the occipital and motor regions of the brain.

The outcomes gained from performing FBCSP/SVM on the EEG data collected from our novel platform for grip type classification open the possibility of exploration of frequency band-specific neural activity that is solely associated with the singular object presented to the participant. This platform facilitates the investigation for understanding the interplay between different brain regions at various frequency bands during motor planning and execution, particularly in the context of complex tasks like power and precision grasps. This novel vision-based-grasping platform presents a new direction for non-invasive BCI systems by exploring the emergence of neural activity during motor planning and visually guided tasks.

#### REFERENCES

- [1] C. E. Vargas-Irwin, L. Franquemont, M. J. Black, and J. P. Donoghue, "Linking objects to actions: Encoding of target object and grasping strategy in primate ventral premotor cortex," *The Journal of Neuroscience*, vol. 35, no. 30, pp. 10888–10897, 2015.
- [2] A. B. Ajiboye, F. R. Willett, D. R. Young, W. D. Memberg, B. A. Murphy, J. P. Miller, B. L. Walter, J. A. Sweet, H. A. Hoyen, M. W. Keith *et al.*, "Restoration of reaching and grasping movements through brain-controlled muscle stimulation in a person with tetraplegia: a proof-of-concept demonstration," *The Lancet*, vol. 389, no. 10081, pp. 1821–1830, 2017.
- [3] K. A. Raichle, M. A. Hanley, I. Molton, N. J. Kadel, K. Campbell, E. Phelps, D. Ehde, and D. G. Smith, "Prosthesis use in persons with lower-and upper-limb amputation," *Journal of rehabilitation research* and development, vol. 45, no. 7, p. 961, 2008.
- [4] A. Schwarz, P. Ofner, J. Pereira, A. I. Sburlea, and G. R. Müller-Putz, "Decoding natural reach-and-grasp actions from human eeg," *Journal of neural engineering*, vol. 15, no. 1, p. 016005, 2017.
- [5] A. Schwarz, C. Escolano, L. Montesano, and G. R. Müller-Putz, "Analyzing and decoding natural reach-and-grasp actions using gel, water and dry eeg systems," *Frontiers in neuroscience*, vol. 14, p. 849, 2020.
- [6] D. J. McFarland, L. A. Miner, T. M. Vaughan, and J. R. Wolpaw, "Mu and beta rhythm topographies during motor imagery and actual movements," *Brain topography*, vol. 12, pp. 177–186, 2000.
- [7] G. Pfurtscheller, A. Stancak Jr, and G. Edlinger, "On the existence of different types of central beta rhythms below 30 hz," *Electroencephalog-raphy and clinical neurophysiology*, vol. 102, no. 4, pp. 316–325, 1997.
- [8] H. Li, G. Huang, Q. Lin, J.-L. Zhao, W.-L. A. Lo, Y.-R. Mao, L. Chen, Z.-G. Zhang, D.-F. Huang, and L. Li, "Combining movementrelated cortical potentials and event-related desynchronization to study movement preparation and execution," *Frontiers in neurology*, vol. 9, p. 822, 2018.
- [9] B. Xu, D. Zhang, Y. Wang, L. Deng, X. Wang, C. Wu, and A. Song, "Decoding different reach-and-grasp movements using noninvasive electroencephalogram," *Frontiers in Neuroscience*, vol. 15, p. 684547, 2021.
- [10] T. Wang, J. Deng, and B. He, "Classifying eeg-based motor imagery tasks by means of time-frequency synthesized spatial patterns," *Clinical Neurophysiology*, vol. 115, no. 12, pp. 2744–2753, 2004.